

# B-CRATOS

## Wireless Brain-Connect inteRfAce TO machineS

### Machine Learning for BCIs

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ICTP - ADVANCED SCHOOL ON APPLIED MACHINE LEARNING

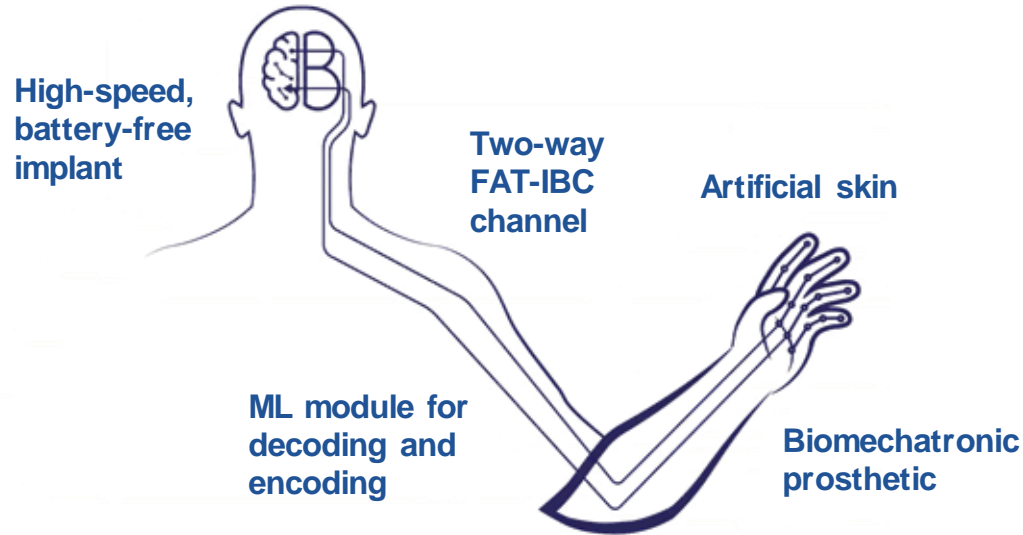
# Speaker introduction

- Theoretical physics Msc – University of Torino
- Computer Science PhD – University of Torino
  - Distributed training of DL models before it was cool
- A couple of years in CAE industry doing numerical/ML stuff
- Now I'm back to research **at Advanced Computing, Photonics and Electromagnetics research domain of LINKS Foundation,** in Torino
  - HPC (and some ML)
  - Quantum Computing



# Background – B-Cratos project

Applied Data Science: focus on application → context of research in a larger project



The goal is to develop a closed-loop BCI and to validate it with NHPs (Non-Human Primates), with the following technical objectives:

1. Proof-of-concept, high-speed, wireless brain implant capable of two-way communication without battery
2. General-purpose, high-speed intra-body communications technology (Fat-IBC)
3. **HPC based ML models deployed on embedded board for low-power inference and control**
4. Improvements of biomechatronic hand prosthesis
5. High-resolution sensorized skin

March 2021 – February 2025  
**FET-OPEN 4.7M EU funding**  
Partners from 5 countries  
Coordinated by University of Uppsala



# What is a BCI?

**The New York Times**

Despite Setback, Neuralink's First Brain-Implant Patient Stays Upbeat

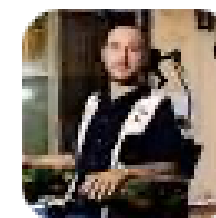
2 days ago • Christina Jewett



**WIRED**

Neuralink's First User Is 'Constantly Multitasking' With His Brain Implant

2 days ago • Emily Mullin



**Bloomberg**

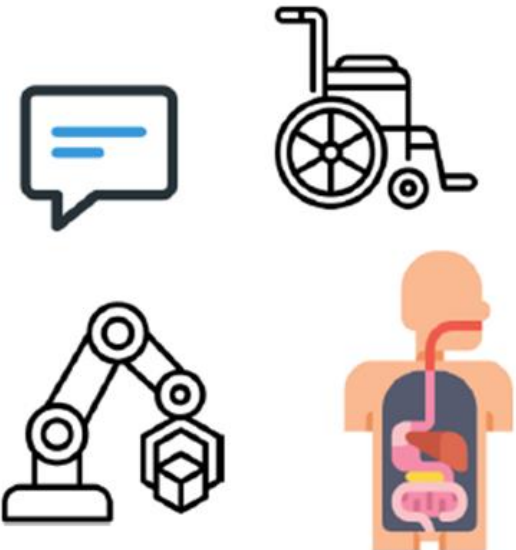
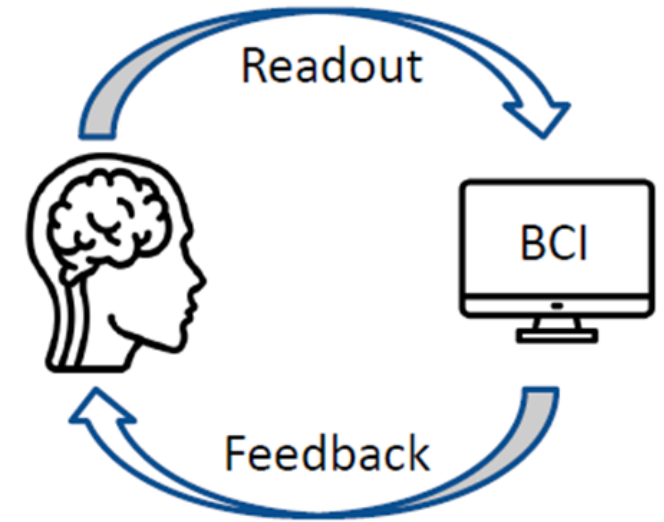
Podcast: What Neuralink's First Patient Is Thinking

3 days ago • Reyhan Harmanci

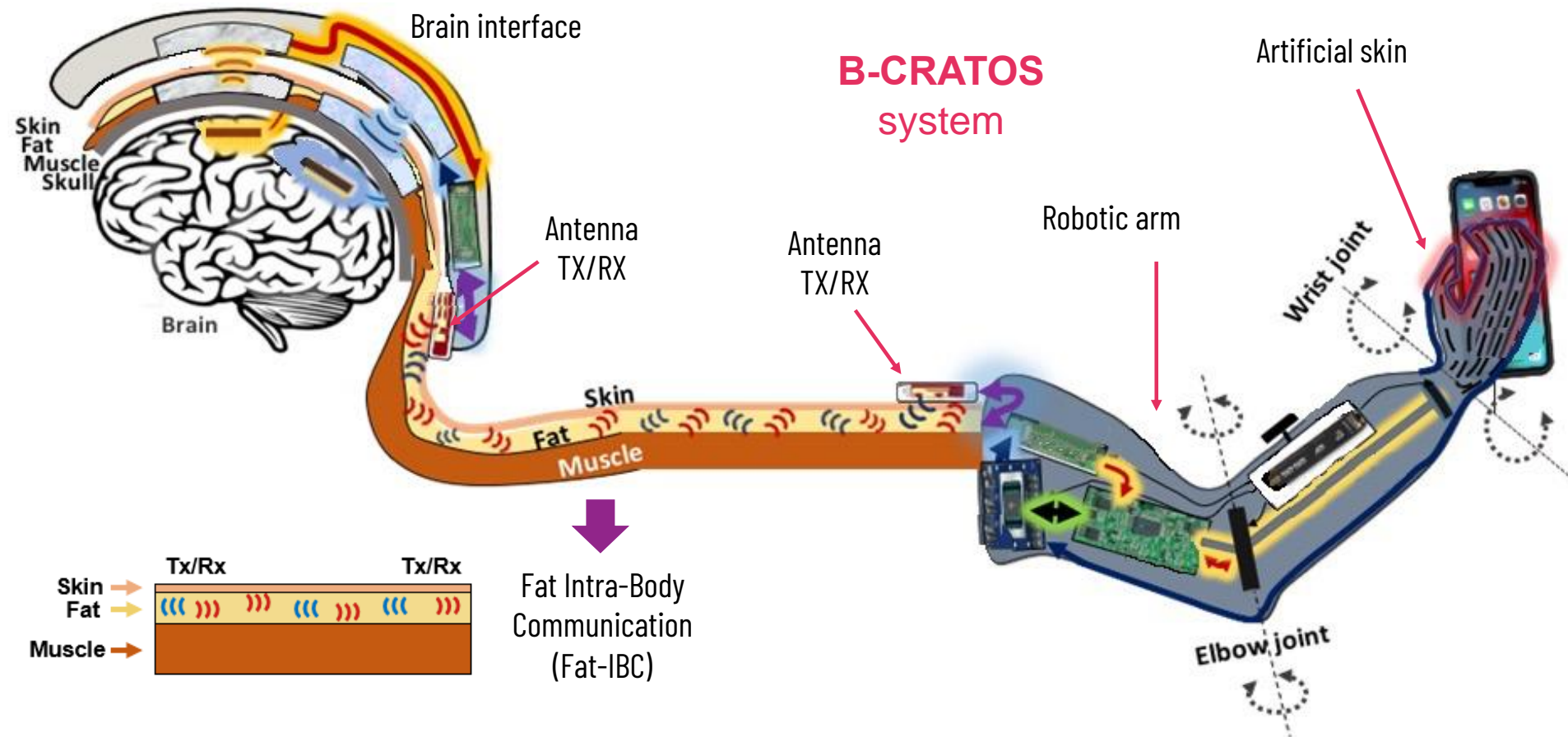


# What is a BCI?

- Brain-Computer Interface
  - A device that enables communication and control without movement (BNCI Roadmap, Horizon 2020)
  - i.e., **readout of brain activity**  
→ **action/control signals**
- “Closing the loop”: providing feedback to the brain
  - E.g., tactile stimulation



# Project Overview



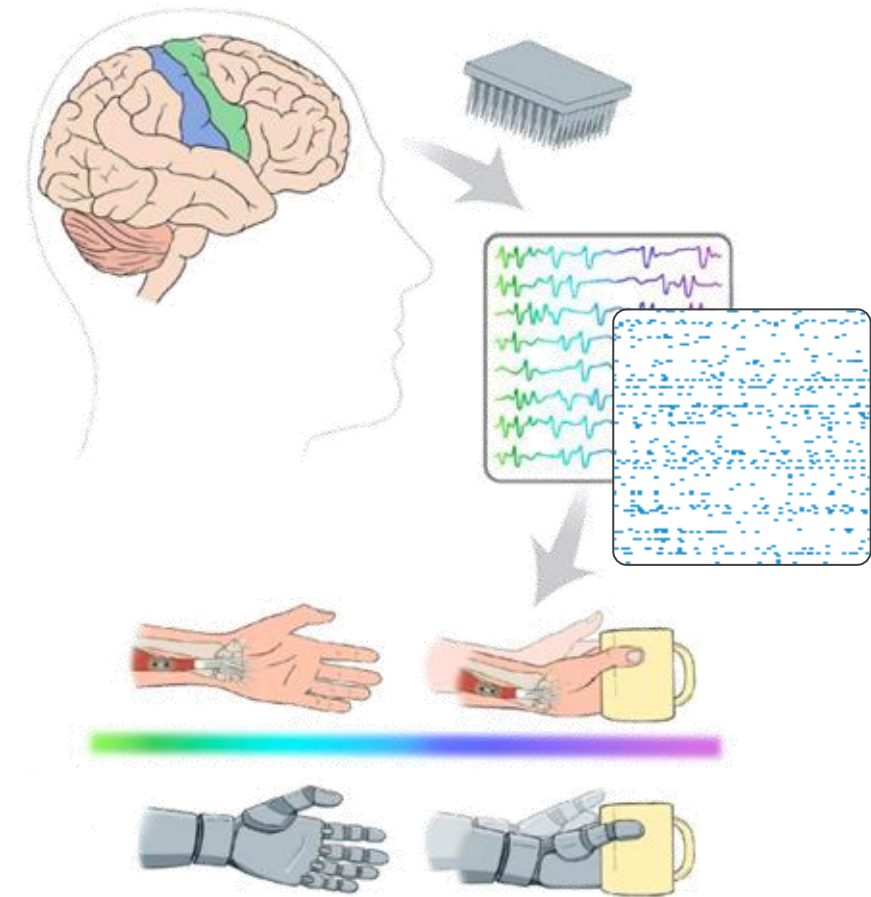
# Why are we discussing BCIs in an ML school?

- To translate brain signals into commands for a computer/prosthesis, we need some kind of model
- The typical approach in **neuroscience** is to **use very simple models** (linear classifiers, Kalman filters, etc.) because neuroscientists want interpretable models
  - to understand how the brain works
  - because they work for their purposes
- **ML can play a role → Neural decoding**
- **“The man was able to train his mind to use the device”**
  - <https://www.technologyreview.com/2022/03/22/1047664/locked-in-patient-bci-communicate-in-sentences/>
- The goal of BCIs is to improve the life of patients, more sophisticated models can improve the experience and go in the direction of reversing this paradigm

# Neural Decoding for Neuroprosthetics

## Overview

- **Goal: translate the signal from brain implants into commands for a prosthesis**
- Main steps
  - Brain electrodes pick up analogue signals from large neuron populations
  - Post-processing is applied to convert the signal to “spike-trains”: multi-channel time series of binary data
  - Decoding algorithm is applied to convert the signal to command for the prosthesis



From C. Pandarinath and S. J. Bensmaia, “The science and engineering behind sensitized brain-controlled bionic hands,” *Physiological Reviews*, p. physrev.00034.2020, Sep. 2021 doi: 10.1152/physrev.00034.2020. **Edited.**

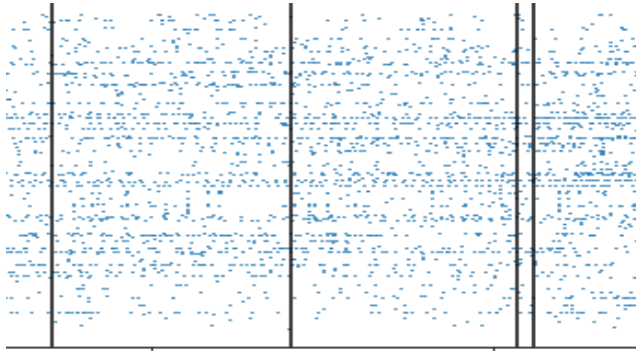




# Neural Decoding

State of the art

Neural  
signal



Decoder



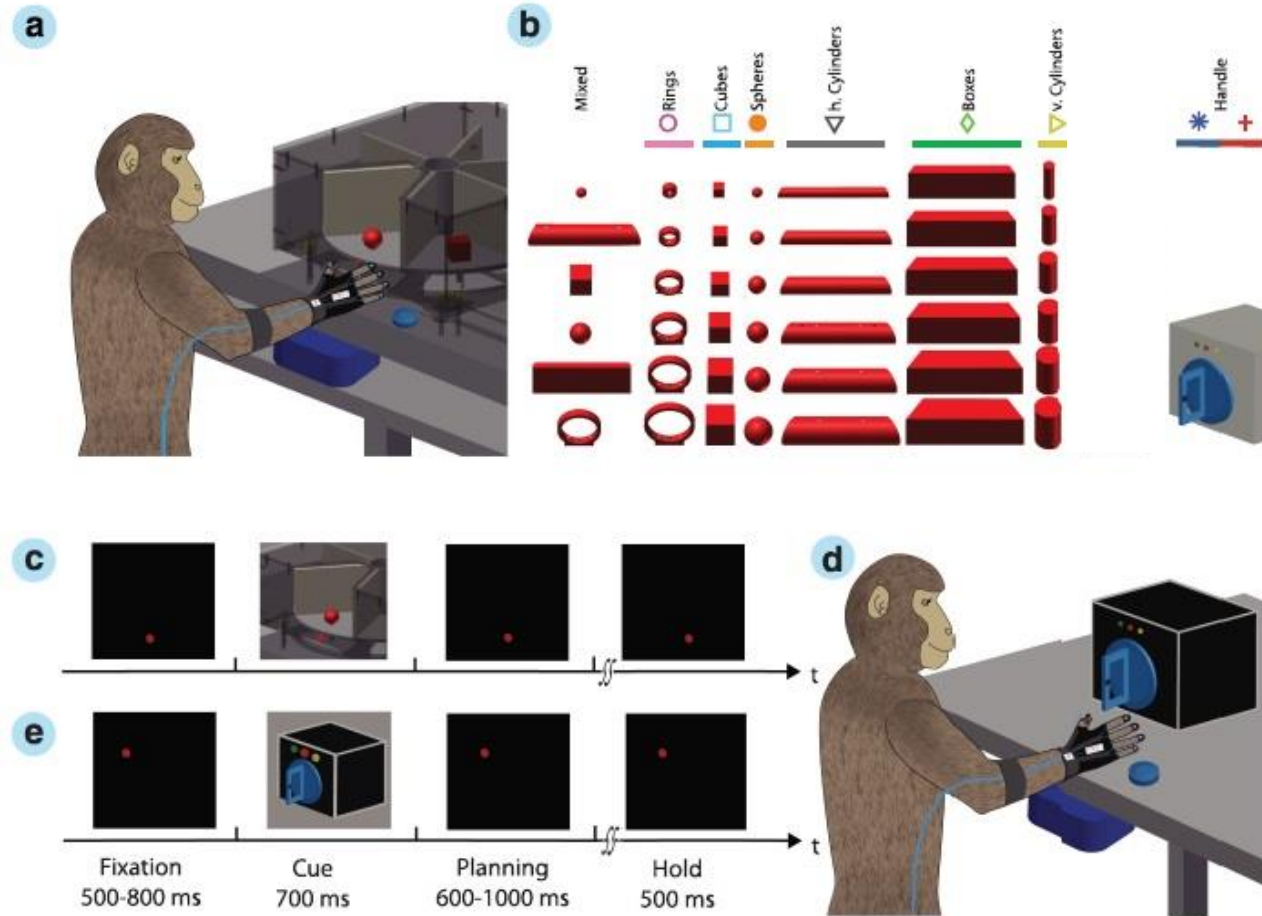
Intended  
outcome

- Off-line decoding is well understood, **real-time decoding is challenging**
- State-of-the-art models are simple: **Patient “learns to drive” the model**
  - Also reflects neuroscientist’s need for explainability
- Neural signal changes over time and requires daily re-training of models
- B-Cratos aims to **improve the overall accuracy of models and to re-use information across sessions**
  - Lower effort for patient, easier adoption, more natural usage
  - **Modern machine learning techniques can support this goal**

# Enough talking, let's get to the ML

No online data yet, but reference dataset was available

- Focused on a reference dataset provided by a partner (German Primate Center)
- Monkey trained for a grasping task
- Neural recording from multiple cortex regions
- Monkey grasping objects presented in sequence
- Objects grouped by shape and size, presented randomly
- 2 monkeys, 6 recording sessions (i.e., different days)
- **Learning Tasks**
  - Grasping phase detection
  - Object classification



S. Schaffelhofer, A. Agudelo-Toro, and H. Scherberger, "Decoding a Wide Range of Hand Configurations from Macaque Motor, Premotor, and Parietal Cortices," *Journal of Neuroscience*, vol. 35, no. 3, pp. 1068–1081, Jan. 2015, doi: [10.1523/JNEUROSCI.3594-14.2015](https://doi.org/10.1523/JNEUROSCI.3594-14.2015).

# Dataset structure

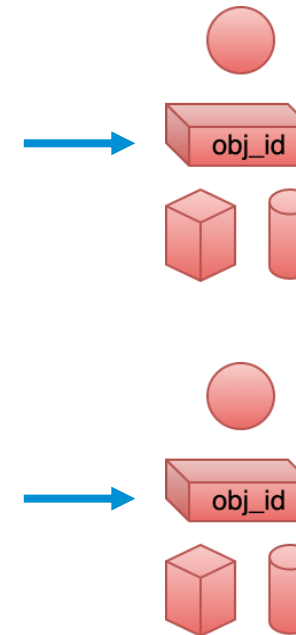
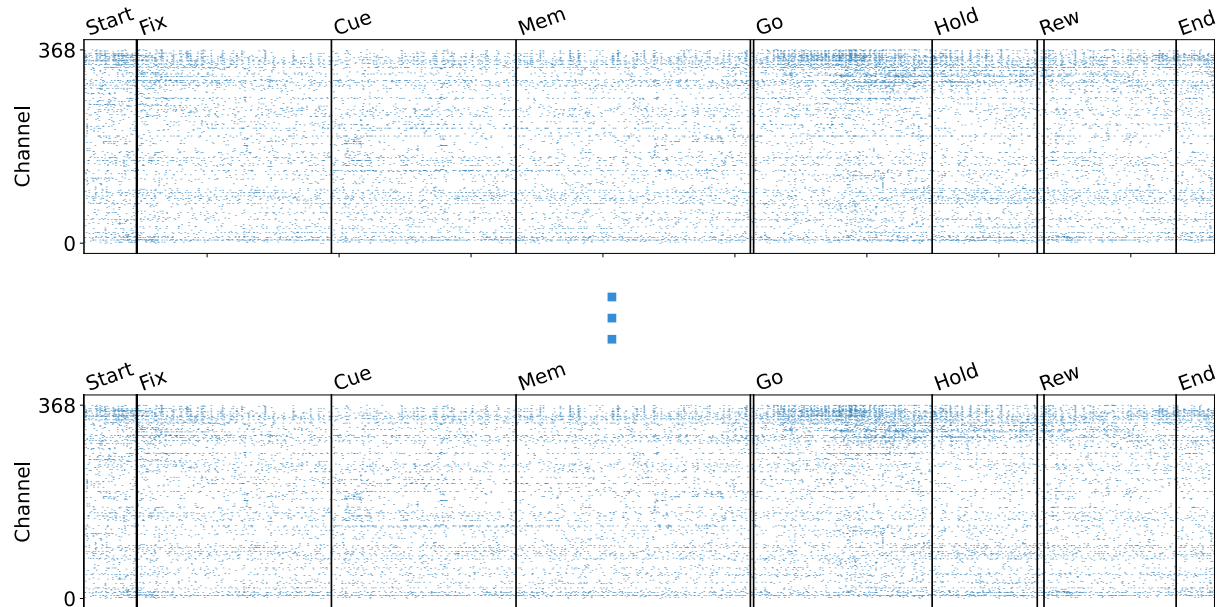
Recording sessions, trials, metadata

## Recording sessions



NHP identifier	Dataset identifier	# Channels	# Trials
M	MRec40	552	745
	MRec41	568	757
	MRec42	554	653
Z	ZRec32	391	687
	ZRec35	388	724
	ZRec50	369	610

Trials



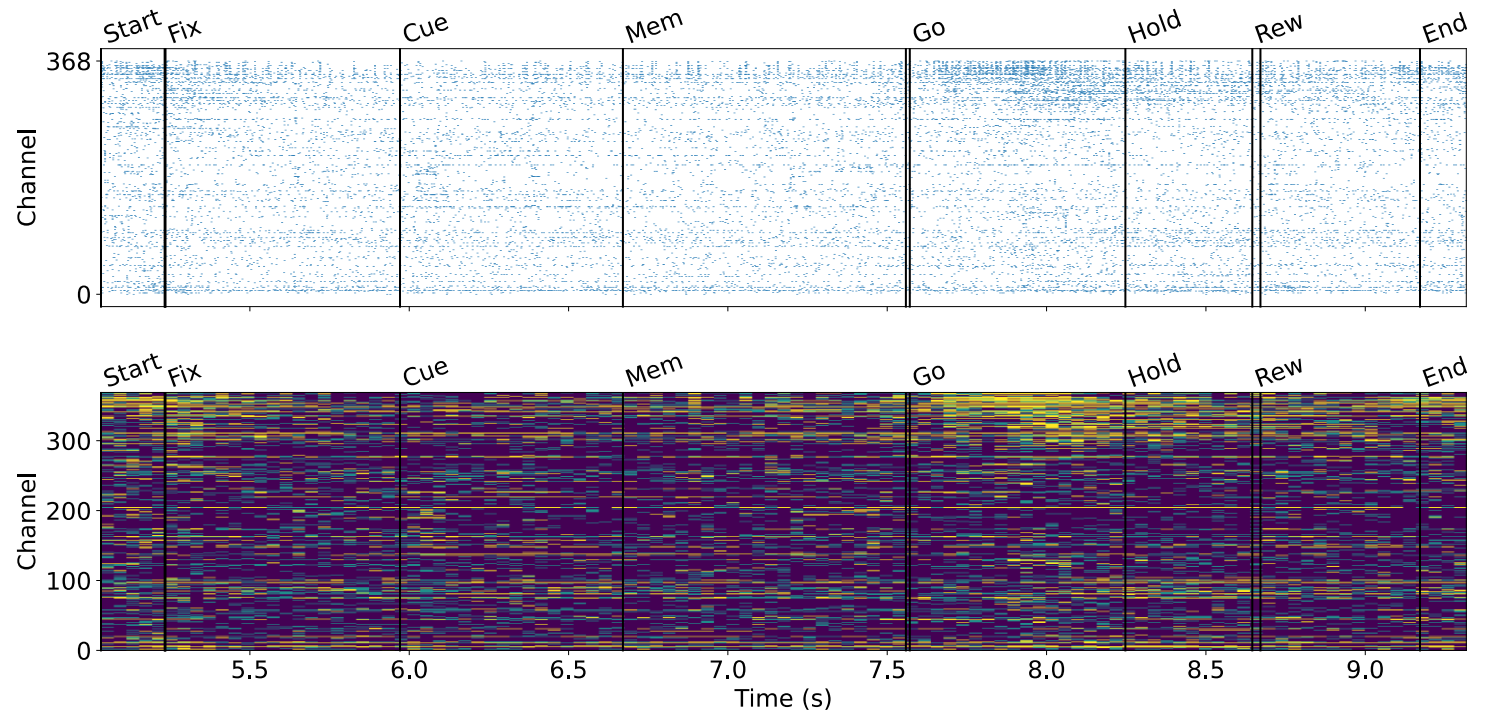
**50 objects**



# Pre-processing

## Time-discretization

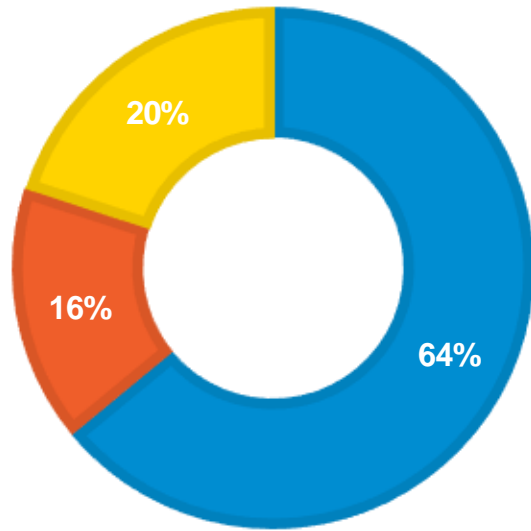
- Each trial discretised in bins of 40ms
- Results in dense matrix
  - *channels x time\_bins*
  - *Each bin contains the number of spikes*
- Time stamps associated to a bin
- Each matrix is Associated to object id



# Pre-processing

## Dataset split

■ Training ■ Validation ■ Test



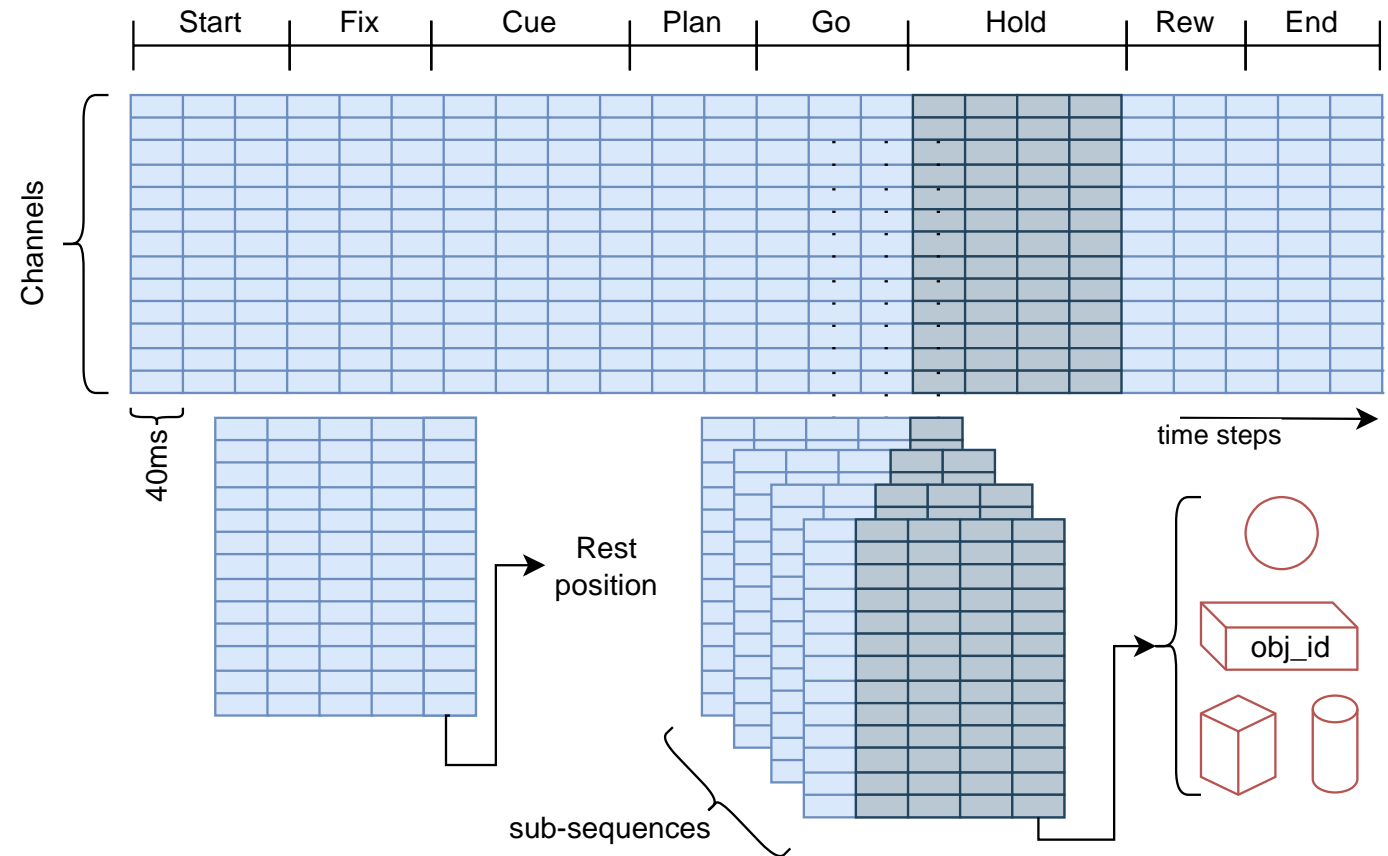
1. Classes are **de-duplicated** (i.e., same object in different groups)
2. Dataset is **split by trial**
  1. 80% training + validation, 20% test)
  2. stratified by class
3. Split is stratified by class
4. Under-represented class are removed (i.e., less than 3 trials per session)
5. Total of 39 classes left

# Pre-processing

## Sequence extraction

### Goal: simulate real-time decoding

1. Sliding windows extract sub-sequences of 12 bins
2. Grasp phase classification includes all data labelled with 0 (no grasp) and 1 (grasp)
3. Object classification includes only the sub-sequences in the grasp phase, labelled with object ID

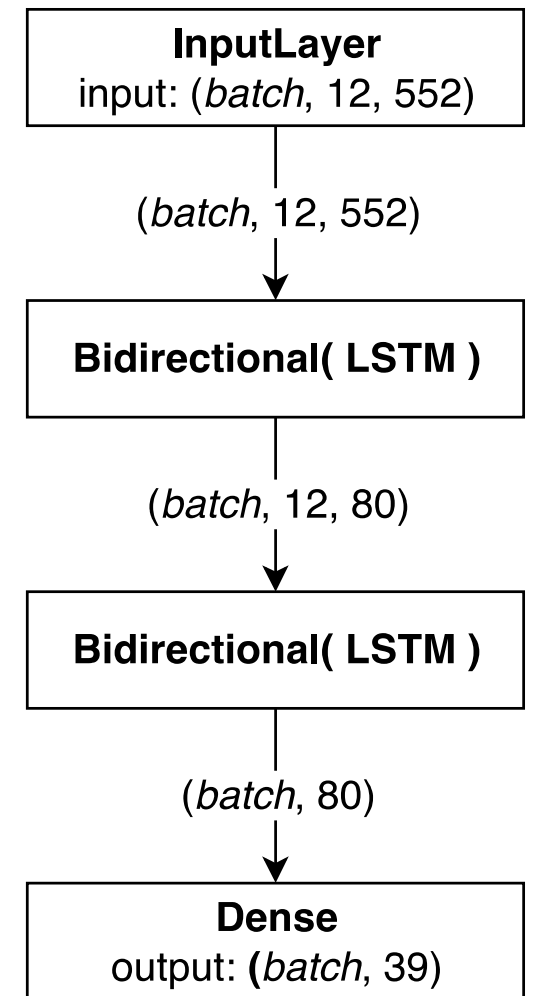


# Decoding approach

## Model selection

- LSTMs demonstrated good performance in literature
- Started from there (quite naïve in fact)
- **Bidirectionality** proved to be very effective
- Lots of **dropout** to prevent heavy overfitting
- Hyperparameter optimization

Hyperparameter	Values (L1=0.01, L2=0.01)	Selected	
		M	Z
LSTM layers	{ 1, 2, 3, 4 }	2	1
Hidden units	{ 16, 32, 40, 64 }	40	40
Dropout	{ 0, 0.2, 0.4, 0.6, 0.7, 0.8 }	0.8	0.7
Kernel regularisation	{ None, L1, L2, L1 + L2 }	L2	L2
Recurrent regularization	{ None, L1, L2, L1 + L2 }	L2	L1+L2
Initial learning rate	{ $10^{-3}$ , $2 \cdot 10^{-4}$ , $10^{-4}$ }	$10^{-3}$	$10^{-3}$



# Results

## Grasping phase detection

- Significant class imbalance here, with no grasp class ~10 times more represented than grasp class
- LSTM model reaches an accuracy of at least 98% for all datasets, the F1 score is always greater than 0.95
- Result relevant for a finite-state prosthesis control scenario
  - Each 40ms time step: predict prosthesis status (grasp vs. no-grasp)
  - 1% of unwanted movement for each time step
  - 0.1% of unresponsive prosthesis

(a) Confusion matrix for grasping phase detection (MRec40).

True	Predicted	
	rest	grasp
rest	12824	173
grasp	25	1347

Unwanted Movement ~1%

Unresponsive prosthesis ~0.1%

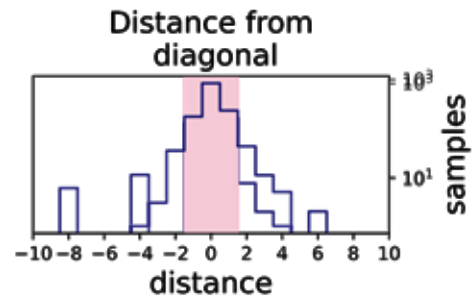
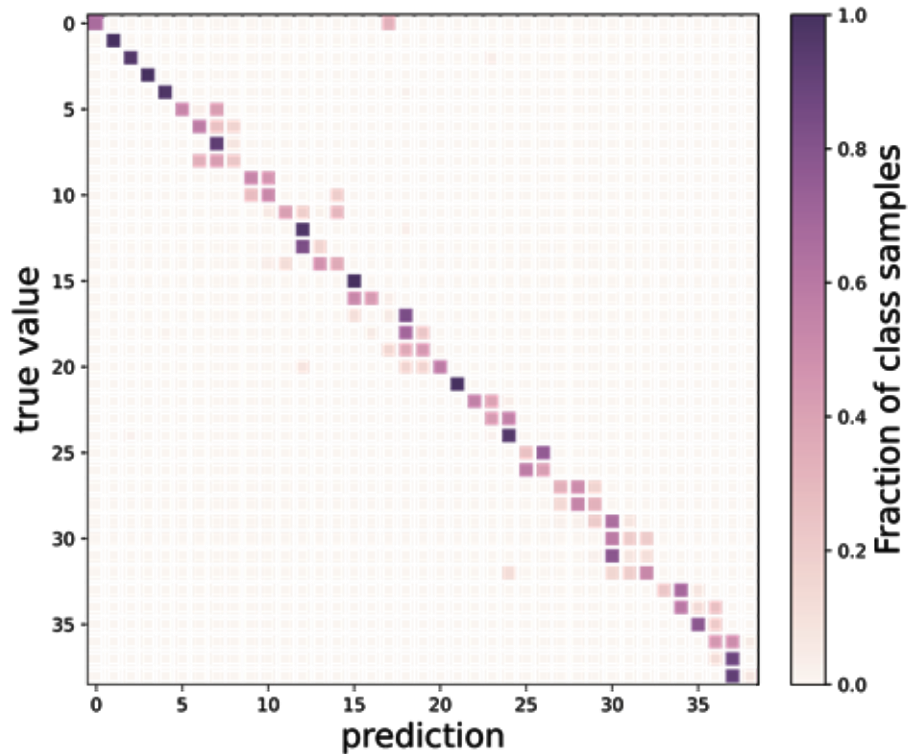
(b) Grasping phase detection accuracy metrics.

Dataset id	Accuracy	F1 score
MRec40	99%	0.96
MRec41	99%	0.96
MRec42	99%	0.97
ZRec32	99%	0.96
ZRec35	98%	0.96
ZRec50	98%	0.95



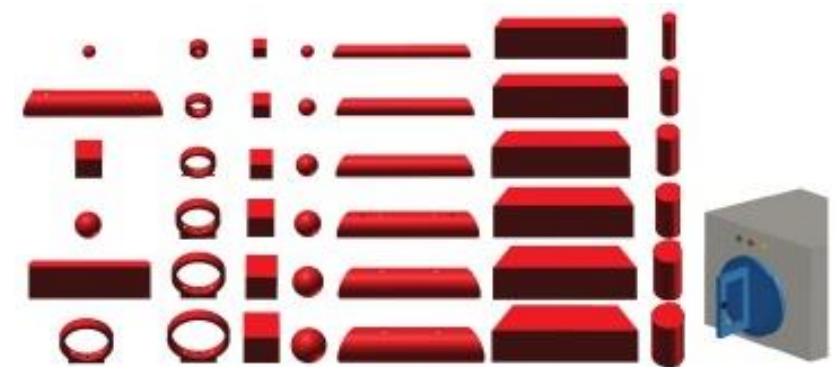
# Results

## Object classification



Accuracy: 61.0%  
Diagonal  $\pm 1$ : 98.5%

- Top 1% accuracy ranging from 61% to 74% across different sessions
- Neighbouring classes referred to similar objects
  - Relaxed accuracy defined as misclassification by 1 class (i.e., distance 1 from diagonal)



# Results

## Object classification – comparison with state of the art

Animal	Metric	Present work	Schaffelhofer, 2015	Fabiani, 2021
M	Accuracy	69.7 ± 4%	62.9 ± 3.6%	n/a
Z	Accuracy	62.3 ± 1.2%	61.4 ± 4.1%	n/a
Global	Accuracy	65.9 ± 4.9%	62%	22%
	Relaxed accuracy	94.4 ± 3.1%	86.5%	59%

- Schaffelhofer et al. report an average accuracy for the hold phase of 62% over a total of 10 recording sessions (against the six available for this work)
  - Offline naive bayesian classifier applied to the whole hold phase vs. sliding window
  - Validated with a leave-one-out (LOO) approach
  - Dataset fraction used for training was significantly higher
  - Significantly better (M) and slightly better (Z)
- accuracy results in a harder set-up. Significantly better relaxed accuracy
- Fabiani reported offline and online accuracy figures
  - This work outperforms both cases, despite the use of similar LSTM architectures
  - Improvement likely due to bidirectional networks and stronger regularization

# Results

## Robustness to reduction of training data

- Real life scenario involves frequent re-training, also during recording sessions
- Neuroscientist's requirement is to limit training to a minimum, and let the model work for most of the time
  - Even more relevant for patients
- Smaller training sets were evaluated
- The model is still outperforming the previous SotA down to 40% of training data

Training + validation set	Accuracy	Relaxed accuracy
80%	74.1%	98.3%
70%	70.1%	97.1%
60%	69%	93.7%
50%	62.8%	94%
40%	63.8%	92.8%
30%*	59.2%	87.5%
20%**	51%	81%

\* validation is 30% of training set to ensure at least one representative per class

\*\* validation is 40% of training set

# Remarks and future work

- LSTM can match and outperform previous approaches on a known dataset
  - More accurate prosthesis control can be enabled by modern architectures, at the expense of some explainability
- Results for relaxed accuracy are very promising for the final application
  - Continuous control of few degrees of freedom (regression on few variables)
  - Finite-state control of 5-6 grasp types (classification on fewer classes)

## Future work

- Neural data evolves with time: robustness/adaptability of models is key to reduce patients and physicians effort
- Fine-tuning with limited data already proven effective
- Semi-supervised training with usage data is an open problem, inputs from the community are welcome!

# Thanks for your attention!

## Acknowledgments

**CINECA**

