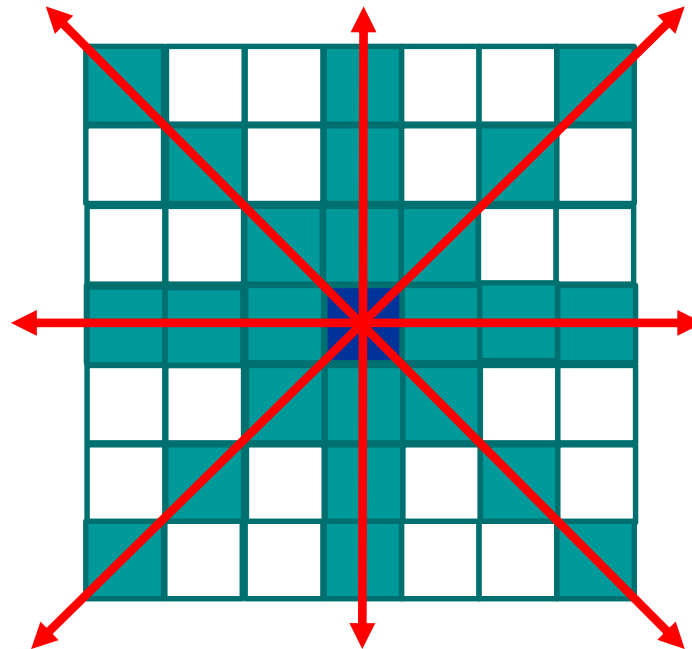


Collapsed Cone Convolution

2D illustration



Energy desposition
decreases very quickly
with distance



8 cones

Energy is absorber in blue pixels only.

IGRT1 technologies

Paweł Kukołowicz
Warsaw, Poland



MARIA
SKŁODOWSKA
-CURIE
MEMORIAL
CANCER CENTER



- The aim
 - to ensure that the delivered dose distribution is as close as possible to the planned dose distribution
 - to solve the problem of set-up uncertainties,
 - to resist the changes of patient anatomy during course of treatment,
 - to resist the changes of position of the target during single treatment session.

imaging

Image-guided radiation therapy (IGRT)



- How does it go
 - the process of frequent two and three-dimensional imaging, during a course of radiation treatment
 - adaptation the actual plan to the intended one

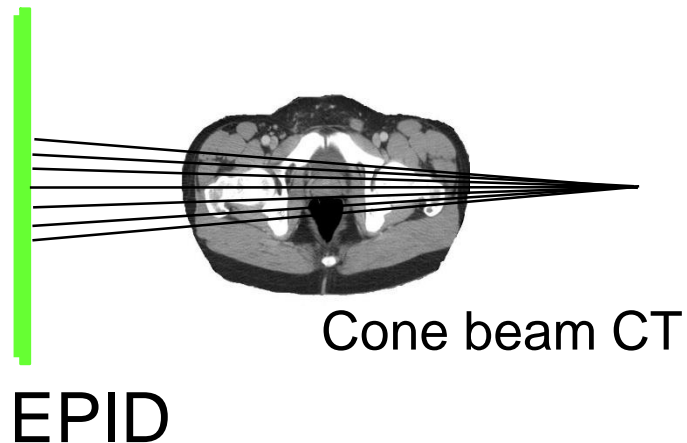
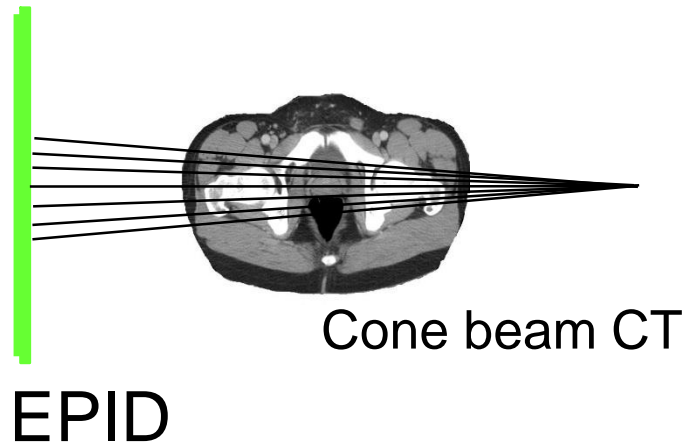


Image-guided irradiation (IGiRT)



- How does it go
 - the process of frequent two and three-dimensional imaging, during a course of radiation treatment
 - adaptation the actual plan to the intended one



Technologies



■ Construction

- ❑ source of ionizing radiation

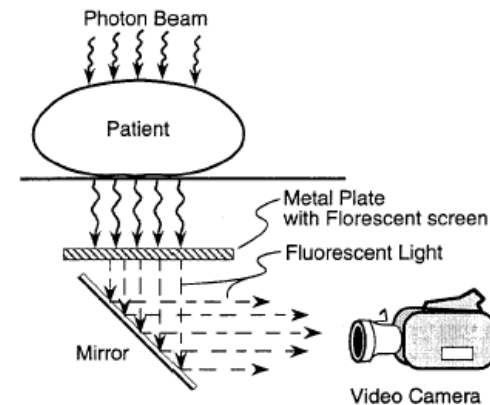
- ❑ detector

■ Systems

- ❑ planar – 2D

- ❑ spatial – 3D

- Ultrasound and laser systems are also used.



Radiation sources



■ MV

- therapeutic beam is used
 - Compton effect
 - very weak contrast – no dependence on atomic number
 - differences in radiological thickness only

■ kV

- additional source of radiation
 - a little photoelectric effect, but it is enough to have
 - much better contrast – dependence on the atomic number
 - bones are visible very well

Contrast



■ Definition

$$C = \frac{\text{signal}}{\text{mean_signal}} = \frac{\Phi_{P2} - \Phi_{P1}}{(\Phi_{P2} + \Phi_{P1})/2}$$

1-cm-thick bone embedded
within 20 cm of soft tissue

100 kVp; contrast 0.5

6 MV; contrast 0.037

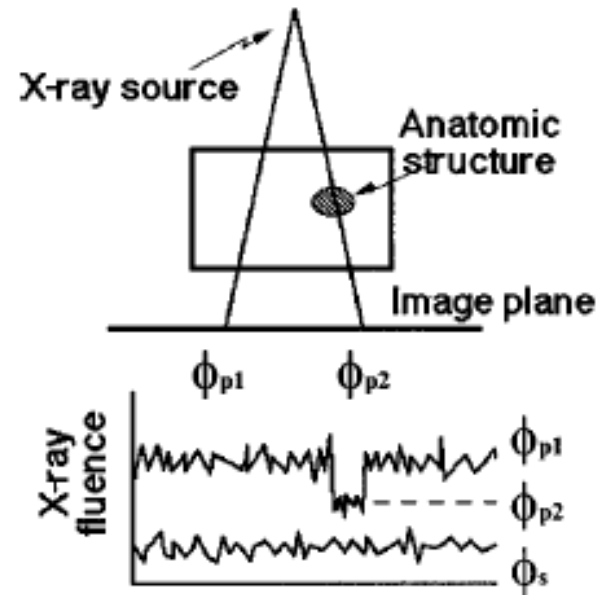


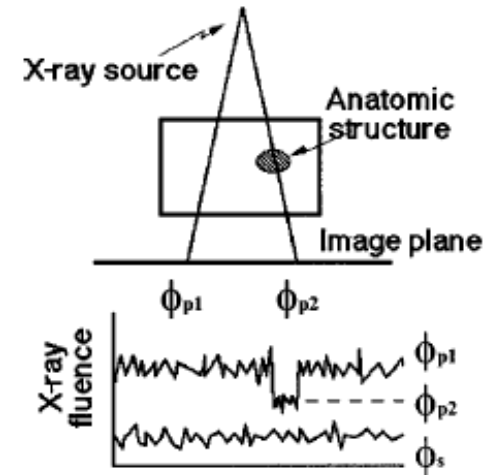
Image detectability (SNR)



■ Signal - to - noise - ratio

$$SNR = \frac{\text{signal}}{\text{noise}} = \frac{\Phi_{P2} - \Phi_{P1}}{\sqrt{(\Phi_{P2} + \Phi_{P1} + 2\Phi_S)/2}}$$

$$SNR = \frac{\text{mean} \therefore \text{signal}}{\text{dispersion}} = \frac{\overline{S}}{\sigma}$$



	100 kVp	6 MV	6 MV	6MV	6 MV
Patient dose (cGy)	0.05	0.05	1.00	10.00	55.00
SNR	71	<1	4.8	15	35

Electronic portal imaging devices



- EPIDs have changed radiotherapy enormously
 - personally: IMRT and EPIDs are the most important achievements in modern radiotherapy
 - IMRT
 - allows for safe treatment most of the concave targets
 - EPIDs
 - allows for safe treatment in general

Commissioning and QA of EPIDs



- What must be verified
 - mechanical and electrical safety
 - safety of mounting the EPID; risk of dropping the device on a patient (for older detachable systems)
 - operation of collision systems (EPIDs are expensive!)
 - geometrical reproducibility
 - the center of EPID should conform to the central axis
 - image quality
 - spatial and contrast resolution
 - software performance



Commissioning and QA of EPIDs



- Vendors usually recommends some tests
- Calibration should be made regularly
 - dark current or noise (image acquired without beam)
 - uniformity of the image
 - for open field intensity across the beam should be uniform

Commissioning and QA of EPIDs



■ Linearity

- distortion of images should be eliminated (simple phantoms with regularly placed objects)

■ Image quality

- specialized phantoms are used
 - Aluminium Las Vegas (AAPM)
 - PTW phantom

Journal of Applied Clinical Medical Physics, Vol 12, No 2 (2011)

A quality assurance phantom for electronic portal imaging devices

Indra J. Das^{1,2,a}, Minsong Cao¹, Chee-Wai Cheng^{1,2}, Vladimir Mistic³, Klaus Scheuring⁴, Edmund Schüle⁴, Peter A.S. Johnstone^{1,2}

Strahlentherapie
und Onkologie

Technical Note

Quality Control of Portal Imaging with PTW EPID QC PHANTOM®

Csilla Pesznyák¹, Gábor Fekete², Árpád Mózes³, Balázs Kiss⁴, Réka Király¹, István Polgár¹, Pál Zaránd¹, Árpád Mayer¹

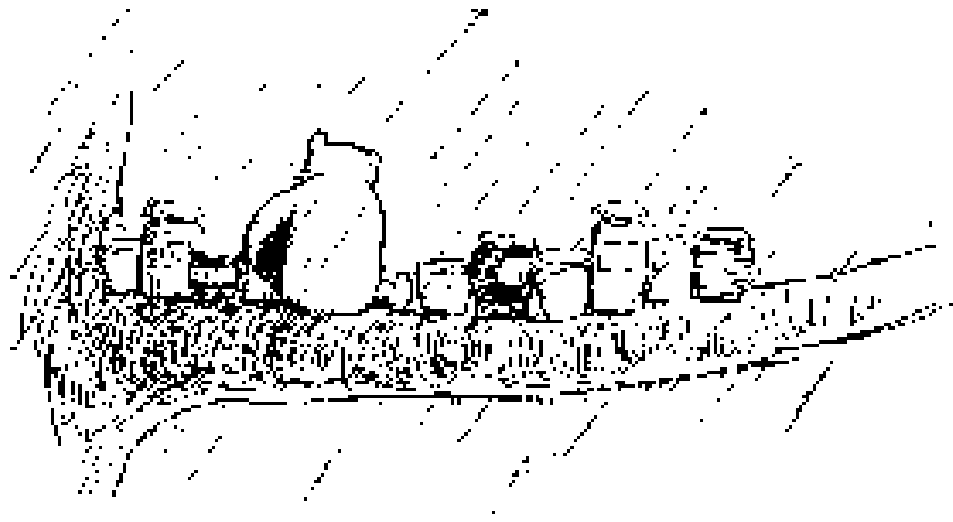
EPIDs' software



- Image quality may be improved with
 - changing window and level
 - more sophisticated digital filtering techniques
 - for edge detection of bones
 - high pass filter
 - Canny and Sobel
 - How we recognize objects?

How objects are recognized?

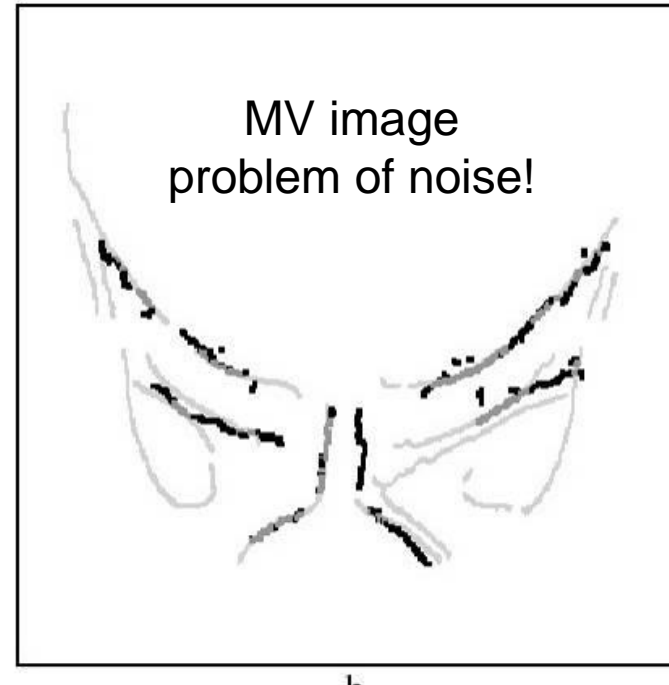
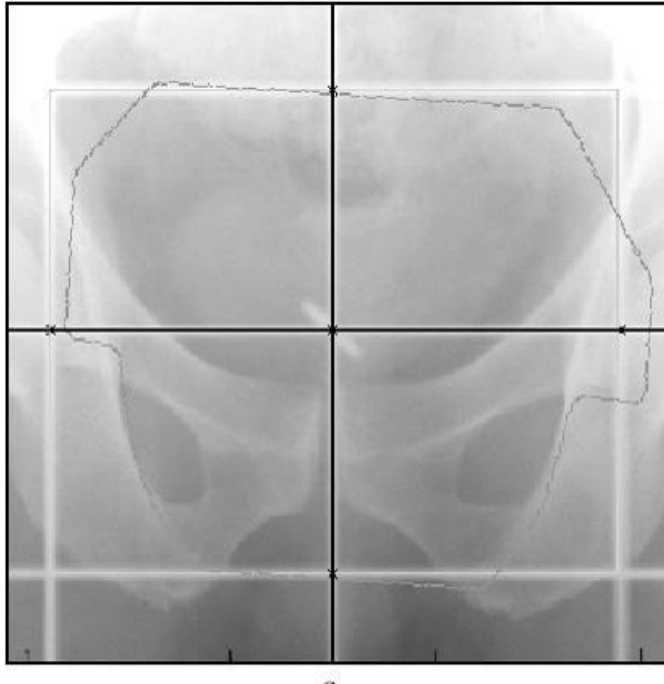
We all are experts!



Recognition is driven by edges!



Edges



Edge is a second derivative of intensity.

Improving quality of images



■ kV radiation

The idea and first solution.
Haynes Radiation



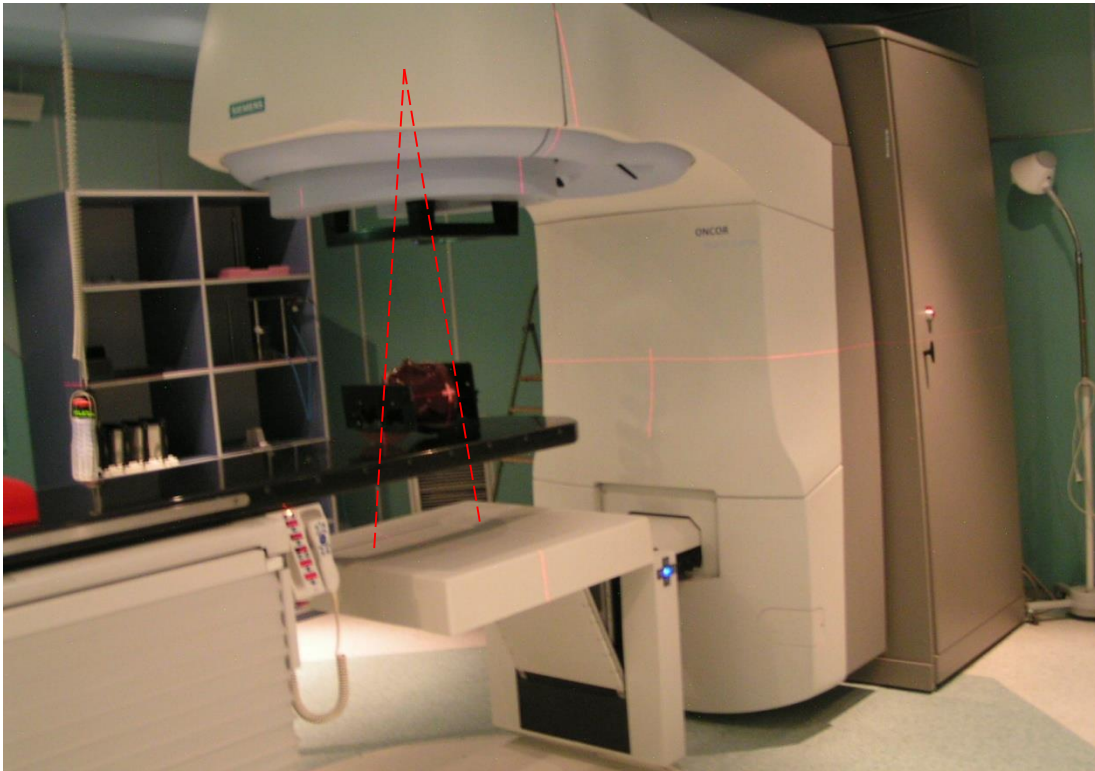
Home of the
RAD II

- Bi-Planer Tumor Verification
- Therapy Attached Simulator & Verification Device

Click here to enter



2D system for set-up control



1 MU – 3 MU

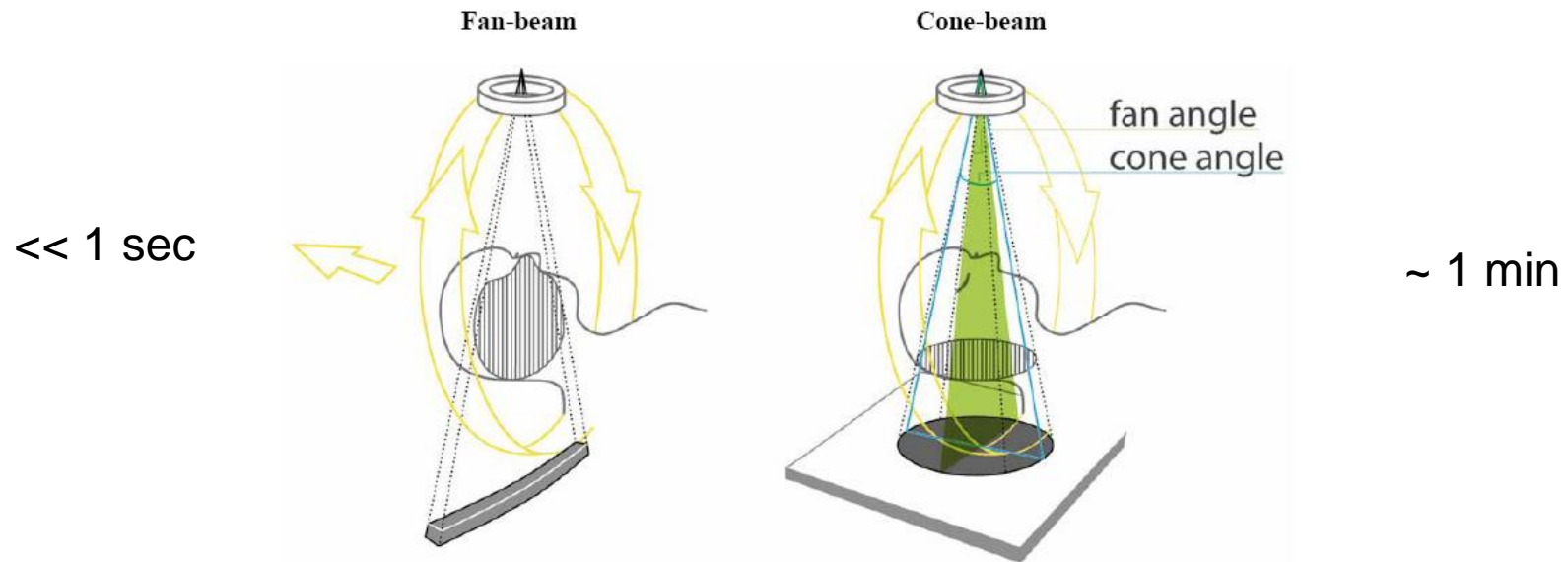
3D Technology



- A set of 2D images → 3D image
 - Computerized tomography
 - conventional (on rails) tomograph
 - cone beam tomograph
 - MV cone beam CT



3D Technology cone beam CT



Difference between the fan (narrow) beam and cone-beam tomography.

$$SNR_{fan} > SNR_{cone}$$

3D Technology cone beam CT



- With kilovoltage radiation
 - ❑ Elekta –
 - ❑ Varian - On Board Imaging
 - ❑ Specialized software for image registration

Detector - EPID

Rtg lamp

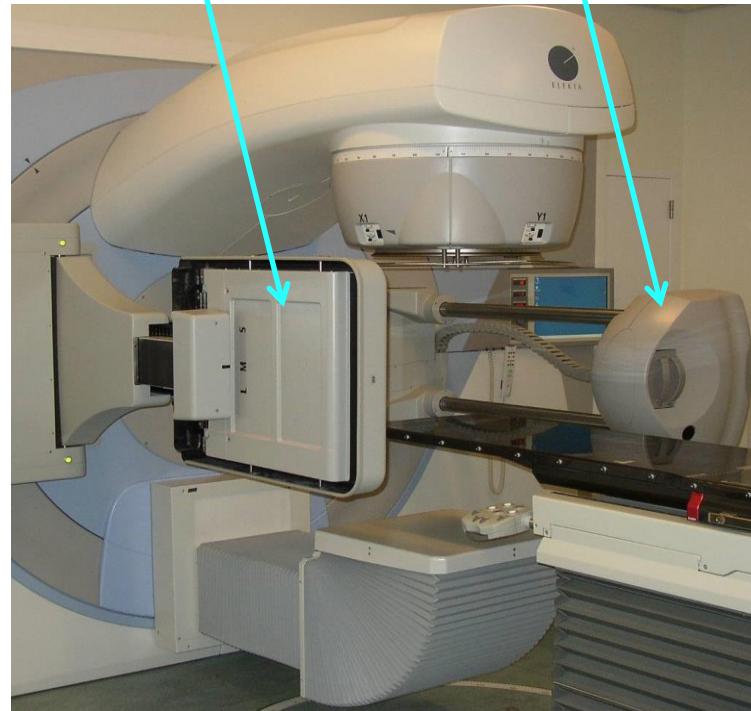


Image quality

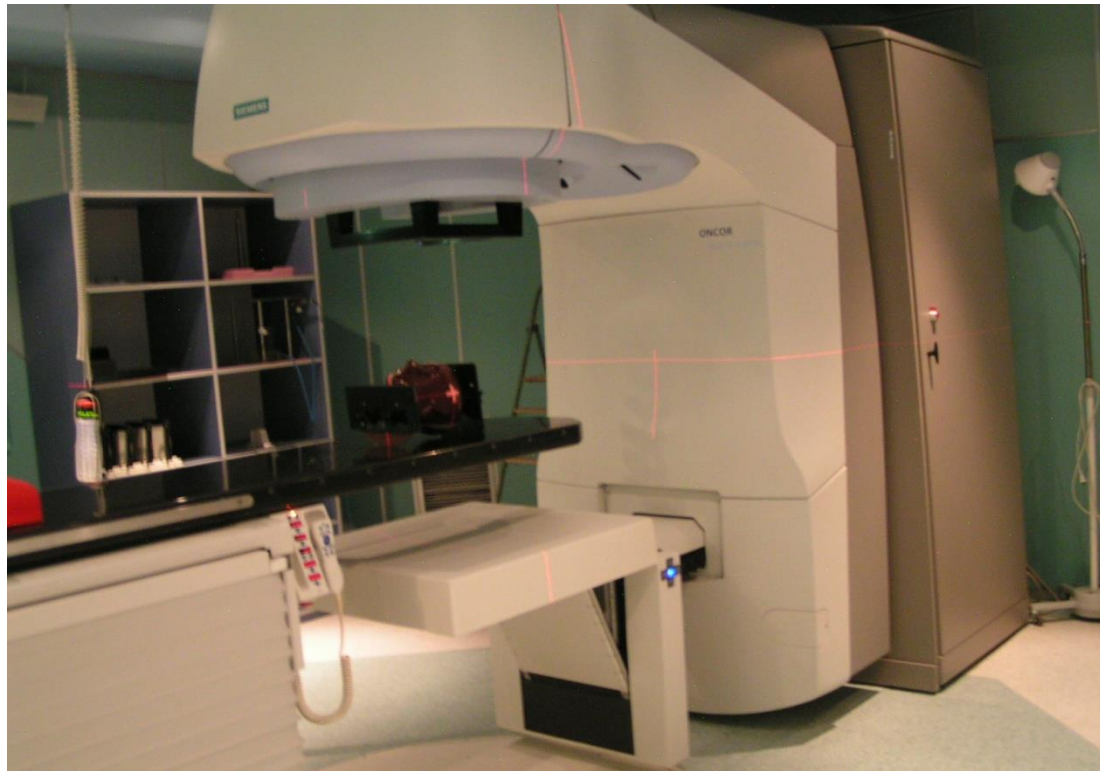
- Worse than for conventional CT
 - smaller SNR
- Good enough for soft tissue registration in some clinical situations
 - distortions due to patient movement



Amer, et al. The British Journal of Radiology, 80 (2007), 476–482

Megavoltage Cone Beam CT

treatment beam



Megavoltage Cone Beam CT image quality



☒ Tx RefPts ▼ List

☒ ☐ Machinelsocenter

Plan Strs ► List

Plan RefPts ► List

Registrati... Views

11/17/2006 9:59:24 AM

Spin: 180 Tilt: -90

Machinelsocenter

10cm

W 1038 C -31

11/17/2006 9:59:24 AM

Spin: -90 Tilt: 180

Machinelsocenter

10cm

W 1038 C -31

11/17/2006 9:59:24 AM

Spin: 180 Tilt: 0

Machinelsocenter

10cm

W 1038 C -31

Acquisition IEC Table Position	Adjusted IEC Table Position	IEC Table Offset
Lat <input type="text"/> cm	<input type="text"/> cm	<input type="text"/> cm
Long <input type="text"/> cm	<input type="text"/> cm	<input type="text"/> cm
Vert <input type="text"/> cm	<input type="text"/> cm	<input type="text"/> cm

accept print

Patient is loaded to Adaptive Targeting

Improving quality of images



■ kV radiation



Home of the
RAD II

- Bi-Planer Tumor Verification
- Therapy Attached Simulator & Verification Device

[Click here to enter](#)



The idea and first solution.
Haynes Radiation



CyberKnife

Exact Track BrainLab



Concomitant dose in IGRT



- The only dose quantity that allows any intercomparison of stochastic risk between the different imaging scenarios ... is **effective dose**, which combines the quality and distribution of radiation throughout the body with its effect on a number of specific organs.
 - If 10,000 individuals received 0.01 Sv each over background during their life, 4 additional deaths would occur of the 2,000 that would naturally occur; (0.01 Sv – 1 cGy)

The management of imaging dose during image-guided radiotherapy:
Report of the AAPM Task Group 75, Medical Physics 34, Oct, 2007

Radiation protection of a patient

Effective dose



$$E = \sum_T (w_T \cdot w_R \cdot D_{T,R})$$

- w_T = tissue weighting factor
- w_R = radiation weighting coefficient
- $D_{T,R}$ = average absorbed dose to tissue T

for radiation used in conventional radiotherapy $w_R = 1$

Effective dose



For photons and electrons $W_R = 1$

Organ/Tissue	W_T	Organ/Tissue	W_T
Bone marrow	0.12	Lung	0.12
Bladder	0.04	Liver	0.04
Bone Surface	0.01	Oesophagus	0.04
Brain	0.01	Salivary glands	0.01
Breast	0.12	Skin	0.01
Colon	0.12	Stomach	0.12
Gonads	0.08	Thyroid	0.04
Liver	0.05	Remainder	0.12

Doses from CBCT



Dose from Elekta XVI kV cone-beam CT.

Parameter	Head	Chest
Mean dose at center (mGy)	29	16
Mean skin dose (mGy)	30	23
Effective dose (mSv)	3.0	8.1

M. K. Islam, T. G. Purdie, B. D. Norrlinger, H. Alasti, D. J. Moseley, M. B. Sharpe, J. H. Siewerdsen, and D. A. Jaffray, “Patient dose from kilovoltage cone beam computed tomography imaging in radiation therapy,” *Med. Phys.* **33**, 1573–1582 (2006).

Murphy, M.J., et al., *The management of imaging dose during image-guided radiotherapy: report of the AAPM Task Group 75. Med Phys*, 2007. **34(10)**: p. 4041-63.

Doses from portal control



Effective dose from 6 MV portal images 18 cm x 15.6 cm taken at SSD=88 cm.

Port View	Gender	Effective Dose E (mSv/MU)
AP pelvis	Male	0.34
	Female	0.52
Lat pelvis	Male	0.32
	Female	0.7
AP chest	Male	1.74
	Female	1.8
Lat chest	Male	2.56
	Female	2.23
Lat neck	N.A.	0.12

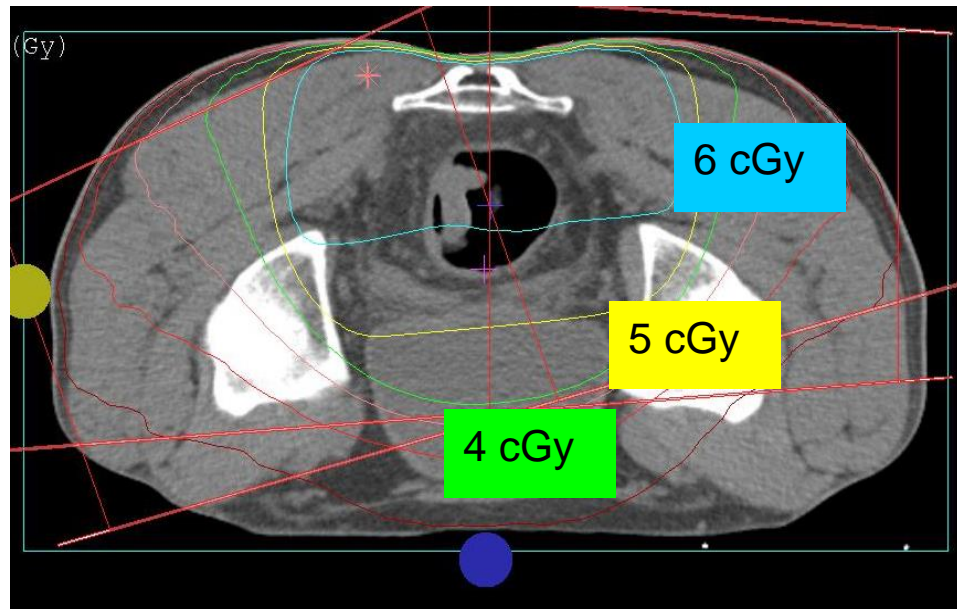
X2

P. Waddington and A. L. McKensie, "Assessment of effective dose from concomitant exposures required in verification of the target volume in radiotherapy," Br. J. Radiol. **77**, 557–561 2004.

Concomitant dose MCBCT



Irradiation of rectum patient
8 MU protocol



In practice for MCBCT we use about 4 MU.

MV images



- Disadvantages in comparison to kV
 - ❑ low contrast
 - ❑ little higher unwanted dose

- Advantages in comparison to kV
 - ❑ in 3D treatment fields might be imaged
 - ❑ lower purchase cost
 - ❑ lower running costs
 - ❑ allow for imaging the H-Z objects

Prosthesis



- H-Z materials



Prosthesis – the most common



	Alloy Co-Cr-Mo	Titanium	Steel
Atomic composition	Co 60% Cr 30% Mo 5%	Ti 90% Al 6% Va 4%	Fe 65% Cr 18% Ni 12 Mo 3
ρ [g/cm ³]	7.9	4.3	8.1
relative electron composition	6.8	3.6	6.7

Attenuation is the most important effect

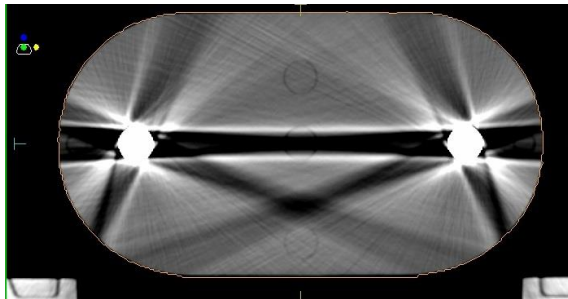
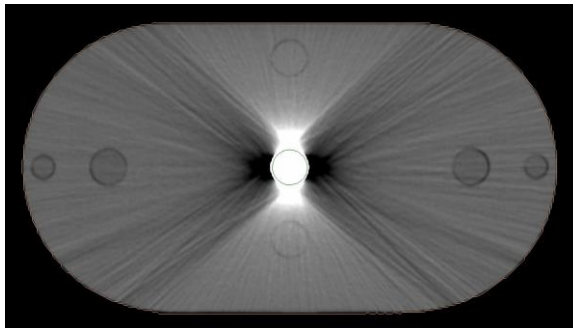


	water	Titanium	Steel
μ/ρ [cm ² /g]	0.0397	0.0351	0.0362
ρ [g/cm ³]	1.0	4.3	8.1
attenuation for 1cm [%]	3.9	14.0	25.4

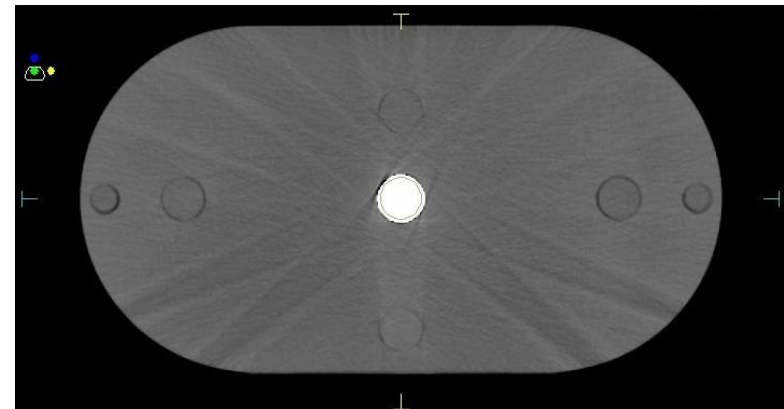
Imaging of H-Z materials



- Is difficult and possible with metal artifact reduction method only



without MAR

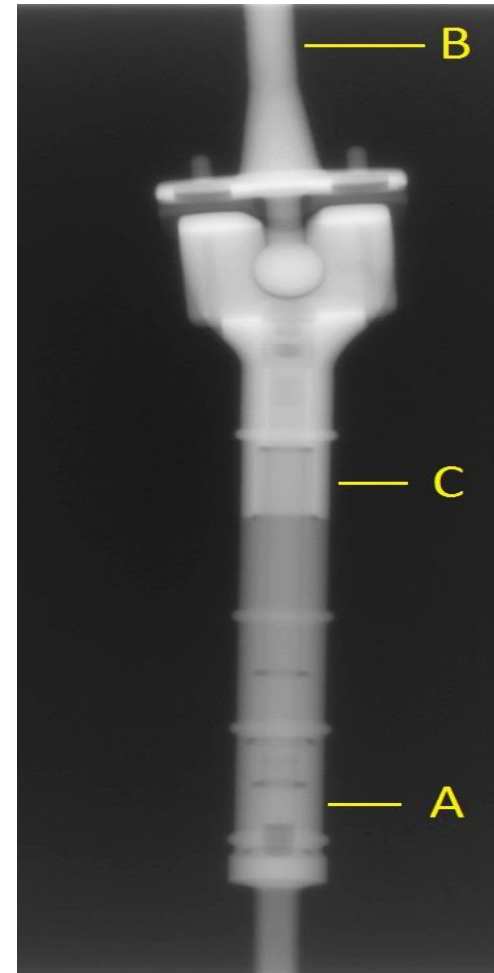


with MAR

Structure of H-Z materials



- can't be imaged with kV radiation
- can be imaged with MV radiation

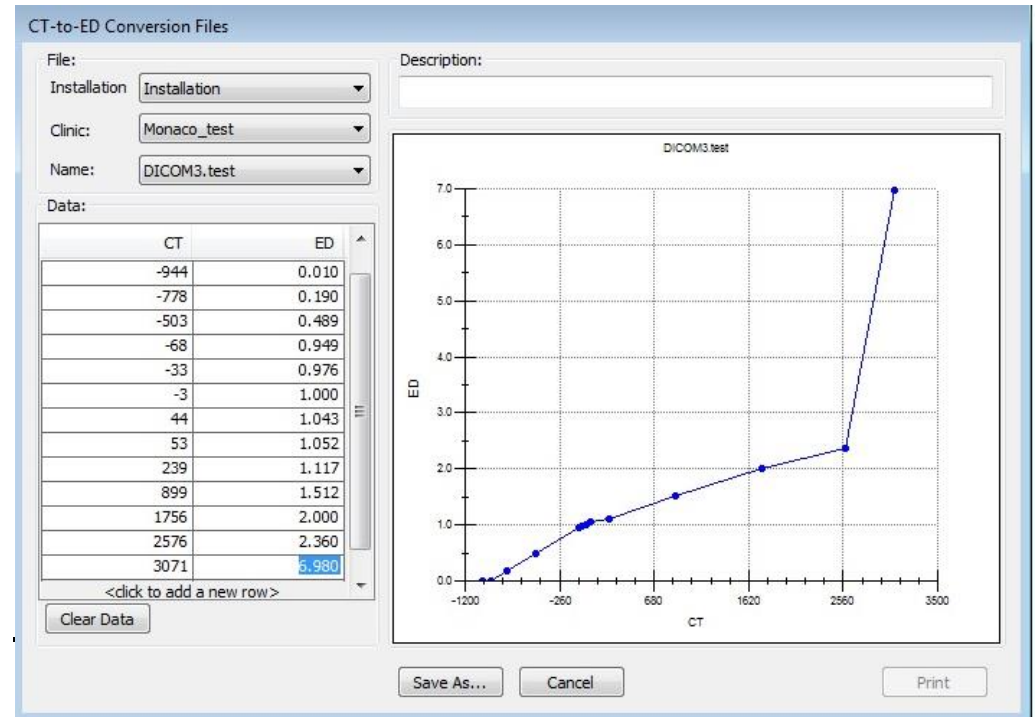


Those who have Tomotherapy are lucky!

Imaging



- Always with MAR module
- With extended mode
 - ❑ 16 bits
up to 2^{16} ; 65536 HU
 - ❑ 12 bits (standard)
up to 2^{12} ; 4096 HU: -1204 +3071 (aluminium)



HU – electron density conversion curve

My recommendation to read



Dosimetric considerations for patients with HIP prostheses undergoing pelvic irradiation. Report of the AAPM Radiation Therapy Committee Task Group 63

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Rodica Alecu

U.S. Oncology, Texas Cancer Center, Sherman, Texas

Indra J. Das

University of Pennsylvania, Philadelphia, Pennsylvania

Bruce J. Gerbi

University of Minnesota Medical School, Minneapolis, Minnesota

Paul Keall

Virginia Commonwealth University, Richmond, Virginia

— . . . —

Doses from CBCT



- To be accounted for in total dose delivered to a patient?
 - different policies

- My opinion: in general there is no reason to take into account the CBCT concomitant dose unless CBCT is performed each fraction
 - on-line protocol

Summary



- The modern radiotherapy is imaged based
 - CT information for planning
 - fusion with other modalities
- Several solutions
 - visualizing high contrast objects
 - bones
 - gold markers
 - visualizing low contrast objects
 - soft tissue

Summary



- Several solutions
 - pre-irradiation information (low frequency)
 - inter-fraction changes
 - continuous (high frequency)
 - Intra-fraction changes
- There are also other very sophisticated solutions
 - very expensive

Summary



■ Good news!

- in more than 80% of cases (my estimation) conventional portal control with EPID is enough,

□ IF

- The right protocols are used, and applied properly
 - the structure, organization and personnel are the most important!

- Thank you very much for your attention!