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Calibration of KAP Meters and CT Chambers

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## **CT chamber calibration**

CT chamber is often called a **pencil chamber** because its active volume is a thin cylinder 100 mm in length or sometimes longer





Partially irradiated (10% of its acive volume) Air kerma-length product,  $P_{KL}$ 

## !!!

The response of the active volume be uniform along its entire axial length
Calibration procedures

# **CT chamber calibration** kerma-length productchambei rectang. aperture monitor F plane of measurement

Use of an aperture (SLIT) to simulate the CT slice





## CT chambers are calibrated in the lab

## NOT in a CT scanner





The air kerma is first determined with the reference ionization chamber in the plane of measurement for the RQT radiation qualities.

Then the lead rectangular aperture is positioned in front of the users' chamber behind the transmission monitor chamber.

The outer dimensions of the aperture assembly shall be large enough to shield the whole of the chamber.

The separation of the lead aperture from the point of test must be precisely known.







The width, w, of the aperture should be between 20 mm and 50 mm and be known to within 0.01 mm.

In the plane of measurement the width of the field is :  $w \cdot dr / da$ 

$$N_{P_{KL}} = \frac{K_i \cdot L}{M} \qquad N_{P_{KL,Q}} = \frac{K_i^{ref}}{M^{CT} \cdot k_{TP}^{CT}} \cdot \left(\frac{w \cdot d_r}{d_a}\right) \qquad \begin{array}{l} N_{PKL,Q} \text{ calibration} \\ \text{ coefficient it terms of} \\ \text{ kerma-length product } P_{KL} \end{array}$$

M : dosimeter reading

AEA



When a **monitor chamber** is used :

$$\overline{N}_{P_{KL,Q}} = \left(\frac{m^{m} \cdot k_{\text{TP}}^{m} \cdot N_{Q}^{m}}{M^{CT} \cdot k_{\text{TP}}^{CT}}\right) \cdot \left(\frac{w \cdot d_{r}}{d_{a}}\right)$$

where :

 $N_Q^m$ , is the calibration coefficient of the monitor chamber in terms of air kerma for radiation quality Q in the plane of measurement

m<sup>m</sup> is the reading of the monitor chamber

M<sup>CT</sup>, is the reading of the CT chamber



## **CT chamber calibration**

Radiation quality	X ray tube voltage	Added filtration	Nominal first half- value layer
	kV		mm Al
RQT 8	100	RQR 8 + 0.2 mm Cu	6.9
RQT 9*	120	<b>RQR 9 + 0.25</b> mm Cu	8.4
RQT 10	150	RQR 10 + 0.3 mm Cu	10.1



## **CT chamber calibration**

 $N_{P_{KL,Q}} = \frac{K w d_r}{M \cdot k_{TP} \cdot d_r} \qquad \text{mGy mm / digit (reading)}$ 



## Then in a CT at clinics :

 $C_{a,100} = \frac{1}{NT} \overline{M} (N_{P_{KL},Q_0} k_Q k_{TP})$ 

 $C_{\text{PMMA,100,c}} = \frac{1}{NT} \overline{M}_{c} N_{P_{\text{KL}},Q_{0}} k_{Q} k_{\text{TP}}$ 



## **KAP meter calibration**

the detector mounted on the tube housing is "transparent" to X rays





Partially irradiated Air kerma-area product,  $P_{KA}$ 

 $P_{KA}$  is the same at any distance from focus

KAP meters use :

- fluoroscopy,
- general radiography
- dental radiography equipment

Provide useful information about patient doses in relation to examination procedures





in calibration of a field KAP meter with a REFERENCE KAP meter

the INCIDENCE radiation to the reference KAP meter

interests

in patient dosimetry the TRANSMITTED radiation interests



Depending on the application the **INCIDENCE** or the **TRANSMITTED** radiation is of interest

## **KAP meter calibration**

N = True quantity / reading N =  $P_{KA}^{ref}$  / reading

Two methods of KAP meter calibration :

 Determination of the air kerma K<sub>i</sub> and the irradiation area, A "kerma-area product" method (or "beam area" (BA) method)

2. Use of a reference KAP meter, which measures directly the  $P_{KA}^{ref}$ 

"KAP" method

$$P_{KA}^{ref} = K_i \cdot A$$

 $P_{KA}^{\quad ref}$ 







## **KAP meter calibration :** Calibration at the laboratory



A circular or square lead aperture of 40 - 60 mm

Known of exact aperture dimension, w

Aperture and plane of measurement  $(KAP) \sim 50 \text{ mm}$ 

Pos 1 : KAP for beam attenuation Pos 2 : reference point of measurement







## KAP calibration in situ : "kerma-area" method, Transmitted radiation





All X rays, both focal and extra focal, pass through KAP's sensitive volume.



## KAP calibration in situ : "kerma-area" method, Transmitted radiation



$$N_{P_{KA},Q} = \frac{M_Q^{ref}}{M_Q^{KAP}} N_{K,Q_0}^{ref} k_Q A_{nom}$$

### **Over-couch installation**

- 1. Reference detector on the central axis at 200 mm above the couch (table top)
- 2. Collimate the X ray beam to 100 mm x 100 mm.
- 3. Expose the detector and the KAP meter using all combinations of tube voltage and total filtration occurring in the clinical applications (beam quality *Q*).
- 4. Register signals from the KAP meter, and the reference dosimeter.
- 5. Remove the reference chamber and position a film-screen cassette (or a direct film) CR cassette perpendicularly to the central axis at the position of the reference detector.
- 6. Expose the film-screen cassette or the film. The maximum optical density must not exceed 0.5 optical density units (OD).
- 7. Develop the film and determine the nominal beam area, *A*, as the area contained within 50% of the maximum optical density.

## KAP calibration in situ : "kerma-area" method, Transmitted radiation

## Under-couch installation

The detector should be positioned on the table top to reflect the beam attenuation and scattering by the table.

The air kerma-area product value should be representative of that in the beam incident on the patient and thus take into account the attenuation in the couch as well as the scatter from the couch that may reach the patient.

The couch may reduce by about 15%–30 % compared to the over-couch situation.





## Calibration using reference KAP meter, KAP METHOD : Transmitted radiation



$$N_{P_{KA},Q}^{KAP} = \frac{M_Q^{KAP_{ref}}}{M_Q^{KAP}} N_{P_{KA},Q_0}^{ref} \cdot k_Q^{KAP_{ref}}$$



## KAP calibration "kerma-area" method

## **Calibration using diagnostic dosimeter**

- This method is usually more useful in clinics because proper dosimeter is easily available and its energy dependence is typically small.  $\uparrow$
- Position of focal spot is not always marked clearly.  $\downarrow$
- In some cases the determination of irradiation area and measurement distance was also difficult and uncertain.
- More and more digital systems are available and estimating field size from softcopy adds an additional uncertainty in the measurement.
- In this method an approximation of KAP quantity is used as a reference value and errors arising from in homogeneity in the field will increase the uncertainty of the calibration (Larsson et al)



From Toroi et al, STUK, 2008

## **Calibration using reference KAP meter : TANDEM method**

## Advantages

- The reference KAP value is measured according to the definition.
- Problems arising from the nonuniformities of the x-ray field is avoided.
- Independent of the measurement of distance and the field size.
- Calibration is easy to do.
- No uncertainties from distance or area measurements.

## Disadvantages

- Extra KAP meter is needed.
- Ccomprehensive calibration for reference meter is needed.
- Inaccuracies if radiation quality is not well known
- Low values because of the small field



From Toroi et al, STUK, 2008

## **Method comparison**



## **Radiation quality dependence of KAP meters**

- KAP meters have large dependence on radiation quality.
- Adjusting the meter correctly with one radiation quality might achieve accuracy < 20%
- Half-value layer (HVL) can not describe alone radiation quality dependence.
- Radiation qualities used in clinical practice should be covered in calibration.
- Calibration should at least be done for all used filtrations and some chosen tube voltages.



From Toroi et al, STUK, 2008

## **Radiation quality dependence of KAP meters**





## **Qualities for KAP calibration**

Filtration	Tube voltage	HVL
inherent 3.5 mm Al plus	kVp	mm Al
0.1 mm Cu	50	2.45
0.1 mm Cu	70	3.92
0.1 mm Cu	90	5.22
0.1 mm Cu	120	6.68
0.2 mm Cu	50	2.68
0.2 mm Cu	70	4.68
0.2 mm Cu	90	6.50
0.2 mm Cu	120	8.11
0.3 mm Cu	50	3.02
0.3 mm Cu	70	5.42
0.3 mm Cu	90	7.27
0.3 mm Cu	120	9.04



## **Radiation quality dependence of KAP meters**



From Toroi et al, STUK, 2008

