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#### ICTP-IAEA Joint Workshop on Nuclear Data for Science and Technology: Medical Applications

30 September - 4 October, 2013

Novel Medical Radionuclides and Related Nuclear Data

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Lecture delivered during the Workshop on Nuclear Data for Science and Technology: Medical Applications, Abdus Salam ICTP, Trieste, Italy, 30 September to 4 October 2013



## **Topics**

- Introduction
- Non-standard positron emitters
  - production using low-energy reactions (Examples: <sup>64</sup>Cu, <sup>94m</sup>Tc, <sup>124</sup>I, etc.)
  - production via intermediate energy reactions (Examples: <sup>52</sup>Fe, <sup>73</sup>Se, <sup>124</sup>I, etc.)
- Novel therapeutic radionuclides (Examples: <sup>67</sup>Cu, <sup>186</sup>Re, <sup>225</sup>Ac, <sup>193m</sup>Pt, etc.)
- Conclusions

## New Directions in Development of Radiotracers for Nuclear Medicine



- Enhancing the yield, purity and specific activity of presently used radiotracers
- Development of new organ specific radiopharmaceuticals, especially using
  - <sup>99m</sup>Tc and <sup>123</sup>I for SPECT
  - <sup>18</sup>F and <sup>68</sup>Ga for PET
- Development of novel longer-lived positron emitters for
  - study of slow metabolic processes
  - improvement of radiation dosimetry
- Development of novel low-energy highly ionising radiation emitters for internal radiotherapy

This lecture deals with development of novel radionuclides

## **Radionuclide Development**



- Nuclear data
  - excitation functions and yield measurements
  - occasionally decay scheme investigations
- High current targetry
- Radiochemical separations
  - dry and wet methods of separation
  - enriched target recovery
- Quality control
- Imaging suitability
  - phantom measurements (PET, SPECT) to determine resolution, background correction, etc.

# This lecture concentrates on nuclear data and some production aspects.

# Novel Positron Emitters in Medicine

### Needs

- Study of slow metabolic processes, e.g. protein synthesis, cell proliferation, etc. (satellite concept)
- Analogue approach
  - Quantification of SPECT-radiopharmaceuticals
  - Therapy planning, exact dosimetry

### **Problems**

- Constraints on production yield and purity
- Imaging difficulties due to high energy positrons and  $\gamma$ -rays
- Demanding metal-chelate chemistry

## **Production Routes of 64Cu**



Nuclear process	Optimum energy range [MeV]	Thick target yield [MBq/µA·h]
<sup>64</sup> Ni(p,n) <sup>64</sup> Cu <sup>a)</sup>	12 → 8	304
<sup>64</sup> Ni(d,2n) <sup>64</sup> Cu <sup>a)</sup>	17 → 11	430
<sup>68</sup> Zn(p,αn) <sup>64</sup> Cu <sup>a)</sup>	$30 \rightarrow 21$ <sup>b)</sup>	116
<sup>66</sup> Zn(p,2pn) <sup>64</sup> Cu <sup>a)</sup>	$52 \rightarrow 37$	316
<sup>64</sup> Zn(d,2p) <sup>64</sup> Cu <sup>a)</sup>	20 → 10	27.1
<sup>66</sup> Zn(d,α) <sup>64</sup> Cu <sup>a)</sup>	13 → 5	13.8
<sup>nat</sup> Zn(d,x) <sup>64</sup> Cu	$25 \rightarrow 10^{\circ}$ c)	57.0

a) Using highly enriched target material. Low enrichment leads to impurities

- b) Below threshold of <sup>67</sup>Cu impurity via the <sup>68</sup>Zn(p,2p)<sup>67</sup>Cu reaction
- c) Below thresholds of <sup>61</sup>Cu and <sup>67</sup>Cu impurities via the <sup>64</sup>Zn(d,αn)<sup>61</sup>Cu and <sup>68</sup>Zn(d,2pn)<sup>67</sup>Cu reaction, respectively

Extensive studies performed at Brussels, Cape Town, Debrecen, Jülich and Segrate

For review cf. Aslam et al., RCA **97**, 669 (2009)

## Excitation Function of <sup>64</sup>Ni(p,n)<sup>64</sup>Cu Reaction





Yield: 304 MBq/µAh



### Radiochemical Separation of <sup>64</sup>Cu Produced via <sup>64</sup>Ni(p,n)-Process

(Szelecsenyi et al., ARI 44, 557 (1993).)

**Target:** 95% enriched <sup>64</sup>Ni electroplated on Au (thin target) **Irradiation:** 16 MeV p, 4 μA, 5 h **Separation:** 

- Irradiated target dissolved in conc. HCI
- Anion-exchange chromatography (Dowex 1x8)
- <sup>64</sup>Ni eluted with 10 M HCl, collected in 1 ml, and reused for electroplating
- Radiocopper separated from radiocobalt by elution with HCI of lower concentration

Yield of <sup>64</sup>Cu: 1 GBq Purity: > 98%

### **Role of Nuclear Data in Optimisation of a Production Route using Charged Particles**







## **Routes for Production of 124**

Nuclear	Energy range	Thick target	Impurity [%]		
reaction	[MeV]	yield of <sup>124</sup> l [MBq/µA·h]	123	<sup>125</sup>	126
<sup>124</sup> Te(d,2n)	14 → 10	17.5	-	1.7	-
<sup>124</sup> Te(p,n)	12 → 8	16	1.0	< 0.1	-
<sup>125</sup> Te(p,2n)	21 → 15	81	7.4	0.9	-
<sup>126</sup> Te(p,3n)	$38 \rightarrow 28$	222	148	1.0	1.0
<sup>nat</sup> Sb(α,xn)	22 → 13	1.02	890	13	16
<sup>121</sup> Sb(α,n)	22 → 13	2.1	895	< 0.2	< 0.2
<sup>nat</sup> Sb( <sup>3</sup> He,xn)	$35 \rightarrow 13$	0.95	3877	0.6	0.6

• All values calculated from excitation functions measured at Jülich

<sup>124</sup>Te(p,n) reaction gives the purest form of <sup>124</sup>I



### **Distillation of Radioiodine**



#### Distillation at 750 °C for 15 min

Batch yield : $480 \text{ MBq} (\approx 13 \text{ mCi})^{124}\text{I}$ Radionuclidic purity (%): $^{124}\text{I} (99), ^{123}\text{I} (<1), ^{125}\text{I} (0.1)$ Radiochemical purity:> 98 % iodideChemical impurity:Te (<1µg)</td>

### **Formation of Isomeric States**



Level depends mainly on type of reaction

#### Example : <sup>94</sup>Mo(p,n)<sup>94m,g</sup>Tc



#### <sup>94g</sup>Tc impurity in <sup>94m</sup>Tc

<sup>94</sup> Mo(p,n)	: 6%
<sup>93</sup> Nb( <sup>3</sup> He,2n)	: 25%
<sup>92</sup> Mo(α,pn)	: 30%

# Fundamental investigations mandatory

Qaim et al., NMB **27**, 323 (2000).



### Novel Positron Emitters for Medical Applications Produced via Low-Energy Reactions (E ≤ 20 MeV)

Nuclide	Major production route	Energy range [MeV]	Application
<sup>55</sup> Co (17.6 h)	<sup>58</sup> Ni(p,α) <sup>54</sup> Fe(d,n)	$\begin{array}{rrrrrrrrrrrrrrrrrrrrrrrrrrrrrrrrrrrr$	Tumour imaging; neuronal Ca marker
<sup>64</sup> Cu (12.7 h)	<sup>64</sup> Ni(p,n)	14 → 9	Radioimmunotherapy
<sup>66</sup> Ga (9.4 h)	<sup>66</sup> Zn(p,n)	13 → 8	Quantification of SPECT
<sup>72</sup> As (26.0 h)	<sup>nat</sup> Ge(p,xn)	<b>18</b> → <b>8</b>	Tumour localisation; immuno-PET
<sup>76</sup> Br (16.0 h)	<sup>76</sup> Se(p,n)	<b>15</b> → 8	Radioimmunotherapy
<sup>82m</sup> Rb (6.2 h)	<sup>82</sup> Kr(p,n)	$14 \rightarrow 10$	Cardiology
<sup>86</sup> Y (14.7 h)	<sup>86</sup> Sr(p,n)	$14 \rightarrow 10$	Therapy planning
<sup>89</sup> Zr (78.4 h)	<sup>89</sup> Y(p,n)	$14 \rightarrow 10$	Immuno-PET
<sup>94m</sup> Tc (52 min)	<sup>94</sup> Mo(p,n)	<b>13</b> → 8	Quantification of SPECT
<sup>120</sup> I (1.3 h)	<sup>120</sup> Te(p,n)	$13.5 \rightarrow 12$	Iodopharmaceuticals
<sup>124</sup> I (4.2 d)	<sup>124</sup> Te(p,n)	12 → 8	Tumour targeting; dosimetry



### Intermediate Energy Nuclear Reactions in Production of Novel Positron Emitters

#### Problems

- Availability of high intensity cyclotrons
- Large number of competing nuclear reactions (higher significance of nuclear data)
- Targetry more challenging
- Radiochemical separations more demanding (impurity level may be higher)

#### Advantages

- Generally higher yield
- Occasionally high isotopic enrichment of target not very crucial

#### Considerable research and development work is called for.

## Nuclear Data for Production of <sup>73</sup>Se via <sup>75</sup>As(p,3n)-Process



#### **Excitation Functions**



- Optimum energy range:  $E_p = 40 \rightarrow 30 \text{ MeV}$
- Yield : 1.4 GBq/µA·h
- <sup>72,75</sup>Se impurity: < 0.2 %

The higher the projectile energy, the more are competing reactions.

Mushtaq et al., ARI **39**, 1085 (1988).



### Production of some Novel Positron Emitters via Intermediate Energy Reactions ( E > 20 MeV)

Nuclide	Production route	Energy range [MeV]	Theor. yield [MBq/μAh]	Radionuclidic impurity (%)
<sup>52</sup> Fe (8.3 h)	<sup>55</sup> Mn(p,4n)	100 → 60	22	<sup>55</sup> Fe (< 2)
<sup>55</sup> Co (17.6 h)	<sup>56</sup> Fe(p,2n)	$38 \rightarrow 14$	163	<sup>56</sup> Co (1.6)
<sup>64</sup> Cu (12.7 h)	<sup>68</sup> Zn(p,αn)	$30 \rightarrow 21$	116	<sup>67</sup> Cu (< 0.5)
<sup>73</sup> Se (7.1 h)	<sup>75</sup> As(p,3n)	$40 \rightarrow 30$	1400	<sup>72,75</sup> Se (<0.2)
<sup>75</sup> Br (1.6 h)	<sup>76</sup> Se(p,2n) <sup>75</sup> As( <sup>3</sup> He,3n)	$\begin{array}{ccc} 24 & \rightarrow 20 \\ 36 & \rightarrow 25 \end{array}$	1200 278	<sup>76</sup> Br (2) <sup>76</sup> Br (1.7)
<sup>83</sup> Sr (32.4 h)	<sup>85</sup> Rb(p,3n)	$37 \rightarrow 30$	160	<sup>85</sup> Sr (0.2)
<sup>124</sup> I (4.2 d)	<sup>125</sup> Te(p,2n) <sup>126</sup> Te(p,3n)	$\begin{array}{ccc} 22 & \rightarrow 15 \\ 36 & \rightarrow 26 \end{array}$	93 190	<sup>125</sup> I (0.7) <sup>125,126</sup> I (~1.5)

• High intensity intermediate energy cyclotrons are very beneficial.

• Several other potentially useful positron emitters could also be produced.



### Production of Novel Positron Emitters via Generator Systems

Parent nuclide (T <sub>1/2</sub> )	Daughter nuclide (T <sub>1/2</sub> )	Production method of parent	Energy range [MeV]	Theor. yield of parent [MBq/μAh]
<sup>44</sup> Ti (60.4 a) <sup>a</sup>	<sup>44</sup> Sc (3.9 h)	<sup>45</sup> Sc(p,2n)	32 → 18	~ 3·10 <sup>-3</sup>
<sup>52</sup> Fe (8.3 h) <sup>b</sup>	<sup>52m</sup> Mn (21 min)	<sup>55</sup> Mn(p,4n)	100 → 60	22
<sup>62</sup> Zn (9.1 h) <sup>b</sup>	<sup>62</sup> Cu (9.7 min)	<sup>nat</sup> Cu(p,xn)	30 → 18	230
<sup>72</sup> Se (8.5 d)	<sup>72</sup> As (26.0 h)	<sup>75</sup> As(p,4n)	$45 \rightarrow 35$	8
<sup>122</sup> Xe (20.1 h) <sup>b</sup>	<sup>122</sup> I (3.6 min)	<sup>127</sup> I(p,6n) <sup>124</sup> Xe(p,3n)	$\begin{array}{ccc} 65 & \rightarrow 43 \\ 43 & \rightarrow 35 \end{array}$	230 500
<sup>140</sup> Nd (3.4 d) <sup>c</sup>	<sup>140</sup> Pr (3.4 min)	<sup>141</sup> Pr(p,2n) <sup>nat</sup> Ce( <sup>3</sup> He,xn)	$\begin{array}{l} 30 \rightarrow 15 \\ 35 \rightarrow 20 \end{array}$	210 12

- a)  $T_{\frac{1}{2}}$  of parent too long
- b)  $T_{\frac{1}{2}}$  of parent rather short
- c) In-vivo generator system



### Production of Novel Positron Emitters via α-Particle Induced Reactions

Nuclide (T <sub>1/2</sub> )	Production route	Energy range [MeV]	Theor. yield [MBq/μAh]	Radionuclidic impurity (%)
<sup>30</sup> P (2.5 min) <sup>a</sup>	<sup>27</sup> Al(α,n)	28 → 10	740	-
<sup>38</sup> K (7.6 min) <sup>a</sup>	<sup>35</sup> Cl(α,n)	22 → 7	270	-
<sup>73</sup> Se (7.1 h) <sup>b</sup>	<sup>70</sup> Ge(α,n)	<b>28</b> → <b>13</b>	126	<sup>72,73</sup> Se (0.5)
<sup>82</sup> Sr (25.3 d) <sup>b</sup>	<sup>82</sup> Kr(α,4n)	60 → 20	~ 3	<sup>85</sup> Sr (120)

- a) Produced exclusively via the  $\alpha$ -particle induced reaction.
- b) Applicable if intermediate energy proton beam not available; yield is, however, considerably smaller than via the (p,xn)-process.



### Development Work Related to Therapeutic Radionuclides

### Aims

- Enhance the yield, purity and specific activity of presently used radionuclides
- Development of novel therapeutic radionuclides
- Improve internal radiation dosimetry

### **New Trends**

 Low-range high-intensity radiation emitters (α-particles, low-energy electrons, X-rays)



Reaction  ${}^{68}$ Zn(p,2p) ${}^{67}$ Cu at  $E_p = 70 \rightarrow 30$  MeV most promising, but needs an intermediate energy accelerator.



### **Rhenium-186** ( $T_{\frac{1}{2}}$ = 3.7 d; $E_{\beta}$ - = 1070 keV; $I_{\beta}$ - = 92.5 %)

#### **Evaluated Data**



Results from three nuclear model calculational codes (EMPIRE, STAPRE, TALYS) are consistent.





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 Production of <sup>225</sup>Ac in GBq quantities is possible and technology is being developed.

## **Pt-193m** ( $T_{\frac{1}{2}}$ = 4.33 d; Auger electrons ~ 33 per decay)

### High-spin isomer

**Production Method**:  $\alpha$ -particles on enriched <sup>192</sup>Os

#### **Excitation Function**





## Actinium-225 Production via <sup>232</sup>Th(p,x)-Process



Data measurements: Ermolaev et al., RCA **100**, 223 (2012) Weidner et al., ARI **70**, 2602 (2012)

#### **Yield and Purity**



All methods of <sup>225</sup>Ac production need further development.



### Production of some Potentially Useful Therapeutic Radionuclides using Intermediate Energy Multiple Particle Cyclotrons

Radionuclide (T <sub>1/2</sub> )	Radiation emitted	Production route	Energy range (MeV)
<sup>67</sup> Cu (2.6 d)	β <sup>-</sup>	<sup>68</sup> Zn(p,2p)	$80 \rightarrow 50$
<sup>77</sup> Br (2.4 d)	Auger electrons	<sup>75</sup> As(α,2n)	35  ightarrow 15
<sup>117m</sup> Sn (13.6 d)	Conversion electrons Auger electrons	<sup>116</sup> Cd(α,3n)	$40 \rightarrow 25$
<sup>131</sup> Cs (9.7 d)	Auger electrons	<sup>133</sup> Cs(p,3n) <sup>131</sup> Ba <b>→</b> <sup>131</sup> Cs	$40 \rightarrow 25$
<sup>153</sup> Sm (1.9 d)	β-	<sup>150</sup> Nd(α,n)	$30 \rightarrow 15$
<sup>193m</sup> Pt (4.3 d)	Conversion electrons Auger electrons	<sup>192</sup> Os(α,3n)	$38 \rightarrow 25$
<sup>211</sup> At (7.2 h)	α	<sup>209</sup> Bi(α,2n)	$30 \rightarrow 20$
<sup>225</sup> Ac (10.0 d)	α	<sup>226</sup> Ra(p,2n)	30 → 18

Increasing use of cyclotrons in production of therapeutic radionuclides



### Conclusions

- There is constant need of development of novel radionuclides. New demands are related to longer lived non-standard positron emitters and low-energy highly ionising radiation emitters for internal radiotherapy.
- Development work involves both nuclear data research and technological innovation; interdisciplinary approach is vital.



## Conclusions (cont'd)

- Small-sized cyclotrons are conveniently used for production of several novel positron emitters, e.g. <sup>64</sup>Cu, <sup>86</sup>Y, <sup>94m</sup>Tc, <sup>124</sup>I, etc.
   Purity of product is high; yield is, however, rather low.
- High intensity intermediate energy cyclotrons have great potential for extending the list of novel positron emitters and therapeutic radionuclides.
- The α-particle beam possesses some advantages regarding production of therapeutic radionuclides.

### Combination of interesting science and useful technology