







#### STEREOTACTIC RADIOSURGERY

#### **CONCEPTS AND IMPLEMENTATION**

ICTP School on Medical Physics for Radiation Therapy

Dosimetry and Treatment Planning for Basic and Advanced Applications

March 27 – April 7, 2017

Miramare, Trieste, Italy

Yakov Pipman, D.Sc

#### OUTLINE

Stereotactic Radiosurgery Concepts – targets and dose distributions

**Some History** 

**Commissioning and Quality Control** 

**Image Fusion and Target delineation** 

**Dose delivery methods** 

**SRS** treatment process

# Stereotactic Radiosurgery

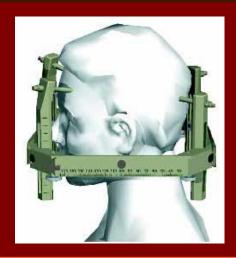
"A single high dose of radiation, stereotactically directed to an intracranial region of interest. May be from X-ray, gamma ray, protons or heavy particles." (Lars Leksell, 1951)

Historical Development of Stereotactic Ablative Radiotherapy Timothy D. Solberg, Robert L. Siddon, and Brian Kavanagh

# Stereotactic Radiosurgery (SRS) – Stereotactic Radiotherapy (SRT)

SRS and SRT use a stereotactic system and high energy beams to irradiate a volume.

- (1) Requires an image based volume defined and indexed to a stereotactic coordinate system.
- (2) Planning and treatment delivery indexed to the same coordinate system.



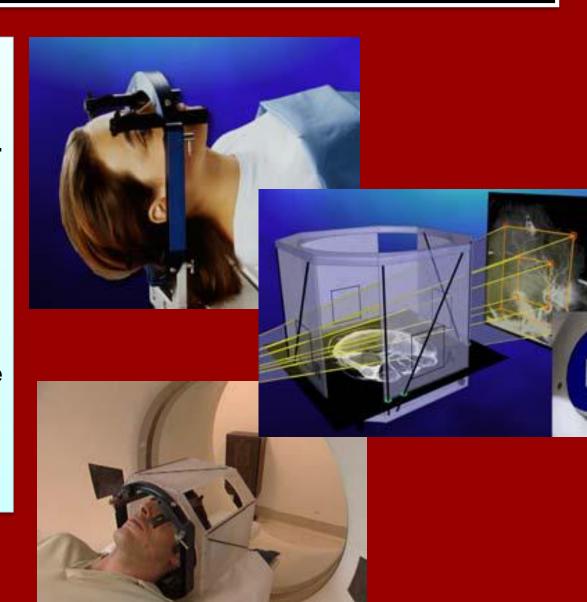
SRS and SRT produce a sharp dose gradient outside the treatment volume.

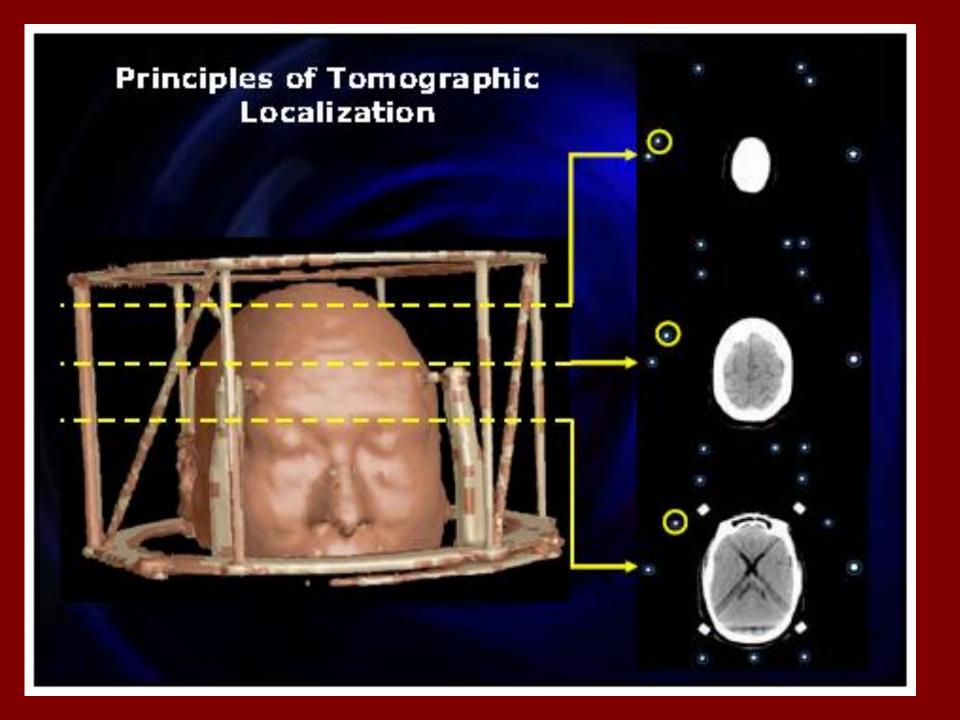
## **Stereotactic Localization**

A localizer head frame, rigidly attached to the cranium, defines a precise and rigid frame of reference.

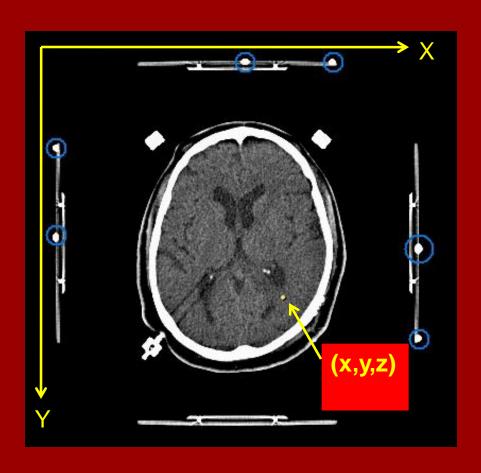
All points within that space can be referenced to a unique coordinate system.

All structures and points can be identified in all the imaging studies that include the localization frame, which is uniquely and rigidly attached to the base frame.





# **Localization of points**



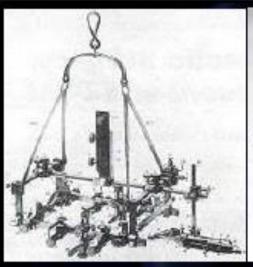
# The "z" coordinate



# **SRS** treatment strategy

Position the point or volume to be treated at the point of convergence or intersection of all the beams

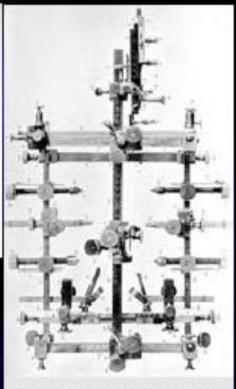
# **History**





Original stereotactic frame

Clarke RH, Horsley VA, On a method of investigating the deep ganglia and tracts of the central nervous system (cerebellum). Br Med J 1799-1800, 1906.

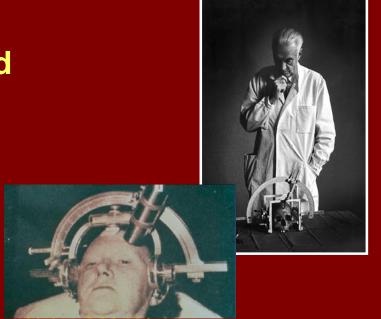


Clorks's steresticité approving for directing an insulated nordle by graduated environment in three planes (from, Horsing V, Clorke RF: The structure and functions of the controllers examined by a sure mutterd. Brain 31:45–124. 1900.

Horsley VA, Clarke RH, The structure and functions of the cerebellum examined by a new method. Brain 31:45-124, 1908.

# **History**

- Dr. Lars Leksell (1951) introduced the concept of Radiosurgery as the ablation of a lesion by radiation in a single procedure, similar to surgery
- Initially used a 200kV x-ray tube
- In 1968 developed the "Gamma knife"
  - 179 Co-60 sources
  - A spherical cavity covering 60° x 160°





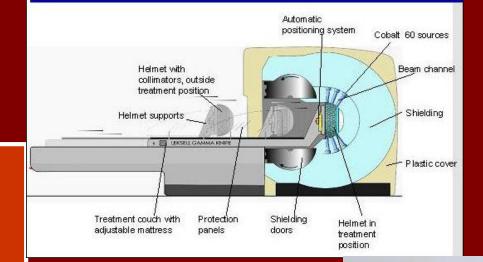
#### **Gamma Knife**

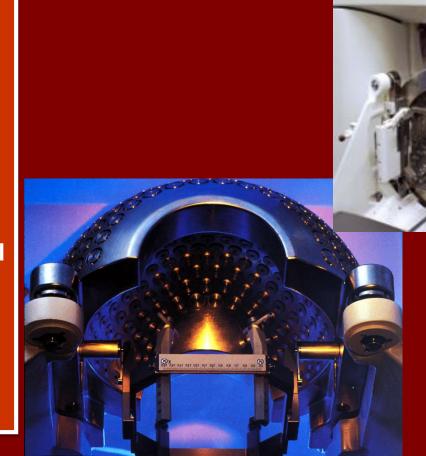
201 Co-60 sources arranged hemispherically around a common 'focal' point

The isocenter precision <0.5mm

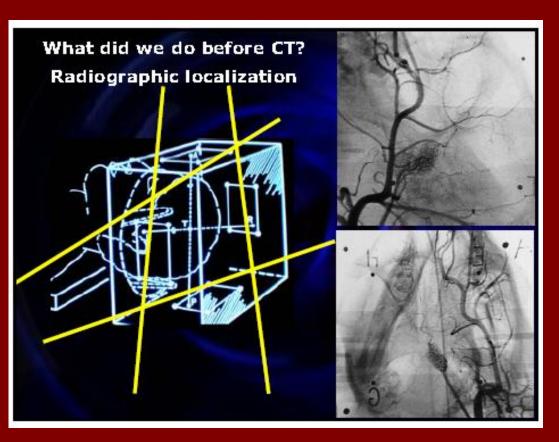
A system of collimators (4, 8, 14 and 18mm) (diameter of 50% isodose level on a 16cm phantom)

Used for spherical targets in one isocenter

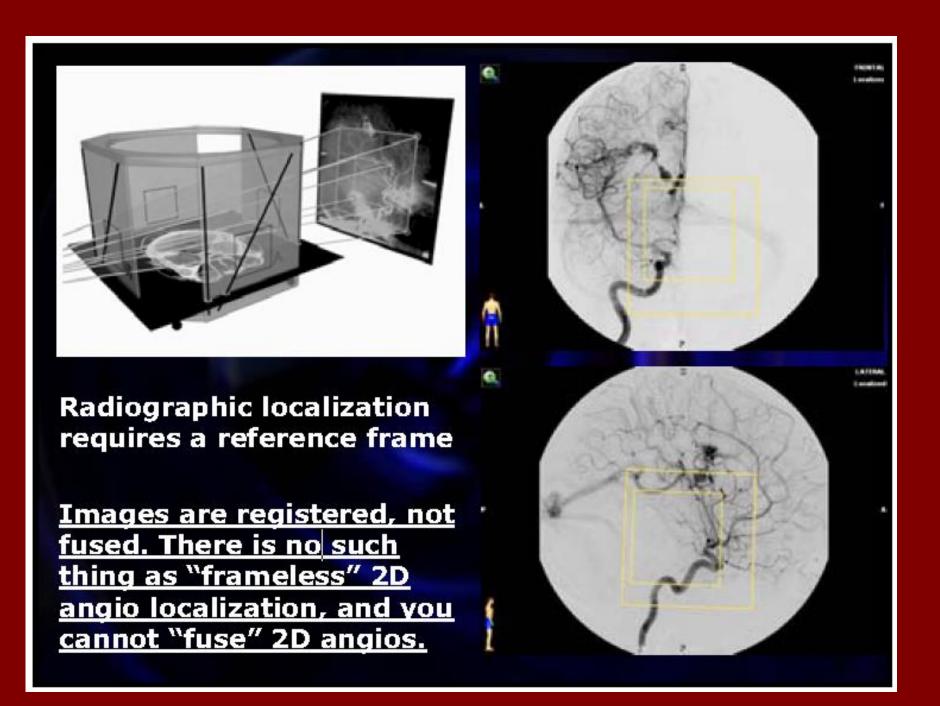




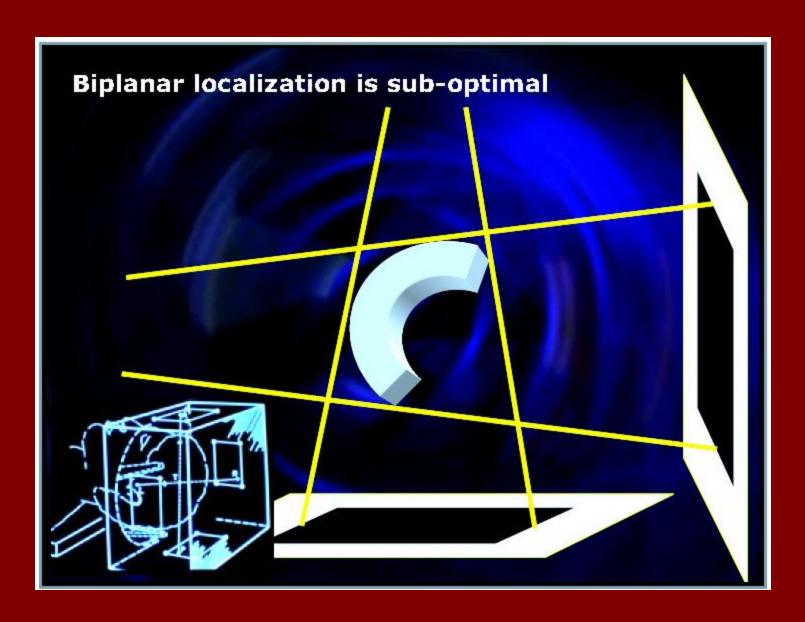
# Initial application for treatment of artero-venous malformations (AVM)







## **Incomplete information**



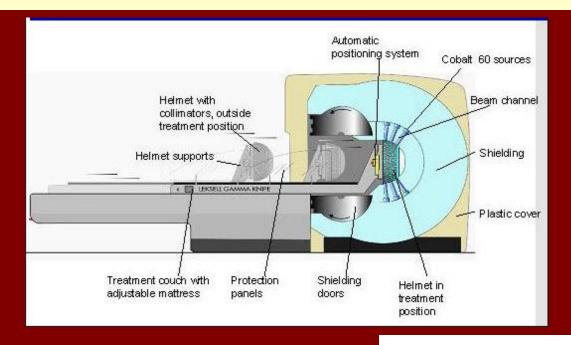
# Laser-Angiographic Target Localizer (LATL)

Used for Angiography to register the nidus to a CT data set



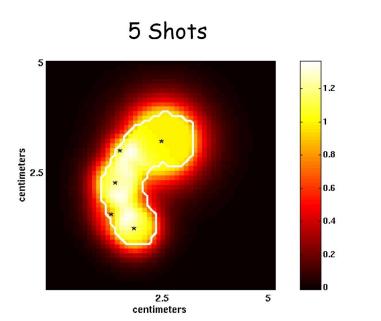


### Gamma knife



 Irregular target volumes require multiple 'shots'





#### X-Knife

- Collimator sizes: 5 to
   45 mm in 2.5 mm steps
- Conformal SRT: with jaws/circles; mMLC; IMRT.
- Extra-cranial: head and neck; body localization, spine localization, other targets

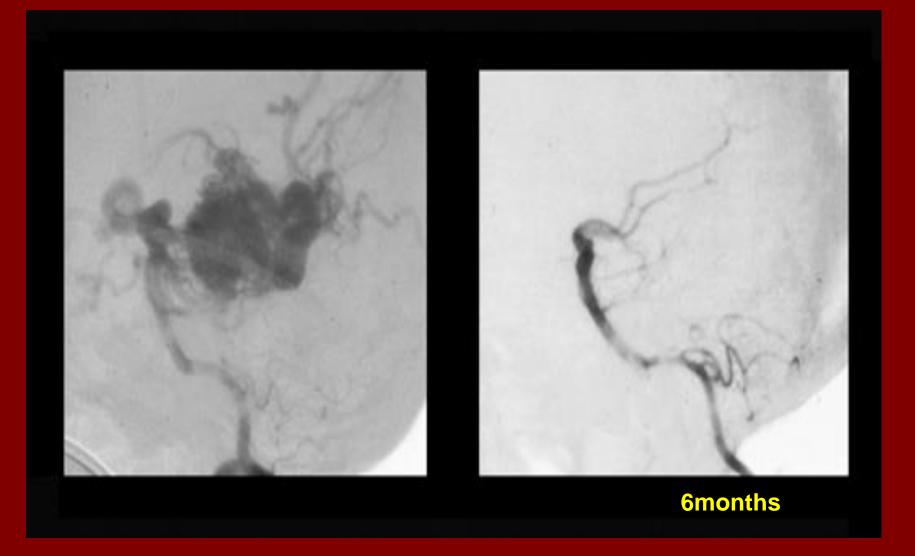
#### **Gamma Knife**

- Collimator sizes: 4,8,14,18 mm
- Conformal is only attained through multiple isocenters
- No extra-cranial targets possible

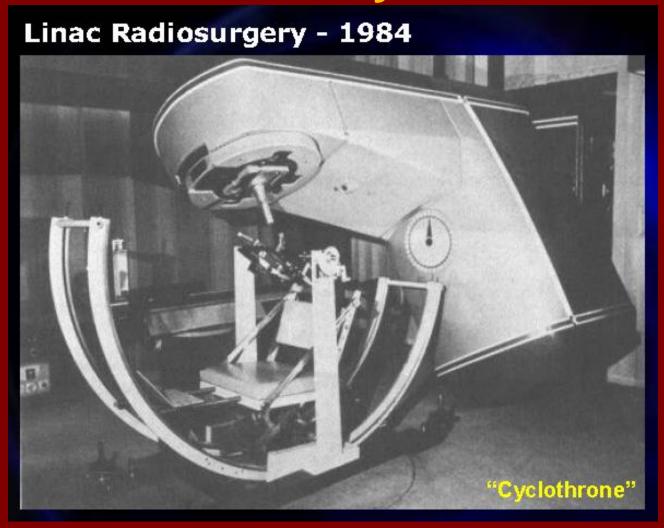
# Radiosurgery AVM

**Pre-Radiosurgery** 

Post-Radiosurgery



# History



First linac- based SRS system. Betti et al., Buenos Aires, Argentina Ref: Historical Development of Stereotactic Ablative Radiotherapy, by Timothy D. Solberg, Robert L. Siddon, and Brian Kavanagh. In S. S. Lo et al. (eds.), Stereotactic Body Radiation Therapy, Medical Radiology. Radiation Oncology,

DOI: 10.1007/174\_2012\_540, Springer-Verlag Berlin Heidelberg 2012

# Radiation delivery techniques

Arcs with circular collimators

Conformal beams

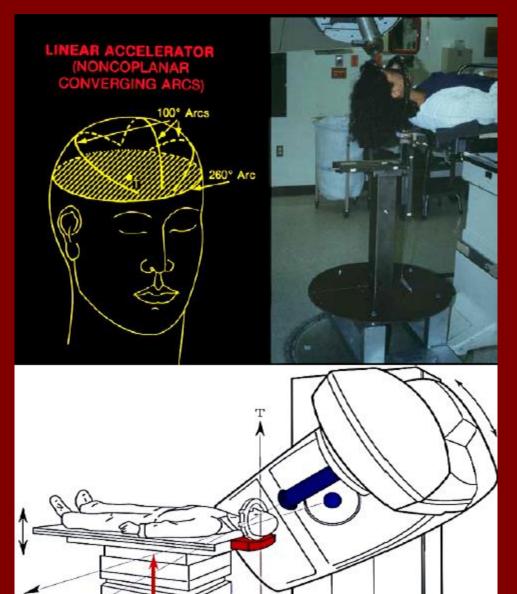
**Arcs with Conformal Dynamic beams** 

**IMRT** 

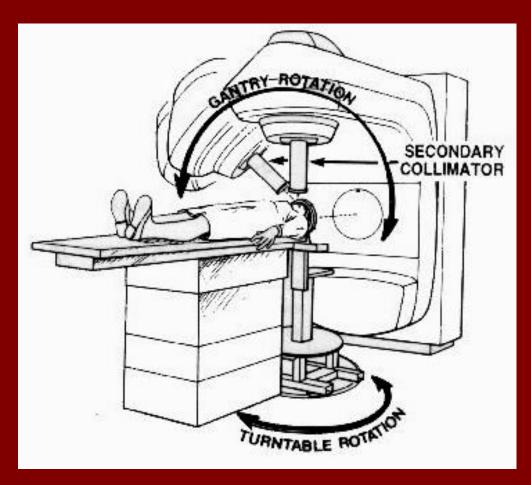
# Linac SRS with cones

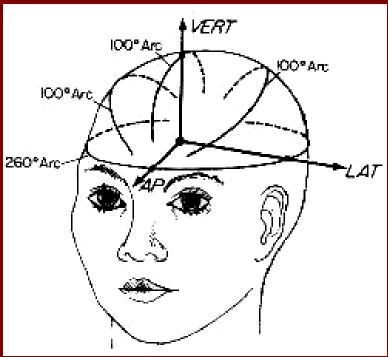
- One or more isocenters
- Multiple arcs per isocenter
  - Arcs of 100° to 160°
  - Fixed couch angle for each arc
  - Spherical dose distributions for each irradiación





Arcs with circular cross sections are obtained by rotating the source (linac gantry) in various planes in the patient, corresponding to various couch angles.

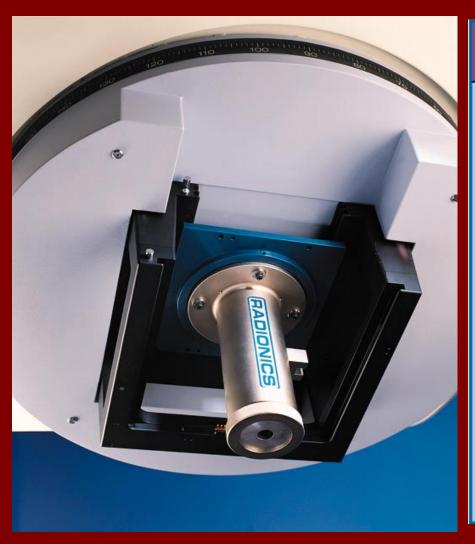


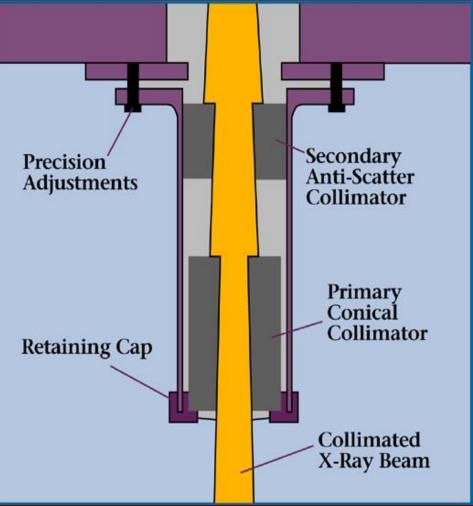


# **Tertiary Collimation Cone**



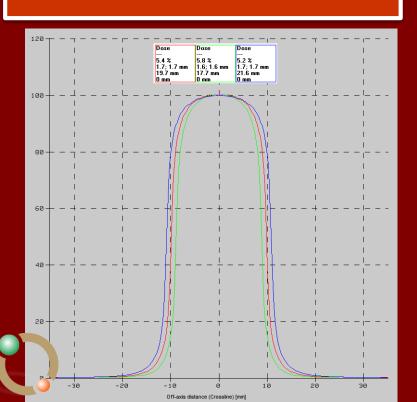
# **Collimation**





# Linac SRS on Linac + cones

- 5-40mm diameter cone set
- Circular beam projection
- Collimator mounted assembly







## Verification of gantry isocenter with cones

## **Laser alignment**









# Stereotactic Set-up QA

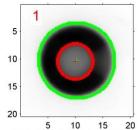
#### **Winston Lutz Quality Assurance**

- Phantom Pointer verifies laser accuracy prior to SRS
- Embossed laser lines for easy alignment with wall lasers
- Integrated tungsten sphere for film verification
- Irradiation of film at different gantry angles
- Shadow in field center verifies accuracy

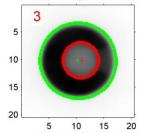




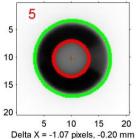
Ball Centroid: Row = 62.22, Column = 59.38 Cone Centroid: Row = 60.87, Column = 60.66 Distance = 1.86 pixels, 0.35 mm



Delta X = -1.28 pixels, -0.24 mm Delta Y = 1.35 pixels, 0.25 mm Ball Centroid: Row = 60.20, Column = 64.43 Cone Centroid: Row = 60.58, Column = 61.11 Distance = 3.34 pixels, 0.62 mm

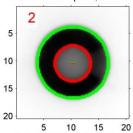


Delta X = 3.32 pixels, 0.62 mm Delta Y = -0.38 pixels, -0.07 mm Ball Centroid: Row = 60.64, Column = 59.42 Cone Centroid: Row = 60.63, Column = 60.49 Distance = 1.07 pixels, 0.20 mm

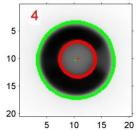


Delta Y = 0.01 pixels, 0.00 mm

Ball Centroid: Row = 61.96, Column = 61.32 Cone Centroid: Row = 61.07, Column = 61.16 Distance = 0.90 pixels, 0.17 mm



Delta X = 0.16 pixels, 0.03 mm
Delta Y = 0.88 pixels, 0.16 mm
Ball Centroid: Row = 59.57, Column = 63.07
Cone Centroid: Row = 61.04, Column = 61.16
Distance = 2.42 pixels, 0.45 mm



Delta X = 1.91 pixels, 0.36 mm Delta Y = -1.48 pixels, -0.27 mm

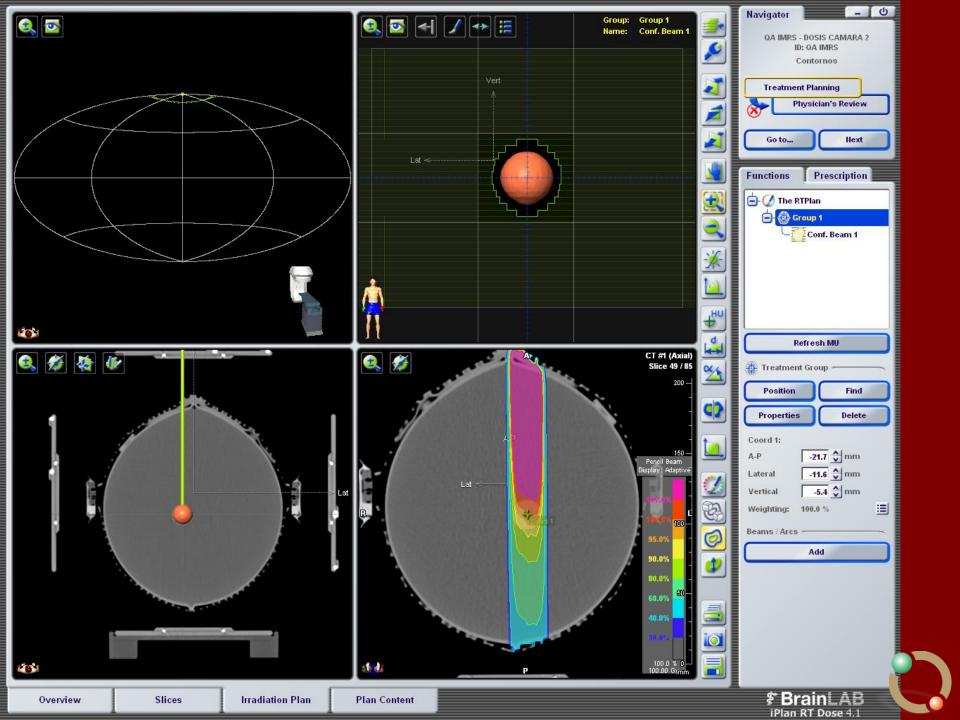
Gantry	210°	270°	00	90°	150°
∆GT (mm)	0.25	0.03	0.62	0.36	0.20
∆AB (mm)	0.24	0.15	0.07	0.27	0.0
Vector (mm)	0.35	0.15	0.62	0.45	0.20

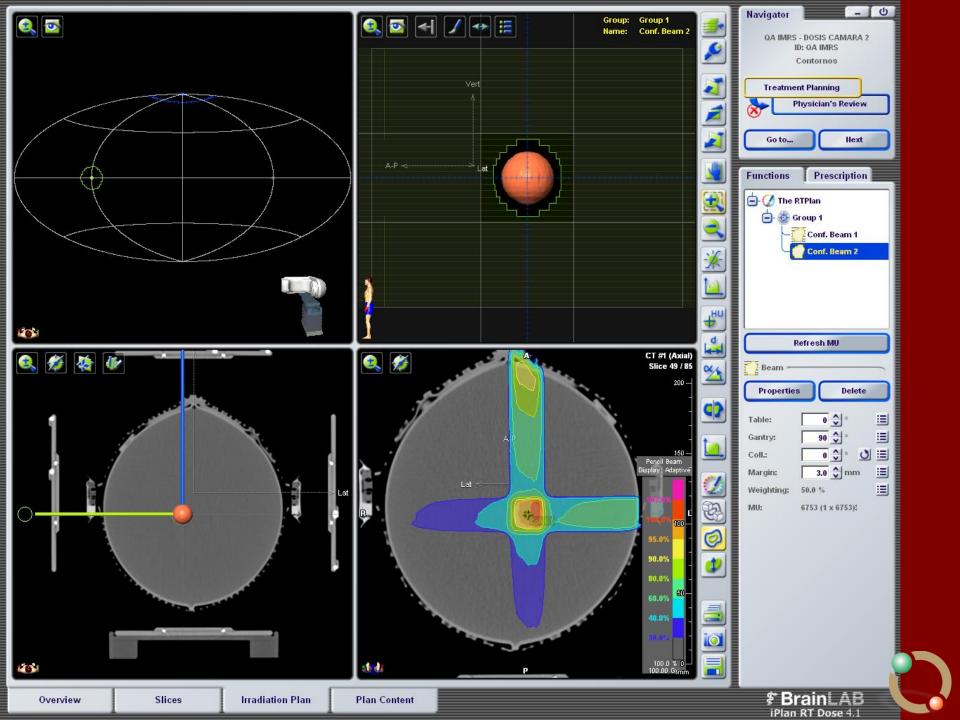
#### **AAPM TG42: Tolerance = 1mm**

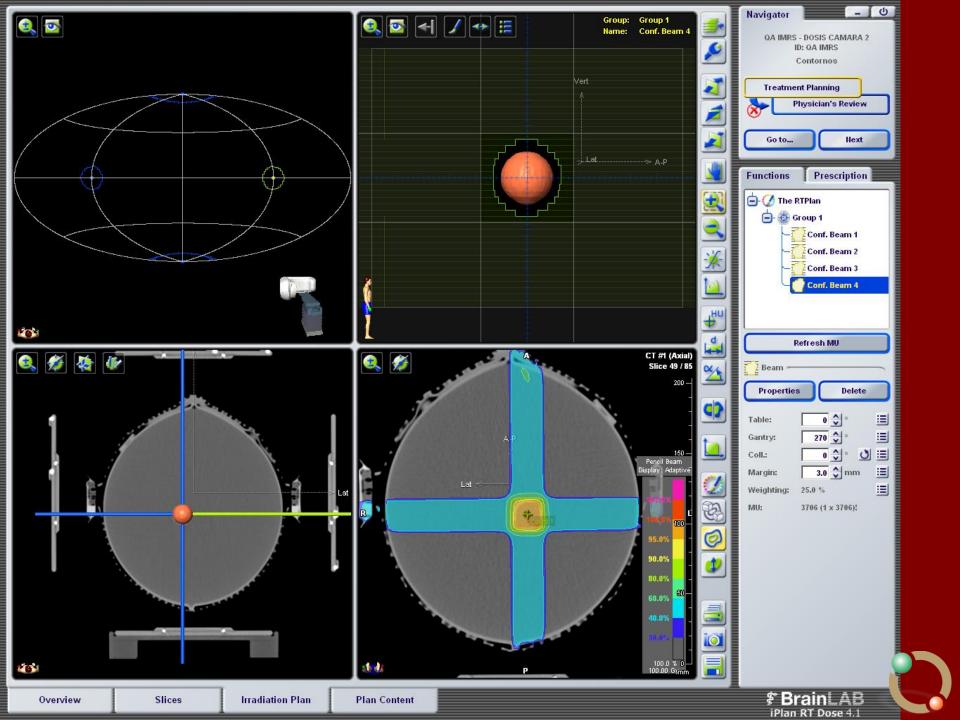
150°

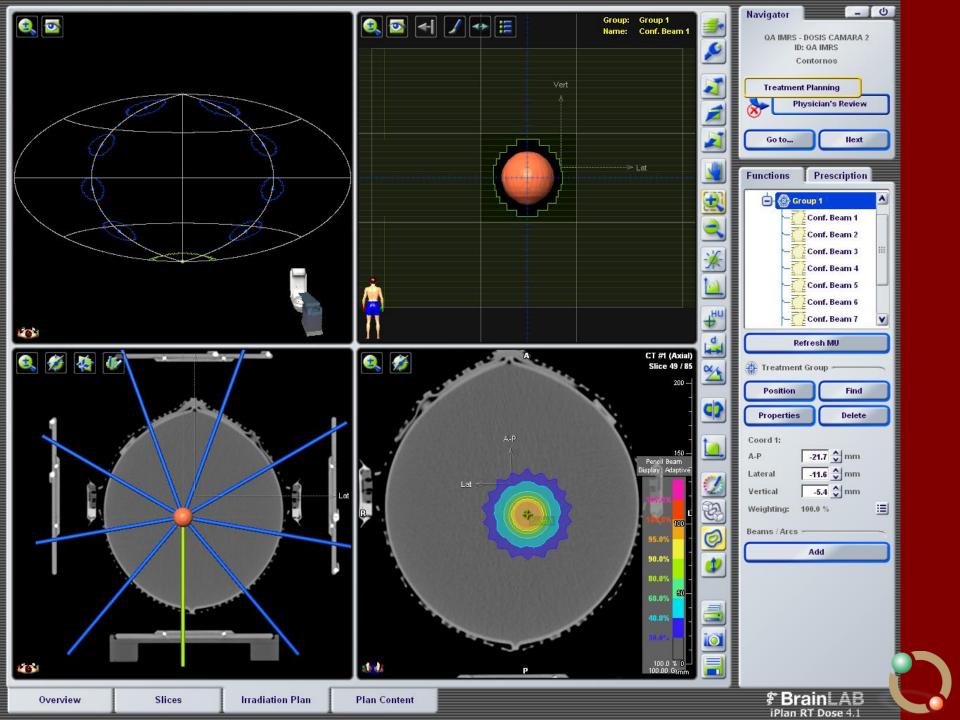


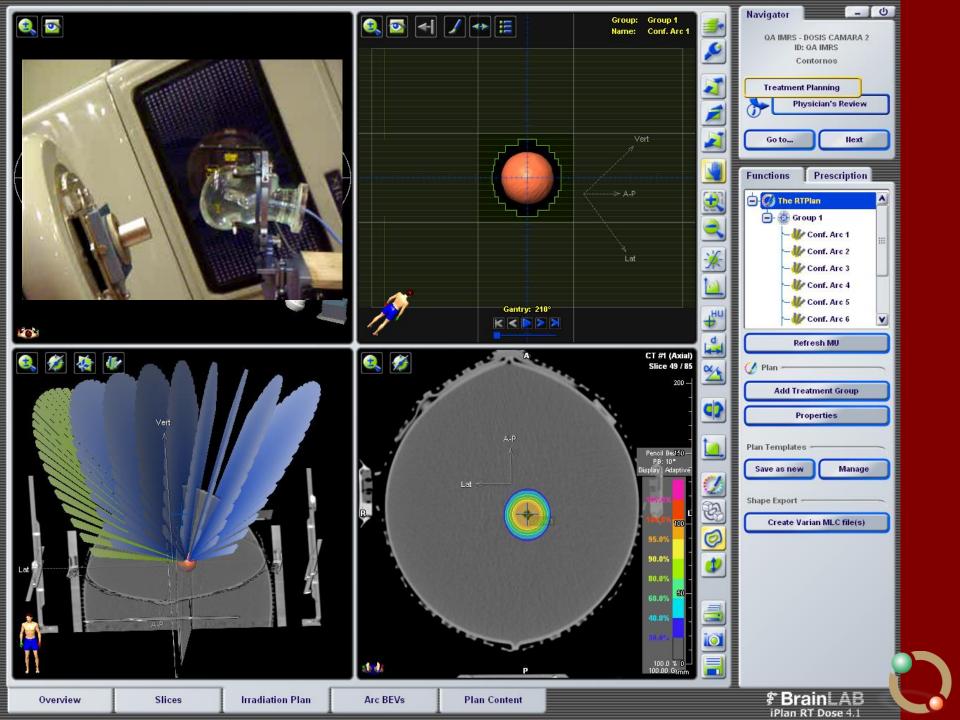
210° 270° 0° 90°

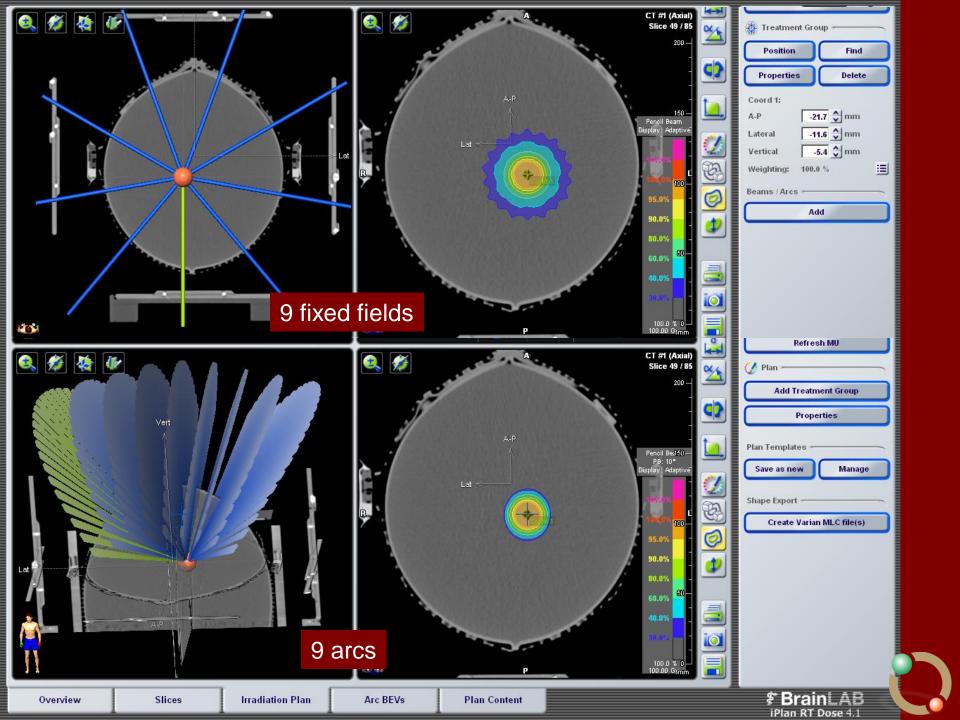


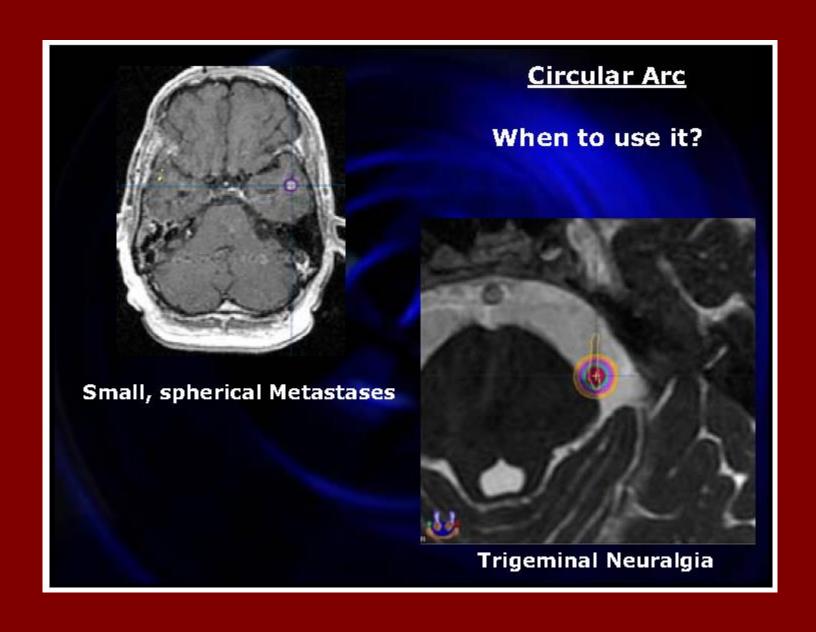












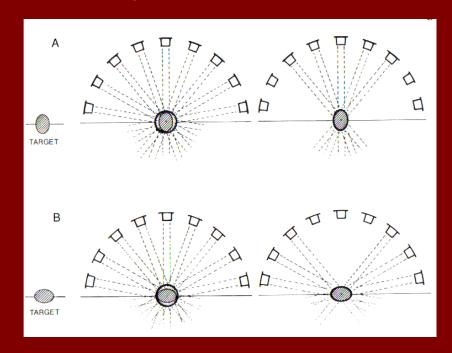
#### Planning strategies for SRS with arcs

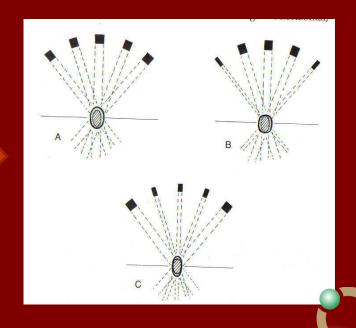
#### Spherical targets:

Use up to 9 arcs with collimator diameter corresponding to the target diameter

#### Elliptical targets:

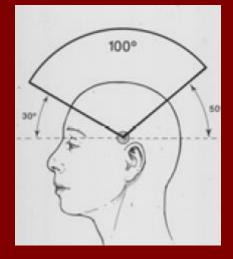
 If the major axis is in the coronal plane, eliminate perpendicular arcs, or use different cone sizes

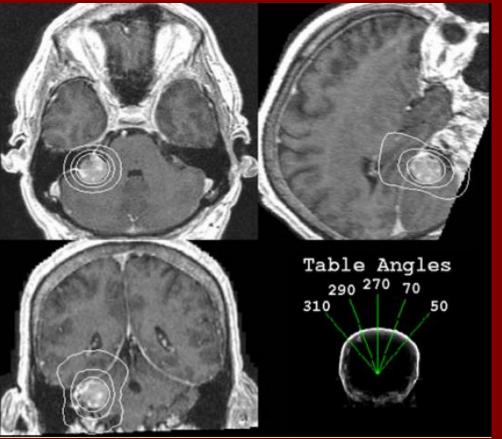


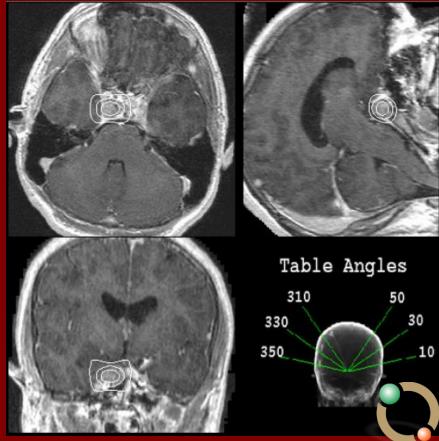


#### **Circular collimators**

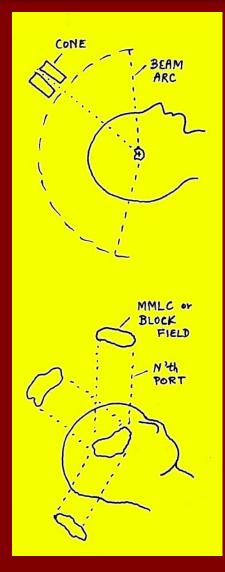








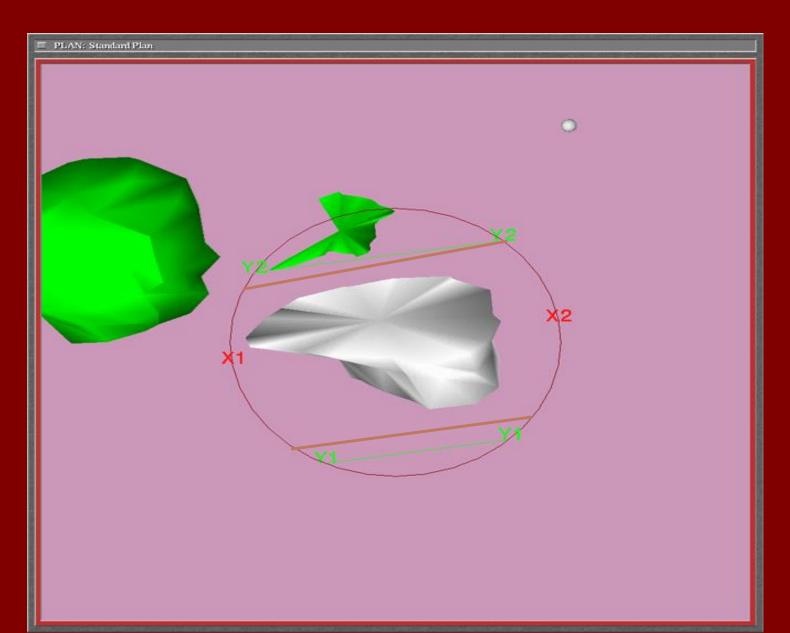
## Considerations according to the type of target



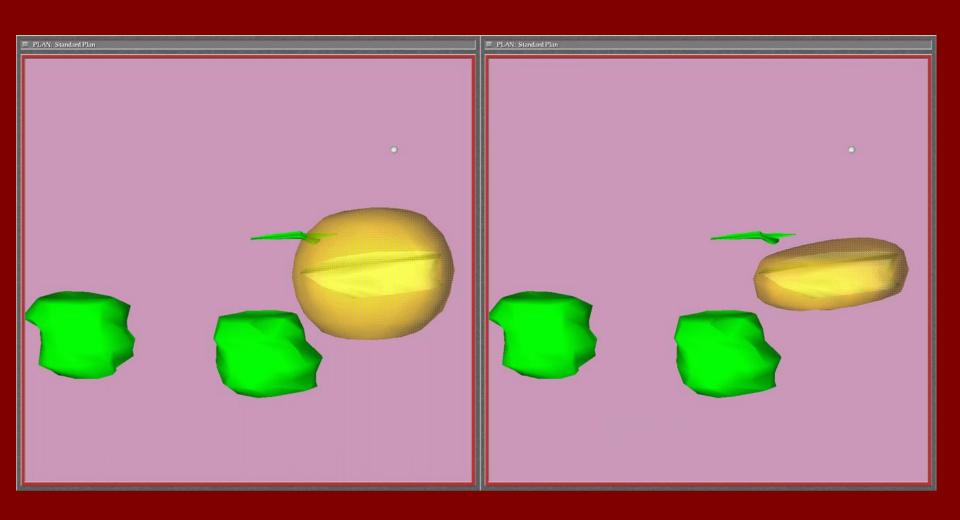
- < 3-4 cm
  - Circular Cones + Arcs Best
  - Sharp Penumbra avoids OAR
  - Precise Geometry
  - Low Integral Dose to Brain
- 3-6 cm
  - (a) XJaws = Jaws andCones and Arcs
  - Simple
  - Low Integral Dose to Brain
  - Optimal Conformal Index
  - (b) MMLC Okay
  - Exact Conformation not an issue.



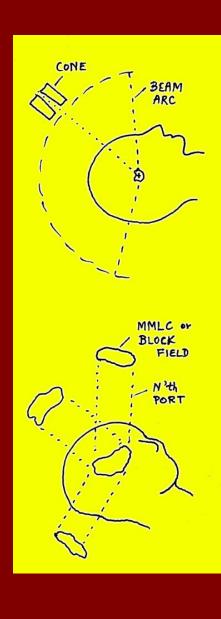
#### **Conformal Arc BEV**



#### Standard Arc Conformal Arc

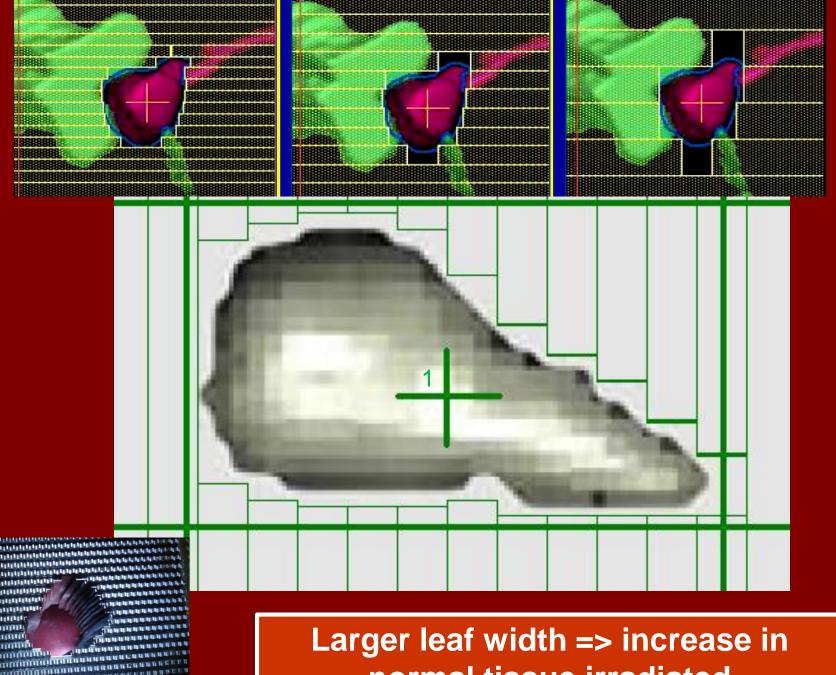


#### Considerations according to the type of target



- < 3-4 cm
  - Circular Cones + Arcs Best
  - Sharp Penumbra avoids OAR
  - Precise Geometry
  - Low Integral Dose to Brain
- 3-6 cm
  - (a) XJaws = Jaws and Cones and Arcs
  - Simple
  - Low Integral Dose to Brain
  - Optimal Conformal Index
  - (b) MMLC Okay
  - Conformation not the issue.
- > 6 cm
  - Penumbra Increases, not very effective to use Cones and Arcs
  - Better N ≥ 6 Non-Coplanar Static Fields
  - Need XPlan, OAR, Beam Model
  - MMLC necessary.
  - 2 π Access Reduces IMRT Need.





normal tissue irradiated







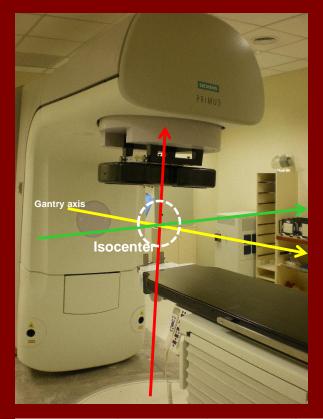
#### Micro MLC (mMLC)

- Add-on system attached to the regular collimator
- MODULEAF, Siemens
  - 80 leaf
  - 40Kg (require special mount to move around)
  - Leaf width at isocenter 2.5 mm
  - Positioning precision 0.5 mm
  - Penumbra 2.5 3.5mm
  - Transmission < 2.5%</p>
  - Maximum field size 12 x 10 cm<sup>2</sup>



#### **Isocenter precision**

#### Winston - Lutz test



Ball Centroid: Row = 52.19, Column = 53.97 Cone Centroid: Row = 51.92, Column = 51.68 Distance = 2.30 pixels, 0.46 mm



5 10 15

Delta X = 2.28 pixels, 0.45 mm Delta Y = 0.27 pixels, 0.05 mm Ball Centroid: Row = 53.48, Column = 53.00 Cone Centroid: Row = 51.57, Column = 51.33 Distance = 2.54 pixels, 0.50 mm



Delta X = 1.67 pixels, 0.33 mm

Delta Y = 1.91 pixels, 0.38 mm

Ball Centroid: Row = 53.04, Column = 50.97

Cone Centroid: Row = 51.47, Column = 52.04

Distance = 1.90 pixels, 0.38 mm



5 10 15
Delta X = -1.07 pixels, -0.21 mm
Delta Y = 1.57 pixels, 0.31 mm
Ball Centroid: Row = 53.53, Column = 50.14
Cone Centroid: Row = 50.98, Column = 51.39
Distance = 2.84 pixels, 0.56 mm



Delta X = -1.26 pixels, -0.25 mm Delta Y = 2.55 pixels, 0.51 mm

Ball Centroid: Row = 54.88, Column = 51.06 Cone Centroid: Row = 51.62, Column = 51.73 Distance = 3.33 pixels, 0.66 mm



5 10 15 Delta X = -0.68 pixels, -0.13 mm

Delta Y = 3.26 pixels, 0.64 mm

Ball Centroid: Row = 52.32, Column = 53.59

Cone Centroid: Row = 51.76, Column = 51.63

Distance = 2.04 pixels, 0.40 mm



5 10 1

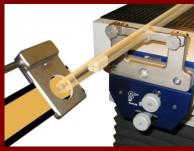
Delta X = 1.96 pixels, 0.39 mm Delta Y = 0.55 pixels, 0.11 mm Ball Centroid: Row = 53.13, Column = 51.08 Cone Centroid: Row = 51.25, Column = 51.52 Distance = 1.83 mm, 1938 mm



5 10 15
Delta X = -0.44 pixels, -0.09 mm
Delta Y = 1.88 pixels, 0.37 mm
Ball Centroid: Row = 53.74, Column = 50.48
Cone Centroid: Row = 51.76, Column = 51.31
Distance = 2.14 pixels, 0.42 mm



Delta X = -0.83 pixels, -0.17 mm Delta Y = 1.97 pixels, 0.39 mm











MRI images

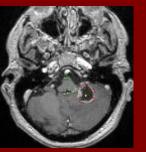


**Patient preparation** 

Placement of Head Ring for SRS

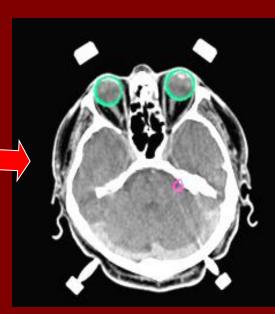






#### **Procedure**

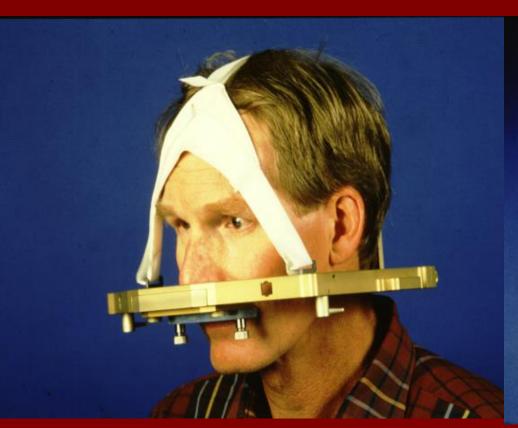


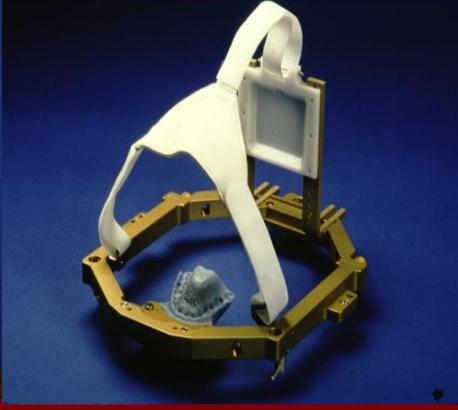






## Relocatable Head Frame (Gill-Thomas-Cosman) for fractionated SRT





#### **SRS** with GTC relocatable head frame



#### Daily reproducibility of the head frame position

<u>DEPTH CONFIRMATION HELMET</u>: Mounts on stereotactic base ring; allows for 25 'helmet to scalp' measurements which are repeated following frame attachment, removal, replacement, and for SRT prior to each treatment (accuracy +/-1.5 mm)



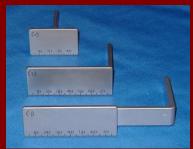




#### **Patient Immobilization (SRT)**

3 piece Mask System
Extends treatment area to T1
Set-up errors from 1.7 to 0.9 mm
Indexed bite plates
Carbon fiber
Tilt compensation for set-up
Suitable for elderly patients & children













#### Frameless Immobilization







MRI

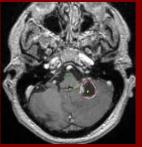


**Patient setup** 

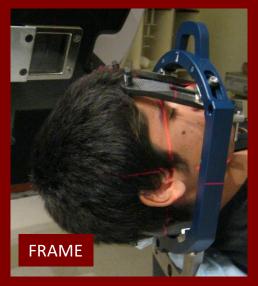


**CT** angiography

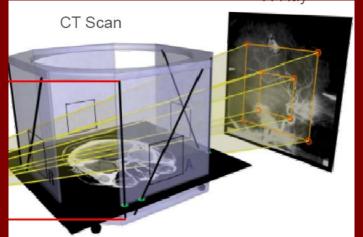




#### **CT** angiography

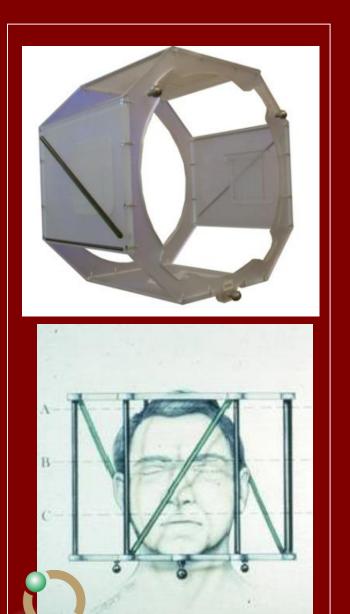


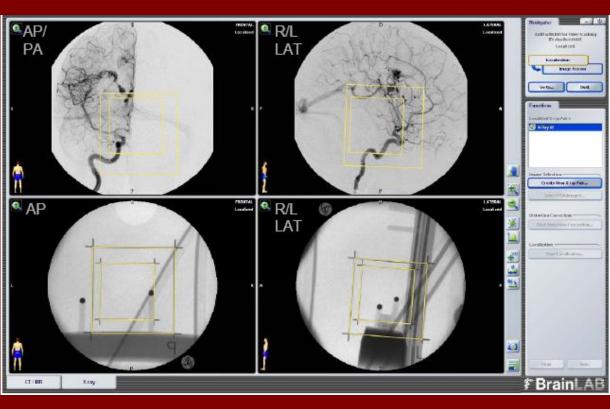






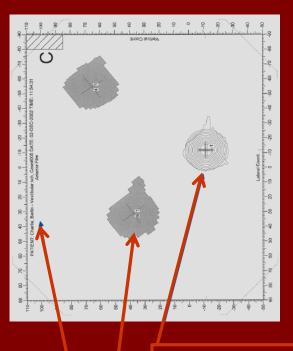
#### **Angiography Localizer frames for Stereotactic Imaging**





#### **Transfer of Coordinates**

#### **TPS plan -> Treatment unit**



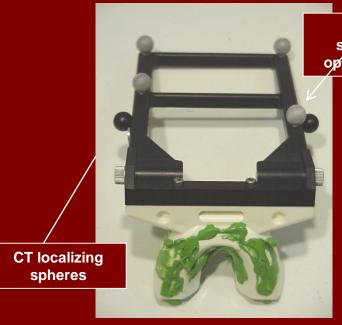
Patient identifier

Laser isocenter alignment

Field shape projection







Reflecting spheres for optical tracking

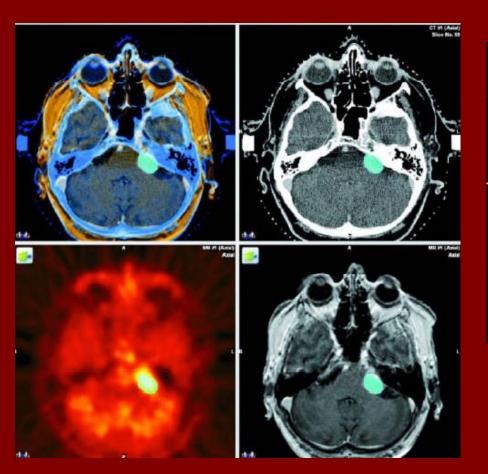
### Optical tracking of Stereotactic position space

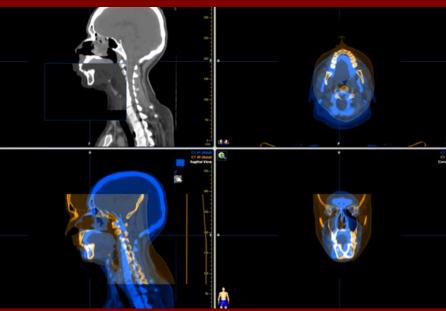
The CT images of the spheres are used to transfer the coordinate space to the treatment room



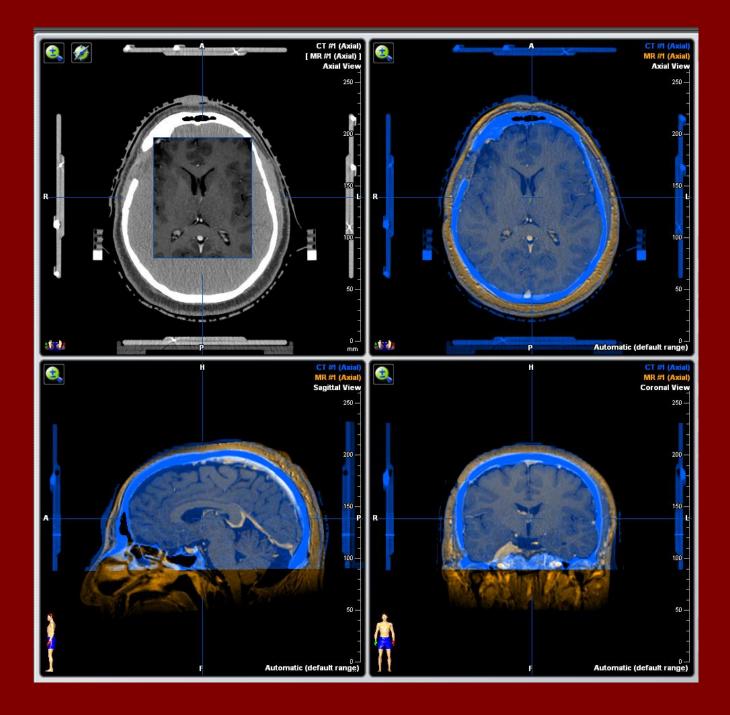


#### **Image fusion or Registration**





CT - MR - SPECT - PET



#### **Patient setup**



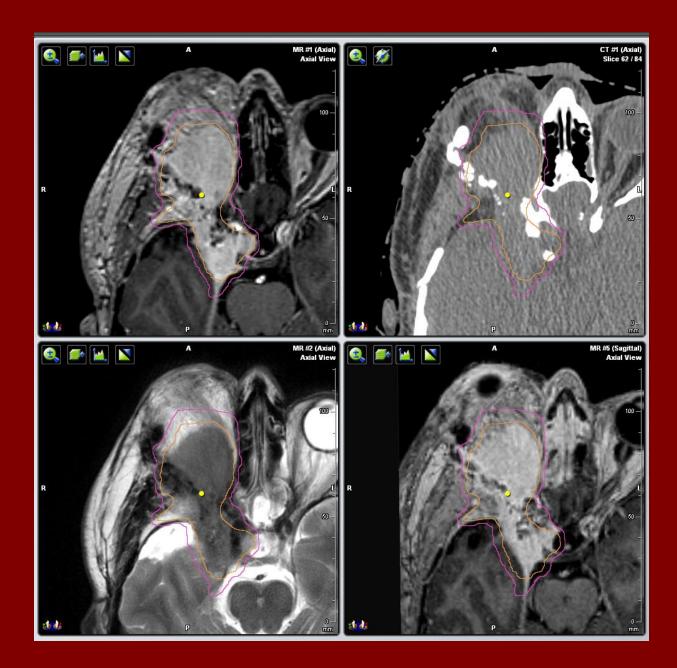
**Stereo Images** 



**Image fusion** 



**Volume definitions** 





#### **Patient setup**



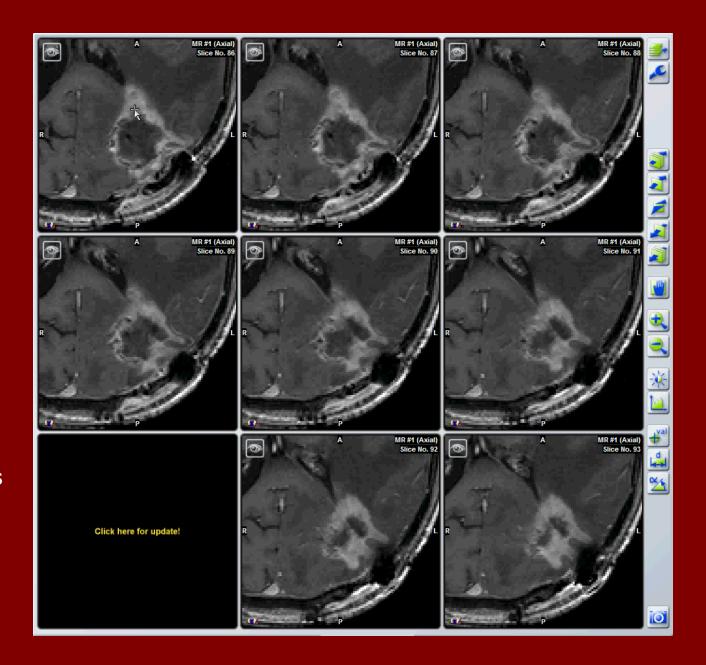
**Stereo Images** 



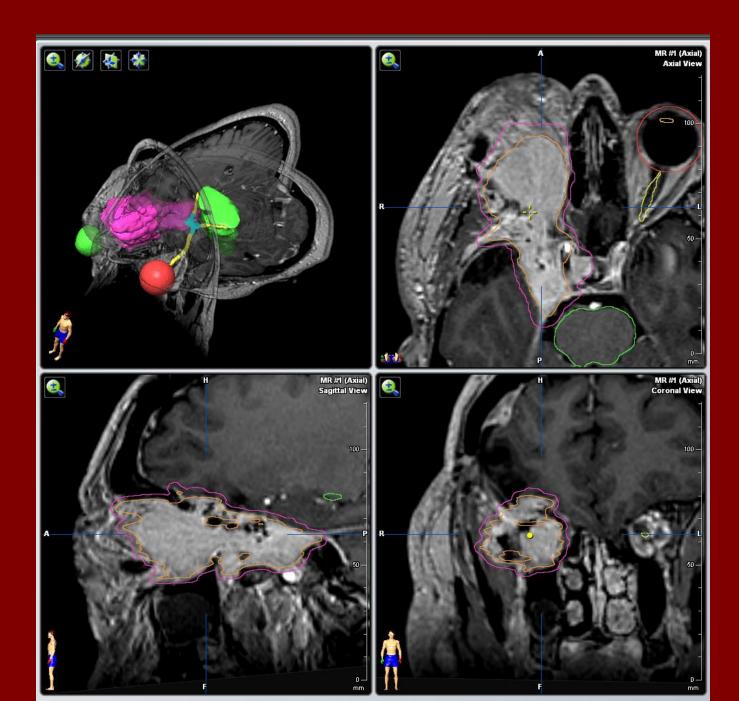
**Image fusion** 



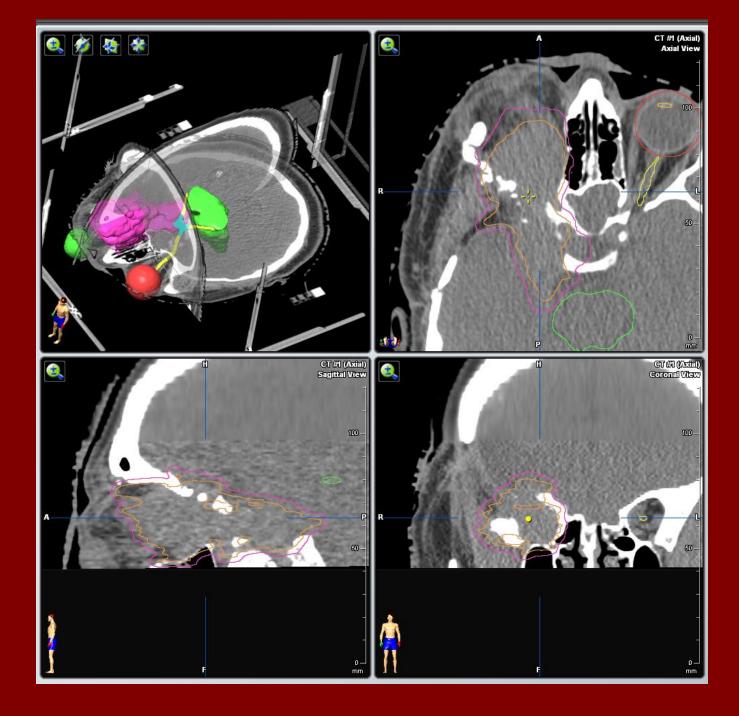
**Volume definitions** 









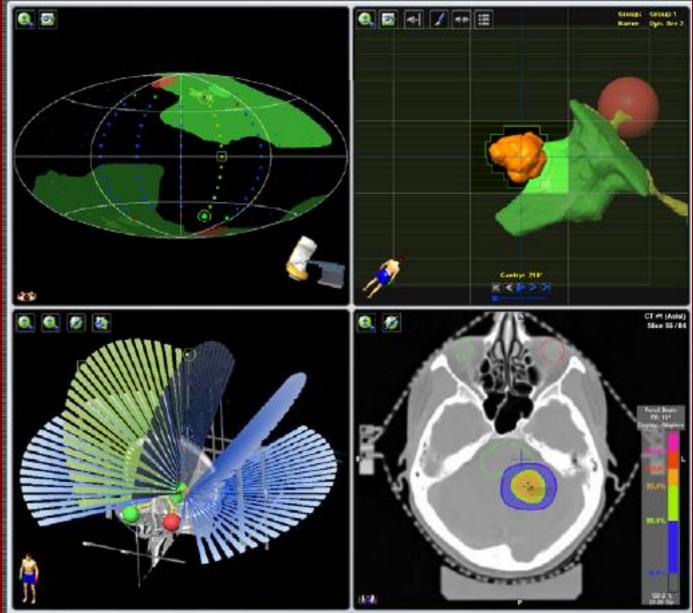


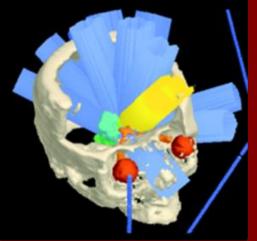
#### Uncertainties achievable in SRS

CT slice Thickness	1 mm	3 mm
Stereotactic Frame	1 mm	1 mm
Isocenter Alignment	1 mm	1 mm
CT Image resolution	1.7 mm	3.2 mm
Tissue Motion	1.0 mm	1 mm
Angio (Point identification)	0.3 mm	0.3 mm
Std. Dev. of Pos. Uncertainty	2.4 mm	3.7 mm

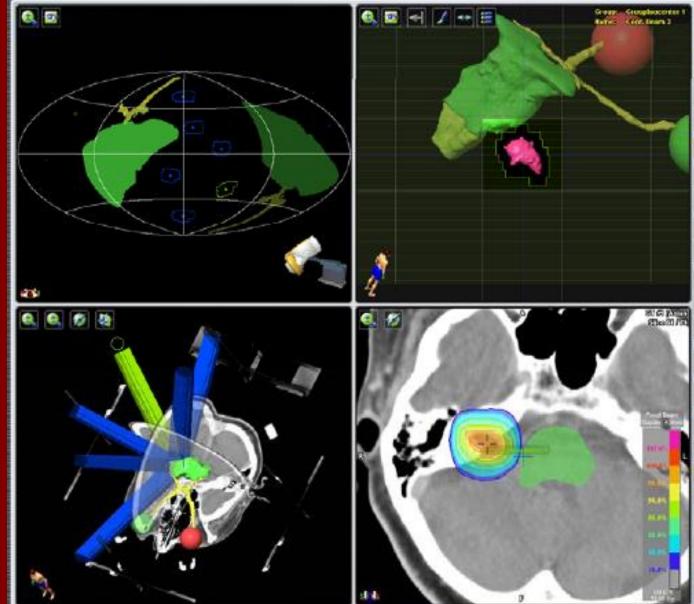


#### **PLANING WITH CONFORMAL ARCS**





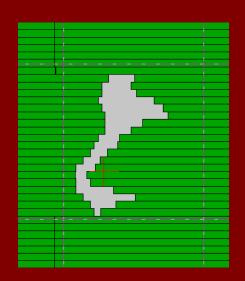
#### PLANING WITH CONFORMAL FIXED FIELDS



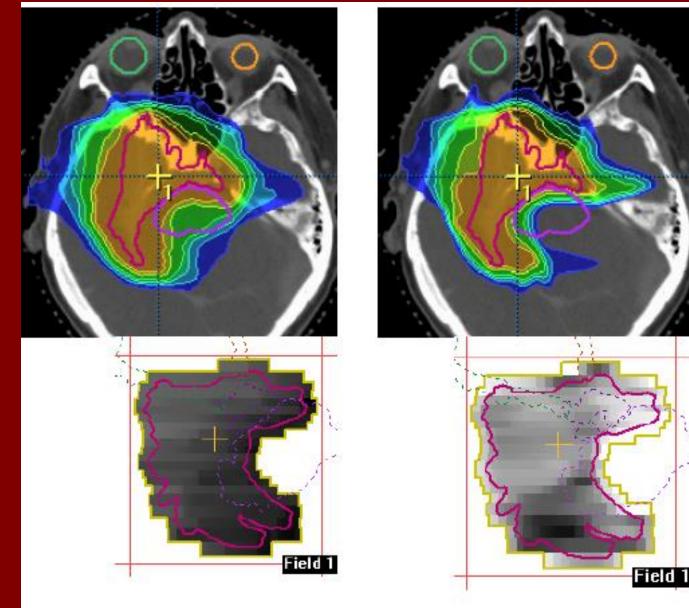


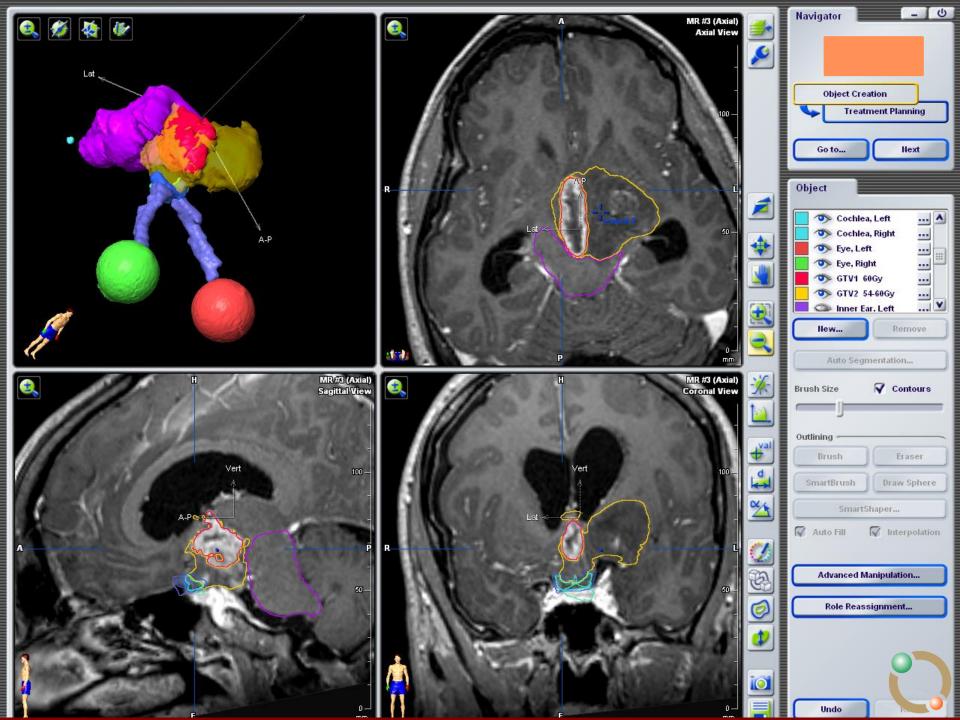
# AXIAL

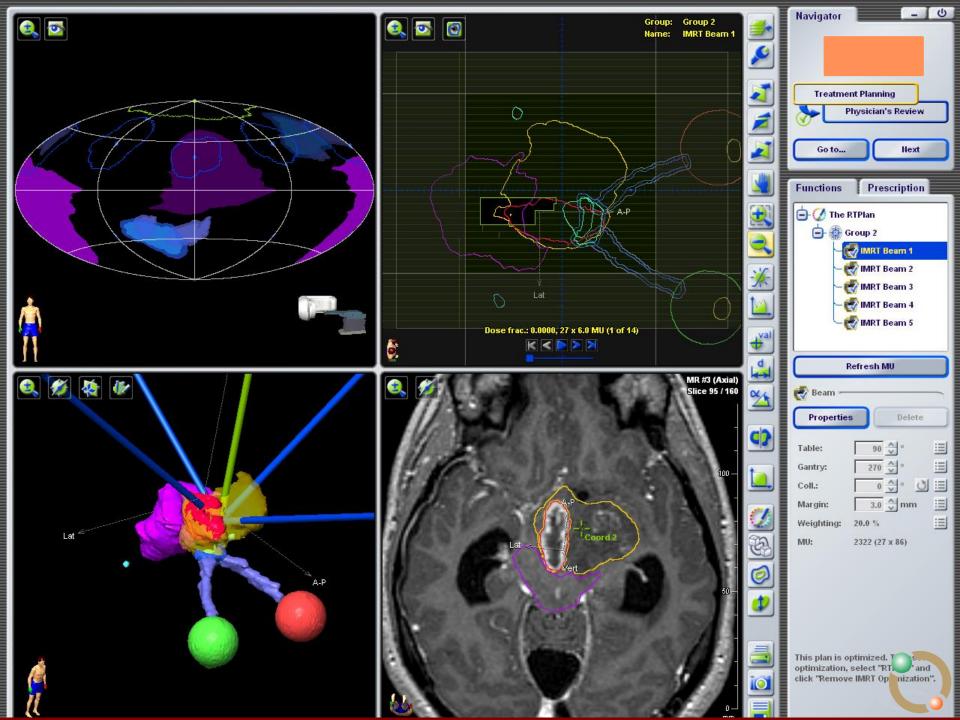
## 

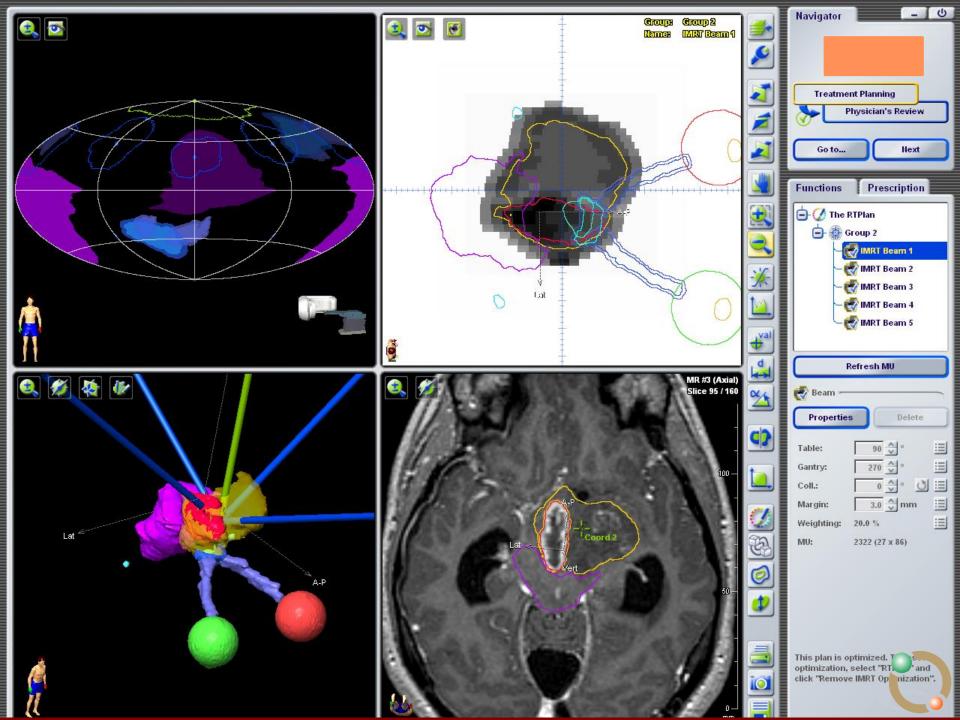


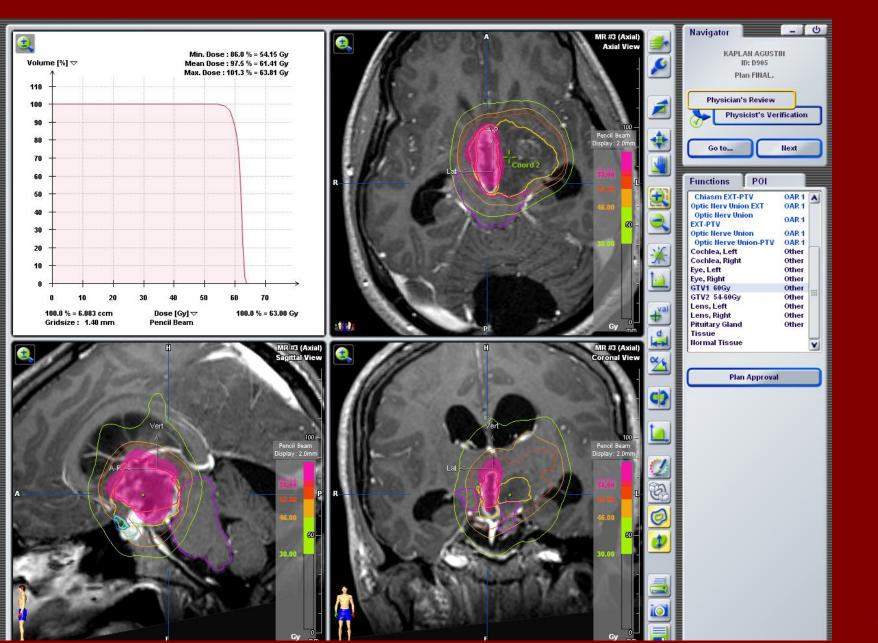
## PLANING with Intensity Modulated Radio Surgery (IMRS)





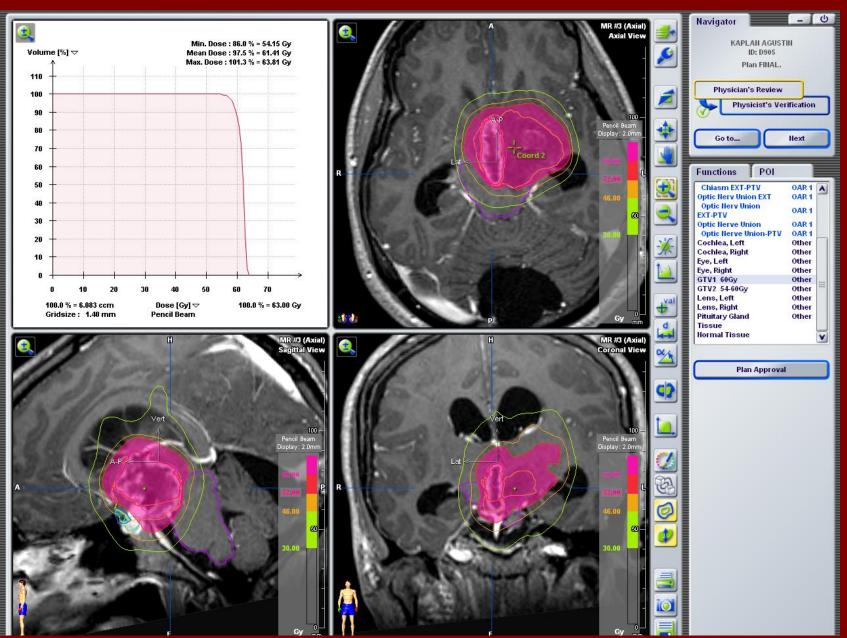








#### Single isocenter for irregular targets with better conformality and homogeneity than cones



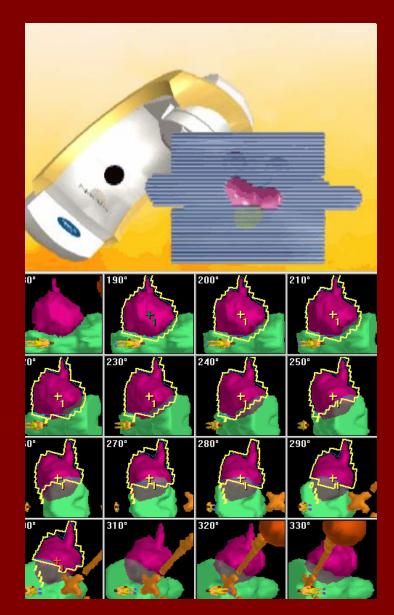


#### Dynamic Conformal Arc

- Automatic leaf adaptation to tumor contour
- Straight-forward arc optimization with collision map
- MLC control must be synchronized with gantry rotation

#### Advantages

- Fast, semi-automatic single isocenter treatment planning
- Critical structures are easier to avoid for most beam angles
- Most conformal and homogeneous dose distribution with reduced irradiation of normal tissue

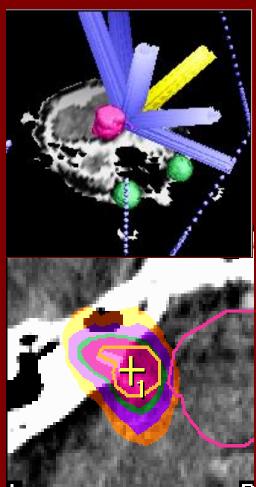


### Comparison of plans

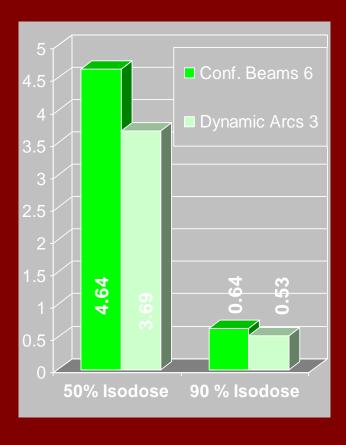
Conformal mMLC Plan
1 Isocenter -6 Static
Fields

**Dynamic Conformal Arc Plan 1 Isocenter - 3 Dynamic Arcs** 

Volume of irradiated Normal Tissue (cm³)





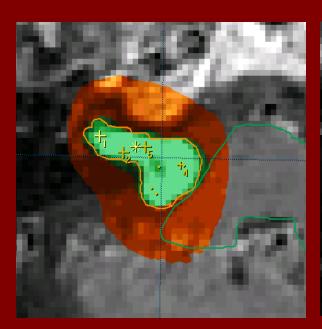


Courtesy of Universitätsklinkum Charité, Berlin

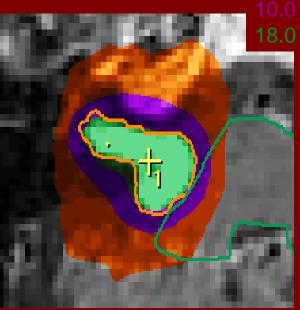
7.2 Gy 18.0 Gy

#### Comparacion Acoustic Neuroma

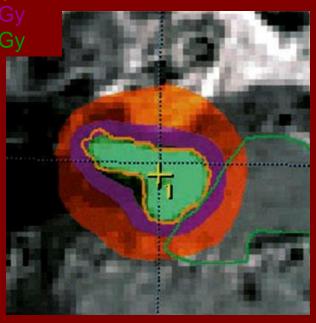
4.0 Gy



Circular Arc, 8 Isocenters



Conformal Beam, 19 Beams (1 isocenter)



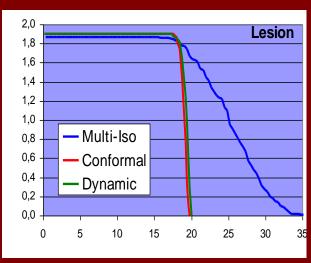
**Dynamic Conformal Arc, 5 Arcs (1 isocenter)** 

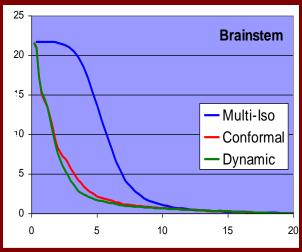
Improved normal tissue sparing Tight margin around target

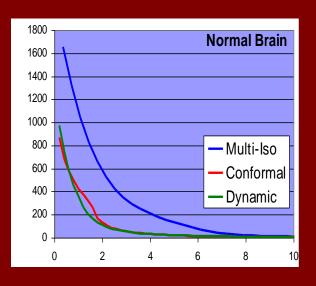
# Comparison

#### **Acoustic Neuroma**

#### Homogenous Dose Distribution Greater sparing of normal tissue and structures at risk





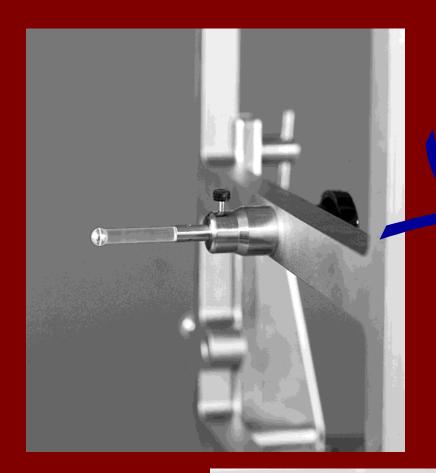


Dose (cGy)

Dose (cGy)

Dose (cGy)

# QA of Isocenter

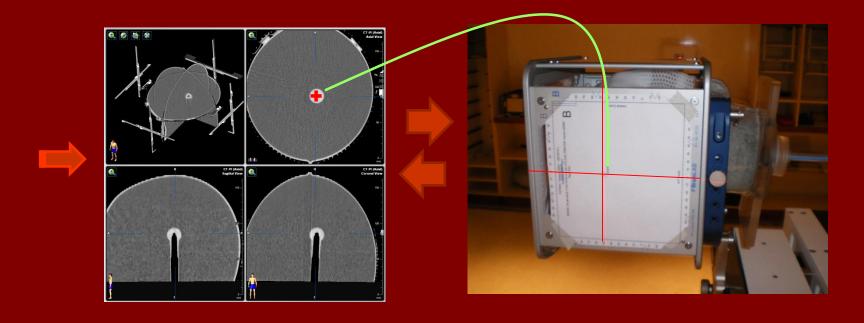




### **Coordinate verification**

- Templates and Laser -





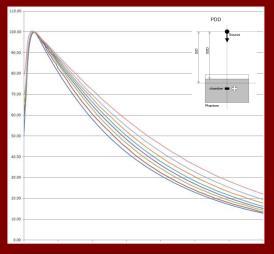


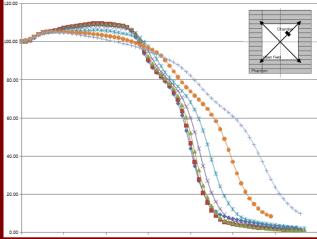
# Beam dosimetry of small fields and treatment planning commisioning

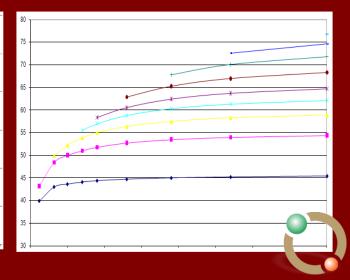
### Beam parameters

- PDD
- Profiles
- Field size dependent output factors
- Transmission
- Absolute dose







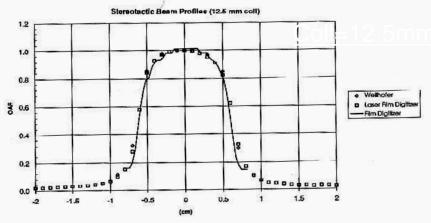


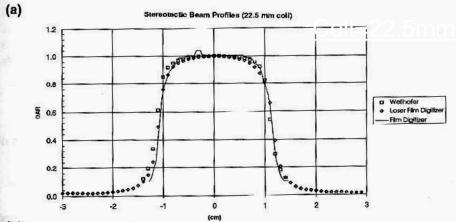
# **Beam Dose Measurements**

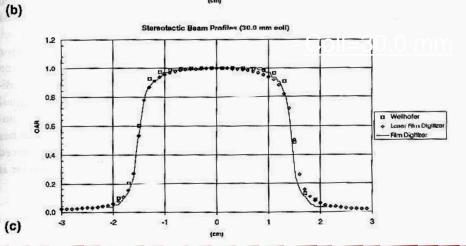
- Issues with small field dosimetry:
  - Detector size vs. Small field dimensions
  - Lack of lateral charged particle equilibrium
  - Large dose gradients in SRS penumbra
- Equipment:
  - Water tank, polystyrene slabs, ion chamber, diodes, TLD's and Film
  - Very small Detector diameter required to reproduce a penumbra of ~1mm

Small Field Dosimetry: Overview of AAPM TG-155 - Indra Das- AAPM AM 2015

http://amos3.aapm.org/abstracts/pdf/99-28443-359478-110238.pdf







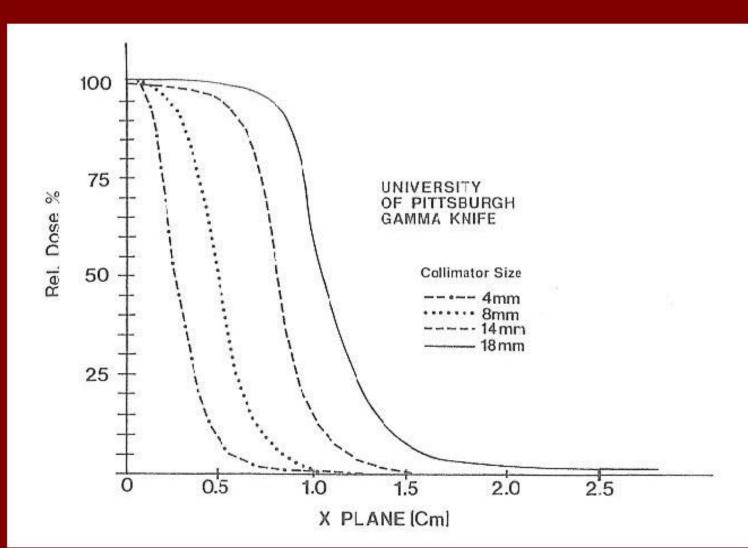
#### **Beam Profiles**

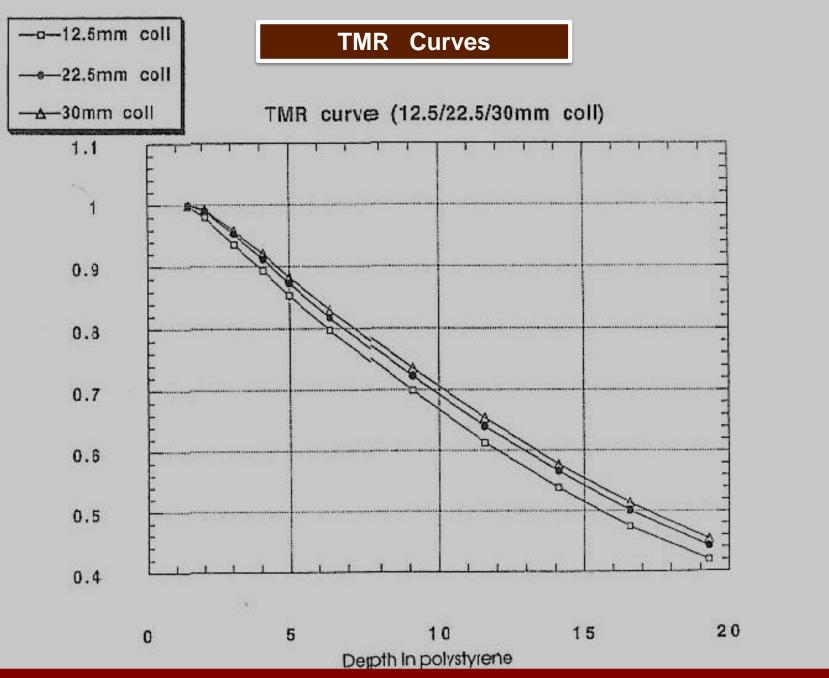
**❖** Welhofer

Laser Film Digitizer (Lumisys)

**Film Digitizer** 

#### **Gamma Knife - Beam profiles**

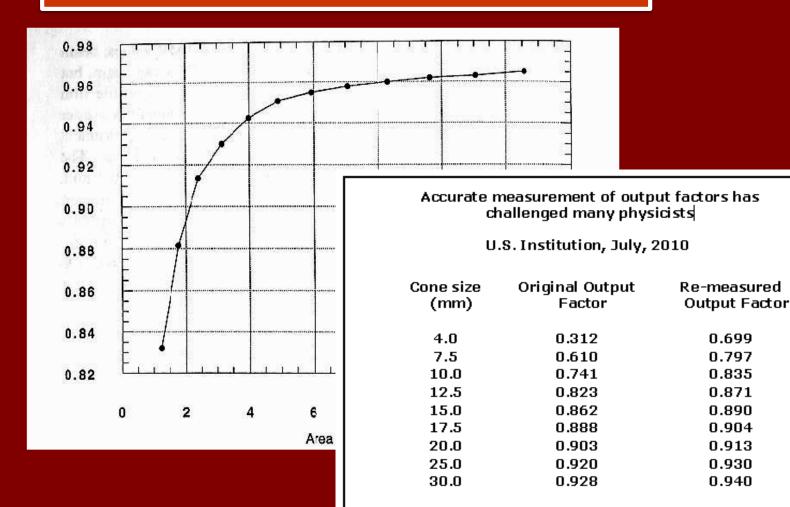




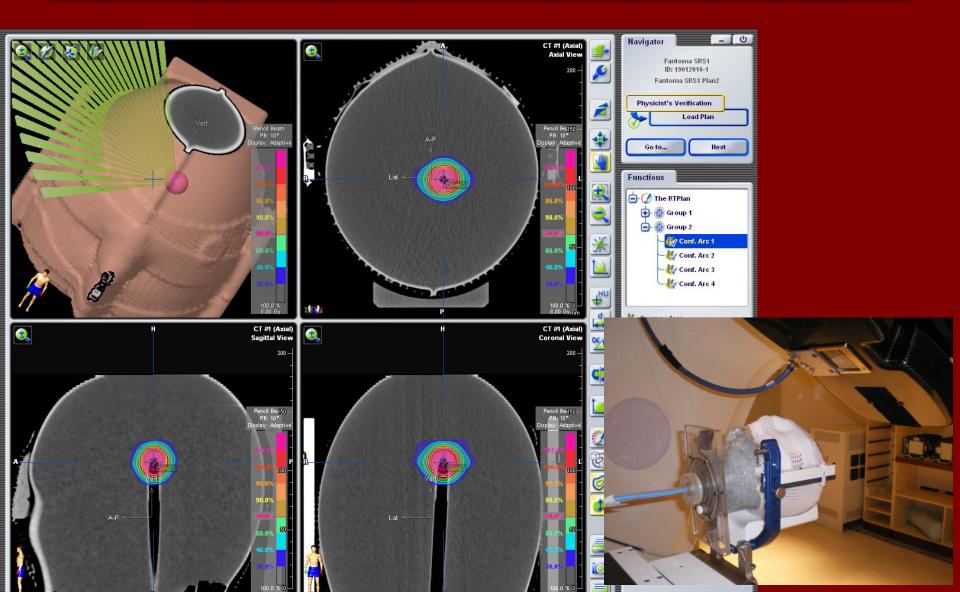
# Stereotatic Output Factor Curve $(S_t=S_c S_p)$

@ Isocenter, d<sub>max</sub>

6 MV Coll. Diam.:12.5mm to 20.0mm



### Verification of dose calculations

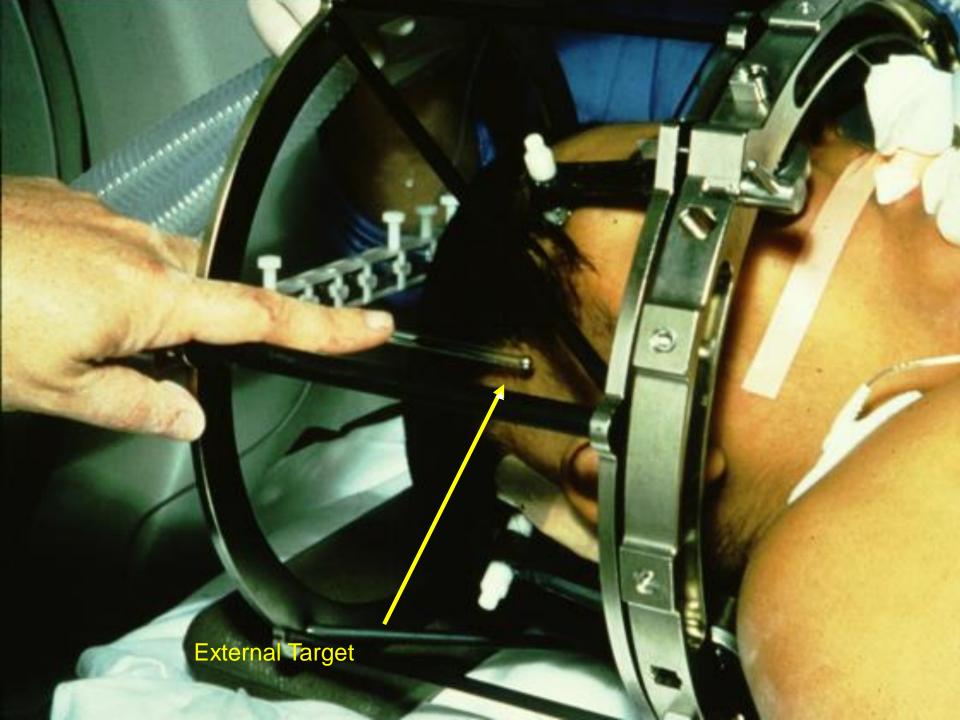


### Verification of dose calculations

- IMRS Patient specific dose measurements
  - Absolute total plan dose
  - Relative doses per field
  - Relative plan dose distribution

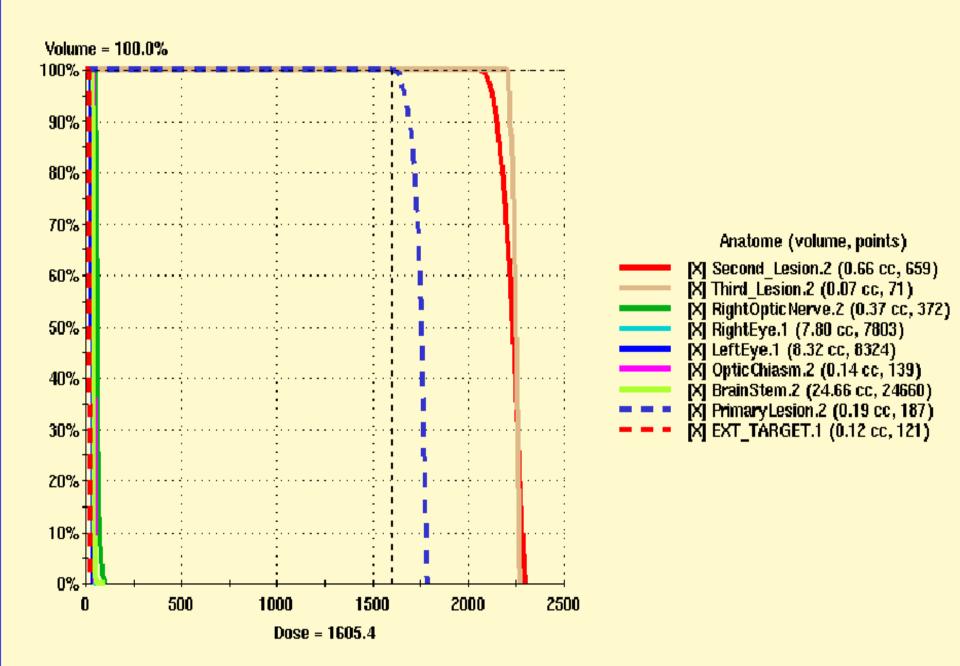


	Verificación DOSIS IM PRIMUS	RT PLANILLA 002 Páglica 1 de 2	AA)			Verificación DOS IS IMRT PRIMUS		MRT	PLANILLA 003 Pagina 0 de 2			
	ntrol de Calidad específico	onRAD):	III. Dosis	relativa sso + 9 fom	en FAN	TOMA P	LANO p tw 729 + 2	or cam	700 runtar			
		Volumes:	FILM	Cam	ро	Archivo PTW 729	mag	en N*	QA	RIT		
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			4		- 4		6				-	
teside =		76075 ((2732+T)/2932) +	5		- 1		-	_			-	
			6				- 6					
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			10		- 3		- 63	-			-	
	soluta en FANTOMA PLANO (a)	(16-CONDICION DETRATAMIENTO)	11		- 1		-	-			-	
Paradasa Fata	ma reservings, raminismi	20	20 8		1.00		(0)	1%			- 500	
L'ampo			l I									
Campo	Nombre L	ao (Lietura acumulata)										
1.	Nombre L	ag (Lecturia scumulada)	IV. Dosis			TOMA D	osis Tot	fal				
0.0000000000000000000000000000000000000	Nombre L	ag (Lind or a sicomolodia)	IV. Dosis	relativa		TOMA D	osis Tot	f <u>al</u>				
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1 2 3 4 5	Nombre L	ao (Just ur a acumulat la)			2	TOMA D	osis Tot	7	8	9	10	11
1 2 3 4 5	Nombre L	ao (Lectura accumulata)	Fantoma I	Facto IMPELS	2			<u>7</u>	8	9	10	11
1 2 3 4 5 6 7	Nombre L	ge Gad ar a muradatai	Fantoma I	Facto IMPELS	2			7	8	9	10	11
1 2 3 4 5 6 7	Nombre L	ac (ded or a mineral de)	Fantoma I	Facto IMPELS	3 4	4 5	6	7	8	9	10	11
1 2 3 4 5 6 7 8 9	Nombre L	gg (Letter seinendati)	Farntoma MEDTEC	1 2	3 4		6	7	8	9	10	11
1 2 3 4 5 6 7 8	Nombre L		Fantoma MEDTEC	1 2	3 4	4 5	6	7	8	9	10	11
1 2 3 4 5 6 7 8 9 10			Fantoma MEDTEC Plano X =	1 2	3 4	4 5	6	7	8	9	10	11
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1 2 3 3 4 5 6 6 7 8 9 10 11 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1	L <sub>30</sub> = 89.15/ L <sub>bef</sub> = 314 (KonRAD) =	Δ%=	Plano X = X = X =	1 2	3 4	4 5	6	7	8	9	10	111
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1 2 3 3 4 5 6 6 7 8 9 10 11 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1	L <sub>30</sub> = 89.15/ L <sub>bef</sub> = 314 (KonRAD) =	Δ%=	Plano X = X = X =	1 2	3 4	4 5	6	7	Roll Roll		10	



# **Dose Evaluation Tools**

- Volume Dose
- Surface Dose
- Dose Summary
- Slice Dose
- Dose Volume Histograms



### Plan quality indices

Conformity (CI): Ratio of the prescription isodose volume V(p)to the

target Volume V(T)

Homogeneity (HI) Ratio of maximum dose D(max) to Prescription Dose

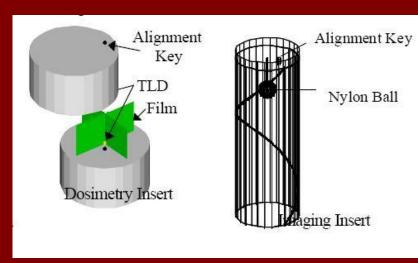
D(p)

Dose gradient: Ratio of V(T) to Volume of the 50% isodose (V<sub>50%</sub>)

	Conformity	Homogeneity	Gradient
Reference value	1 – 2	<u>HI &lt;</u> 2	≥ 0.3
Minor deviation (acceptable)	0.9< CI < 1 o 2 < CI < 2.5	2 < HI <u>&lt; </u> 2.5	
Major deviation (unacceptable)	CI < 0.9 o CI <u>&gt; </u> 2.5	HI > 2.5	

#### Total system verification – external audit





- ■Plan according to "RTOG Quality Assurance Guidelines"
- ■Phantom
  - *Target F* = 19mm
  - Gafchromic film in two orthogonal planes
  - 2 TLD-100at the target center
  - •http://rpc.mdanderson.org/rpc



#### Report



Preliminary studies suggest that the precision of the TLD is  $\pm 3\%$ , and the localization precision from the film is  $\pm 1$  mm.

Summary of results:

	Ratio	Criteria (a)
Dose to the center of the target (RPC/Institution)	0.98	0.95 - 1.05
Treated Volume (b): (Measured/Institution)	0.78	0.75 - 1.25 (c
Ratio of Measured Treated Volume to Target Volume (d)	1.17	1.00 - 2.00
Minimum Dose to Target (Minimum Dose/Prescription Dose) <sup>(e)</sup>	0.91	> 0.90

- (a) Criteria are adapted from the RTOG QA guidelines. Int. J. Onc. Biol. Phys. 27, 1231-39, 1993.
- (b) The treated volume is assumed to be an ellipsoid with diameters taken from the "Film Results" table.
- (c) Average discrepancy of approximately 2 mm on each diameter.
- (d) The target is the 1.9 cm. sphere.
- (e) Minimum dose is taken from the 3 dose profiles.

TLD and Film Analysis by: Paola Alvarez, MS

#### TLD Results:

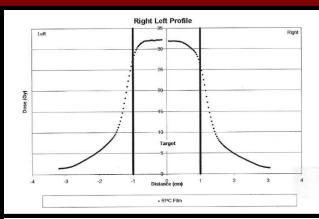
Dose to TLD Caps	ules (Gy)	Average Dose (Gy)	Institution Dose	Ratio	
Upper Lower		(Dose to Center)	(Gy)	Measured/Institution	
30.5 29.4		30.0	30.5	0.982	

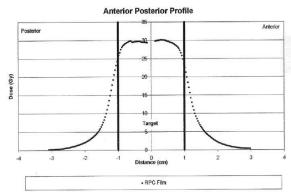
#### Film Results:

	Fi	Offset (80% Line)		
Measured Along	Measured (cm)	(cm)		
Right/Left Profile (x)	2.1	2.2	-0.1	0.0
Anterior/Posterior Profile (y)	2.0	2.1	-0.2	0.0
Superior/Inferior Profile (z)	1.9	2.2	-0.3	-0.1

Treated Volume (cm <sup>3</sup> )**	4.10	5.40
rreated volume (cm.)	4.19	5.40
	The second secon	

- \* Offset is the distance between the center of the specified isodose line and the center of the physical target.
- \*\* Treated Volume= (11 x y z)/6





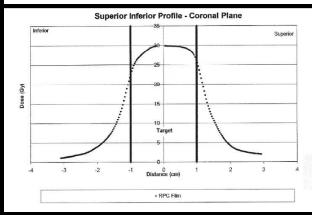


Table 1. List of radiosurgery events reported to the NRC during the period 2005-2010

Event Description	Treatment Implication
Patient orientation entered incorrectly at MR Scanner	Wrong location treated
Fiducial box not seated properly during CT imaging	Wrong location treated
Malfunction of automatic positioning mechanism following re-initialization	Wrong location treated
Right trigeminal nerve targeted instead of left	Wrong location treated
Facial nerve targeted instead of trigeminal nerve	Wrong location treated
Mistake in setting isocenter coordinates	Wrong location treated
Head not secured to stereotactic device (2 events)	Wrong location treated
Selected collimators did not match planned	Wrong dose/distribution delivered
Physician mistakenly typed 28 Gy instead of 18 Gy into planning system	Wrong dose delivered
Physicist calculated prescription to 50% isodose instead of 40%	Wrong dose delivered
Microphone dislodged, causing stereotactic device to break	Treatment halted after 2 of 5 fractions
Couch moved during treatment	None; personnel interrupted treatment

from: Quality and safety in stereotactic radiosurgery and stereotactic body radiation therapy: can more be done? Timothy D. Solberg, and Paul M. Medin

Jour. of Radiosurgery and SBRT, Vol. 1, pp. 13-19

#### LESSONS FROM RECENT ACCIDENTS IN RADIATION THERAPY IN FRANCE

S. Derreumaux\*, C. Etard, C. Huet, F. Trompier, I. Clairand, J.-F. Bottollier-Depois, B. Aubert and P. Gourmelon.

Institut de Radioprotection et de Sûreté Nucléaire, Direction de la Radioprotection de l'Homme, IRSN, BP 17, F-92262 Fontenav-aux-Roses Cedex, France

Radiation Protection Dosimetry (2008), Vol. 131, No. 1, pp. 130-135





Figure 2. Stereotactic radiotherapy treatment delivery with successive beam entrance positions as a function of accelerator and table rotation angles (left). The plate used in the centre (Case 2) to hold the cylindrical additional collimator (right).

Single fraction SRS for AVM, November, 2004

Prescription dose not reported; plan/treatment used multiple isocenters, with collimators from 10 -30 mm

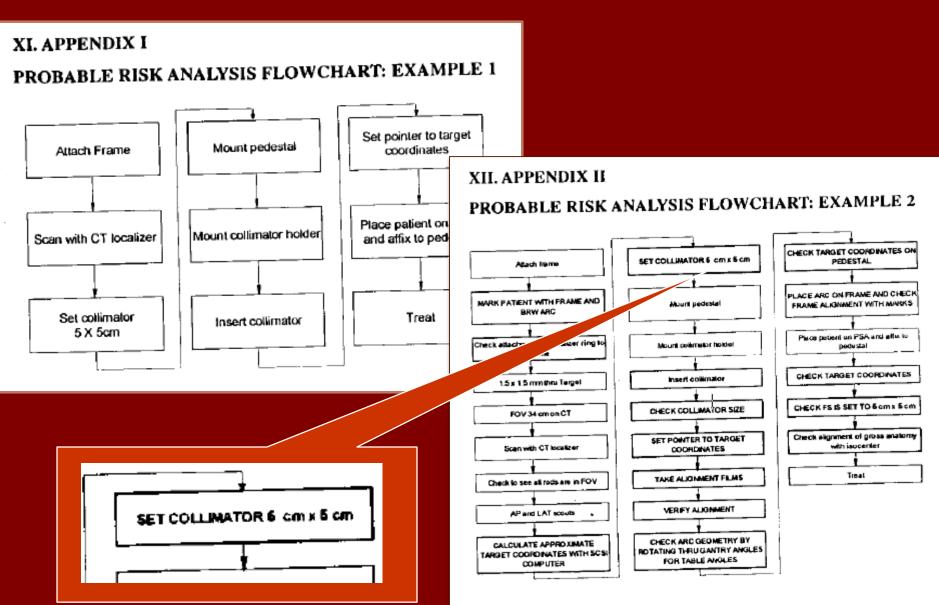
Jaws set to 40 x 40 cm<sup>2</sup> instead of 40 x 40 mm<sup>2</sup>. Physicist told therapist "40 x 40"

Some areas of normal brain received in more than dose to intended target

Severe complications: "fibrosis and oseotracheal fistula that required surgical operation." Patient died several days later as a result of a "brutal haemorrhage."

A written checklist system, and/or a proper R/V system can minimize events like this

#### AAPM Report 54 (1995) Task Group #42 - Stereotactic Radiosurgery

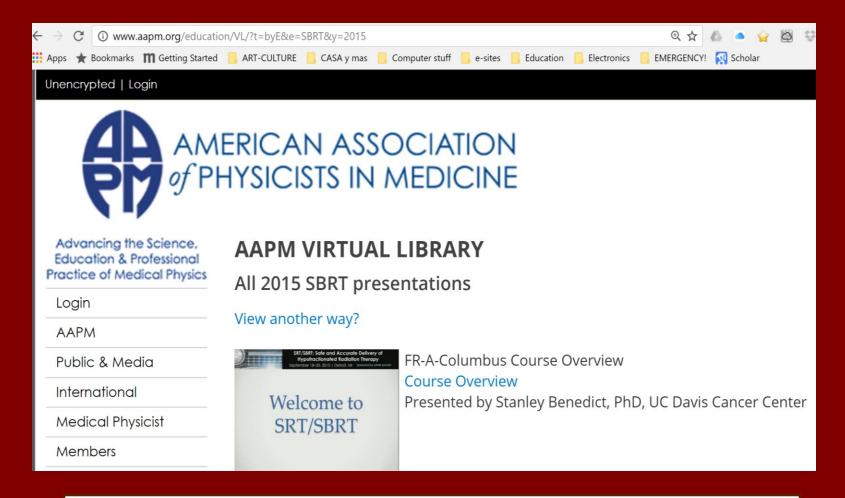


#### RADIOSURGERY PROCEDURE CHECK LIST

Patient Name:		I	Date:	
ISOCENTER NAME:				
EXTERNAL TARGET	AP	LAT	VERT	SIGNATU RE
Phantom Base Measurements			+ 2.4 =	
Plan-32 Calculation				
External test target acceptable:				
TRUE TARGET (ISO)	AP	LAT	VERT	
Floor, Stand (target) coord				
Floor Stand Redout Check				
Collimator size				
Collimator Inserted				
Jaw 5 x 5, Collimator: 270°				
Target Simulator	AP	LAT	VERT	
Coordinates			+15.4 =	
Target Simulator Film Acceptabble	Exposure	Gantry	Couch	
	1	130°	180°	
	2	65°	180°	
	3	295°	180 °	
	4	230°	180°	
	5	130°	270°	
	6	67°	270°	
	7	230°	90°	$\bot$
	8	297°	90°	
Anti-collision switches in place				
Couch Disabled				

#### LONG ISLAND JEWISH MEDICAL CENTER DEPARTMENT OF RADIATION ONCOLOGY RADIOSURGERY PROCEDURE CHECK LIST

Patient Name:		ID:		Date:				
ISOCENTER NA	AME:							
EXTERNAL TARGE	AP(Y)	LAT(X)		VERT(Z)	SIGNATURES			
Phantom Base Mean	urements				+2.4 =			
Radionics, Calculation	ı (mm)							
Treatment Planning	System(mm)							
External test targe	t acceptable:	Yes		N	0			
TRUE TARGET (IS	O)	AP(Y)	LAT(X)		VERT (Z)			
Rectiliniar Phantom	Pointer(RLPP)							
RLPP(target) Coord	inates (mm)							
RLPP read out check	(mm)							
Collimator (cone)	size planed			m	m (diameter)			
Collimator Inserte	d	mm (diameter)						
Jaw 5 x 5,Collimat	or: 0°	Yes No						
Laser Target Localiz	er Frame (LTLF)	AP(Y)	LAT(	X) VERT(Z)				
LTLF Coordinates (	mm)							
Target Simulator l	Film Acceptable	Exposure	Gantry		Couch			
		1	0.	90*				
Yes	No	2	270°	0-				
		3	90*	0.				
		4	0.	270°				
Couch Morion Disab	led	Yes	No					
Depth	Point	Helmet	Port	I	epth (mm)			
Confirmation	1							
Helmet Check	2							
	3							
	4							
	5							
	6	l						



http://www.aapm.org/education/VL/?t=byE&e=SBRT&y=2015



Strategies and Technologies for Cranial Radiosurgery Planning: MLC-Based Linac - Grace Gwe-Ya Kim- AAPM AM 2015 <a href="http://amos3.aapm.org/abstracts/pdf/99-28341-359478-110407.pdf">http://amos3.aapm.org/abstracts/pdf/99-28341-359478-110407.pdf</a>

Strategies and Technologies for Cranial Radiosurgery Planning: Gamma Knife - D. Schlesinger, -AAPM AM 2015 <a href="http://amos3.aapm.org/abstracts/pdf/99-28342-359478-110662-163112814.pdf">http://amos3.aapm.org/abstracts/pdf/99-28342-359478-110662-163112814.pdf</a>

Overview of CyberKnife Radiosurgery - M Descovich - AAPM AM 2014 <a href="http://amos3.aapm.org/abstracts/pdf/90-25583-333462-107361.pdf">http://amos3.aapm.org/abstracts/pdf/90-25583-333462-107361.pdf</a>

Clinical Applications of Surface Imaging: Frameless (Maskless, Bite-blockless) Intracranial Radiosurgery - G Kim –AAPM AM 2013

Dankie Gracias Спасибо Köszönjük Grazie Dziękujemy Dėkojame Dakujeme Vielen Dank Paldies
Kiitos Täname teid 油油 Obrigado Teşekkür Ederiz 감사합니다 Σας ευχαριστούμε Bedankt Děkujeme vám ありがとうございます Tack

תודה