Relative dosimetry: output factors, profiles, penumbra and depth functions

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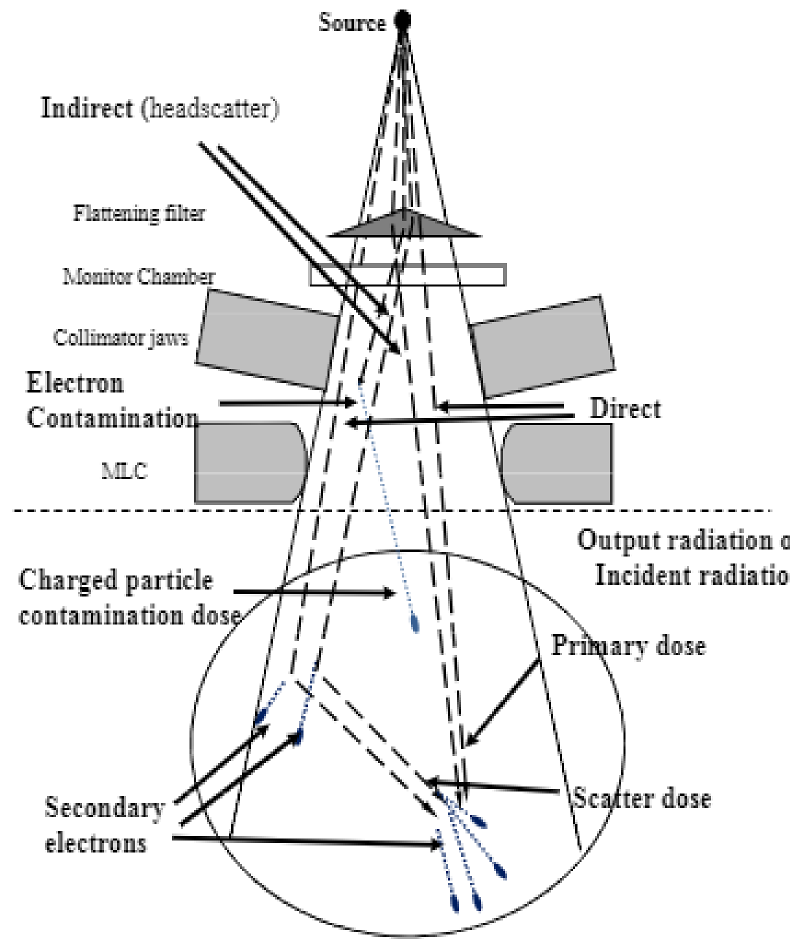
Introduction

The dose deposition in a patient is a very complicated process.

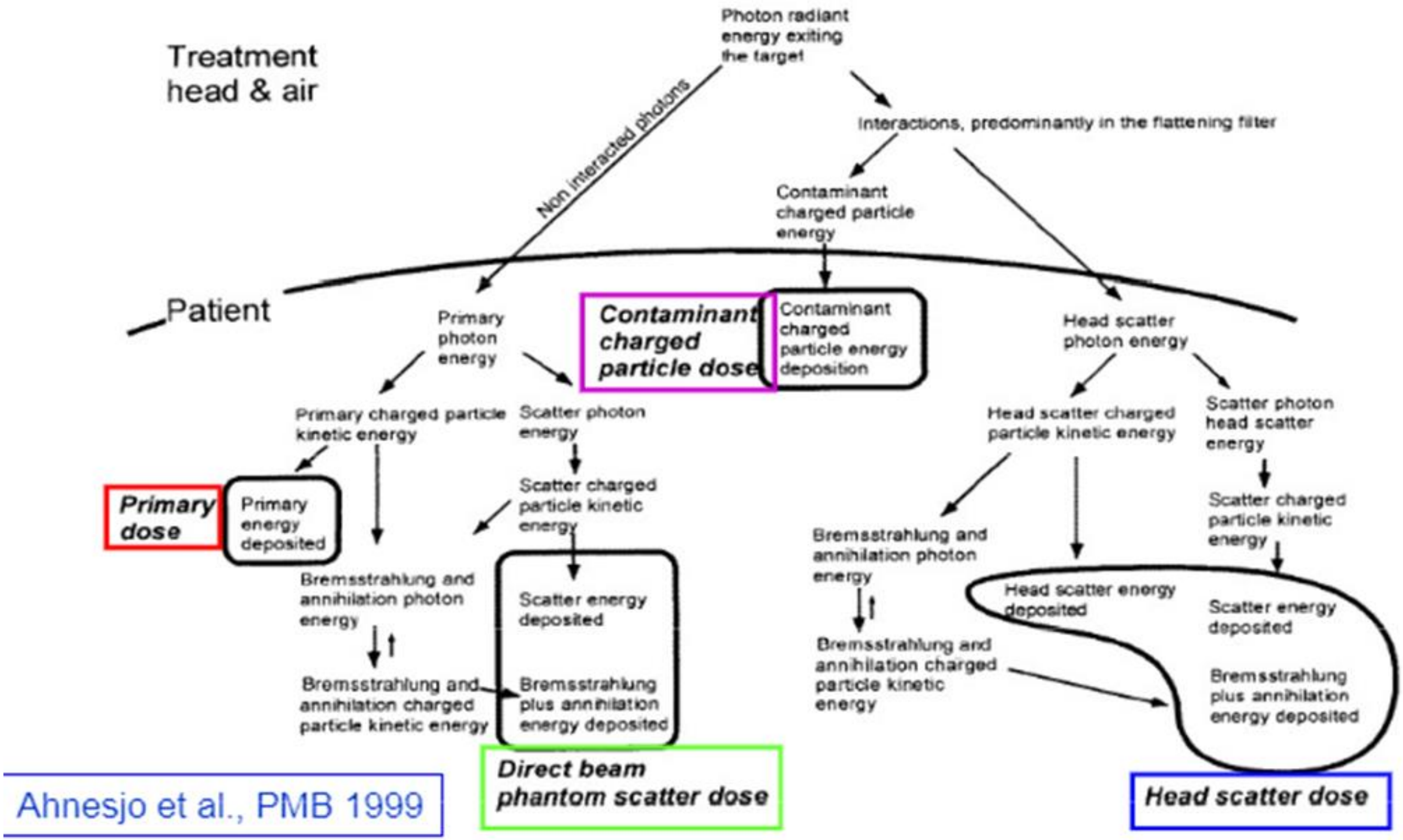
It's must take in account the ***attenuation*** and ***scattering*** of the photon beam inside a large and various volume.

Data on dose distribution in patients is derived from measurements in *tissue-equivalent-phantoms* large enough to provide full scatter conditions.

Several empirical functions are used to link the dose at any arbitrary point inside the patient/phantom to the known dose at the reference point in a phantom.



Introduction



Dosimetric functions

Dosimetric functions are measured in tissue equivalent phantoms with suitable radiation detectors.

Dosimetric functions are determined for a specific set of reference conditions:

- ***Depth z***
- ***Field Size***
- ***Source-Surface Distance*** *(SSD) or* ***Source-Axis Distance*** *(SAD)*

There are two types of data :

1) **scanned data**
2) **non-scanned data or point dose data**

Scanned beam data collection is carried out with a scanning *water phantom*; typically, a plastic tank filled with water to a level deep enough to allow central axis PDD and profile measurements to a depth of 40 cm.

Point dose data can be measured in a *solid phantom* or in a *water phantom*.

Dosimetric data

- ✓ ***Central axis depth dose at standard SSD set-up:***
  - *PDD*
- ✓ ***Central axis depth dose at standard SAD set-up:***
  - *Tissue Air Ratio (TAR)*
  - *Tissue Phantom Ratio (TPR)*
  - *Tissue Maximum Ratio (TMR)*
- ✓ ***Total scatter factor S_{cp}***
- ✓ ***In-air output ratio S_c***
- ✓ ***Phantom scatter factor S_p***
- ✓ ***Beam profiles, penumbra and off axis factors***

Phantoms

Water phantom closely approximates the radiation absorption and scattering properties of muscle and soft tissues.

Main dosimetrical data are measured in water but for particular conditions it's not possible and solid water-equivalent phantom were developed.

The electron density $\boldsymbol{\rho_e}$ of material must be equal to water $\boldsymbol{\rho_e}$ **:**

$$\rho_e = \rho_m N_A (Z/A)$$

TABLE II. Physical characteristics of commerically avialable water equivalent materilas. NA: Nuclear Associates, NY; Radiation Product Design, Albertsville, MN; RMI. Radiation Measurements, Inc., Middleton, WI; CIRS: Computerized Imaging Reference Systems, Inc. Norfolk, VA.

			$(\mu_{en}/\rho)^{water}_{med}$			
Material, manufacturer	Color	Density (kg/m^3)	6 MV	10 MV	15 MV	18 MV
Polystyrene, NA, RPD	Opaque	1050	1.035	1.037	1.049	1.059
Acrylic/PMMA, RPD	Clear	1185	1.031	1.033	1.040	1.044
Solid water, RMI	Maroon	1030	1.032	1.039	1.049	1.052
Plastic water, CIRS	Lavender	1012	1.032	1.031	1.030	1.030
White water-RW-3, NA	White	1045	1.035	1.036	1.049	1.056

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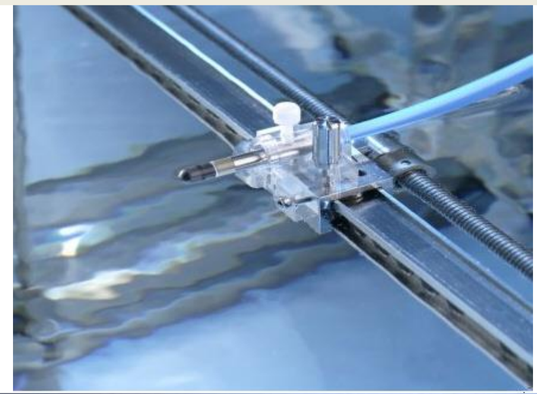
Water Phantom

To perform isodose measurement in water with different type of ionization chamber, diodes.

Software dedicated to evaluate parameters of beams



Water Phantom

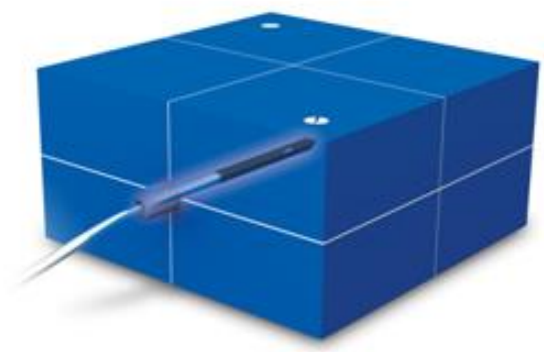
The size of the water tank should be large enough:

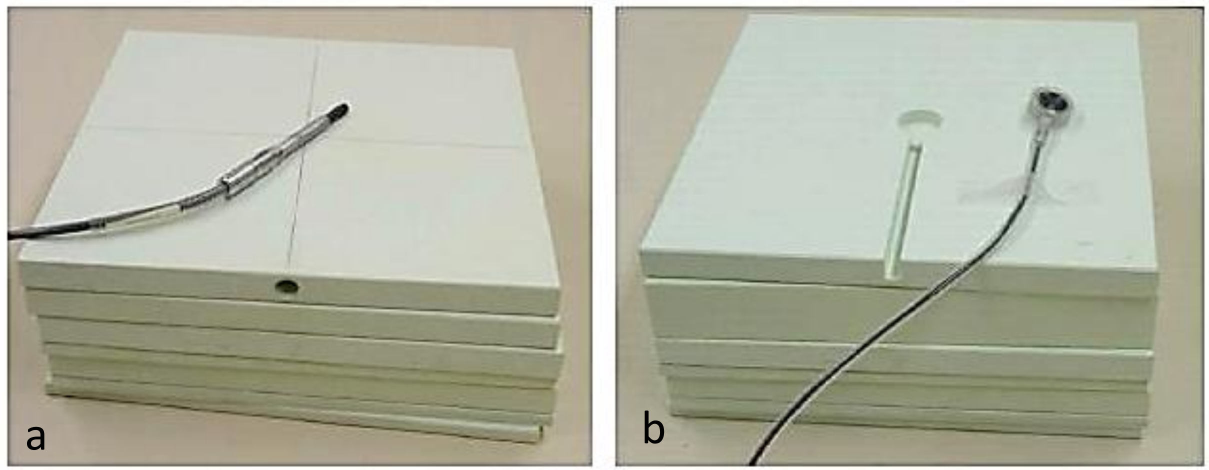
- ✓ to allow scanning of beam profiles up to the largest field size required (e.g., for *photon beams*, 40x40 cm^2 with sufficient lateral buildup 5 cm and overscan distance)

- ✓ to allow larger lateral scans and diagonal profiles for the largest field size and at a depth of 40 cm for modeling as required by some planning systems

to determine the appropriate size of the scanning tank, the overscan and the beam divergence at 40 cm depth should be considered.

Solid water-water equivalent Phantom





Water equivalent phantom with (a) Farmer-type ion chamber and (b) parallel-plate chamber

The **solid plate phantom (PMMA)** may be used for dosimetry measurements in photon and electron beams, based on the relation between ionization chamber reading in plastic and water in the user beam with different types of ionization chambers.

Percent depth dose PDD

For indirectly ionizing radiations, energy is imparted to matter in a **two step process**:

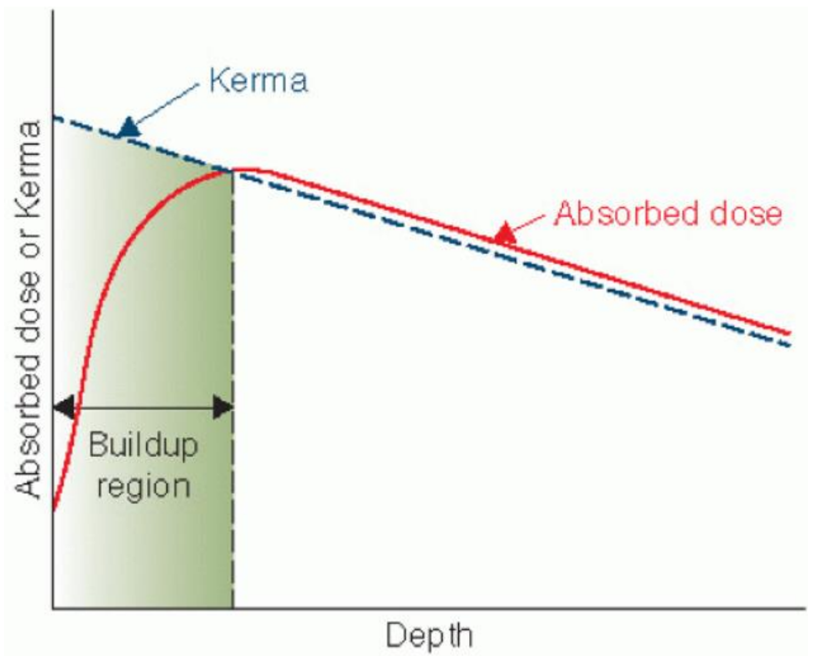
1) the indirectly ionizing radiation transfers energy as kinetic energy to secondary charged particles (***kerma***).
2) These charged particles transfer some of their kinetic energy to the medium (***absorbed dose***) and lose some of their energy in the form of radiative losses.

Kerma (**kinetic energy released per unit mass**) is defined as the mean energy transferred from the indirectly ionizing radiation to charged particles (electrons) in the medium per unit mass dm:

$$K = \frac{d\bar{E}_{tr}}{dm}$$

The ***absorbed dose D*** is defined as the mean energy **ε** imparted by ionizing radiation to matter of mass **dm** in a finite volume **V** by:

$$D = \frac{d\bar{\varepsilon}}{dm}$$



Percent depth dose PDD

Photon beam attenuation is governed by:

- ***inverse square law***
- ***exponential attenuation***
- ***scattering component***.

$$\boxed{\boldsymbol{PDD(z, A, f, h\nu) \propto \left(\frac{f+zmax}{f+z}\right)^2 \,.\, e^{-\mu_{eff}(z-zmax)} \,.\, K_s}}$$

Percent Depth Dose uniquely varies with depth due to attenuation, with SSD due to inverse square law, and with field size due to scattering effect.

The dose at point Q in the patient consists in two component:

primary component *and* ***scatter component***

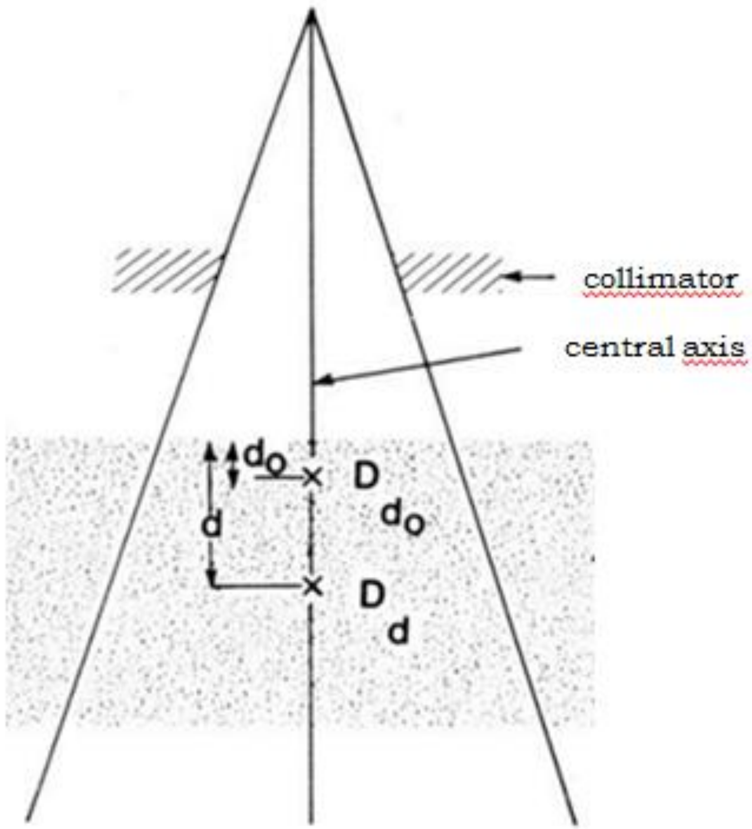
- The ***primary component*** is the photon contribution to the dose at point Q that arrives directly from the source.
- The ***scatter dose*** is delivered by photons produced through Compton scattering in the patient, machine collimator, flattening filter or air.

Percent depth dose PDD

The ***percentage depth dose*** is defined as the quotient of the absorbed dose at any depth **d** to the absorbed dose at a fixed reference depth $\mathbf{d_0}$ along the central axis of the beam:

$$P = \frac{D_d}{D_{d0}} \times 100$$

For high energies the reference dose is taken at the position of the **peak absorbed dose**



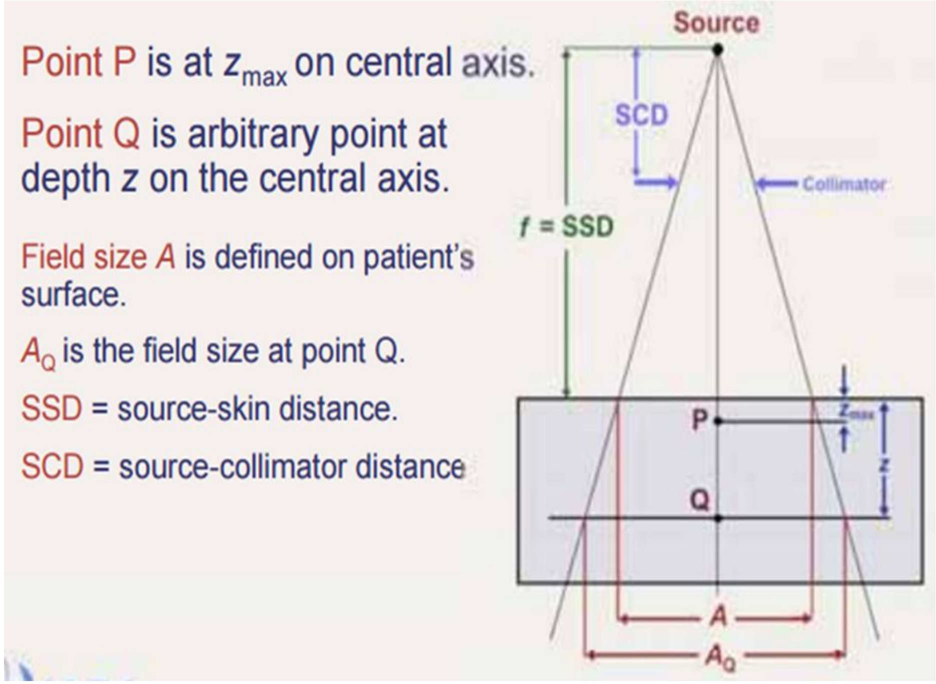
Percent depth dose PDD

As the beam is incident on a phantom (as on a patient) the absorbed dose varies with depth.

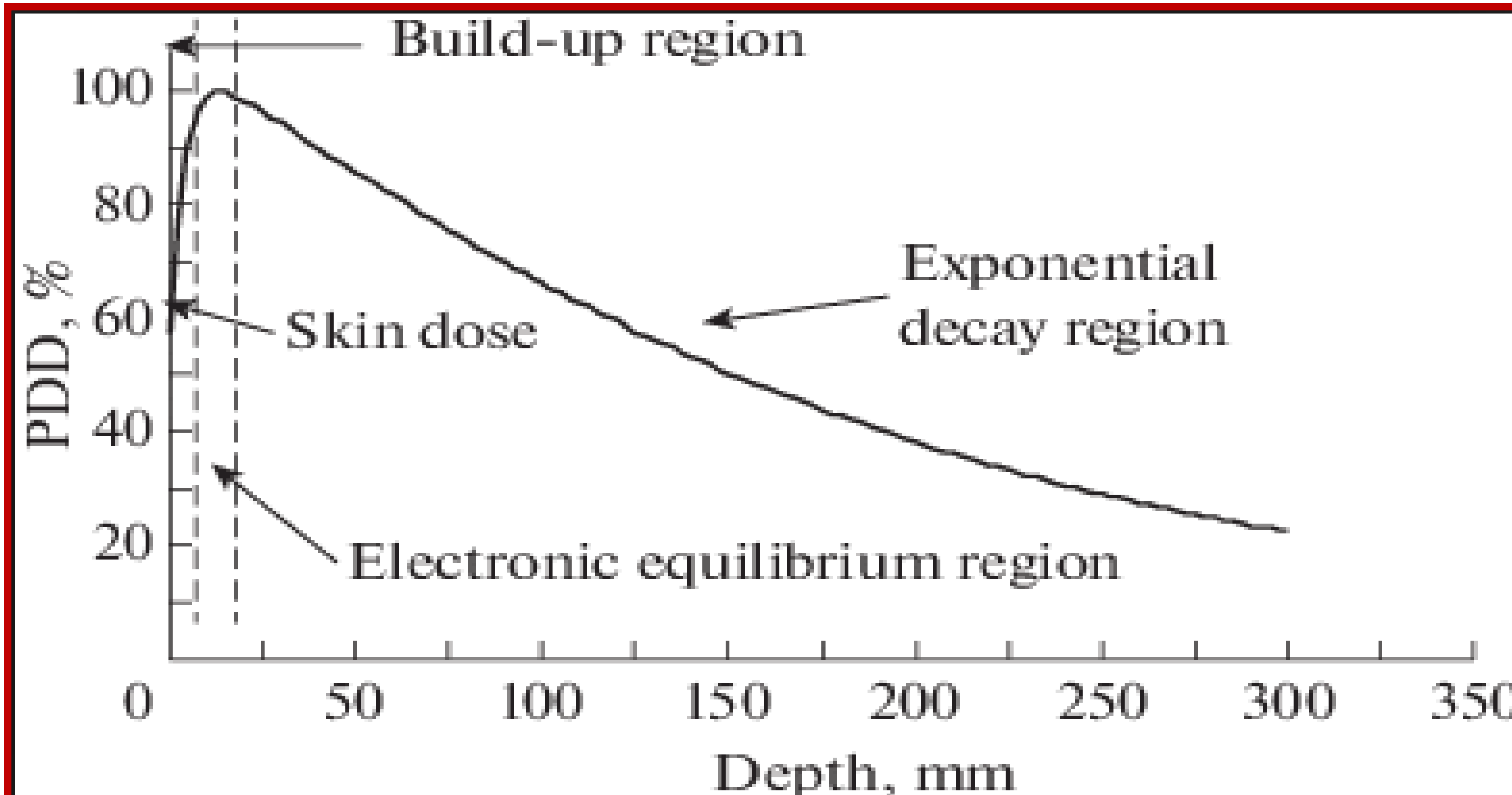
This variation depends on many condition:

- ✓ ***beam energy (hν)***
- ✓ ***Depth (z)***
- ✓ ***field size (A)***
- ✓ ***distance from source (SSD)***
- ✓ ***beam collimation system.***

$$PDD\,(z, A, f, h\nu) = \frac{D_Q}{D_P} \times 100$$



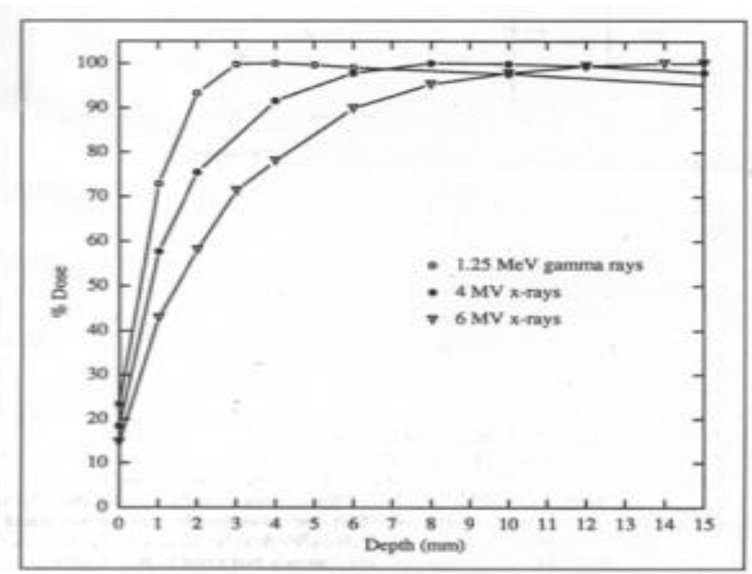
Percent depth dose PDD: dependence on depth

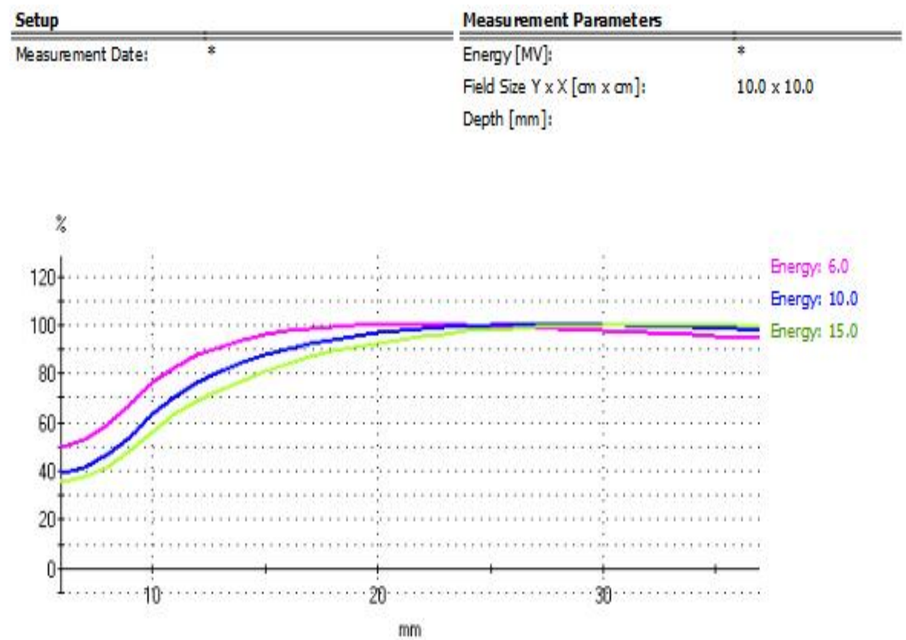


build-up region

Dose build-up region: dose region between the surface and depth $z = z_{max}$
Its depth is related to the long range of energetic secondary charged particles

The depth of dose maximum z_{max} beneath the patient's surface depends on the beam energy and beam field size.





Surface Dose

The ***surface dose:***

- is generally much lower than the maximum dose at a depth z_{max}
- depends on beam energy and field size
- decreases as photon beam energy increases
- increases with field size

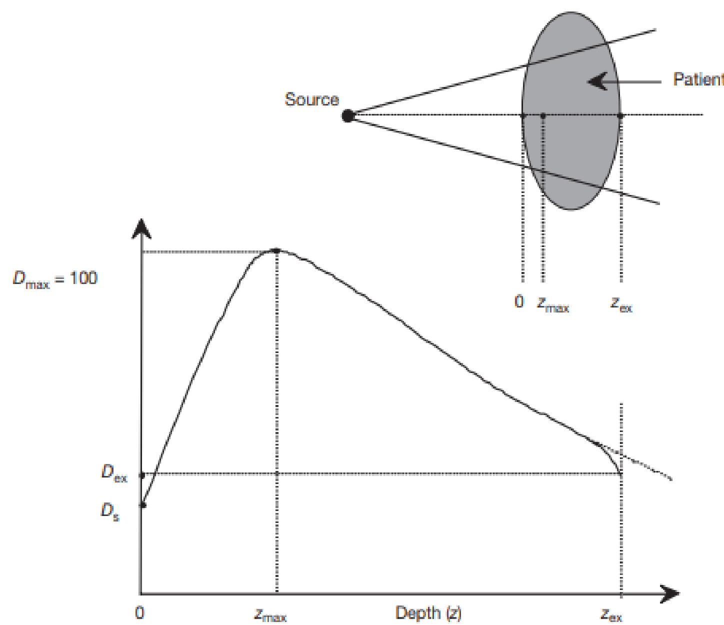
The low surface dose compared to the maximum dose is referred to as the <u>skin sparing effect</u>

Contributions to the surface-dose:

(1) Photons scattered from the collimators, flattening filter and air;

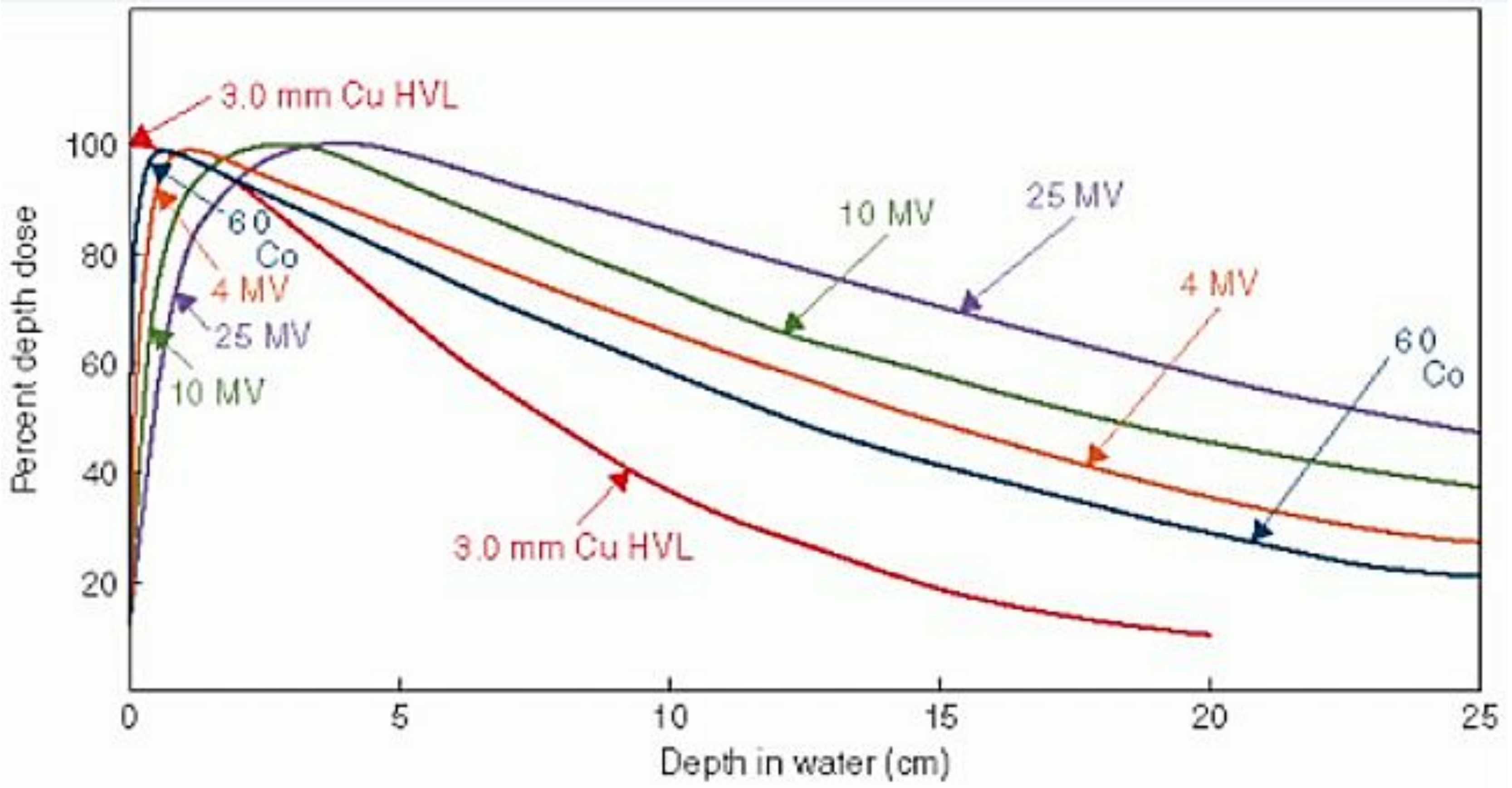
(2) Photons backscattered from the patient;

(3) High-energy electrons produced by photon interactions in air and any shielding structures close to the patient.

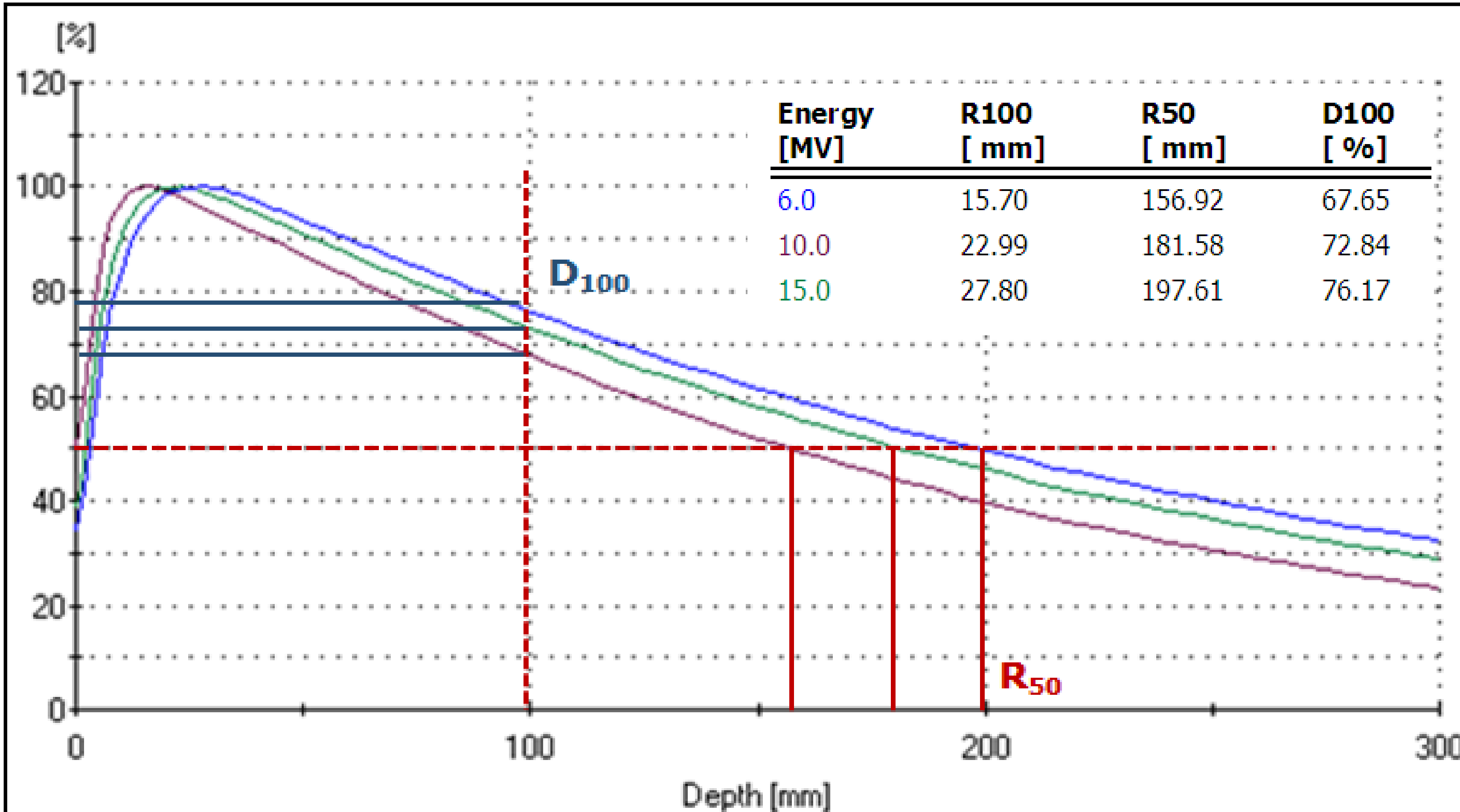


PDD dependence on energy

- The percentage depth dose increases with beam energy
- Higher energy have greater penetrating power



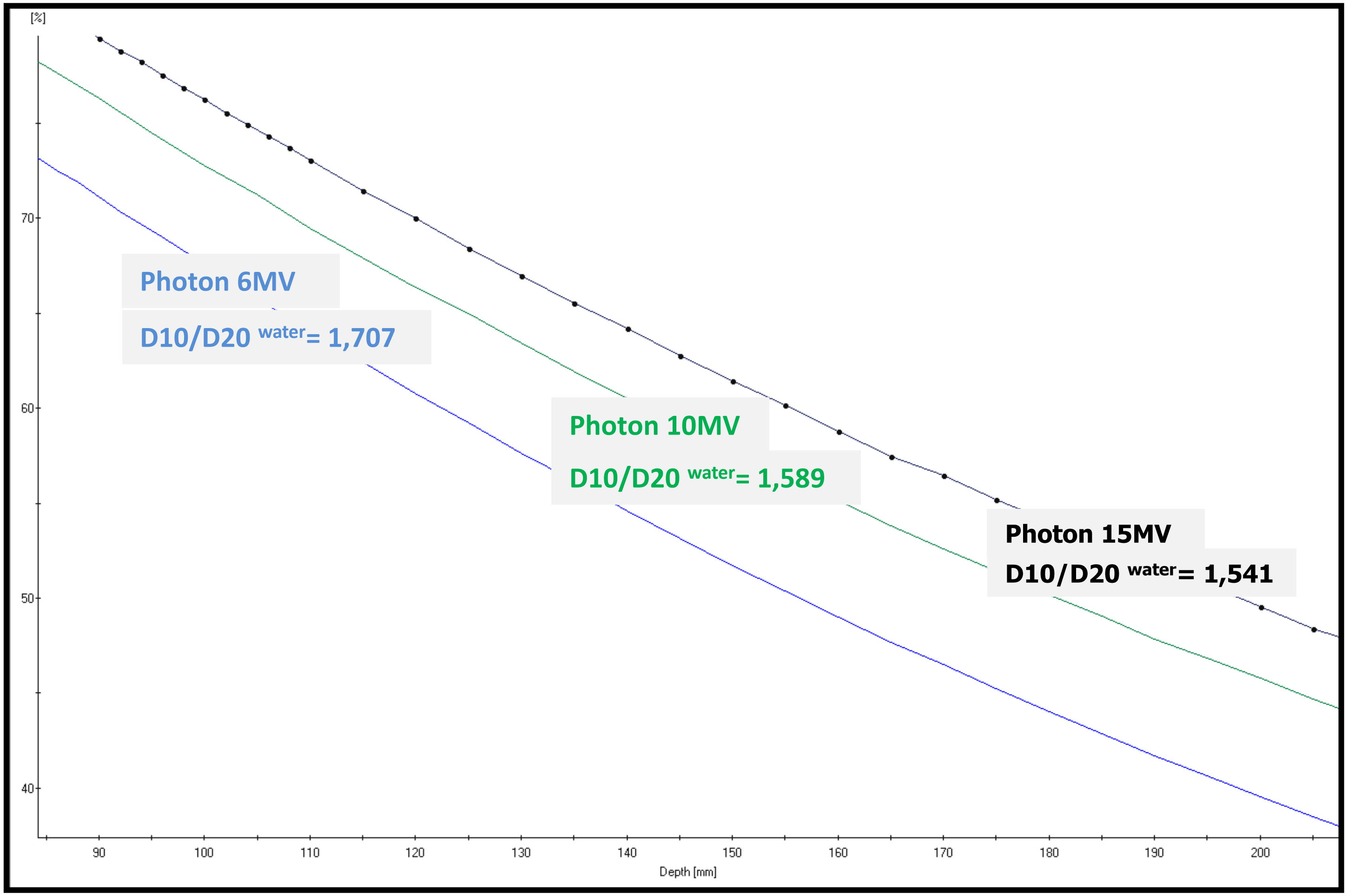
PDD dependence on energy



Energy [MV]	R100 [mm]	R50 [mm]	D100 [%]
6.0	15.70	156.92	67.65
10.0	22.99	181.58	72.84
15.0	27.80	197.61	76.17

Trieste measuraments

PDD dependence on energy



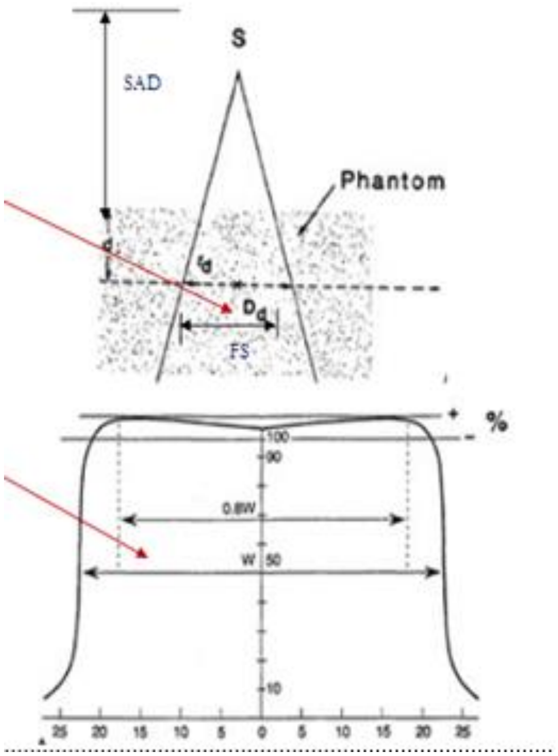
PDD dependence on field size

Geometrical field size

it's defined as the projection on a plane perpendicular to the beam axis of the distal end of the collimator as seen from the front center of the source.

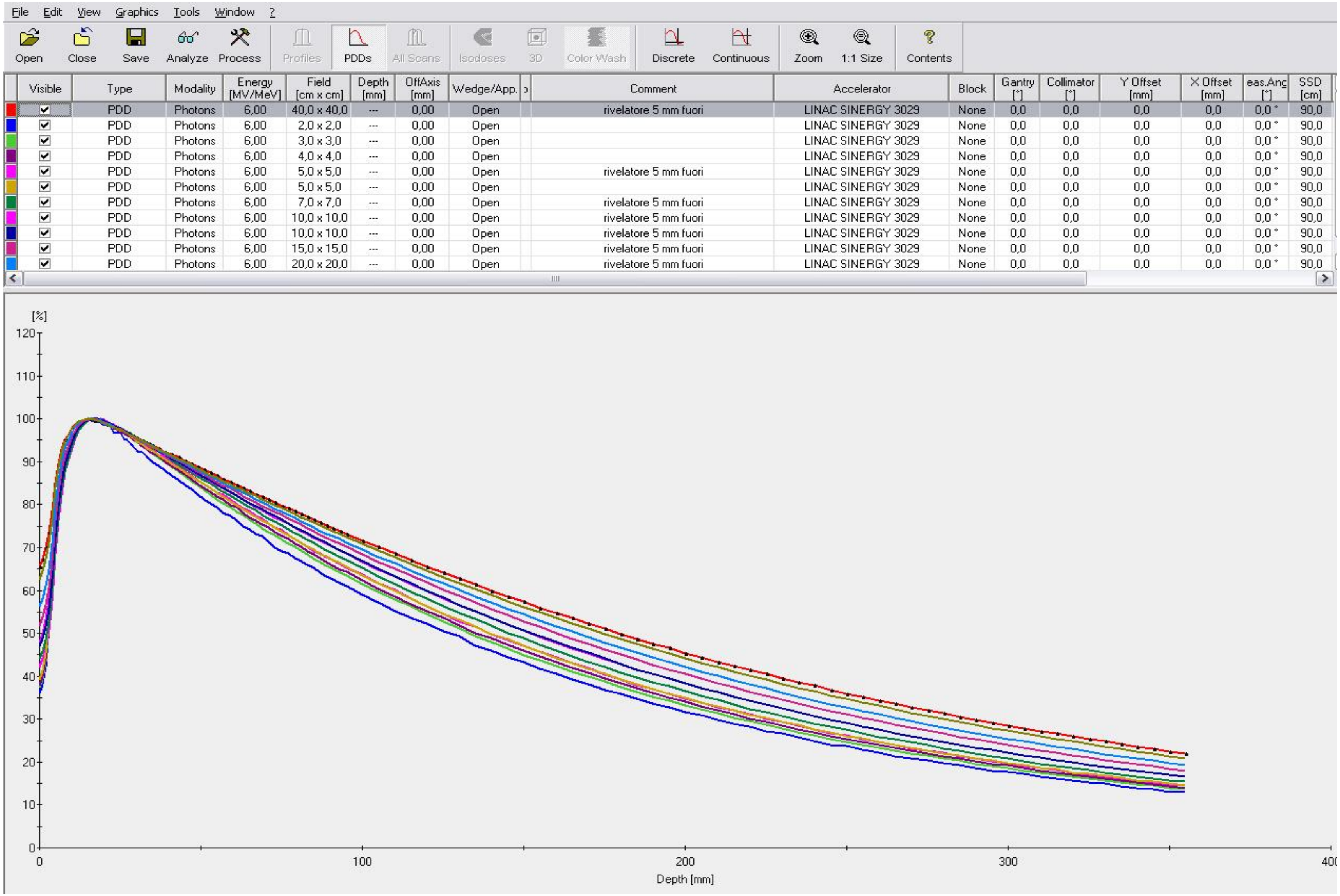
Dosimetric field size

it's defined as the distance intercepted by a given isodose curve (usually 50% isodose) on a plane perpendicular to the beam axis at a stated distance from a source (100cm).



- *As the field size increases the contribution of scattered radiation to the absorbed dose increases.*
- *The field size dependence of PDD is less pronounced for the higher energy beams than for the lower energy beams.*

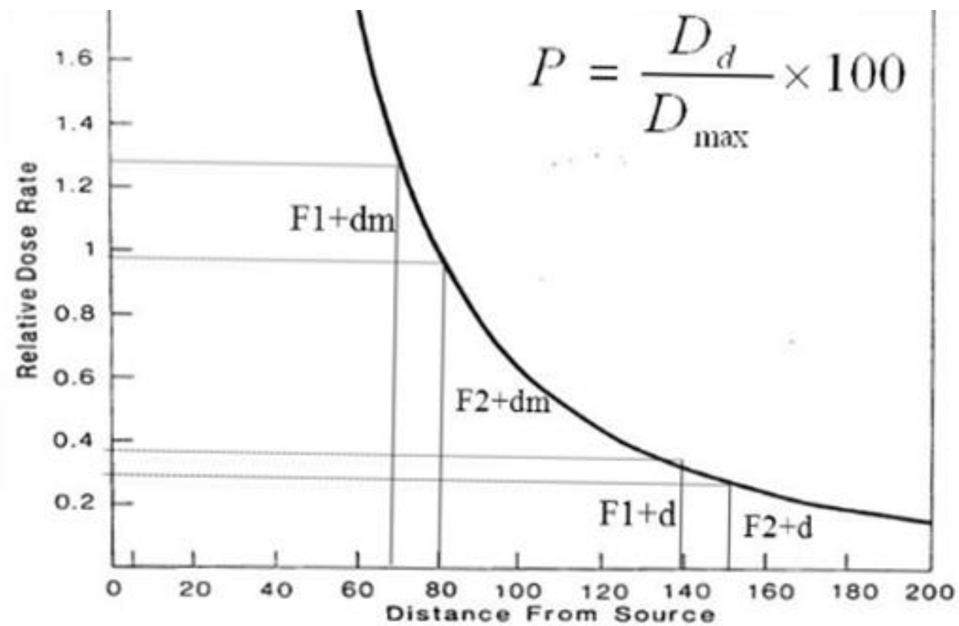
PDD dependence on field size



Visible	Type	Modality	Energy [MV/MeV]	Field [cm x cm]	Depth [mm]	OffAxis [mm]	Wedge/App.	Comment	Accelerator	Block	Gantry [°]	Collimator [°]	Y Offset [mm]	X Offset [mm]	eas.Ang [°]	SSD [cm]
☑	PDD	Photons	6,00	40,0 x 40,0	---	0,00	Open	rivelatore 5 mm fuori	LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0
☑	PDD	Photons	6,00	2,0 x 2,0	---	0,00	Open		LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0
☑	PDD	Photons	6,00	3,0 x 3,0	---	0,00	Open		LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0
☑	PDD	Photons	6,00	4,0 x 4,0	---	0,00	Open		LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0
☑	PDD	Photons	6,00	5,0 x 5,0	---	0,00	Open	rivelatore 5 mm fuori	LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0
☑	PDD	Photons	6,00	5,0 x 5,0	---	0,00	Open		LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0
☑	PDD	Photons	6,00	7,0 x 7,0	---	0,00	Open	rivelatore 5 mm fuori	LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0
☑	PDD	Photons	6,00	10,0 x 10,0	---	0,00	Open	rivelatore 5 mm fuori	LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0
☑	PDD	Photons	6,00	10,0 x 10,0	---	0,00	Open	rivelatore 5 mm fuori	LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0
☑	PDD	Photons	6,00	15,0 x 15,0	---	0,00	Open	rivelatore 5 mm fuori	LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0
☑	PDD	Photons	6,00	20,0 x 20,0	---	0,00	Open	rivelatore 5 mm fuori	LINAC SINERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	90,0

PDD dependence on SSD

The percentage depth dose (PDD) increases with SSD due to the effects of inverse square law.



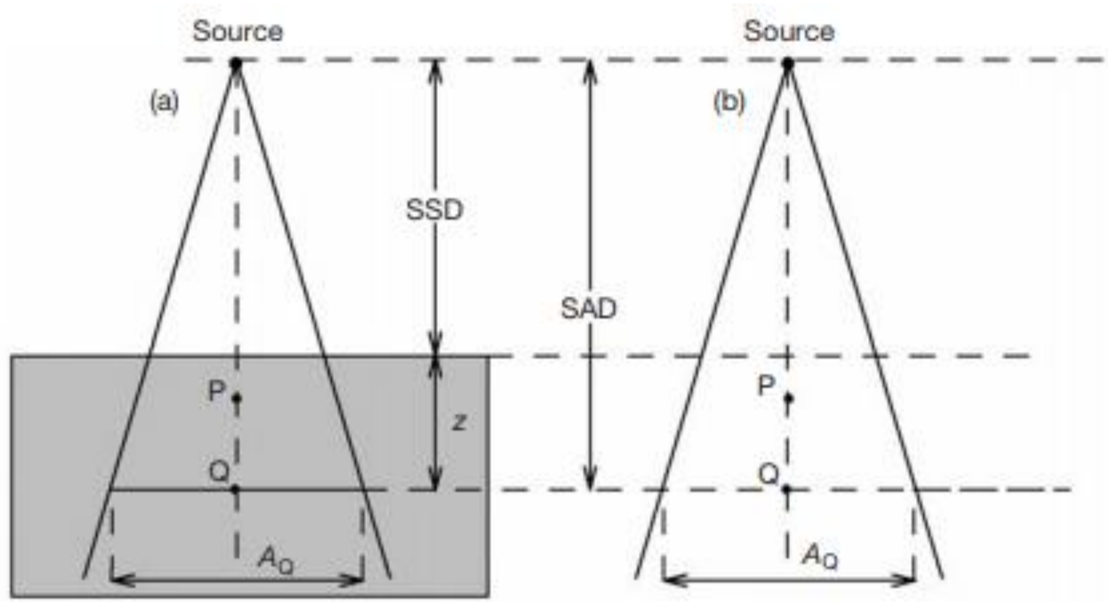
The plot shows that the drop in doserate between two points is much greater at smaller distances from the source then at large distance

Tissue Air Ratio TAR

Tissue Air Ratio (TAR) is the ratio of the absorbed dose at a given depth in tissue (phantom/patient) to the absorbed dose at the same point in air:

$$\mathrm{TAR}(z, A_Q, h\nu) = \frac{D_Q}{D'_Q}$$

- *TAR increases with the Beam energy*
- *TAR increases with the Field size*
- *TAR decreases with the Depth*
- ***TAR is indipendent from SSD***



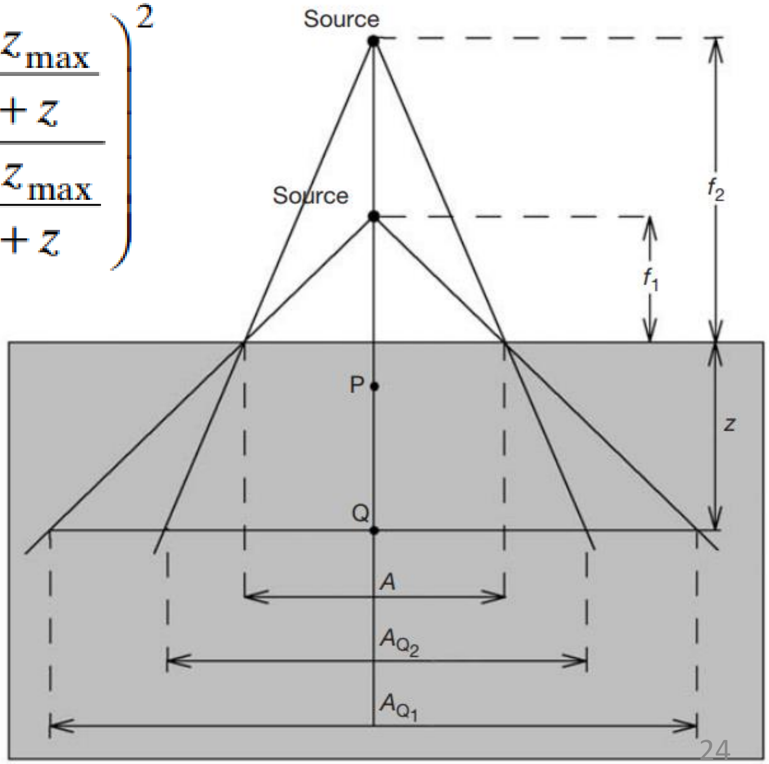
TAR and PDD

$$\mathrm{TAR}(z, A_Q, h\nu) = \frac{D_Q}{D'_Q}$$

$$\mathrm{PDD}(z, A, f, h\nu) = 100\,\frac{D_Q}{D_P}$$

$$D_Q = D_P\,\frac{\mathrm{PDD}(z, A, f, h\nu)}{100} = D'_Q\,\mathrm{TAR}(z, A_Q, h\nu)$$

$$\frac{\mathrm{PDD}(z, A, f_1, h\nu)}{\mathrm{PDD}(z, A, f_2, h\nu)} = \left(\frac{\mathrm{TAR}(z, A_{Q1}, h\nu)}{\mathrm{TAR}(z, A_{Q2}, h\nu)}\right)\left(\frac{\dfrac{f_1 + z_{\max}}{f_1 + z}}{\dfrac{f_2 + z_{\max}}{f_2 + z}}\right)^2$$



Pick Scatter Factor (PSF)

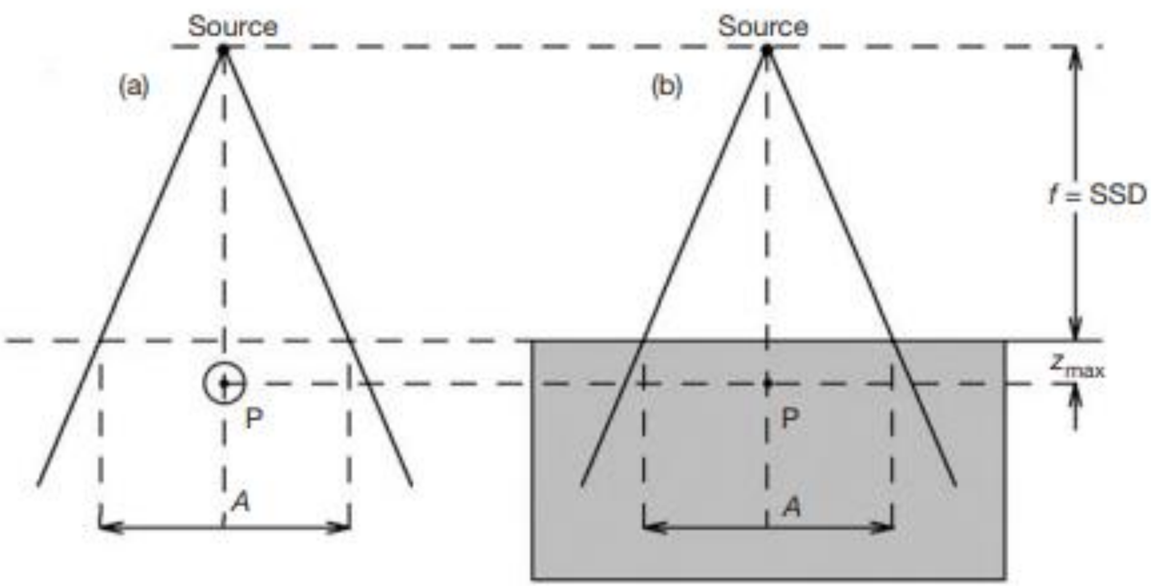
In a phantom the ratio of the dose maximum to the dose in air at the same depth is called **pickscatter factor (PSF)**

1. PSF increases as the field size increases

2. PSF decreases as the energy increases

3. PSF is indipendent of SSD

4. PSF increases with field size from unity linearly then saturates at very large field

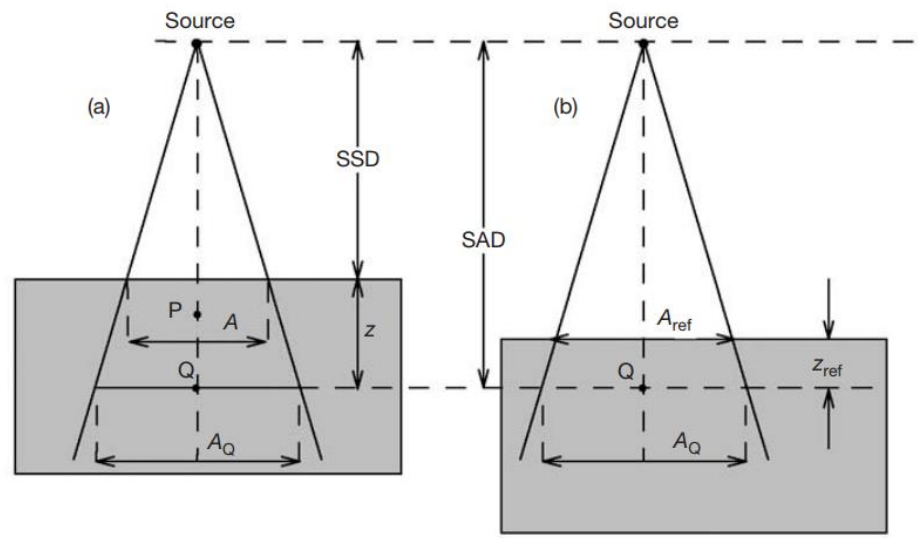


Tissue Phantom Ratio TPR and Tissue Maximum Ratio TMR

The tissue phantom ratio TPR is defined as the ratio of the dose at a given point in phantom to the dose at the same point at a fixed reference depth:

$$\mathrm{TPR}(z, A_{\mathrm{Q}}, h\nu) = \frac{D_{\mathrm{Q}}}{D_{\mathrm{Qref}}}$$

$$\mathrm{TMR}(z, A_{\mathrm{Q}}, h\nu) = \frac{D_{\mathrm{Q}}}{D_{\mathrm{Qmax}}}$$



TPR and TMR depend on the three parameters: ***z*, *A*$_Q$, *hν***
NO dependance on the SAD or SSD.

- ***A*$_Q$ and *hν* constant TMR decreases with increasing *z***
- ***z* and *hν* constant TMR increases with increasing *A*$_Q$**
- ***z* and *A*$_Q$ constant TMR increases with increasing *hν***

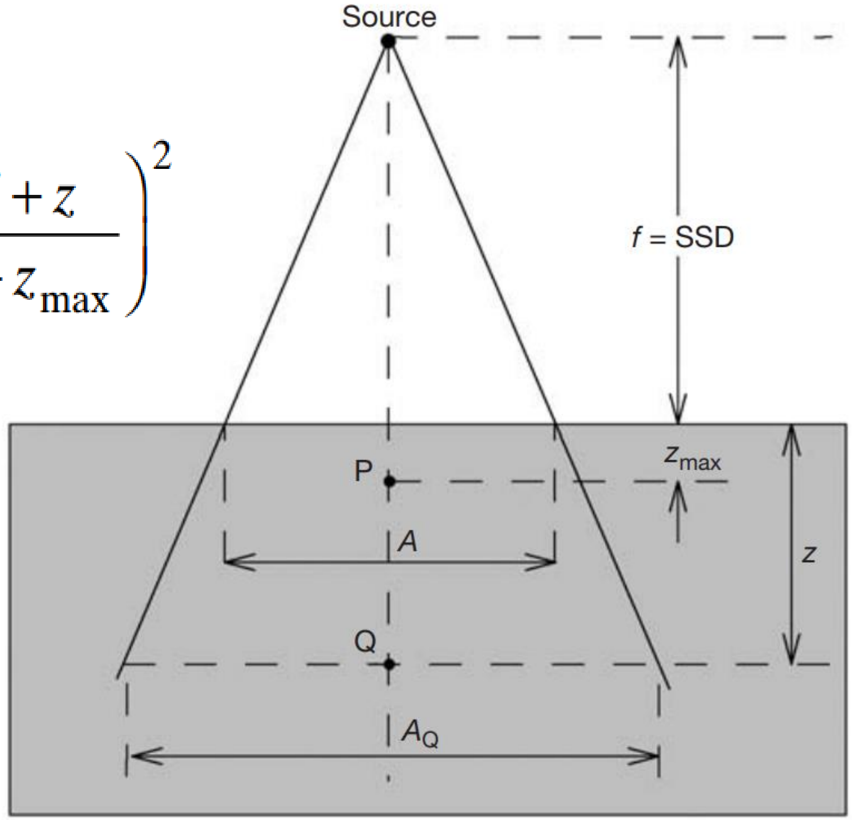
TMR and PDD

$$\mathrm{TMR}(z, A_Q, h\nu) = \frac{D_Q}{D_{Q\max}}$$

$$\mathrm{PDD}(z, A, f, h\nu) = 100\frac{D_Q}{D_P}$$

$$D_Q = D_P \frac{\mathrm{PDD}(z, A, f, h\nu)}{100} = D_{Q\max}\mathrm{TMR}(z, A_Q, h\nu)$$

$$\mathrm{TMR}(z, A_Q, h\nu) \approx \frac{\mathrm{PDD}(z, A, f, h\nu)}{100}\left(\frac{f+z}{f+z_{\max}}\right)^2$$

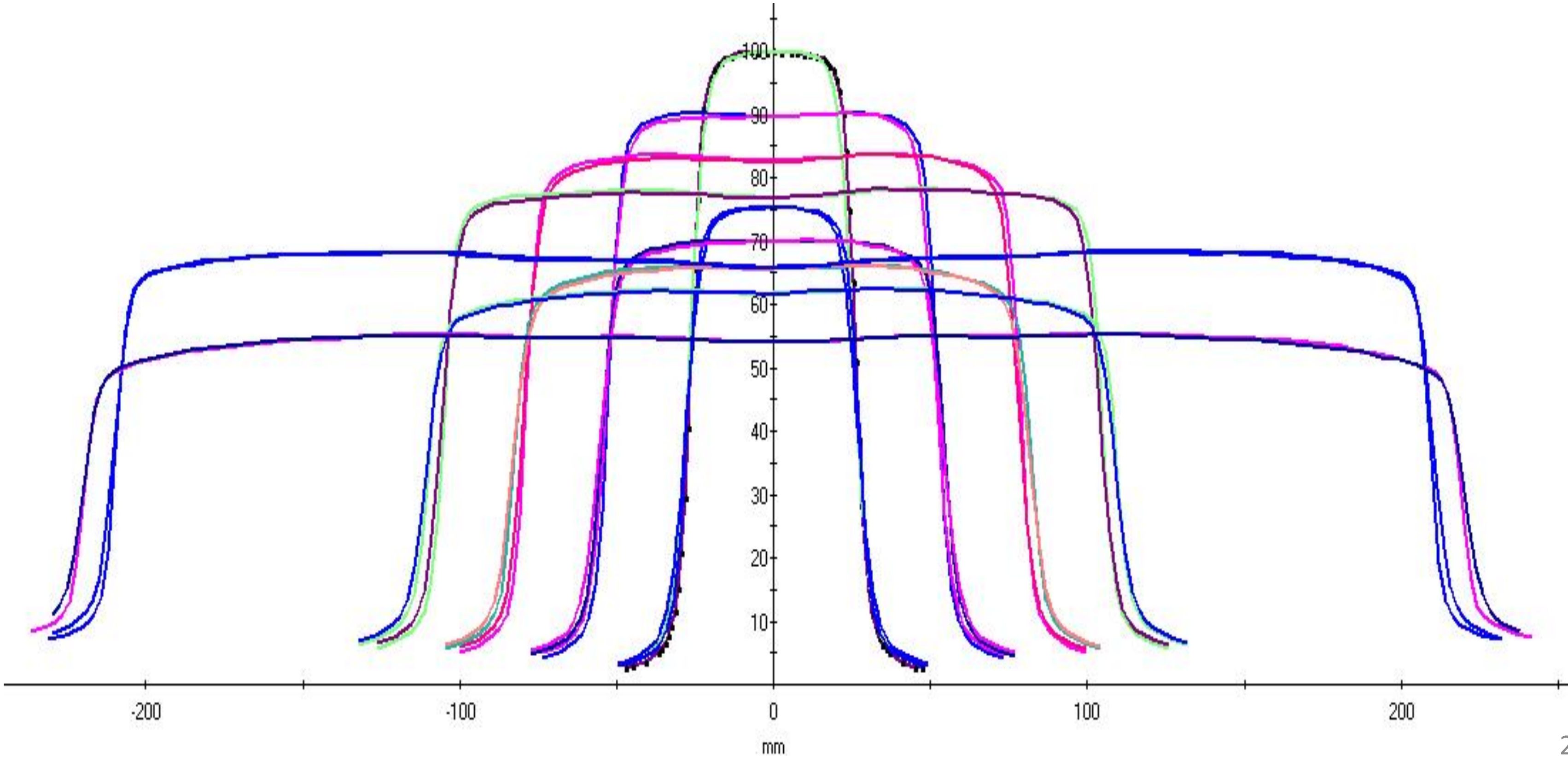


Off-axis ratios and beam profiles

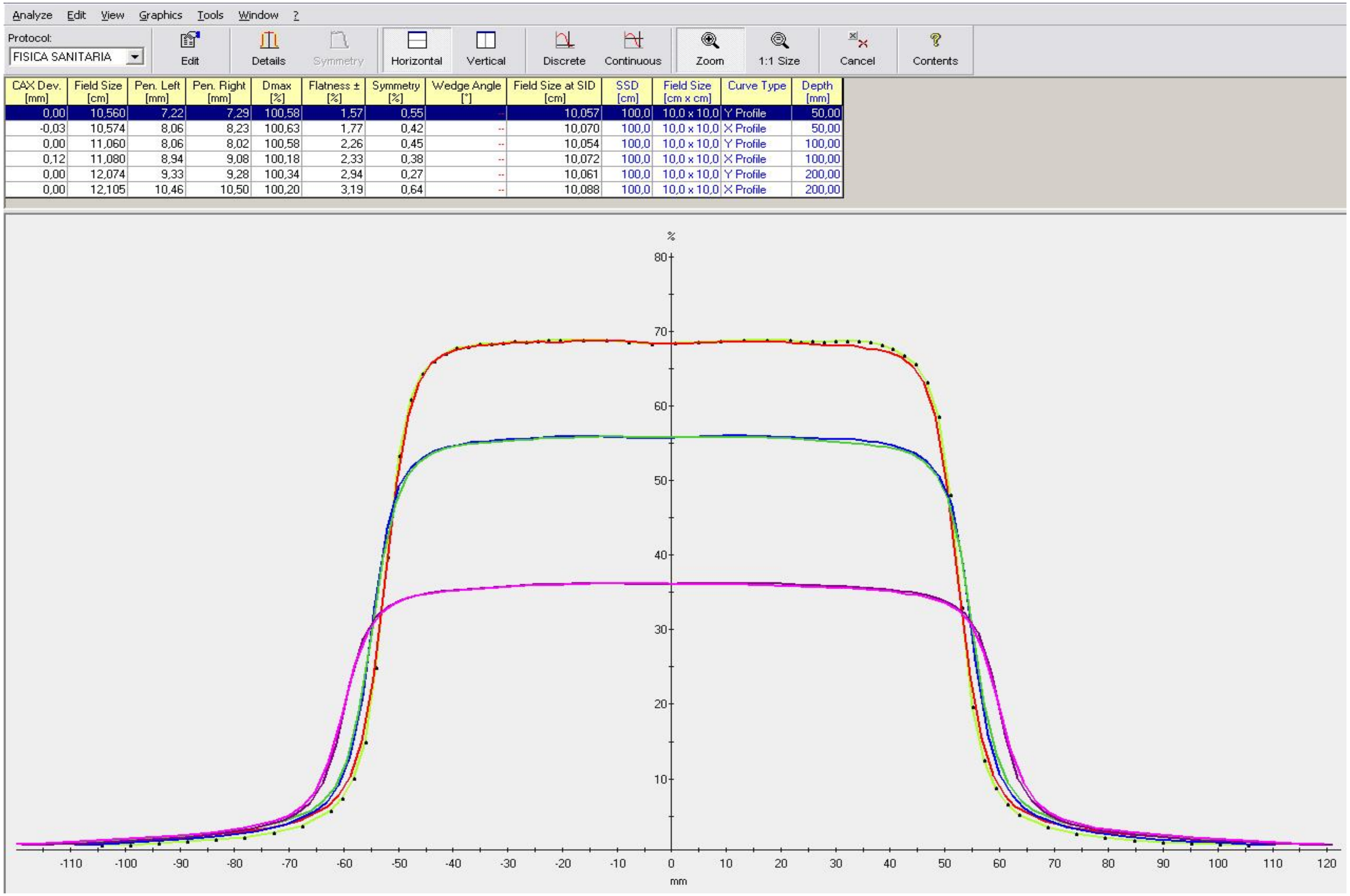
Dose distributions in 2-D and 3-D are determined with central axis data in conjunction with off-axis dose profiles.

The off-axis data are given with beam profiles measured perpendicularly to the beam central axis at a given depth in a phantom.

The off-axis ratio (OAR) is usually defined as the ratio of dose at an off-axis point to the dose on the central beam axis at the same depth in a



beam profiles at different depths



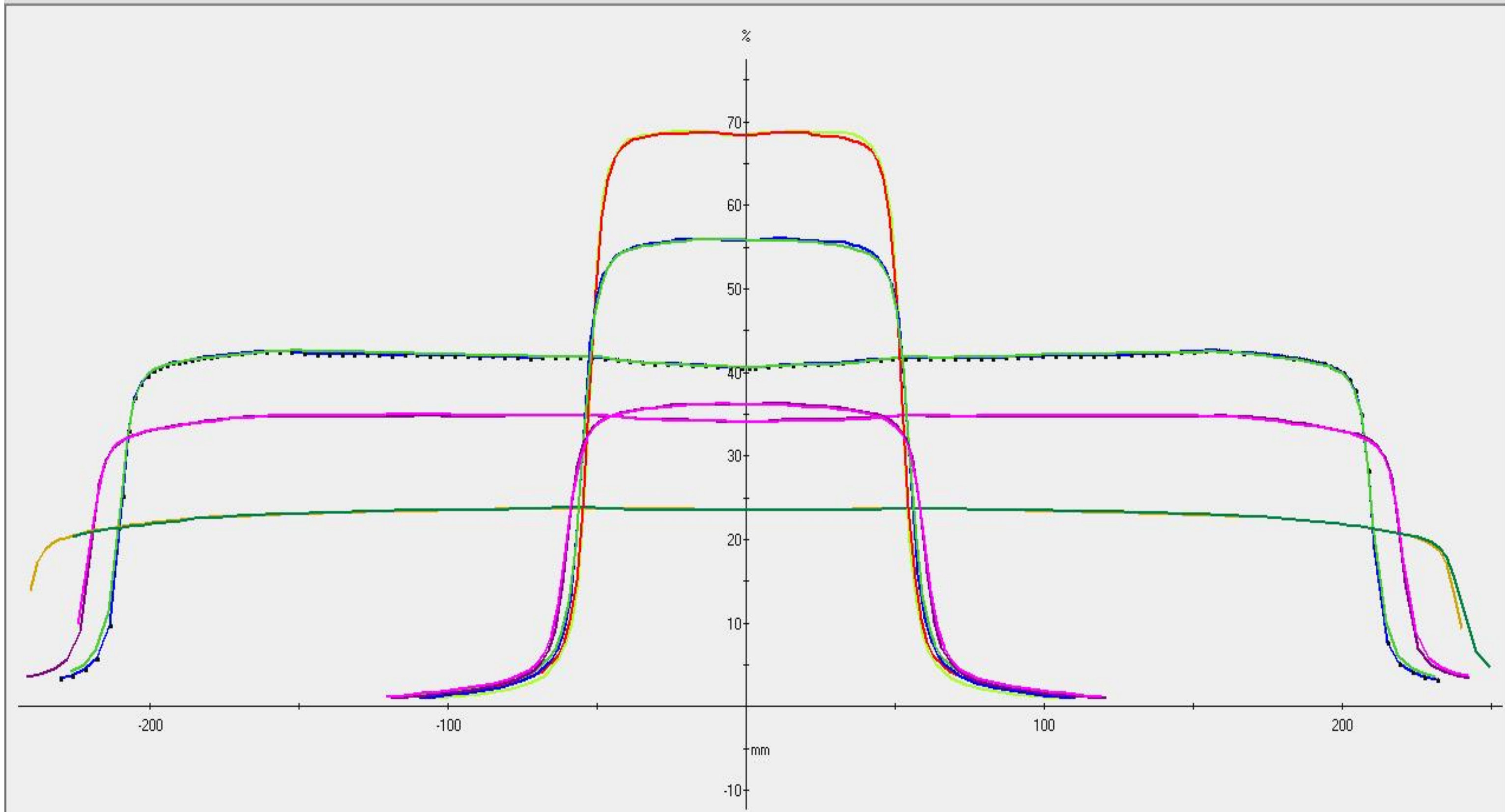
CAX Dev. [mm]	Field Size [cm]	Pen. Left [mm]	Pen. Right [mm]	Dmax [%]	Flatness ± [%]	Symmetry [%]	Wedge Angle [°]	Field Size at SID [cm]	SSD [cm]	Field Size [cm x cm]	Curve Type	Depth [mm]
0,00	10,560	7,22	7,29	100,58	1,57	0,55	--	10,057	100,0	10,0 x 10,0	Y Profile	50,00
-0,03	10,574	8,06	8,23	100,63	1,77	0,42	--	10,070	100,0	10,0 x 10,0	X Profile	50,00
0,00	11,060	8,06	8,02	100,58	2,26	0,45	--	10,054	100,0	10,0 x 10,0	Y Profile	100,00
0,12	11,080	8,94	9,08	100,18	2,33	0,38	--	10,072	100,0	10,0 x 10,0	X Profile	100,00
0,00	12,074	9,33	9,28	100,34	2,94	0,27	--	10,061	100,0	10,0 x 10,0	Y Profile	200,00
0,00	12,105	10,46	10,50	100,20	3,19	0,64	--	10,088	100,0	10,0 x 10,0	X Profile	200,00

The field flatness changes with depth

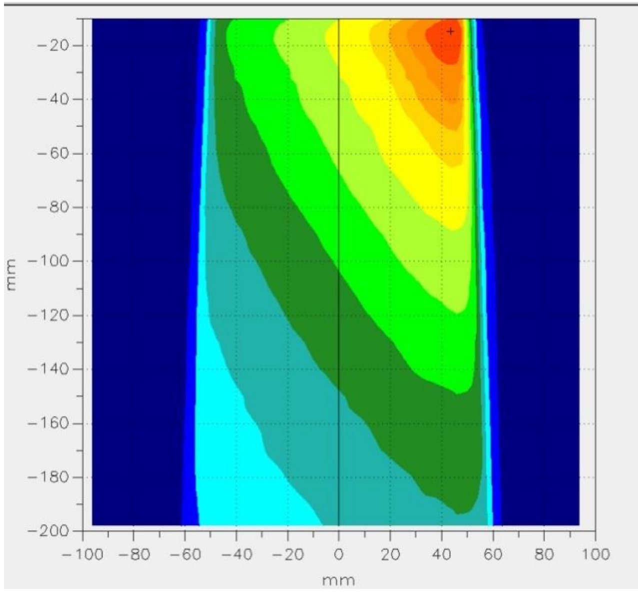
This is attributed to an increase in scatter to primary dose ratio with increasing depth and decreasing incident photon energy off axis

beam profiles at different depths

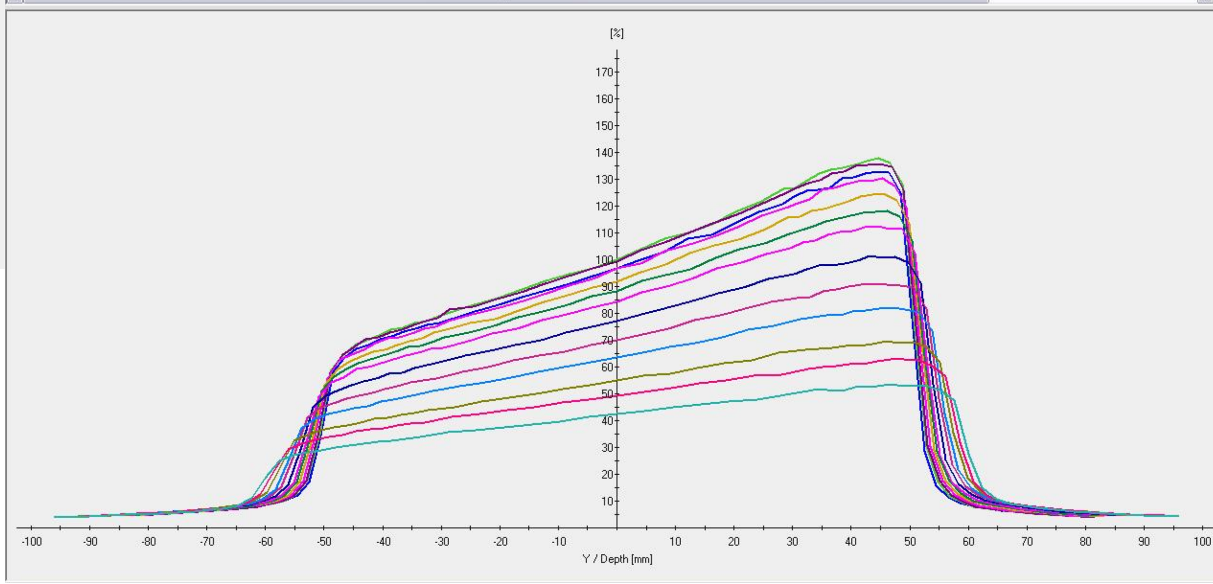
CAX Dev. [mm]	Field Size [cm]	Pen. Left [mm]	Pen. Right [mm]	Dmax [%]	Flatness ± [%]	Symmetry [%]	Wedge Angle [°]	Field Size at SID [cm]	SSD [cm]	Field Size [cm x cm]	Curve Type	Depth [mm]
0,00	42,106	7,92	7,46	105,04	2,47	0,43	--	40,101	100,0	40,0 x 40,0	Y Profile	50,00
0,00	42,196	9,45	9,58	104,91	2,44	0,53	--	40,186	100,0	40,0 x 40,0	X Profile	50,00
0,00	44,080	9,86	8,97	102,48	1,25	0,34	--	40,073	100,0	40,0 x 40,0	Y Profile	100,00
0,00	44,173	--	--	102,47	1,29	0,48	--	40,157	100,0	40,0 x 40,0	X Profile	100,00
--	--	--	--	--	--	--	--	--	100,0	40,0 x 40,0	Y Profile	200,00
--	--	--	--	--	--	--	--	--	100,0	40,0 x 40,0	X Profile	200,00
0,00	10,560	7,22	7,29	100,58	1,57	0,55	--	10,057	100,0	10,0 x 10,0	Y Profile	50,00
-0,03	10,574	8,06	8,23	100,63	1,77	0,42	--	10,070	100,0	10,0 x 10,0	X Profile	50,00
0,00	11,060	8,06	8,02	100,58	2,26	0,45	--	10,054	100,0	10,0 x 10,0	Y Profile	100,00
0,12	11,080	8,94	9,08	100,18	2,33	0,38	--	10,072	100,0	10,0 x 10,0	X Profile	100,00
0,00	12,074	9,33	9,28	100,34	2,94	0,27	--	10,061	100,0	10,0 x 10,0	Y Profile	200,00
0,00	12,105	10,46	10,50	100,20	3,19	0,64	--	10,088	100,0	10,0 x 10,0	X Profile	200,00



beam profiles with wedge



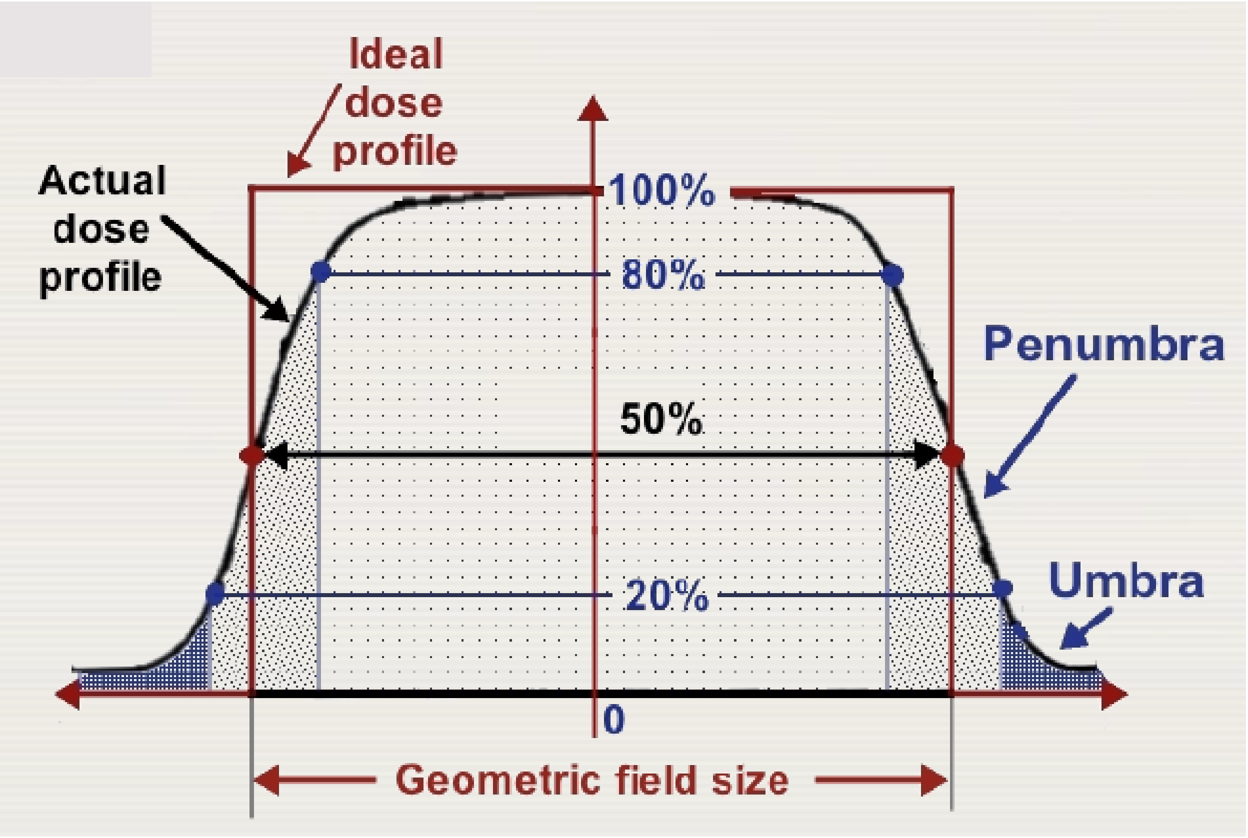
Visible	Type	Modality	Energy [MV/MeV]	Field [cm x cm]	Depth [mm]	OffAxis [mm]	Wedge/App.	Comment	Accelerator	Block	Gantry [°]	Collimator [°]	Inplane Offset [mm]	ssplane Off [mm]	eas.Ang [°]	SSD [cm]
☐	PDD	Photons	6,00	10,0 x 10,0	---	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	10,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	15,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	20,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	30,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	40,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	50,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	60,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	80,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	100,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	120,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	150,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0
☑	Y Profile	Photons	6,00	10,0 x 10,0	170,00	0,00	W60	ISODOSE WEDGE	LINAC SYNERGY 3029	None	0,0	0,0	0,0	0,0	0,0 °	100,0



Beam profiles

Megavoltage X ray beam profiles consist of three distinct regions:

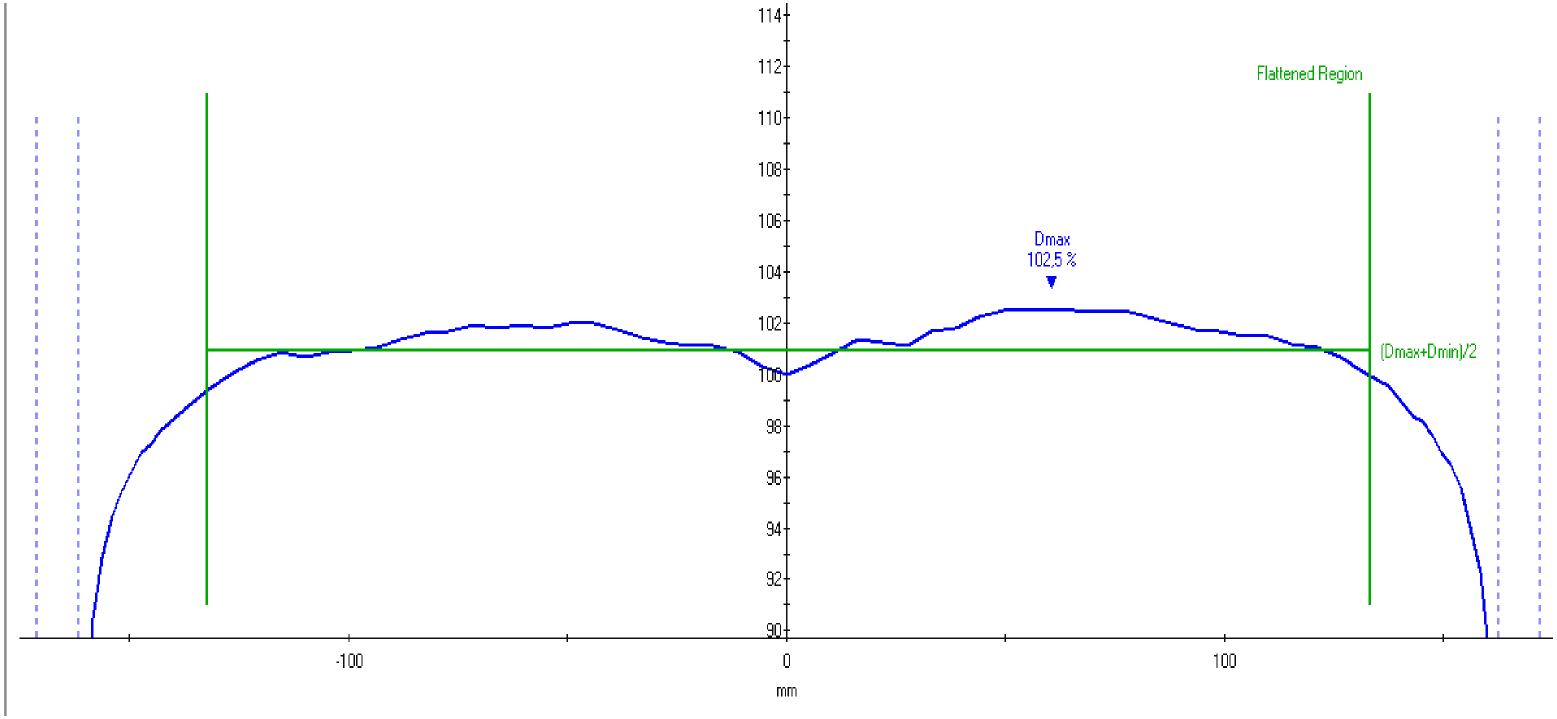
- ***Central***
- ***Penumbra***
- ***Umbra***



Beam profiles: central region

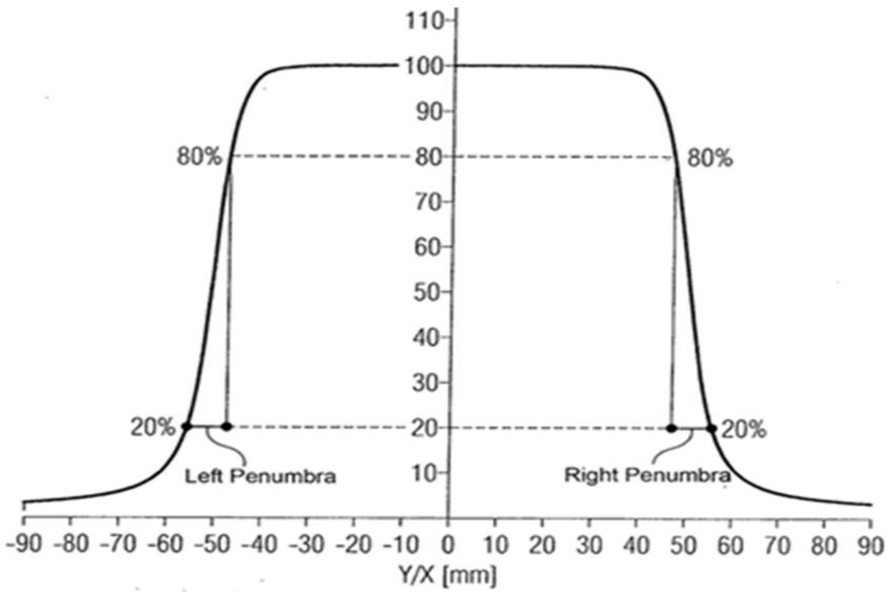
The ***central region*** represents the central portion of the profile extending from the beam central axis to within 1–1.5 cm from the geometric field edges of the beam.

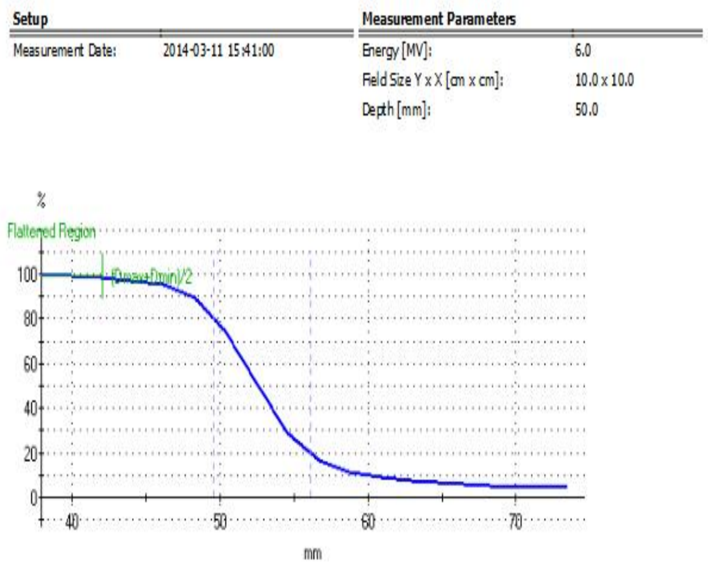
The ***central region*** is affected by the energy of electrons striking the thick target, by the target atomic number and by the flattening filter atomic number and geometric shape.



Beam profiles: penumbral region

In the penumbral region the dose changes rapidly and depends also on the **collimators**, the **finite size of the focal spot** (source size) and the **lateral electronic disequilibrium.**





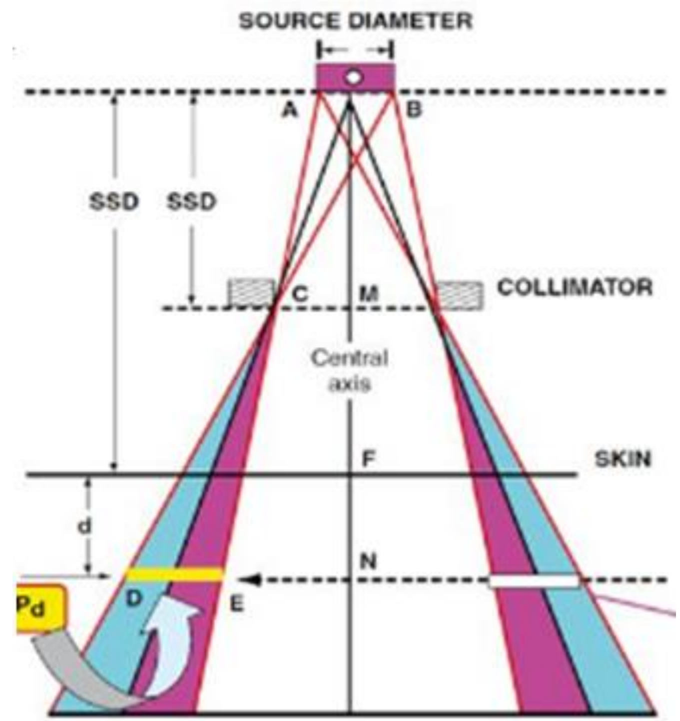
The dose falloff around the geometric beam edge is sigmoid in shape and extends under the collimator jaws into the penumbral tail region.

The ***physical penumbra*** is the sum of the three individual penumbras: ***transmission, geometric* and *scatter***.

Beam profiles: penumbral and umbra region

The physical penumbra depends on:

- ***beam energy***
- ***source size***
- ***SSD***
- ***source to collimator distance***
- ***depth in a phantom***



Umbra is the region outside the radiation field, far removed from the field edges and results from radiation transmitted through the collimator and head shielding.

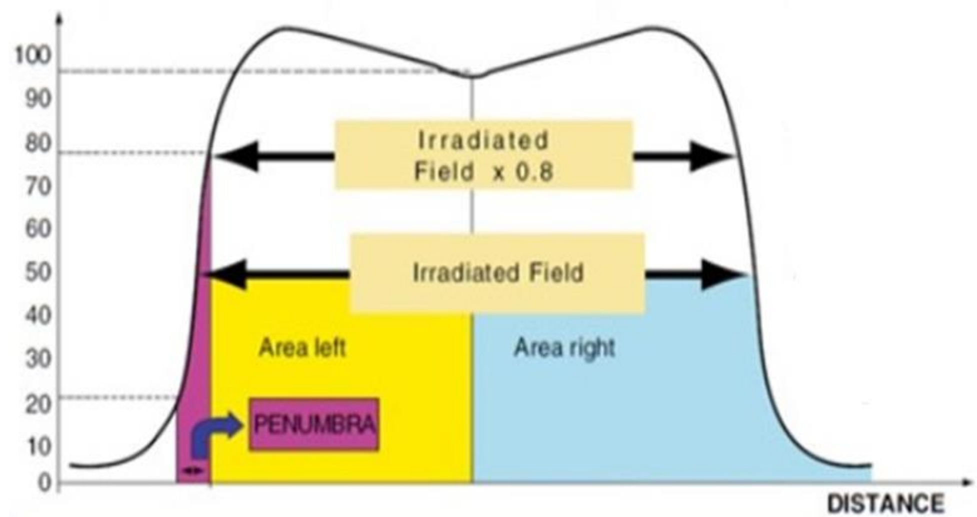
Beam profiles: flatness and symmetry

Dose profile uniformity is measured by a scan along the centre of both major beam axes for various depths in a water phantom.

Two parameters quantify the **field uniformity**:

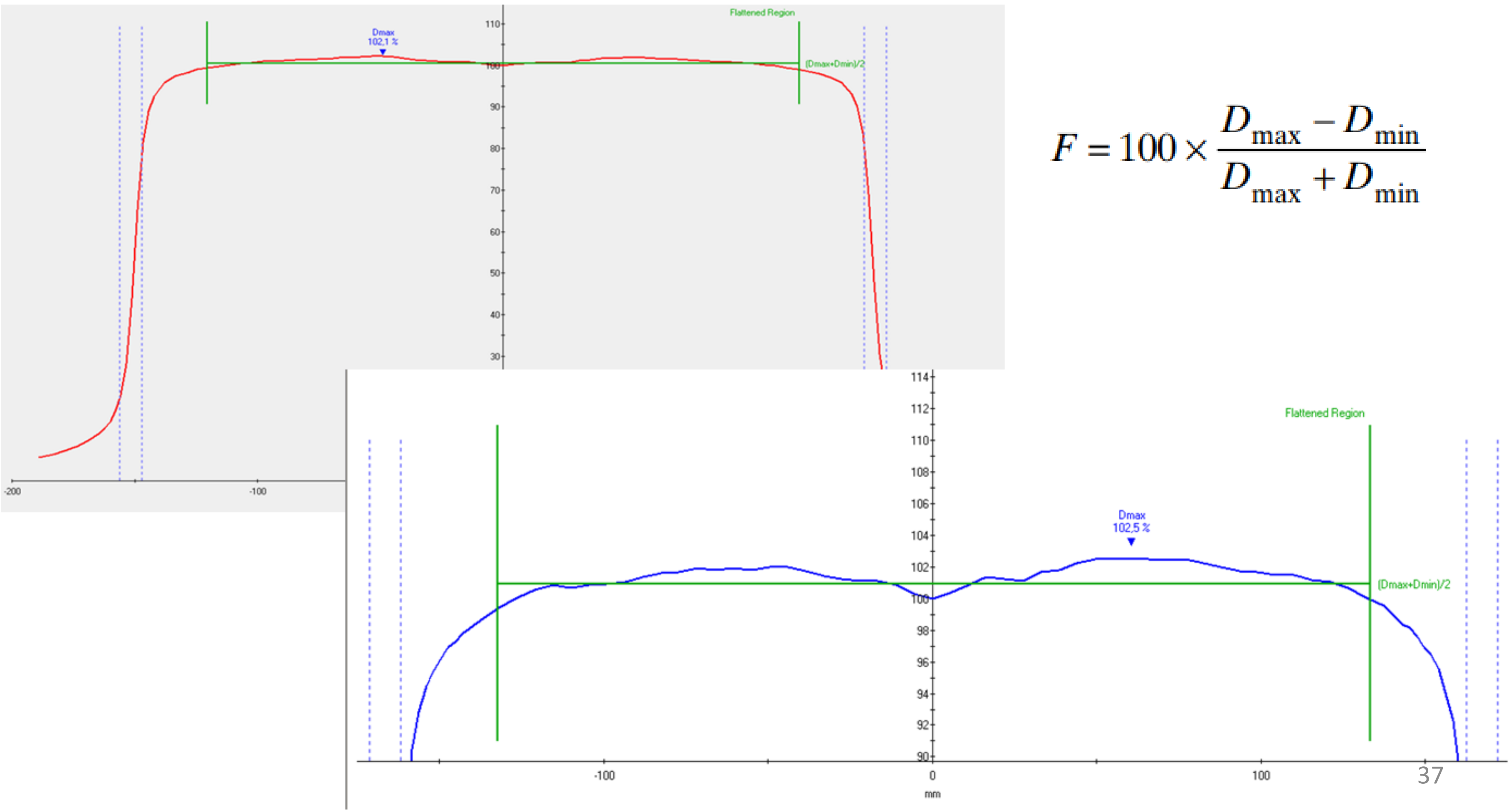
- ***field (beam) flatness***

- ***field (beam) symmetry***



Beam profiles: flatness

The beam flatness **F** is assessed by finding the maximum $\mathbf{D_{max}}$ and minimum $\mathbf{D_{min}}$ dose point values on the beam profile within the central 80% of the beam width (**flatness region**):



$$F = 100 \times \frac{D_{\max} - D_{\min}}{D_{\max} + D_{\min}}$$

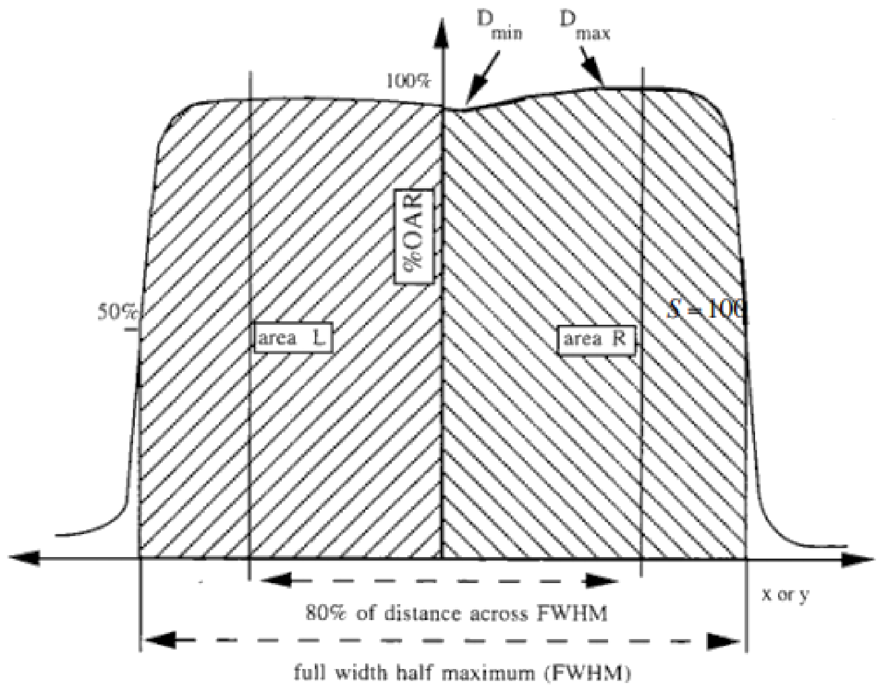
Beam profiles: symmetry

A typical symmetry specification is that any two dose points on a beam profile, equidistant from the central axis point, are within 2% of each other.

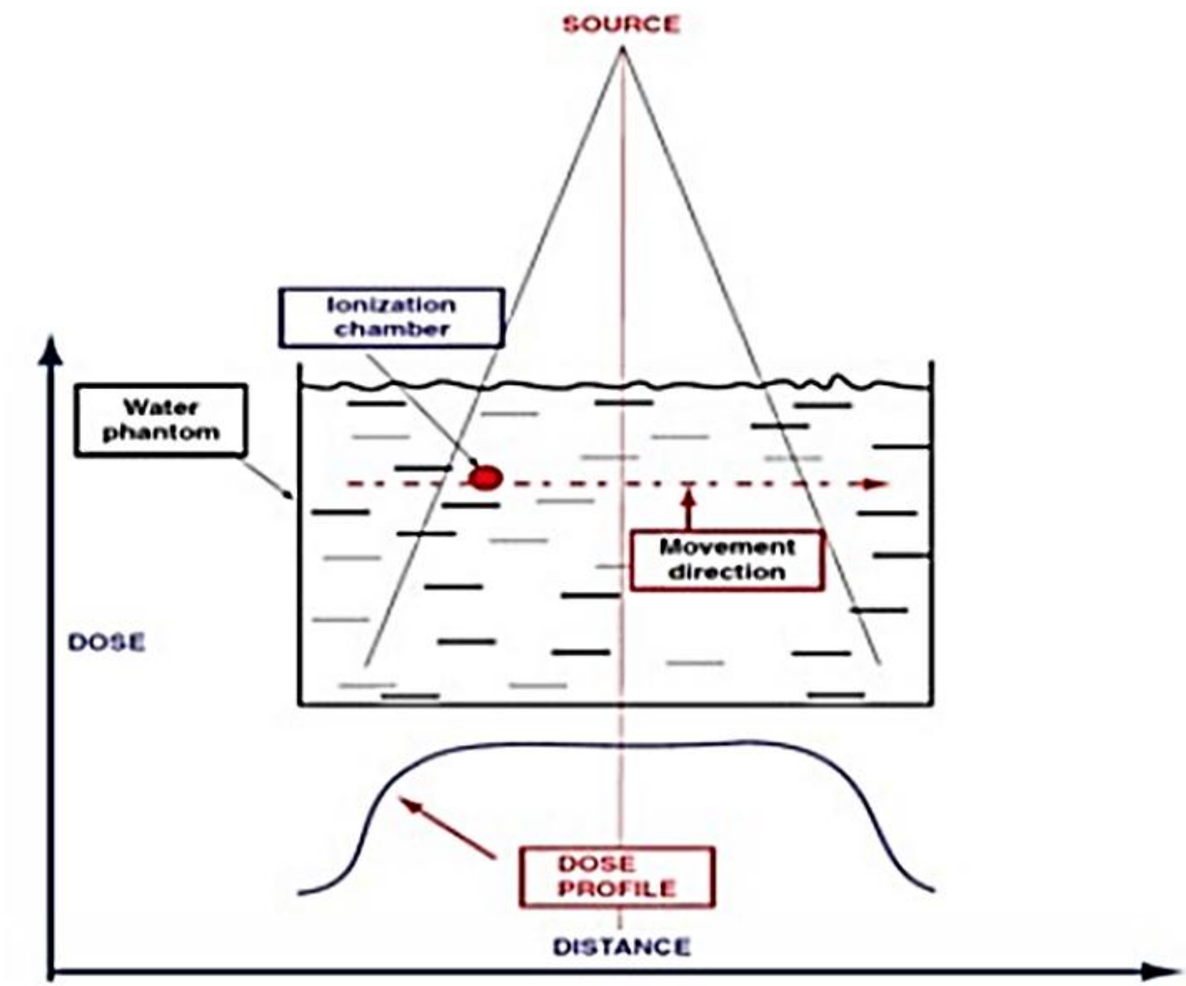
Alternately, areas under beam profile on each side (left and right) of the central axis extending to the 50% dose level (normalized to 100% at the central axis point) are determined.

Symmetry S is calculated from:

$$S = 100 \times \frac{\text{area}_{\text{left}} - \text{area}_{\text{right}}}{\text{area}_{\text{left}} + \text{area}_{\text{right}}}$$



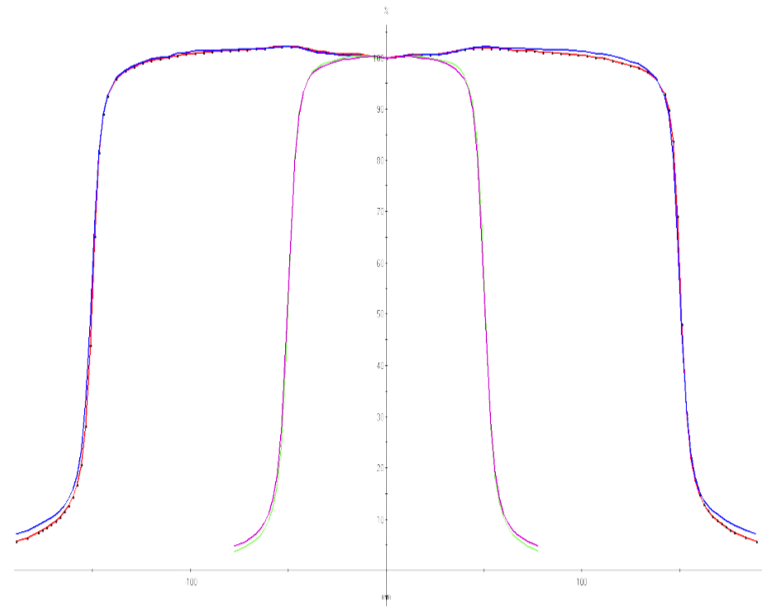
Dose profile measurements



Dose profile measurements

Profile parameters (ELEKTA protocol)

Energy	FIELD	Axis	FIELD Size(mm)		Flatness(%)		Simmetry(%)	
			I	II	I	II	I	II
6MV	10X10	Y(INPLANE)	10,1	10,1	104,36	104,84	100,44	101,10
	10X10	X(CROSSPLANE)	10,1	10,1	105,16	105,37	100,25	100,50
	30X30	Y(INPLANE)	30,1	30,1	103,97	104,39	100,23	100,70
	30X30	X(CROSSPLANE)	30,1	30,2	104,15	104,28	100,46	100,40
10MV	10X10	Y(INPLANE)	10,1	10,1	104,94	105,23	100,48	10,46
	10X10	X(CROSSPLANE)	10,1	10,1	105,57	105,89	100,2	100,67
	30X30	Y(INPLANE)	30,1	30,1	103,36	103,24	100,37	100,35
	30X30	X(CROSSPLANE)	30,2	30,2	103,53	103,02	100,65	100,62
15MV	10X10	Y(INPLANE)	10,1	10,1	104,78	105,14	100,35	100,44
	10X10	X(CROSSPLANE)	10,1	10,1	105,47	105,94	100,22	100,95
	30X30	Y(INPLANE)	30,1	30,1	103,29	103,7	100,52	100,32
	30X30	X(CROSSPLANE)	30,2	30,2	102,59	103,8	100,43	100,6



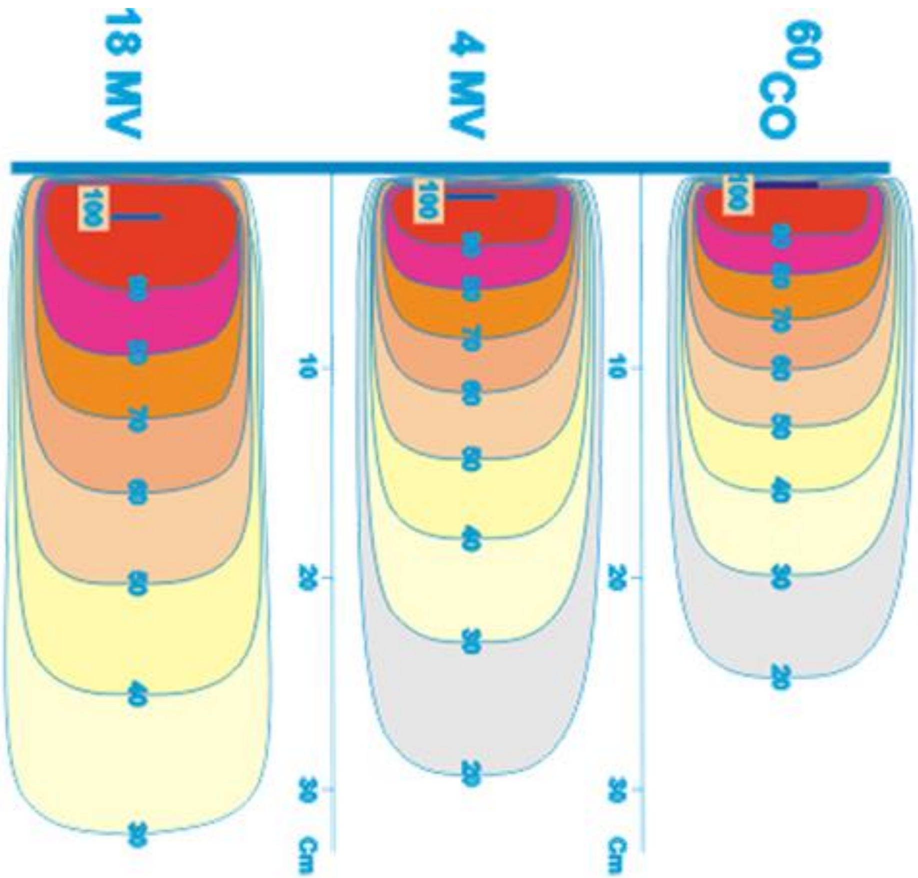
Profile parameters (home protocol)

Energy	FIELD	Axis	FIELD Size(mm)		Penombra left(mm)		Penombra right(%)		Dmax(%)		Flatness(%)		Simmetry(%)	
			I	II	I	II	I	II	I	II	I	II	I	II
6MV	10X10	Y(INPLANE)	10,1	10,1	7	7,4	7	7,2	100,3	100,2	2,14	2,37	0,43	1,07
	10X10	X(CROSSPLANE)	10,1	10,1	8,5	9,1	8,7	9,2	100,2	100,0	2,51	2,61	0,25	0,48
	30X30	Y(INPLANE)	30,1	30,1	9,3	9,7	9,1	9,0	101,3	101,5	1,94	2,14	0,23	0,71
	30X30	X(CROSSPLANE)	30,1	30,2	11,1	11,4	11,1	11,2	101,2	101,0	2,02	2,08	0,46	0,38
10MV	10X10	Y(INPLANE)	10,1	10,1	7,5	7,9	7,4	7,7	101,0	100,3	2,41	2,55	0,46	0,35
	10X10	X(CROSSPLANE)	10,1	10,1	8,5	8,8	8,8	8,7	100,4	100,2	2,71	2,86	0,21	0,63
	30X30	Y(INPLANE)	30,1	30,1	9,1	9,4	8,8	9,5	102,0	101,7	1,65	1,59	0,37	0,45
	30X30	X(CROSSPLANE)	30,2	30,2	10,3	10,5	10,5	10,4	101,7	102,0	1,72	1,47	0,65	0,64
15MV	10X10	Y(INPLANE)	10,1	10,1	7,8	7,4	7,9	7,4	100,6	101,1	2,33	2,51	0,34	0,44
	10X10	X(CROSSPLANE)	10,1	10,1	8,6	8,7	8,6	8,7	100,4	100,6	2,66	2,88	0,21	0,92
	30X30	Y(INPLANE)	30,1	30,1	9,1	9,6	9,2	9,1	102,1	101,6	1,61	1,81	0,51	0,33
	30X30	X(CROSSPLANE)	30,2	30,2	10,2	10,7	10,1	10,6	102,2	101,4	1,27	1,85	0,43	0,60

Isodose curves

In order to represent volumetric and planar variation in absorbed dose, distribution are depicted by means of ISODOSE CURVES

Isodose curve are the lines joining the points of equal Percentage Depth Dose (PDD).

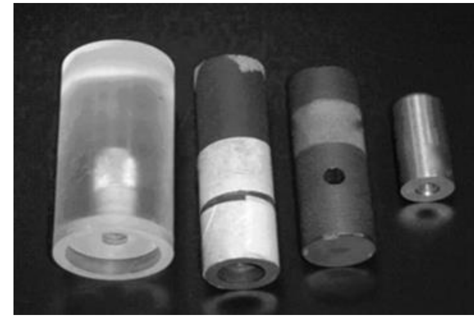


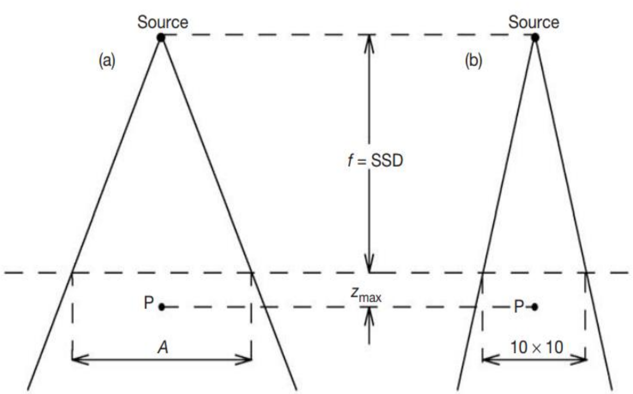
Collimator scatter correction factor (S_c) or Output factor

Collimator scatter correction Factor (S_c) is commonly called the ***Output factor.***

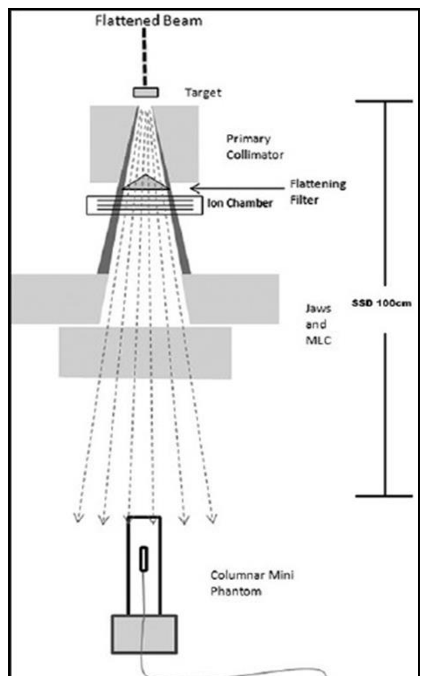
It 's defined as the ratio of the output in air for a given field to that for a reference field (e.g. 10x10cm^2)

S_c may be measured with an ion chamber with a build cap of size large enough to provide maximum dose buildup for the given energy beam.





Measurement Set-up of S_c



diodo	field	X6MV	X10MV	X15MV
1x1	1	0,673	0,644	0,622
2x2	2	0,791	0,799	0,786
3x3	3	0,834	0,854	0,852
4x4	4	0,867	0,886	0,891
5x5	5	0,895	0,912	0,917
7x7	7	0,943	0,951	0,956
Pin Point	field	X6MV	X10MV	X15MV
1x1	1	0,618	0,585	0,569
2x2	2	0,798	0,799	0,785
3x3	3	0,847	0,863	0,861
4x4	4	0,879	0,897	0,900
5x5	5	0,906	0,922	0,926
7x7	7	0,950	0,958	0,963
10x10	10	1,000	1,000	1,000
FARMER	field	X6MV	X10MV	X15MV
5x5	5	0,904	0,919	0,922
7x7	7	0,950	0,959	0,962
10x10	10	1,000	1,000	1,000
15x15	15	1,056	1,046	1,039
20x20	20	1,093	1,073	1,064
30x30	30	1,137	1,103	1,093
40x40	40	1,154	1,114	1,102

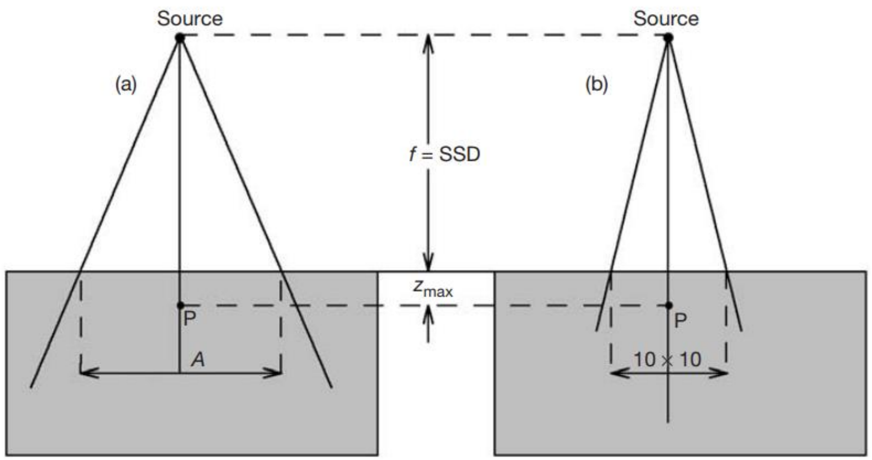
Phantom scatter correction factor S_p and total scatter correction factor S_{cp}

The ***phantom scatter factor S_p*** is as the ratio of dose for a given field size at a reference depth to the dose at the same depth for the reference field size $10 \times 10\ cm^2$.

The <u>phantom scatter describes the influence of the scatter originating in the phantom only.</u>

The ***total scatter factor S_{cp}*** is defined as defined as the ratio of $\mathbf{D_P}(z_{max}, A, f, h\nu)$, the dose at P in a phantom for field A, to $\mathbf{D_P}(z_{max}, 10, f, h\nu)$, the dose at P in a phantom for a $10 \times 10\ cm^2$ field.

$$S_{c,p}(A, h\nu) = \frac{D_P(z_{max}, A, f, h\nu)}{D_P(z_{max}, 10, f, h\nu)}$$

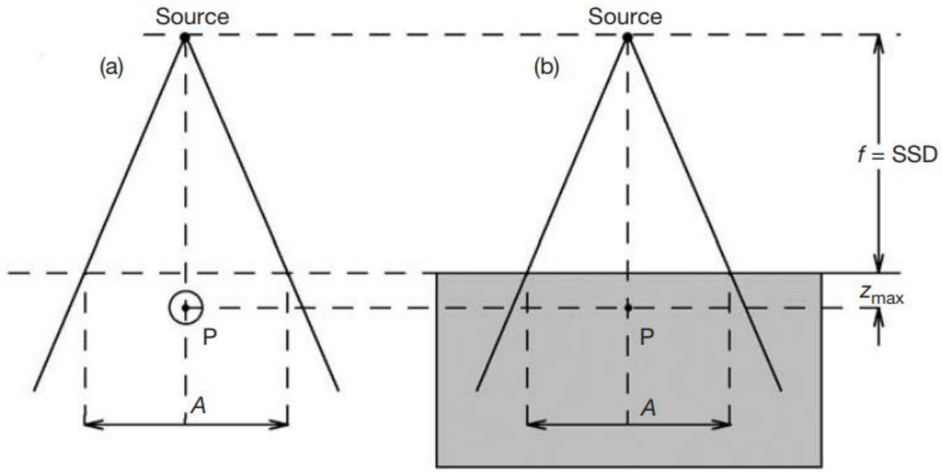


Measurement Set-up of S_{cp}

Phantom scatter correction factor S_p and total scatter correction factor S_{cp}

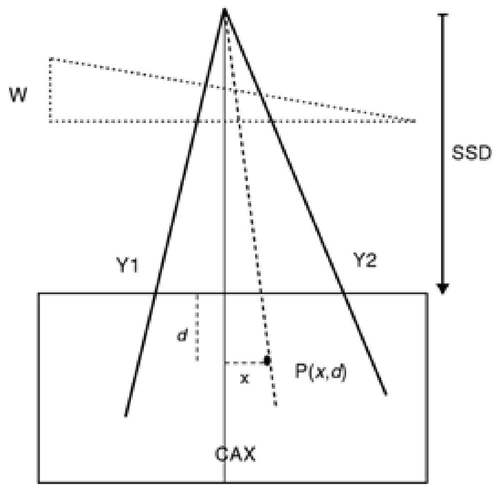
S_p is derived from the total scatter correction factor **S_{cp}**, as the ratio between S_{cp} and S_c :

$$S_p(s) \approx \frac{S_{cp}}{S_c}.$$



Measurement Set-up of S_c and S_{cp}

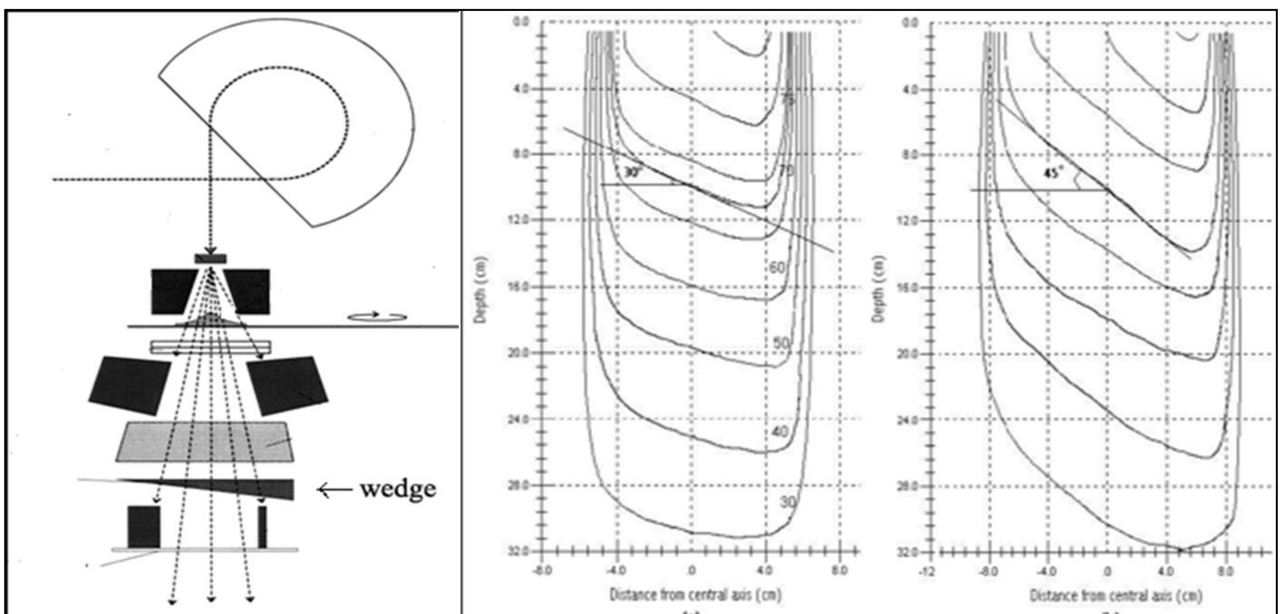
Wedge transmission factor WF



Measurement Set-up of WF

The ***wedge transmission factor*** **(WF)** or *wedge factor* is defined as the ratio of the outputs for a given field size (FS), at the reference depth d_{ref}(d), in a full scatter phantom at standard geometry, with and without the presence of a wedge filter :

$$WF(FS,d) = \frac{D_w(FS,d)}{D_O(FS,d)}$$



Wedge transmission factor WF

Motorized wedge: Nominal wedge angle 60°

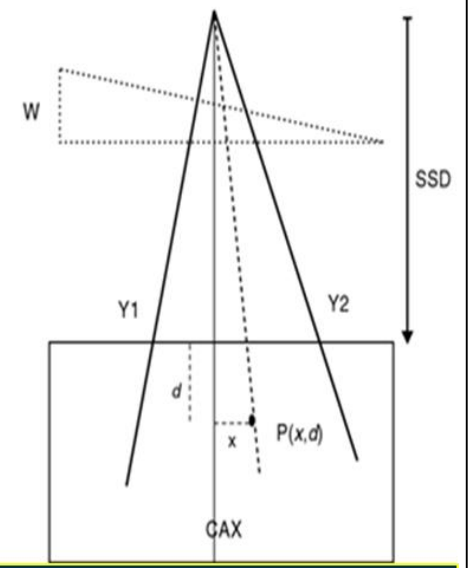
Energy	wedge	direction	Measured wedge factor	Reference wedge factor	D(%) <2%
X6MV	60°	IN	0,265	0,263	-0,7
X10MV	60°	IN	0,280	0,278	-0,7
X15MV	60°	IN	0,276	0,273	-0,9

Physical wedge

Energy	wedge	direction	Measured wedge factor	Reference wedge factor	D(%) <2%
X6MV	15°	IN	0,775	0,774	-0,2
	30°	IN	0,619	0,622	0,4
	45°	IN	0,498	0,501	0,6
X15MV	15°	IN	0,827	0,826	-0,1
	30°	IN	0,692	0,699	1,0
	45°	IN	0,527	0,521	-1,2

Enhanced Dynamic Wedges

Energy	wedge	direction	Measured wedge factor	Reference wedge factor	D < 2%
X6MV	10°	Y1-IN	0,952	0,951	0,2
	15°	Y1-IN	0,929	0,927	0,2
	20°	Y1-IN	0,905	0,903	0,2
	25°	Y1-IN	0,882	0,879	0,3
	30°	Y1-IN	0,857	0,855	0,3



The chamber positioning is very critical.

The axis of chamber must be perpendicular to the direction of wedge