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Simulation and Synthesis**

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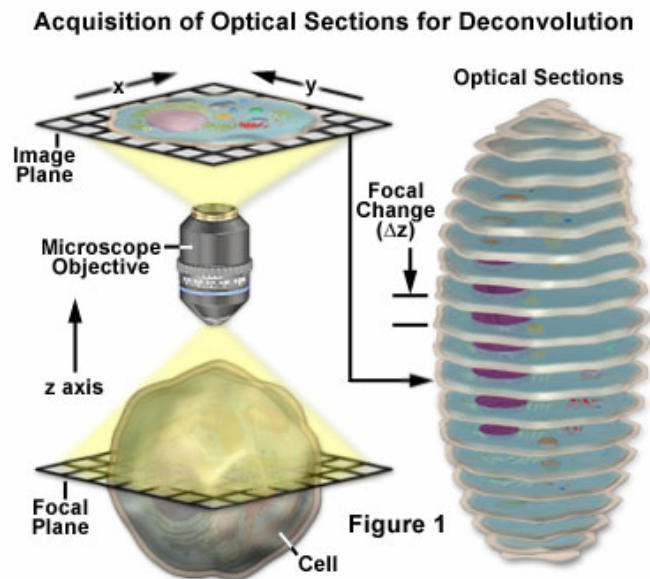
Three-dimensional deconvolution in FPGA

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***Three-dimensional
deconvolution
in FPGA***

Summary of deconvolution

Deconvolution is a computationally intensive image processing technique that is being increasingly utilized for **improving the contrast and resolution** of digital images captured in the microscope. The foundations are based upon a suite of methods that are designed to remove or reverse the blurring present in microscope images induced by diffraction.



The basic concepts surrounding acquisition of serial optical sections for deconvolution analysis are presented with a schematic diagram in Figure 1.

- The specimen is an idealized cell from which a series of optical sections are recorded along the z-axis of an optical microscope.
- For each focal plane in the specimen, a corresponding image plane is recorded by the detector and subsequently stored in a data analysis computer.
- During deconvolution analysis, the entire series of optical sections is analyzed to create a three-dimensional montage.

Modeling the effect of an optical system: 3D input-output relationship

$i(x, y, z)$: **Input light distribution**

$s(x, y, z)$: **Impulse response (3D PSF):** describes a process causing the output distribution to be different from the original scene.

$o(x, y, z)$: **Output light distribution**

Model equation:

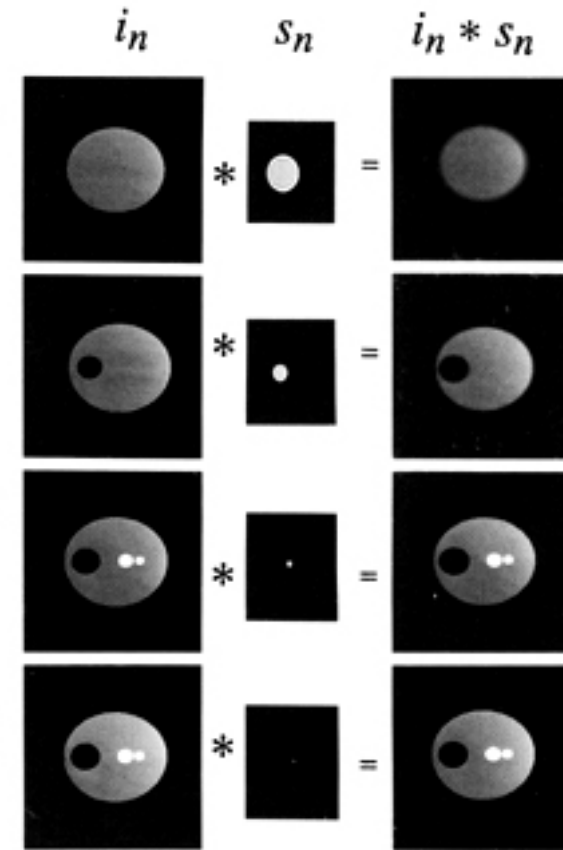
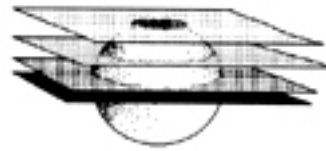
$$o(x, y, z) = i(x, y, z) \otimes s(x, y, z)$$

The 3D convolution operation is defined as:

$$o(x, y, z) = \iiint_{u,v,w} i(u, v, w) s(x-u, y-v, z-w) du \, dv \, dw$$

The impulse response (3D PSF), is the output light distribution in image space for a point source input in object space.

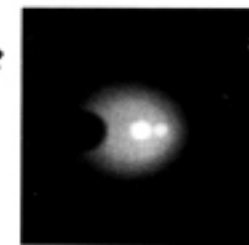
Z-stack decomposition



We can start by trying to decompose the 3D model equation

$$o(x, y, z) = i(x, y, z) \otimes s(x, y, z)$$

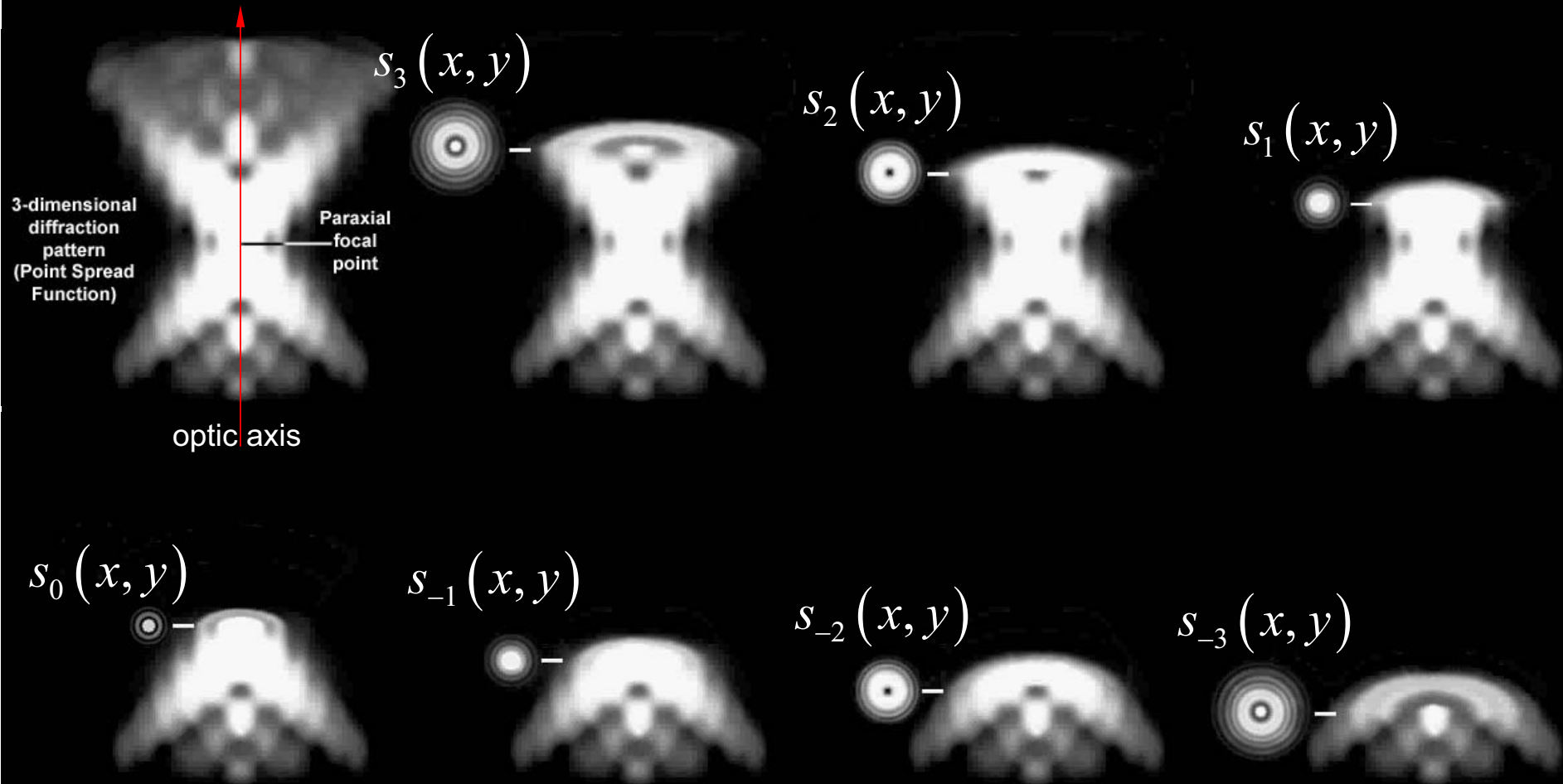
Observed Image



into a set of through-focus two-dimensional series expansions (z-stack)

$$o_z(x, y) = i_0(x, y) \otimes s_0(x, y) + i_{-1}(x, y) \otimes s_{-1}(x, y) + i_{+1}(x, y) \otimes s_{+1}(x, y) + \dots$$

Function $s_k(x,y)$, $k = -N, -N+1 \dots, 0, 1, 2 \dots N$, are sections through the 3-D PSF taken in planes orthogonal to the optic axis of the system



$$o_z(x,y) = i_0(x,y) \otimes s_0(x,y) + i_{-1}(x,y) \otimes s_{-1}(x,y) + i_{+1}(x,y) \otimes s_{+1}(x,y) + \dots$$

To convert these equations into an algorithm that can be used in practice, we will make two simplifying assumptions:

1. **Out-of-focus light contribution other than those from the adjacent planes are negligible, i.e. terms with index different from 0 or ± 1 can be ignored:**

$$\begin{aligned} o_z(x, y) \cong & i_0(x, y) \otimes s_0(x, y) + \\ & + i_{-1}(x, y) \otimes s_{-1}(x, y) + \\ & + i_{+1}(x, y) \otimes s_{+1}(x, y) \end{aligned}$$

(this assumption is not strictly necessary and will be relaxed later).

2. **Light originating from planes immediately above or below the plane of focus can be approximated by images taken while focusing on these planes, i.e.**

$$i_{-1} \cong o_{-1}$$

$$i_{+1} \cong o_{+1}$$

(Castelman, 1979)

Z-stack decomposition

Taking plane $z=0$ as the reference focal plane,

we write the simplified equation

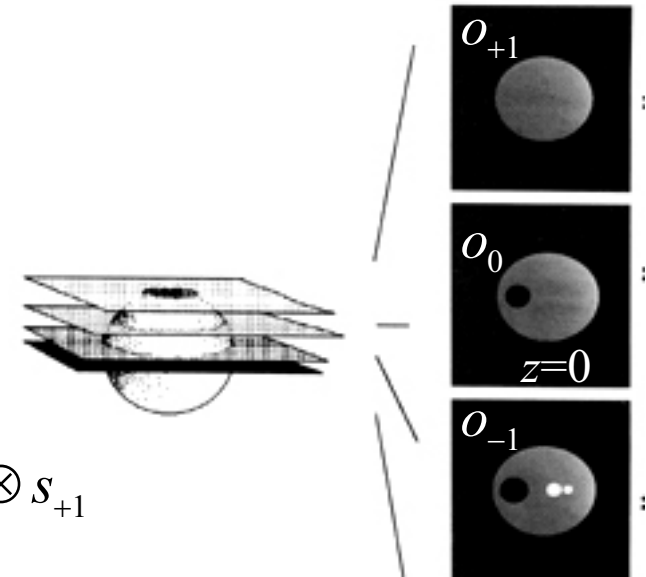
$$o_0 = i_0 \otimes s_0 + o_{-1} \otimes s_{-1} + o_{+1} \otimes s_{+1}$$

in the form

$$i_0 \otimes s_0 = o_0 - o_{-1} \otimes s_{-1} - o_{+1} \otimes s_{+1}$$

Now we take the Fourier transform, F , of both sides:

$$F(i_0 \otimes s_0) = F(o_0 - o_{-1} \otimes s_{-1} - o_{+1} \otimes s_{+1})$$



By applying the convolution theorem we obtain

$$F(i_0) \cdot F(s_0) = F(o_0 - o_{-1} \otimes s_{-1} - o_{+1} \otimes s_{+1})$$

and therefore

$$F(i_0) = F(o_0 - o_{-1} \otimes s_{-1} - o_{+1} \otimes s_{+1}) \cdot \frac{1}{F(s_0)}$$

Taking the inverse Fourier transform, F^{-1} , of both sides finally yields:

$$i_0 = F^{-1} \left[F(o_0 - o_{-1} \otimes s_{-1} - o_{+1} \otimes s_{+1}) \cdot \frac{1}{F(s_0)} \right]$$

Nearest neighbor (NN) deconvolution

With the stated assumptions, the in-focus light distribution i_o can be recovered (restored) from the equation:

$$i_o = (o_0 - o_{-1} \otimes s_{-1} - o_{+1} \otimes s_{+1}) \otimes F^{-1} \left(\frac{1}{F(s_0)} \right)$$

In practice, nearest neighbor deconvolution is performed using a modified form of the above equation:

$$i_o = (o_0 - c_{-1} o_{-1} \otimes s_{-1} - c_{+1} o_{+1} \otimes s_{+1}) \otimes F^{-1} \left(\frac{F^*(s_0)}{|F(s_0)|^2 + c_0} \right)$$

where c_{-1} , c_{+1} and c_0 are empirical factors and all PSFs are normalized.

Coefficients $c_{\pm 1}$ are used to limit errors caused by over-compensating out-of-focus contributions and their value falls generally in the range from 0.01 to 0.1.

$$F^{-1} \left(\frac{F^*(s_0)}{|F(s_0)|^2 + c_0} \right)$$

usually complex ≈ 0.045

c_0 is required to handle exceptions caused by the possible presence of zeros in $F(s_0)$; values for c_0 fall in the range from 0.045 to 0.050. Note that:

- Too large a value for c_0 causes loss of details and yields blurry images.
- Too small a value causes amplification of random noise into bright spots, rings, or patches.

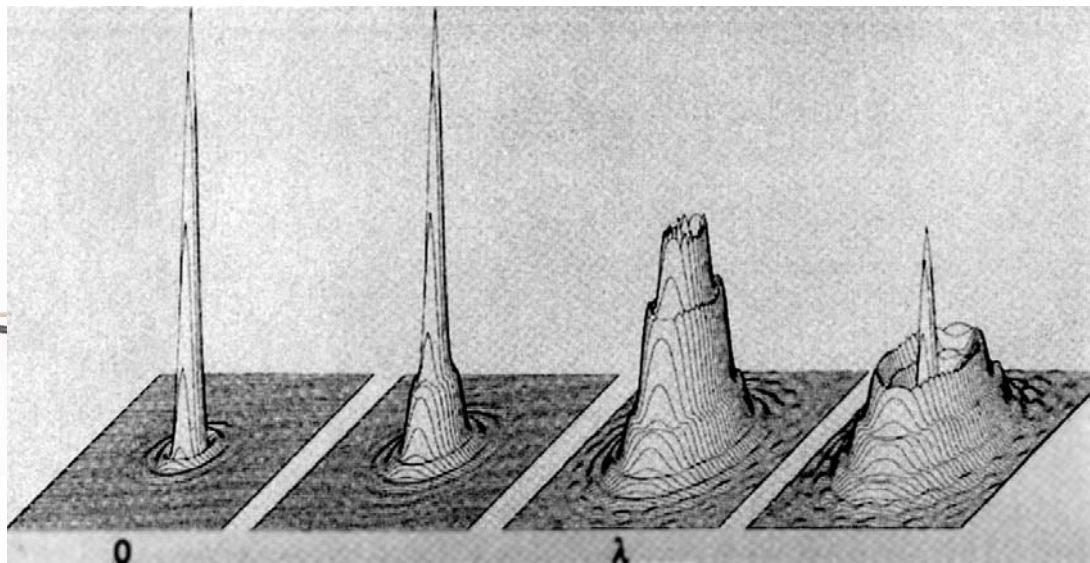
Multi-neighbour deconvolution

Relaxing condition 1 and generalizing to N neighbours yields the result:

$$i_0 = \left(o_0 - \sum_{j=1}^N (c_{-j} o_{-j} \otimes s_{-j} + c_{+j} o_{+j} \otimes s_{+j}) \right) \otimes F^{-1} \left(\frac{F^*(s_0)}{|F(s_0)|^2 + c_0} \right)$$

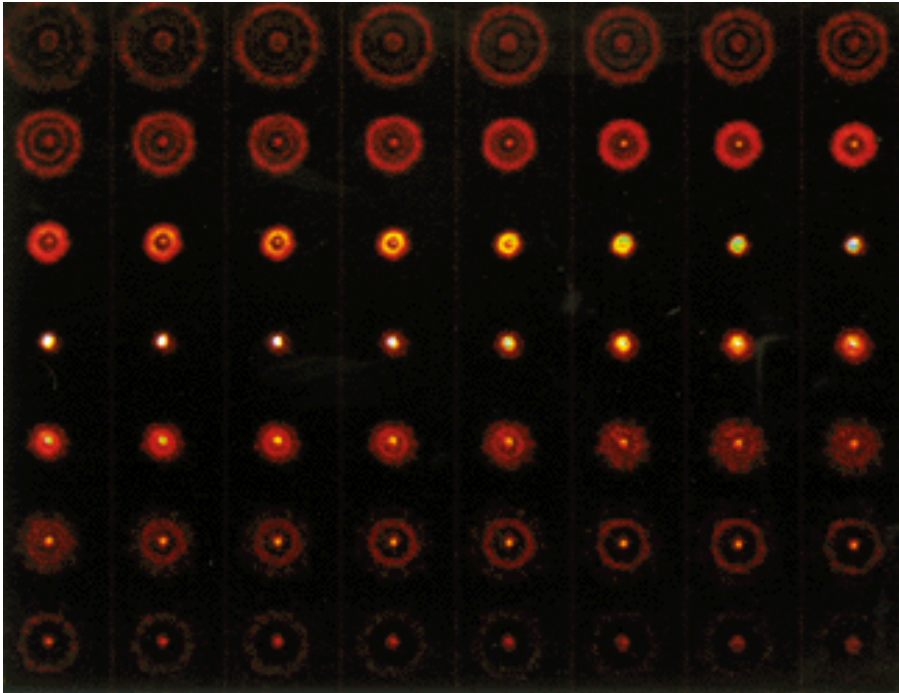
In summary, this procedure requires:

- in focus and out-of-focus image collection
- in focus and out-of-focus PSF measurement

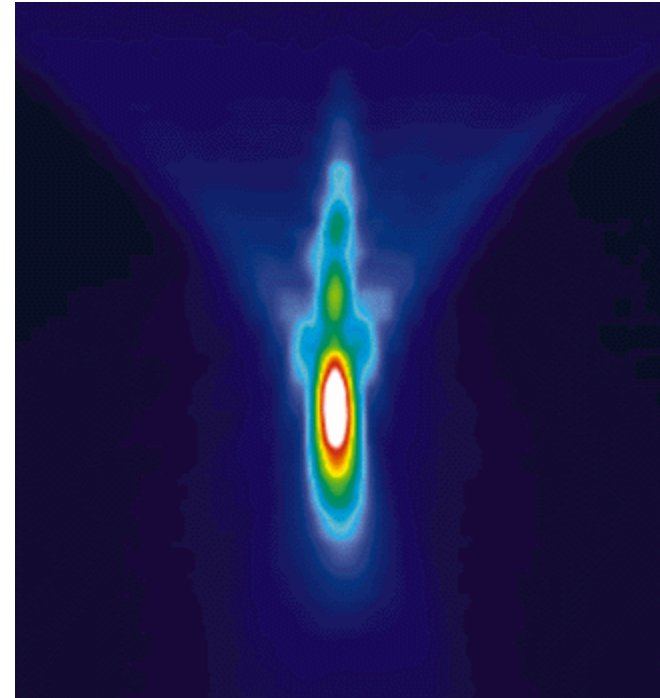


Deconvolution

Through-focus behaviour of point images



Serial focal sequence of fluorescence images of a 200 nm bead used to measure x - y sections of the 3D PSF at various distances above and below the focal plane



Meridional (y - z) section through the PSF. This pseudo-color image was generated electronically from the series of bead images shown at left.

The asymmetry in the axial direction is due to spherical aberration and is very common in imaging biological specimens. There is additional path length through a layer of water, glycerol or other mounting medium, which leads to increased spherical aberration.

Measuring the 3D PSF

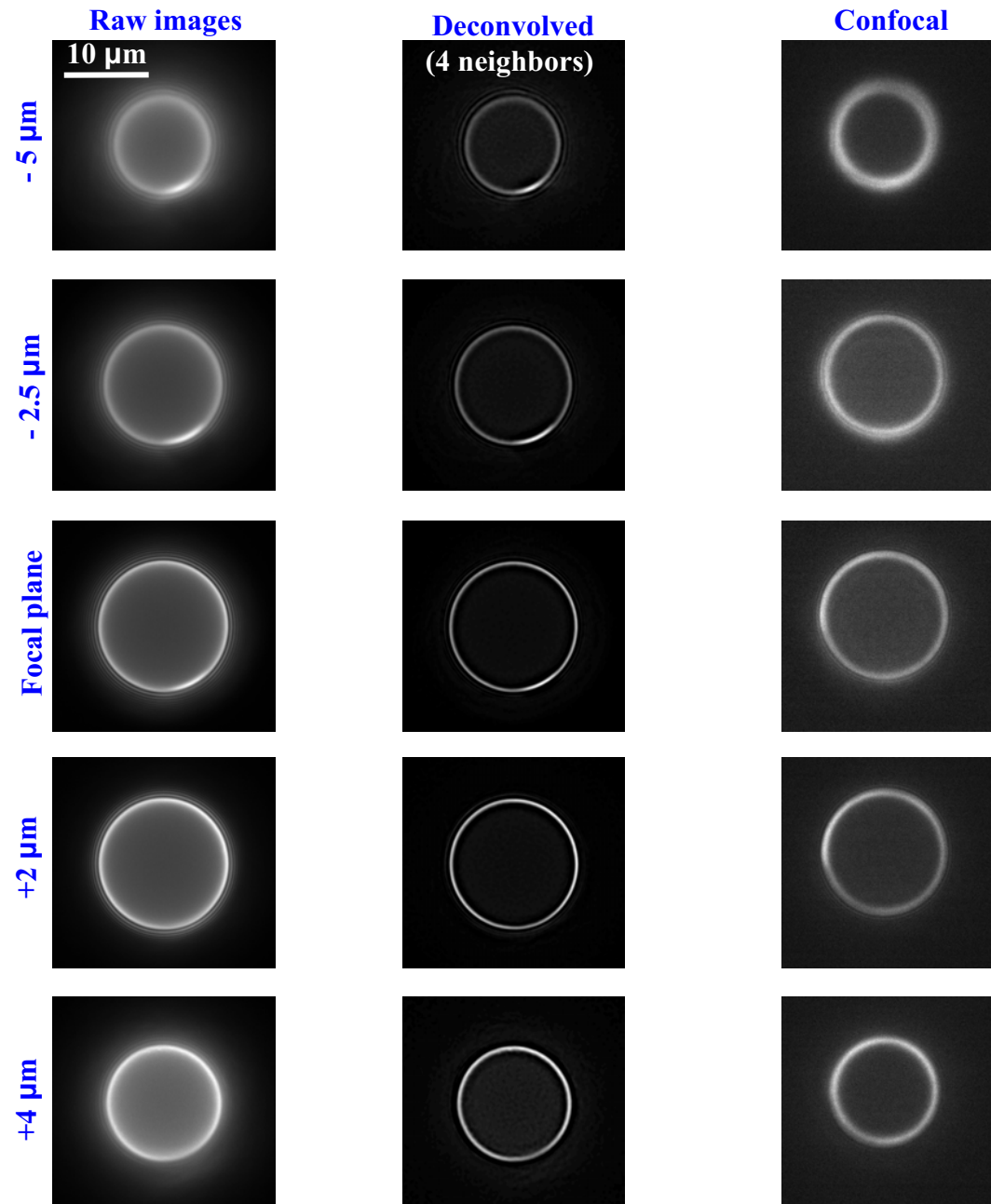
The 3D PSF must be measured on the same system used to acquire the images to be deconvolved. For fluorescence imaging, this process requires:

- **Embedding** sub-resolution fluorescent beads into the medium of interest. If this is cytoplasm, the beads can be incorporated by cell *electroporation*.
- **Setting the step** of the z -stack: Nyquist theorem.
- **Finding** the (closest approximation to) the focal plane; by definition, this is the plane where the lateral extent of the PSF is minimal and its peak value is maximal
- **Symmetrization**: in the absence of aberrations, the PSF has rotational symmetry around the optical axis; raw x - y PSF sections are made symmetric by a circular averaging procedure.
- **Normalization**: in an ideal widefield microscope, the total integrated intensity at each out-of-focus plane is constant.

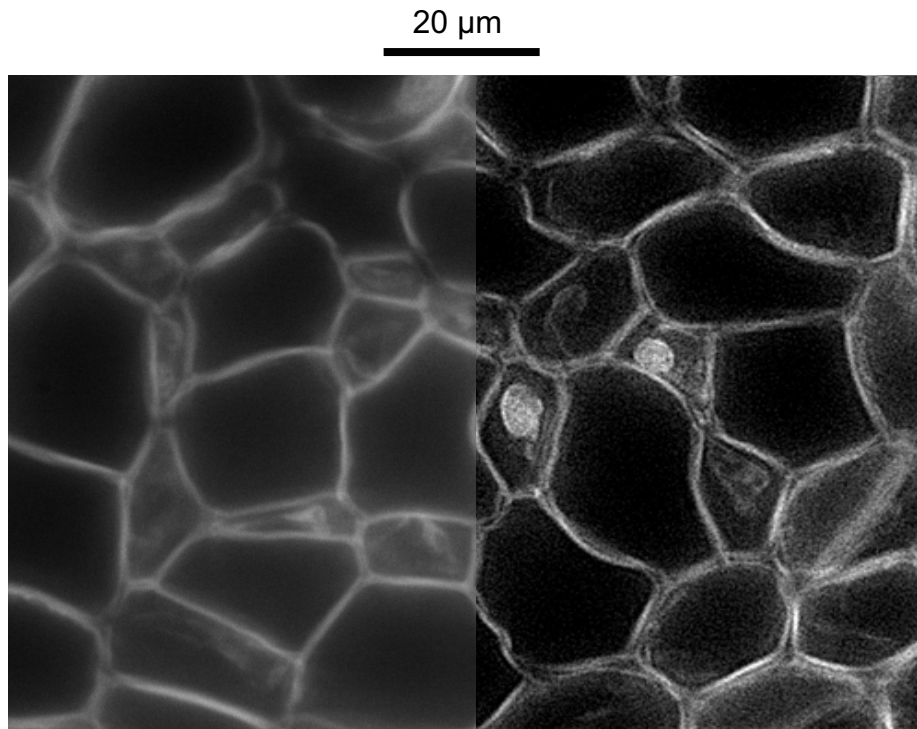
A typical 11×11 kernel

| | | | | | | | | | | |
|----|----|----|----|-----|-----|-----|----|----|----|----|
| 32 | 51 | 51 | 51 | 51 | 50 | 50 | 51 | 51 | 50 | 33 |
| 52 | 80 | 81 | 79 | 79 | 80 | 80 | 81 | 80 | 81 | 51 |
| 51 | 80 | 79 | 81 | 82 | 81 | 81 | 81 | 80 | 80 | 51 |
| 50 | 81 | 80 | 82 | 86 | 87 | 84 | 82 | 81 | 81 | 52 |
| 52 | 82 | 83 | 85 | 104 | 154 | 103 | 84 | 82 | 81 | 52 |
| 52 | 83 | 82 | 88 | 116 | 395 | 148 | 87 | 82 | 81 | 52 |
| 51 | 82 | 83 | 85 | 98 | 116 | 102 | 86 | 80 | 81 | 52 |
| 52 | 81 | 82 | 84 | 85 | 84 | 83 | 83 | 81 | 82 | 52 |
| 52 | 82 | 81 | 81 | 82 | 82 | 82 | 82 | 82 | 82 | 51 |
| 51 | 80 | 81 | 82 | 80 | 81 | 82 | 81 | 82 | 82 | 52 |
| 33 | 50 | 51 | 51 | 51 | 51 | 50 | 51 | 51 | 52 | 33 |

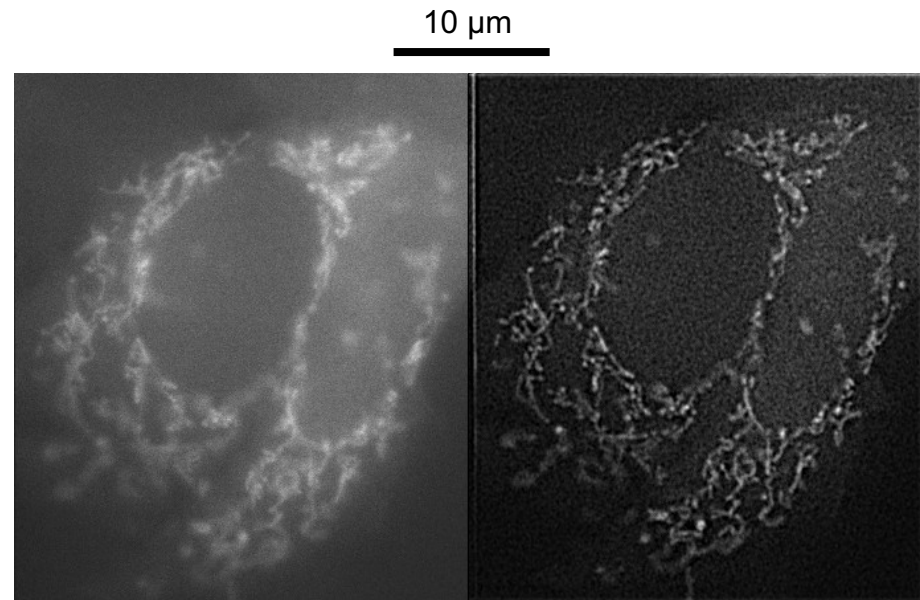
Algorithm validation: optical sections of a 15 μm test sphere



Application to biological specimens



Conventional (wide-field) fluorescence image of *Convallaria Rhizom* (*left*), deconvolved with the nearest neighbour algorithm (*right*).



Z-stack of mitochondria targeted with cameleon

NN deconvolution in real time: FPGA

One deconvolved image requires 3 consecutive images. However, the last one of a frame triplet is also the first one of the following triplet. Therefore deconvolved frames are generate at half the acquisition frame rate.

CCD camera target frame rate:

60 frames per second (fps), to obtain 30 fps of NN deconvolved images

CCD size:

512 × 512 pixels (binnig = 2×2 on a Mpixel sensor)

Reasonable kernel size:

11 × 11 pixels

Number of multiplications (and additions) per frame:

(512 × 512) × (11 × 11) = 31.7 M

At 60 fps:

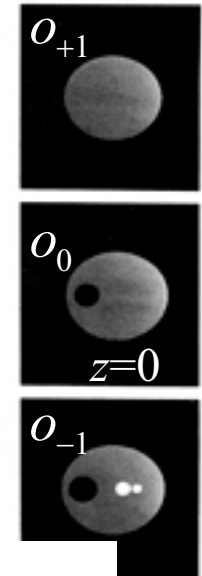
31.7 M × 60/s = 1.9 G/s

Computational parallelism is a must!

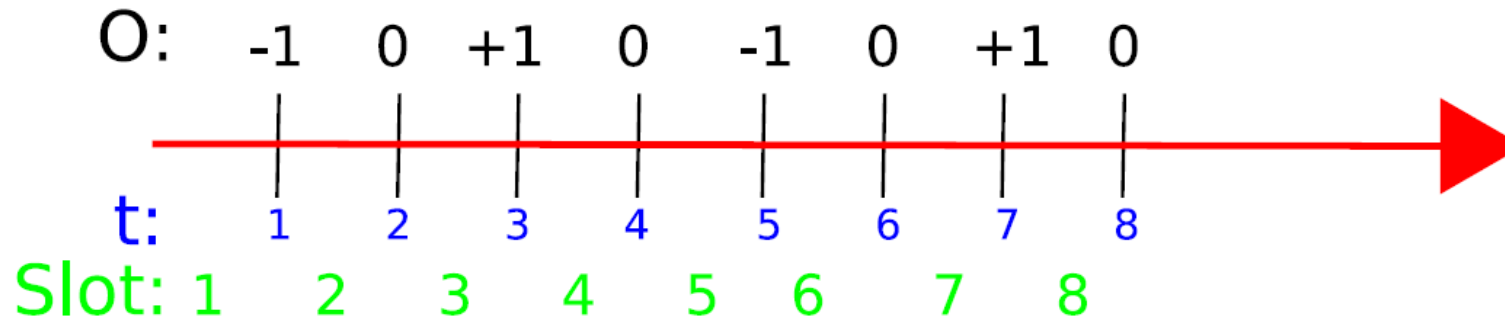
Breaking down the problem into time slots

$$i_0 = \left(\underbrace{o_0}_{\text{constant scalar}} - \underbrace{c_{-1} o_{-1}}_{\text{constant scalar}} \otimes \underbrace{s_{-1}}_{\text{constant scalar}} - \underbrace{c_{+1} o_{+1}}_{\text{constant scalar}} \otimes \underbrace{s_{+1}}_{\text{constant scalar}} \right) \otimes F^{-1} \left(\frac{F^*(s_0)}{|F(s_0)|^2 + c_0} \right)$$

constant matrix

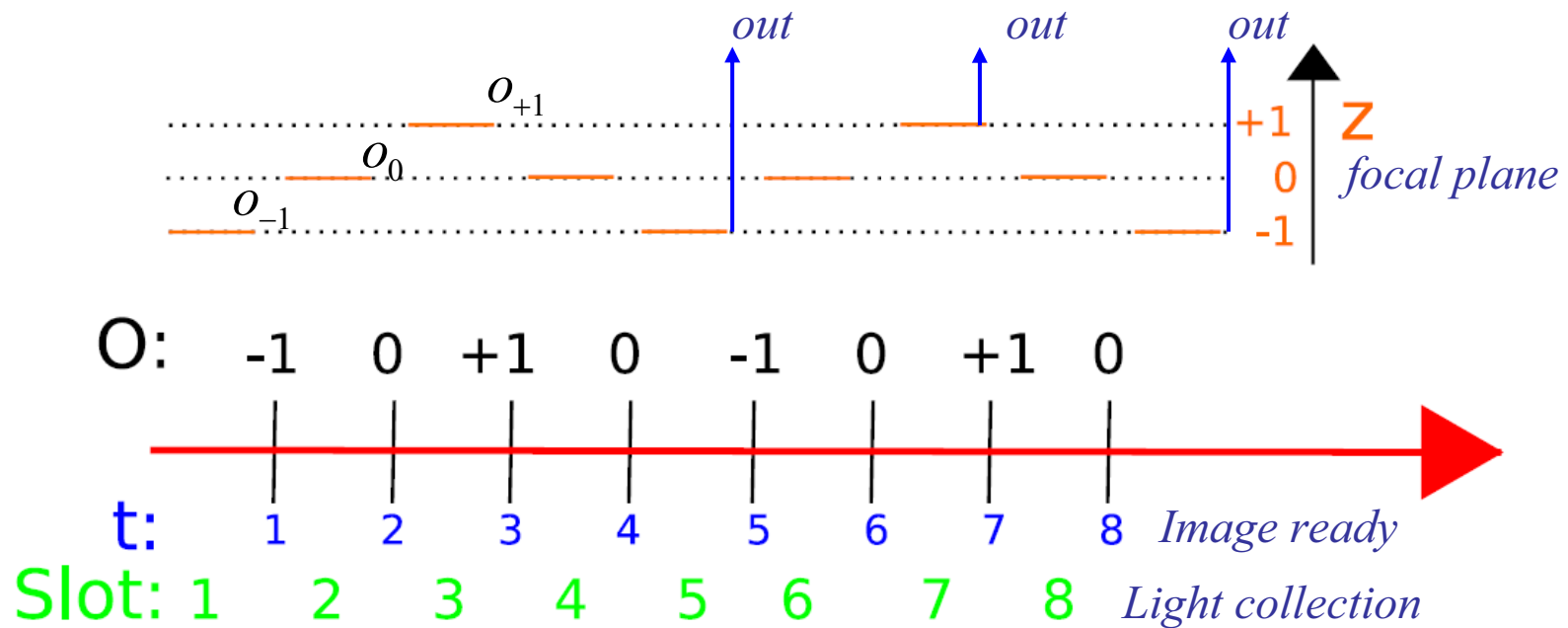


Frame exposure intervals




Overview of Slots 1, 2 and 3

- **Slot 1:** collect light to form image o_{-1}
- **Slot 2:** download image o_{-1} data while collecting light to form image o_0
- **Slot 3:** download image o_0 data while collecting light to form image o_{+1}
-



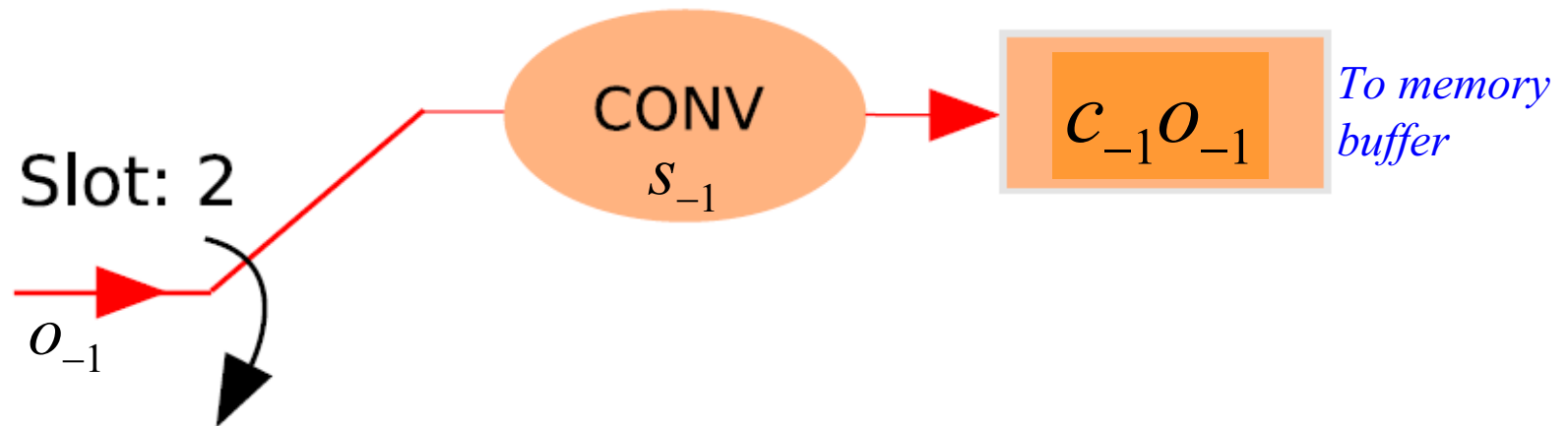
Slot 2 in detail

$$i_0 = \left(o_0 - \underbrace{c_{-1} o_{-1} \otimes s_{-1}}_{i_{-1}} - c_{+1} o_{+1} \otimes s_{+1} \right) \otimes F^{-1} \left(\frac{F^*(s_0)}{|F(s_0)|^2 + c_0} \right)$$


- **Collect light to form image o_0 ;**
- **in parallel, as o_{-1} data come through, compute**

$$i_{-1} = c_{-1} o_{-1} \otimes s_{-1}$$

- **store the result into a memory buffer.**

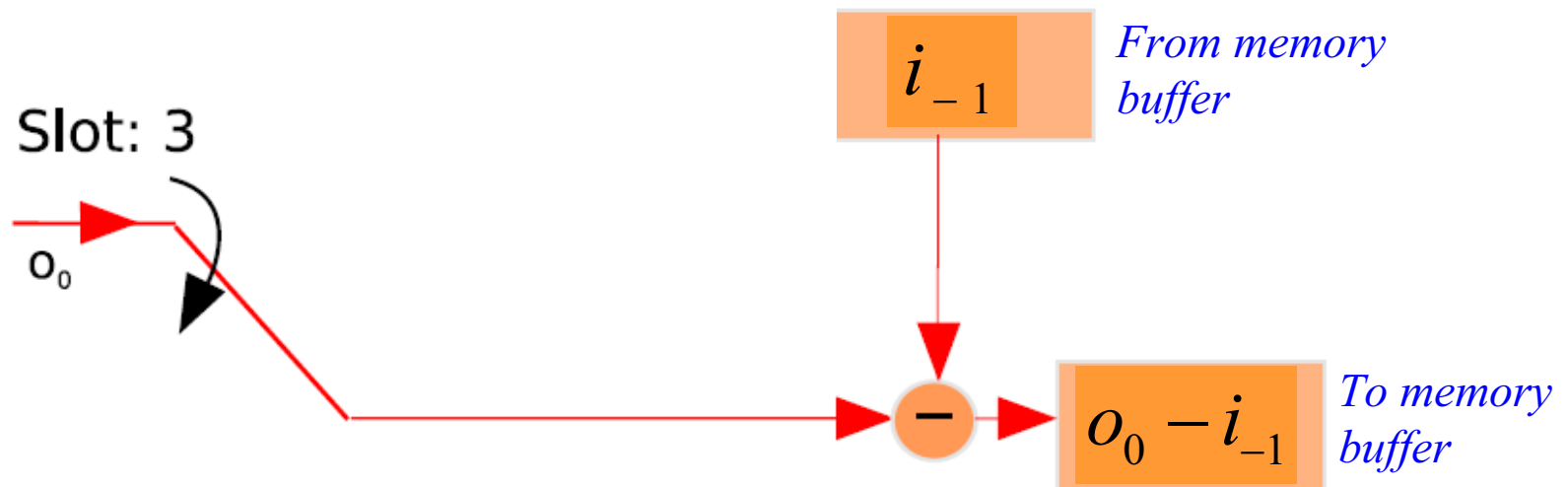


Slot 3 in detail

$$i_0 = \left(o_0 - \underbrace{c_{-1} o_{-1} \otimes s_{-1}}_{i_{-1}} - c_{+1} o_{+1} \otimes s_{+1} \right) \otimes F^{-1} \left(\frac{F^*(s_0)}{|F(s_0)|^2 + c_0} \right)$$

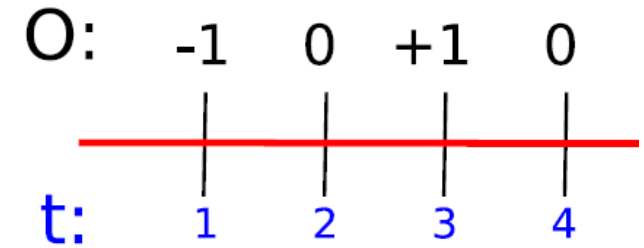
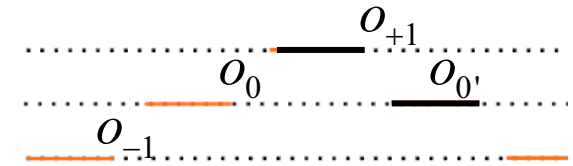
*Computed
in Slot 2*

- collect light to form image o_{+1} ;
- in parallel, as o_0 data come through, subtract the result (i_{-1}) obtained in Slot 2;
- store also this new result into a memory buffer.



Slot 4 in detail

$$i_0 = \left(o - c_{-1}o_{-1} \otimes s_{-1} - \underbrace{c_{+1}o_{+1} \otimes s_{+1}}_{i_{+1}} \right) \otimes F^{-1} \left(\frac{F^*(s_0)}{|F(s_0)|^2 + c_0} \right)$$

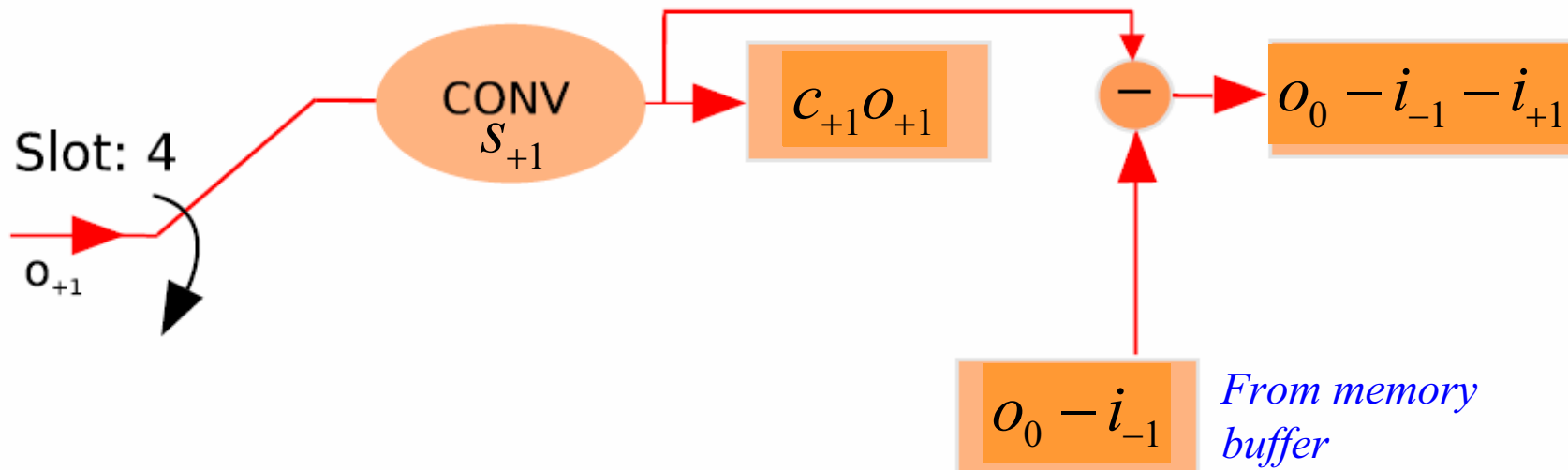


- collect light to form a new image o_0 ;
- as o_{+1} data from Slot 3 come through compute:

$$i_{+1} = c_{+1}o_{+1} \otimes s_{+1}$$

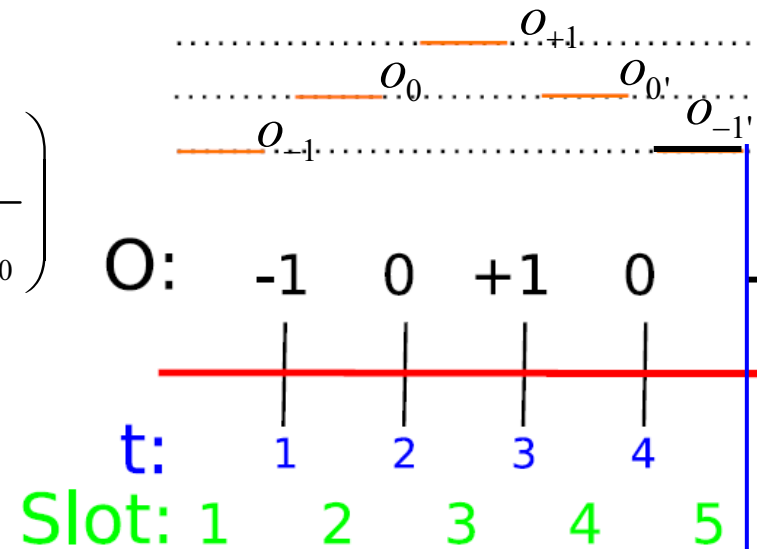
Slot: 1 2 3 4 5

- subtract this new result from the partial difference ($o_0 - i_{-1}$) obtained in Slot 3.



Slots 5 in detail

$$i_0 = \underbrace{(o - c_{-1}o_{-1} \otimes s_{-1} - c_{+1}o_{+1} \otimes s_{+1})}_{\text{Computed in Slot 4}} \otimes F^{-1} \left(\frac{F^*(s_0)}{|F(s_0)|^2 + c_0} \right)$$



- collect light to form a new image o_{-1} ,
- in parallel, convolve the result of Slot 4, that is

$$o_0 - i_{-1} - i_{+1}$$

with matrix

$$F^{-1} \left(\frac{F^*(s_0)}{|F(s_0)|^2 + c_0} \right)$$

(which must have been previously stored in memory)

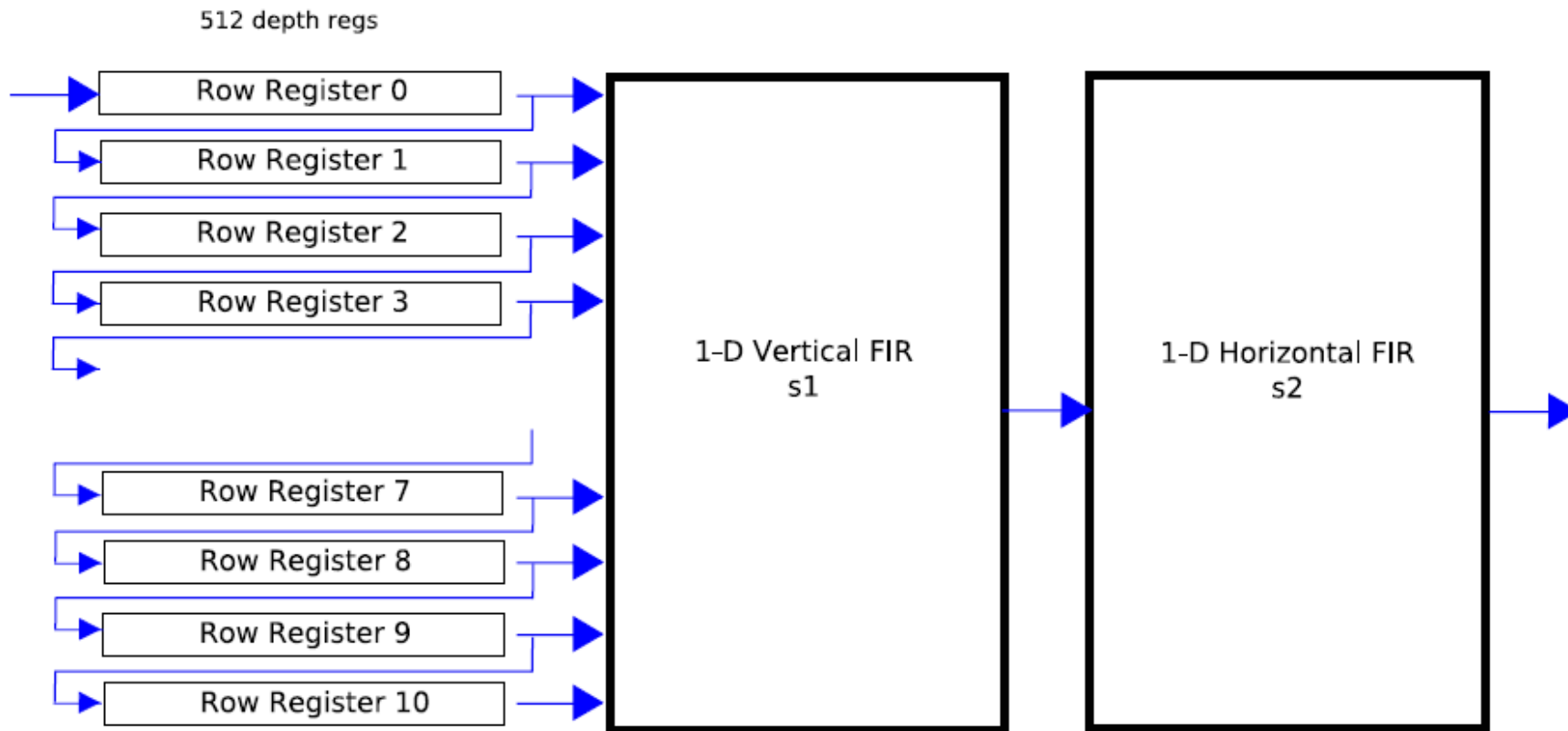
- the results is the first deconvolved image, which is sent to the host PC



FPGA example: convolution with a separable kernel

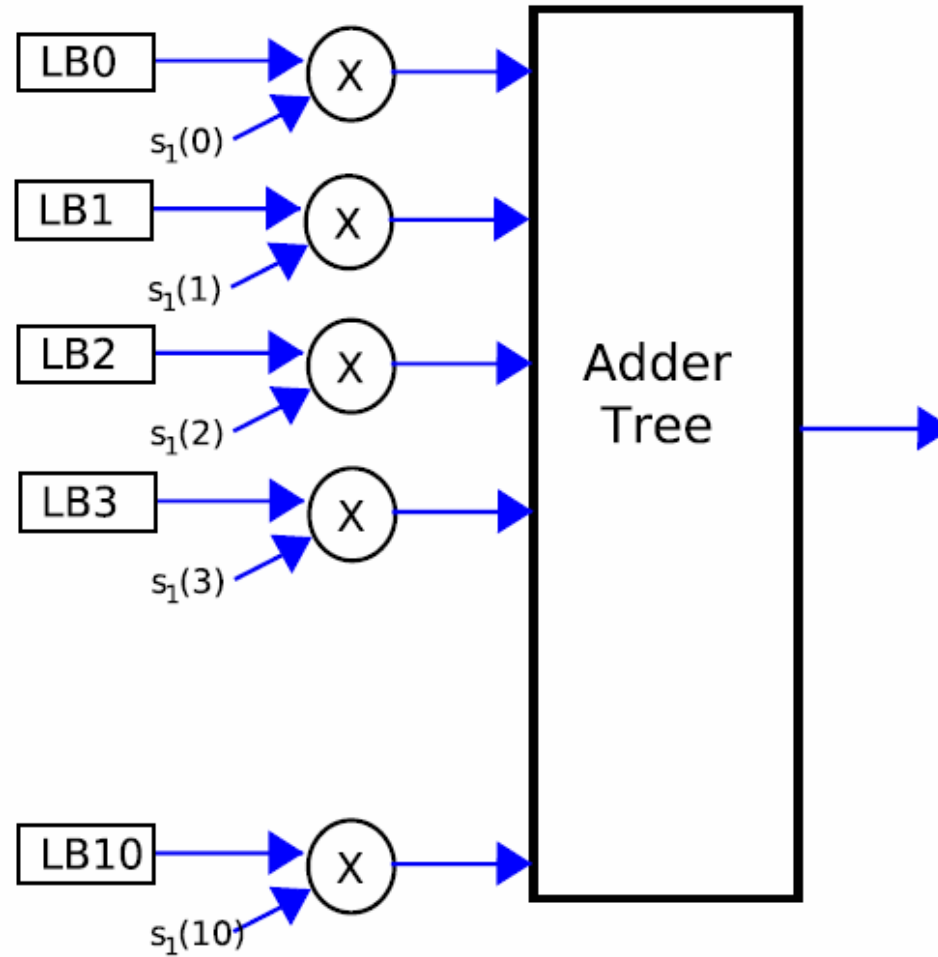
$$s(j, k) = s_1(j)s_2(k)$$

$$o(m, n) = \sum_{k=1}^{N_2} s_2(n-k) \sum_{j=1}^{N_1} i(j, k) s_1(m-j)$$



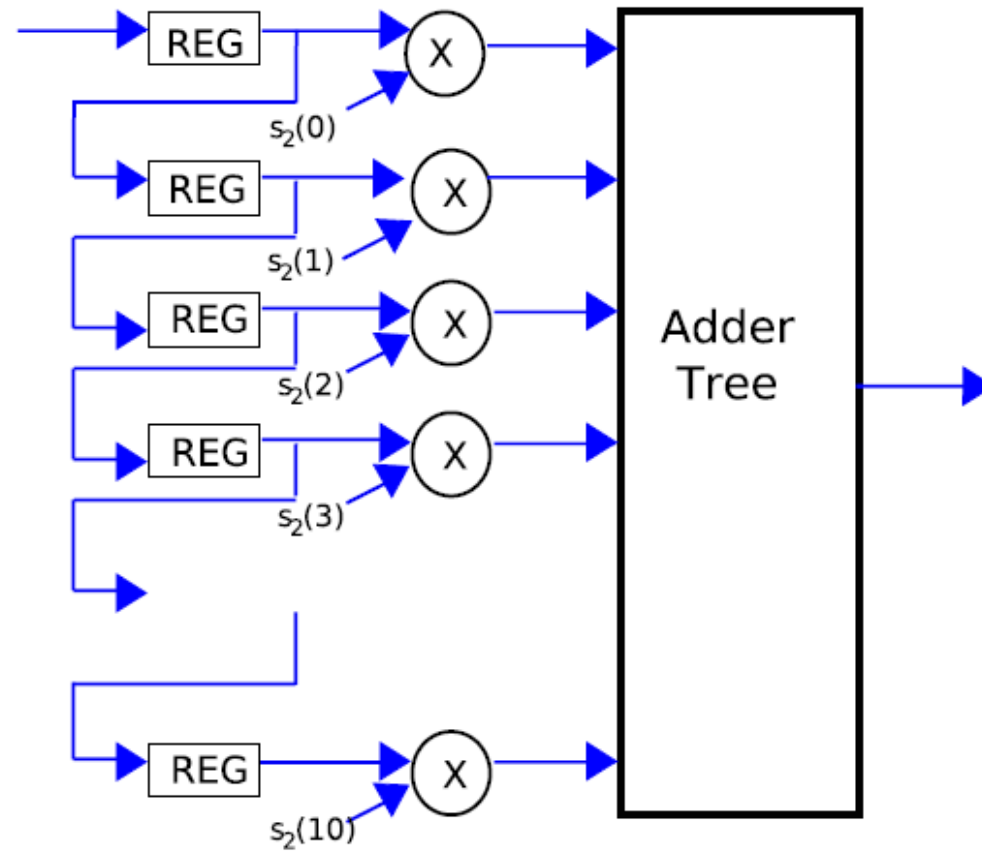
Vertical filter

Col pixels



This 1D filter has kernel s_7 and multiplies all pixels in a column of 11 pixels by the kernel coefficients, followed by the adder tree that sums up the results two by two.

Horizontal filter



This 1D filter has kernel s_2 and its inputs are delayed and organized in rows through a series of cascaded registers that reconstruct the spatial dependence.

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