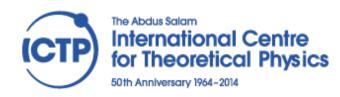
# **ORGAN MOTION MANAGEMENT**





CARLO CAVEDON MEDICAL PHYSICS UNIT VERONA UNIVERSITY HOSPITAL - ITALY

ICTP SCHOOL ON MEDICAL PHYSICS FOR RADIATION THERAPY TRIESTE – ITALY – 16 APR 2015



#### ORGAN MOTION IN RADIATION ONCOLOGY

### - respiratory motion

- pseudo-regular motion — predictable in a short interval (50-500 ms)

#### - skeletal-muscular motion

- irregular motion – can be controlled

#### - cardiac motion

- (pseudo-)regular motion — generally not explicitly accounted for in RT

#### - gastrointestinal motion

- unpredictable – can be partly limited

## - genitourinary system - e.g. bladder filling

- large displacements - can be partly limited

### **RESPIRATORY MOTION IN RADIATION ONCOLOGY**

**AAPM REPORT NO. 91** 



# The Management of Respiratory Motion in Radiation Oncology

Report of AAPM Task Group 76

July 2006

# **RESPIRATORY MOTION** – organs that move with respiration

**SHALLOW BREATHING RANGE OF MOTION** 

- **lung** up to 50 mm

- esophagus

- **liver** up to 40 mm

- pancreas up to 35 mm

- breast

- prostate (!)

- **kidneys** up to 40 mm

- ...

## **RESPIRATORY MOTION IN RADIATION ONCOLOGY**

Table 2. Lung tumor-motion data. The mean range of motion and the (minimum-maximum) ranges in millimeters for each cohort of subjects. The motion is in three dimensions (SI, AP, LR).

Observer	Direction		
Observer	SI	AP	LR
Barnes <sup>85</sup> : Lower lobe	18.5 (9-32)		
Middle, upper lobe	7.5 (2-11)		
Chen et al.84	(0-50)		
Ekberg et al. <sup>26</sup>	3.9 (0-12)	2.4 (0-5)	2.4 (0-5)
Engelsman et al. <sup>28</sup> :			
Middle/upper lobe	(2-6)		
Lower lobe	(2-9)		
Erridge et al. <sup>101</sup>	12.5 (6-34)	9.4 (5-22)	7.3 (3-12)
Ross <sup>76</sup> : Upper lobe		1 (0-5)	1 (0-3)
Middle lobe		0	9 (0–16)
Lower lobe		1 (0-4)	10.5 (0-13)
Grills et al. <sup>91</sup>	(2-30)	(0-10)	(0-6)
Hanley et al. <sup>77</sup>	12 (1-20)	5 (0-13)	1 (0-1)
Murphy et al.87	7 (2-15)		
Plathow <sup>220</sup> : Lower lobe	9.5 (4.5-16.4)	6.1 (2.5-9.8)	6.0 (2.9-9.8)
Middle lobe	7.2 (4.3-10.2)	4.3 (1.9-7.5)	4.3 (1.5-7.1)
Upper lobe	4.3 (2.6-7.1)	2.8 (1.2-5.1)	3.4 (1.3-5.3)
Seppenwoolde et al. <sup>67</sup>	5.8 (0-25)	2.5 (0-8)	1.5 (0-3)
Shimizu et al.52		6.4 (2-24)	
Sixel et al. <sup>92</sup>	(0-13)	(0-5)	(0-4)
Stevens et al. <sup>66</sup>	4.5 (0-22)		

AP: anterior-posterior; LR: left-right; SI: superior-inferior.

## **RESPIRATORY MOTION IN RADIATION ONCOLOGY**

**Table 3.** Abdominal motion data. The mean range of motion and the (minimum–maximum) ranges in millimeters for each site and each cohort of subjects. The motion is in the superior–inferior (SI) direction.

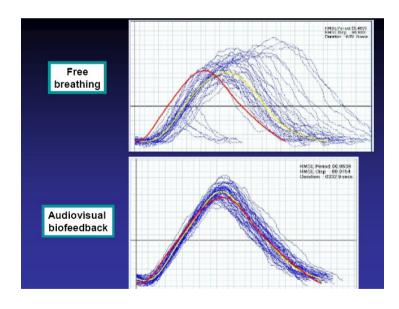
Site	Observer	Breathing mode	
		Shallow	Deep
Pancreas	Suramo et al. <sup>74</sup>	20 (10–30)	43 (20–80)
	Bryan et al.75	20 (0–35)	
Liver	Weiss et al.89	13 +/- 5	
	Harauz et al.90	14	
	Suramo et al. <sup>74</sup>	25 (10–40)	55 (30–80)
	Davies et al. <sup>68</sup>	10 (5–17)	37 (21–57)
Kidney	Suramo et al.74	19 (10–40)	40 (20–70)
	Davies et al. <sup>68</sup>	11 (5–16)	
Diaphragm	Wade <sup>80</sup>	17	101
	Korin et al. <sup>79</sup>	13	39
	Davies et al. <sup>68</sup>	12 (7–28)	43 (25–57)
	Weiss et al.89	13 +/- 5	
	Giraud et al. <sup>78</sup>		35 (3–95)
	Ford et al.86	20 (13–31)	

### **SOURCES OF INFORMATION – RESPIRATORY MOTION**

- radiography (e.g. double exposure or cine)
- fluroscopy (with or without fiducial markers)
- ultrasound
- CT and 4D-CT (amplitude- or phase-based / prospective or retrospective / ...)
- MR and 4D-MR
- PET and 4D-PET

#### MITIGATION OF MOTION AND MOTION IRREGULARITY

- patient training
- audiovisual feedback
- oxygen administration?



	Air	O <sub>2</sub>
Breath Hold time (sec)	20 (11-40)	100 (85-230)
% O <sub>2</sub> Pre BH	95% (90-97)	100%
%O <sub>2</sub> After BH	94%(90-97)	100%

M Romano, C Cavedon, A Porcaro, M Palazzi, M Gabbani, N Marciai, A D'Amico, S Dall'Oglio, F Pioli, MG Giri, A Grandinetti, "Does pre-radiation oxygen breathing prolong deep inspiration breath hold?" ASTRO meeting 2013

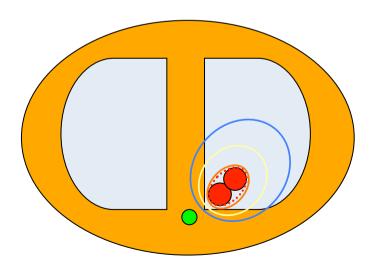
R George et al., "Audio-visual biofeedback for respiratory-gated radiotherapy: Impact of audio instruction and audio-visual biofeedback on respiratory-gated radiotherapy", Int J Rad Onc Biol Phys 65, 924-933 (2006)

# RESPIRATORY MOTION – 5 MAJOR STRATEGIES FOR MANAGEMENT

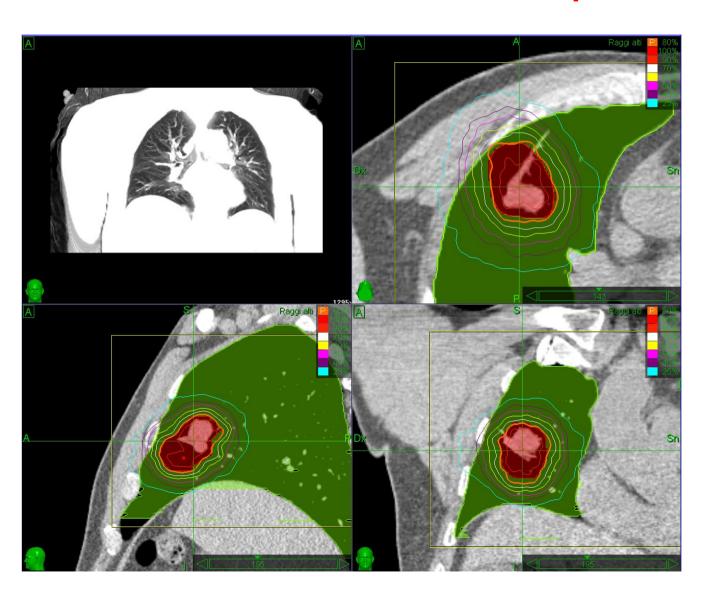
- motion encompassing techniques
- respiratory-gating techniques
- breath-hold techniques
- forced shallow-breathing techniques
- respiration-synchronized techniques (tracking)

#### **RESPIRATORY MOTION - IMPLICIT MANAGEMENT**

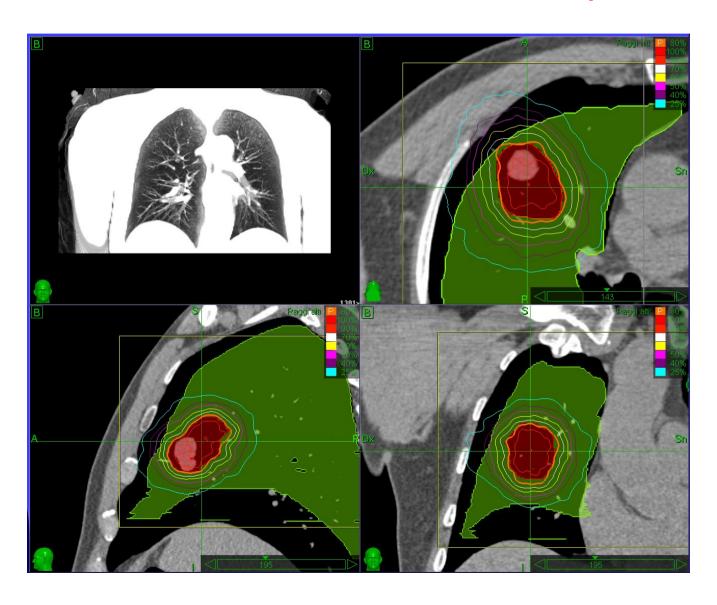
- motion encompassing techniques
  - concept: treat the whole volume defined by the envelope of positions during respiration
- ITV = internal target volume (ICRU 62) = CTV+IM



# **MOTION ENCOMPASSING – EXAMPLE - expiration**

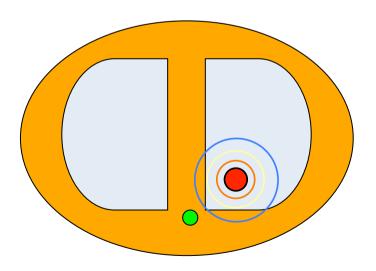


# **MOTION ENCOMPASSING – EXAMPLE - inspiration**

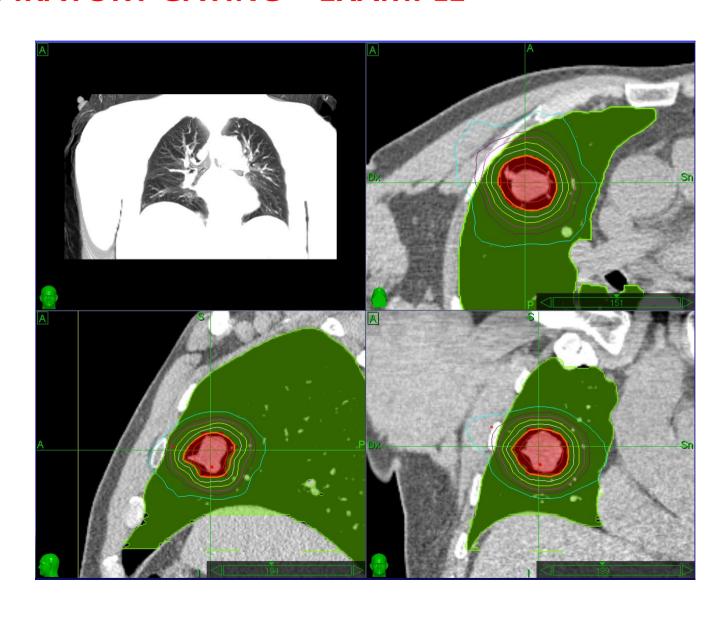


## **RESPIRATORY MOTION – EXPLICIT MANAGEMENT**

- respiratory gating techniques
  - concept: treat only when the target is within the "gating window"
  - volume / normal tissue preservation
  - long treatment times

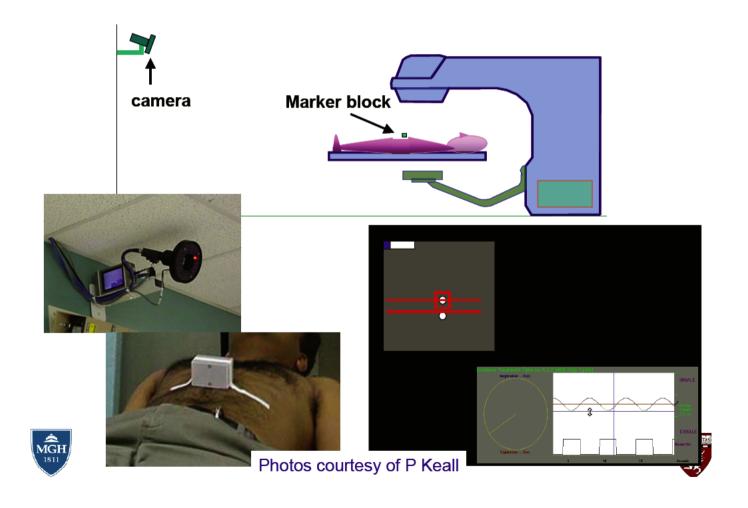


# **RESPIRATORY GATING – EXAMPLE**



# **RESPIRATORY GATING**

- surrogate signal needed to describe motion in real time



# **RESPIRATORY GATING – need for surrogate signal**

 possible inaccuracy from the relation between tumor motion and surrogate signal

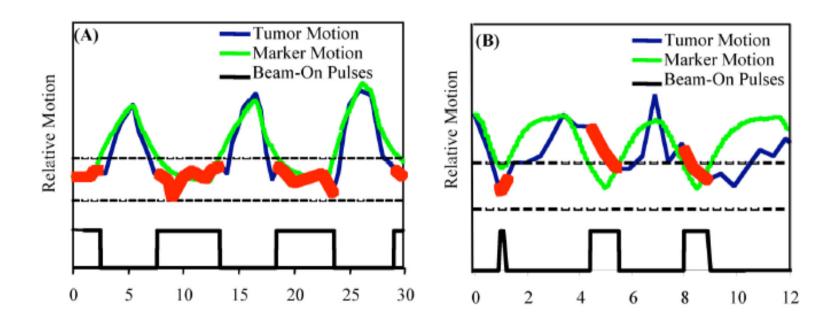
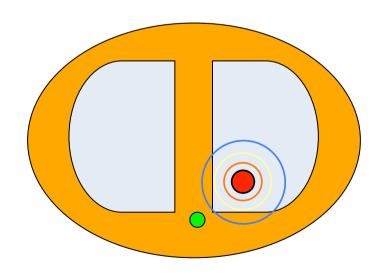


Figure 7. Comparison of external marker block motion with internal motion of the clinical target volume (CTV) for a patient with (a) no phase shift and (b) a patient with significant phase shift. The respiratory gating thresholds are set using the external marker block motion. The beam-on pulses are highlighted in red over the internal CTV position. [Reproduced from reference 227: Int J Radiat Oncol Biol Phys, vol 48, "Clinical experience with a commercial respiratory gating system." C. R. Ramsey, D. D. Scaperoth, and D. C. Arwood, pp. P164-165. © 2000, with permission from Elsevier.]

#### **RESPIRATORY MOTION – EXPLICIT MANAGEMENT**

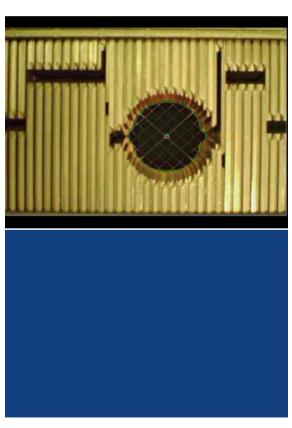
- respiratory tracking (synchronized) techniques
  - concept: redirect beam to the target position in real time
  - volume / normal tissue AND treatment time preservation



# **RESPIRATORY MOTION – EXPLICIT MANAGEMENT**

# - respiratory tracking (synchronized) techniques

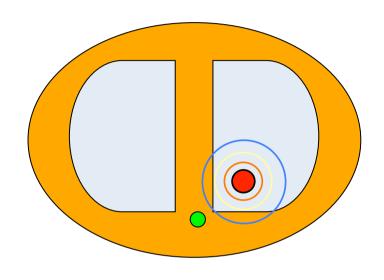


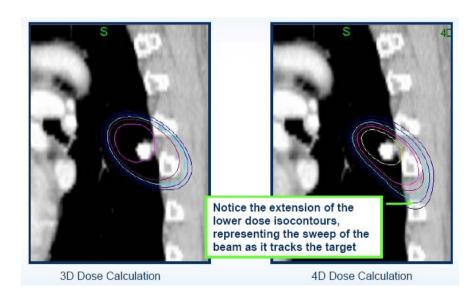


#### **RESPIRATORY TRACKING**

#### - need for 4D PLANNING

 planning on one phase does not guarantee dosimetric accuracy on nearby tissues





- 4D planning requires a complete description of the respiratory phase (e.g. 4DCT – see below)

# MOTION CONTROL IN IMAGING FOR TREATMENT PLANNING AND TREATMENT VERIFICATION

- need for **temporal coherence** between **imaging** for treatment planning and **treatment** administration
- imaging shall describe the treatment condition
- quantitative imaging (e.g. BTV based on SUV map)
  shall account for motion in order to avoid
  quantification errors

# MOTION CONTROL IN IMAGING FOR TREATMENT PLANNING AND TREATMENT VERIFICATION





**Figure 1.** Coronal views of CT scans of the same patient taken during free breathing (FB) (a) and with respiratory-gated scanning at exhale (b). [Reproduced from reference 53: P. J. Keall, V. R. Kini, S. S. Vedam, and R. Mohan, "Potential radiotherapy improvements with respiratory gating," *Australas Phys Eng Sci Med* 25(1):1–6, Figure 1. © 2002, with permission from APESM.]

- effect of motion on a free-breathing patient (CT left) and at exhale (right)

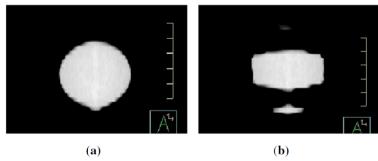


Figure 2. Coronal views of CT scans of a static sphere (a) and a sinusoidally moving sphere (b) (2-cm range of motion and a 4-second period). [Reproduced from reference 56: S. S. Vedam, P. J. Keall, V. R. Kini, H. Mostafavi, H. P. Shukla, and R. Mohan, "Acquiring a four-dimensional computed tomography dataset using an external respiratory signal," *Phys Med Biol* 48(1):45–62, Figure 1. © 2003, with permission from IOP Publishing Limited.]

- static sphere seen at CT (left) and effect of sinusoidal motion (right)

# **4D-CT:** principle



# **4D-CT:** modes of operation

# - prospective acquisition

- x-ray on only in the phase chosen for acquisition (e.g. full exhale)
- dose sparing limited information
- useful e.g. in breath-hold treatment

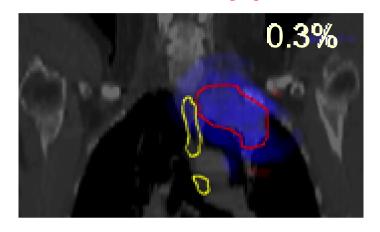
# - retrospective sorting

- redundant acquisition "a posteriori" sorting
- higher dose -full information
- necessary e.g. for 4D planning and to estimate the full envelope of positions – tumor trajectory

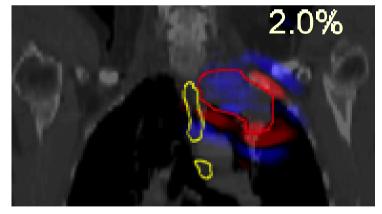
#### 4D-CT: how to use the information

- information from 4D-CT used for planning shall be **coherent with the delivery technique**, e.g.:
  - free-breathing treatment => MIP or other method to estimate envelope of positions
  - gating and breath-hold: use the phase(s) that will be used to treat
  - tracking: use all information for 4D planning

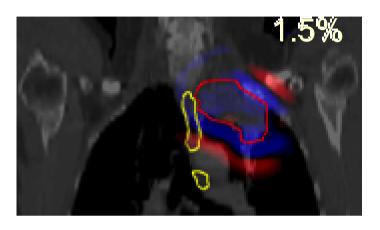
# **4D-CT:** how many phases?



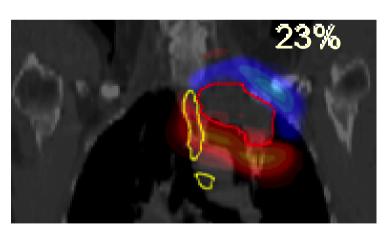
11 Phases - 6 Phases



11 Phases - AVE Phase



11 Phases - 2 Phases



11 Phases - Exhale

Courtesy Mihaela Rosu, Virginia Commonwealth Univ.

#### **4D-MR:** methods

- **4D-MR** is less frequently used for RT treatment planning than 4D-CT

#### - Breath-hold

- long acquisition times
- poor reproducibility
- dynamic behaviour might be poorly described in breath-hold

### - Cine-MR / Echo Planar Imaging (SSh, EPI, ...)

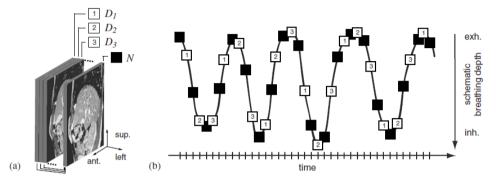
- poor spatial resolution
- artifacts at tissue interfaces

#### - 4D-MR - sorting

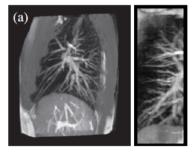
- external surrogate: volume, strain-gauge, IR markers ...
- internal surrogate: pencil-beam excitation, 2D slice-stacking
- generally available as phase-based (limited TR => limited T2 weighting)

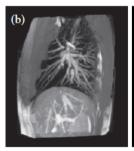
#### **4D-MR:** methods

- "navigator" sagittal slice
- sorting based on diaphragm position and vascular details
- axial slice acquisition at 2.8 Hz
- acquisition time ~ 1h (200 frames/slice)



**Figure 1.** (a) Sagittal slices covering the volume of interest. One dedicated slice *N* is used as navigator slice for image sorting. (b) Interleaved acquisition of data and navigator frames.





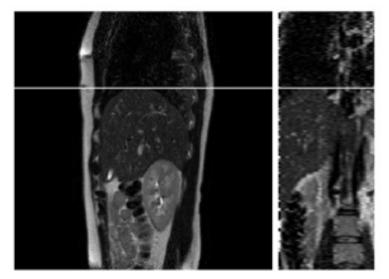


**Figure 6.** Sagittal and coronal maximum intensity projections after 3D interpolation showing the right part of the lung at (a) inhalation and (b) exhalation.

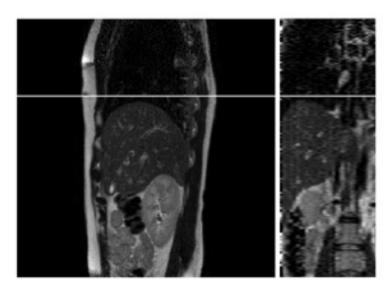
- very good temporal resolution
- generates deformation maps that can be used in CT etc.
- potentially useful for *dose tracking* in treatment adaptation
- sensitive to breathing irregularities
- not clinically available yet with full functionality

#### **4D-MR:** methods

- 4D-MRI in RT is constantly growing
- generally phase-based triggering => T1-weighting only (limited TR comparable to breathing cycle => non applicable to new quantitative techniques)
- recent studies on amplitude-based triggering (strain gauge) => T2 weighting



max expiration



max inspiration

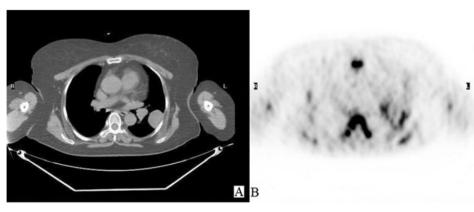
Y Hu, SD Caruthers, DA Low, PJ Parikh, S Mutic, "Respiratory Amplitude Guided 4-Dimensional Magnetic Resonance Imaging", Int J Radiation Oncol Biol Phys, Vol. 86, No. 1, pp. 198e204 (2013)

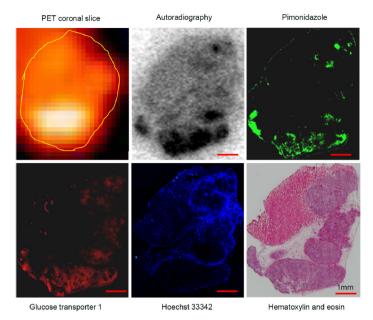
# **PET-CT:** quantitative imaging

- reference volumes based on SUV (<sup>18</sup>F-FDG)
- imaging of hypoxia (<sup>18</sup>F-MISO, <sup>64</sup>Cu-ATSM, ...)
- cell proliferation (<sup>18</sup>F-FLT)
- transport of amino acids synthesis of proteins (<sup>18</sup>F-FET)
- neo-angiogenesis

- ...

#### => dose-painting by numbers?





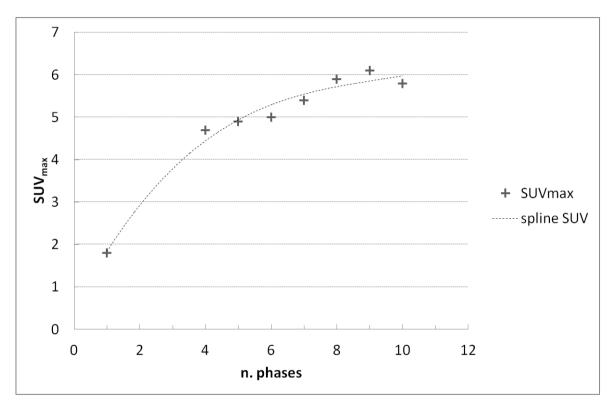
# example of <sup>18</sup>F-MISO PET-CT – accumulation in hypoxic areas (NSCLC – animal model)

T Huang et al., "18F-misonidazole PET imaging of hypoxia in micrometastases and macroscopic xenografts of human non-small cell lung cancer: a correlation with autoradiography and histological findings", Am J Nucl Med Mol Imaging 2013;3(2): 142-153

# example of <sup>18</sup>F-FLT PET-CT – evidence of cell proliferation areas

W Yang et al., "Imaging proliferation of <sup>18</sup>F-FLT PET/CT correlated with the expression of microvessel density of tumour tissue in non-small-cell lung cancer", Am J Nucl Med Mol Imaging 2013;3(2):142-153

### THE EFFECT OF MOTION ON SUV VALUES

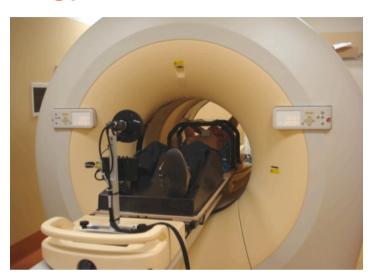




- excursion 19 mm
- $SUV_{max}$ =1.8 non-gated
- SUV<sub>max</sub> =6.1 @9ph
- SUV<sub>max</sub> in expiration as a function of the number of phase-bins

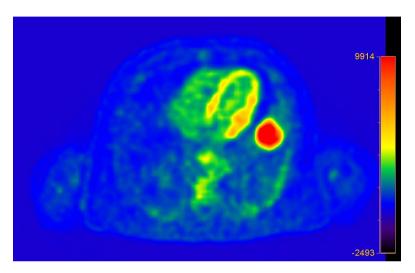
# **4D-PET-CT – INSTRUMENTS (gating)**

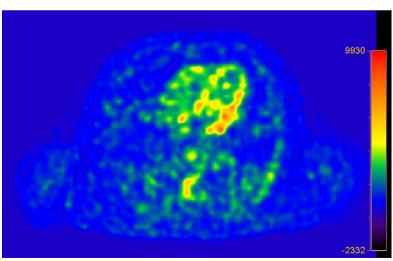
- -gating 4D PET-CT
- -surrogate signal:
- optical
- "strain-gauge" belt
- "tidal volume" measurement
- thermometry
- ...
- -phase-based gating
- -prospective or retrospective CT
- -loss of SNR compared to uncontrolled acquisition



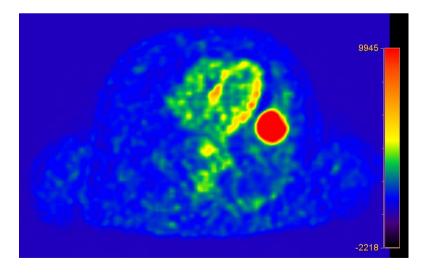


# **4D-PET-CT – INSTRUMENTS (gating)**





- above: free-breathing uncontrolled acquisition
- lower left: "gated" acquisition max inspiration
- lower right: "gated" acquisition max expiration



# **4D-PET-CT – INSTRUMENTS (virtual 4D-CT)**

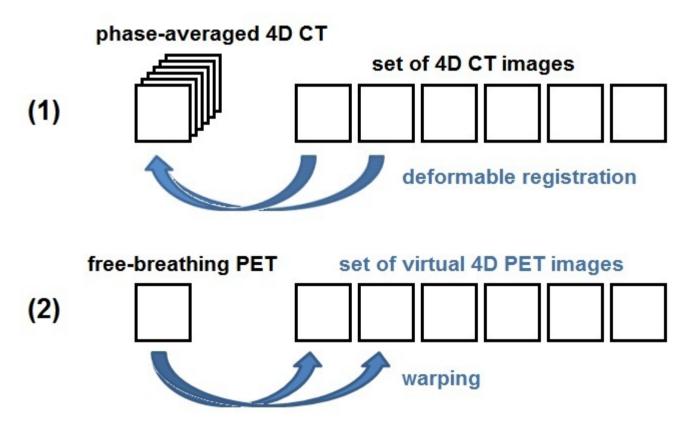
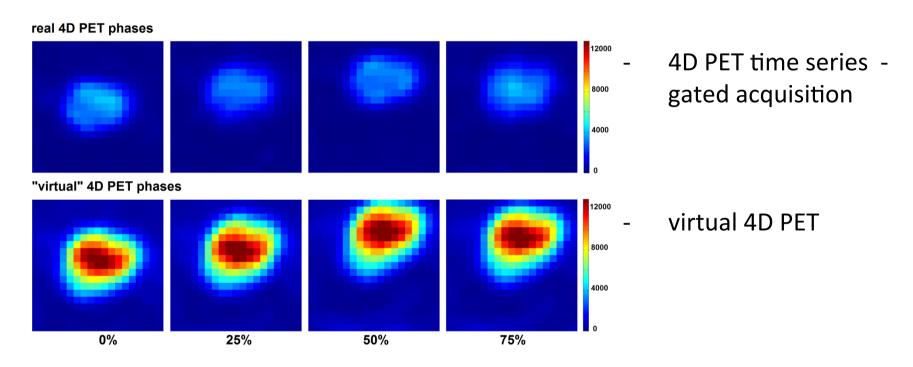


Figure 1. Scheme of the proposed "virtual 4D PET strategy": computation of 4D CT motion model (1); PET warping according to the 4D CT motion model (2)

C Gianoli, G Fontana, M Riboldi, C Cavedon, G Baroni, "Enhanced 4D PET optimization based on 4D CT motion modeling", ESTRO Anniversary Meeting, London, May 2011

# **4D-PET-CT – INSTRUMENTS (virtual 4D-CT)**

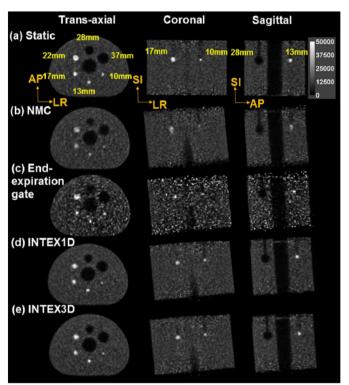


#### - open issues:

- how to recover loss of signal due to motion blurring (models?)
- difficult management and control of the deformable registration technique (e.g. at lung-chest wall interface)

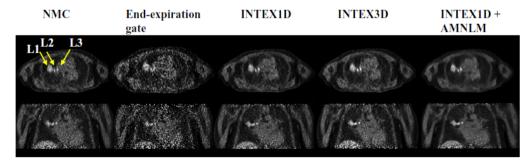
C Gianoli, G Fontana, M Riboldi, C Cavedon, G Baroni, "Enhanced 4D PET optimization based on 4D CT motion modeling", ESTRO Anniversary Meeting, London, May 2011

# **4D-PET-CT – INSTRUMENTS (motion compensation)**



3D event-by-event motion compensation

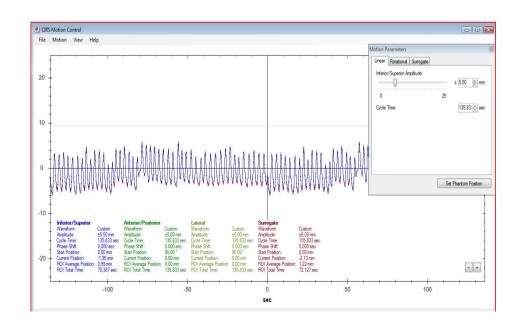
- 8-phase gating (=> poor SNR)
- segmentation –calculation of organ COMs
- acquisition of surrogate signal at 40 Hz
- => motion model of COMs
- => used to compensate for motion in listmode reconstruction
- below: first example of event-by-event reconstruction applied to <sup>18</sup>F-MISO map of hypoxia



C Chan, X Jin, EK Fung, M Naganawa, T Mulnix, RE Carson, C Liu, "Event-by-event respiratory motion correction for PET with 3D internal-1D external motion correlation", Med. Phys. 40, 112507 1-13 (2013)

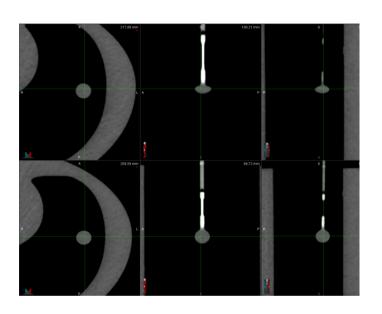
### **EXPERIMENTAL VALIDATION – VERIFICATION**

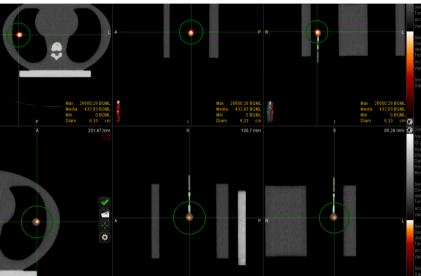
- use of programmable **motion phantoms** (recommended AAPM TG76)
- capable of simulating **realistic motion patterns** (ideally, real-patient motion)
- capable of reproducing both tumor motion and surrogate motion





### **EXPERIMENTAL VALIDATION – VERIFICATION**



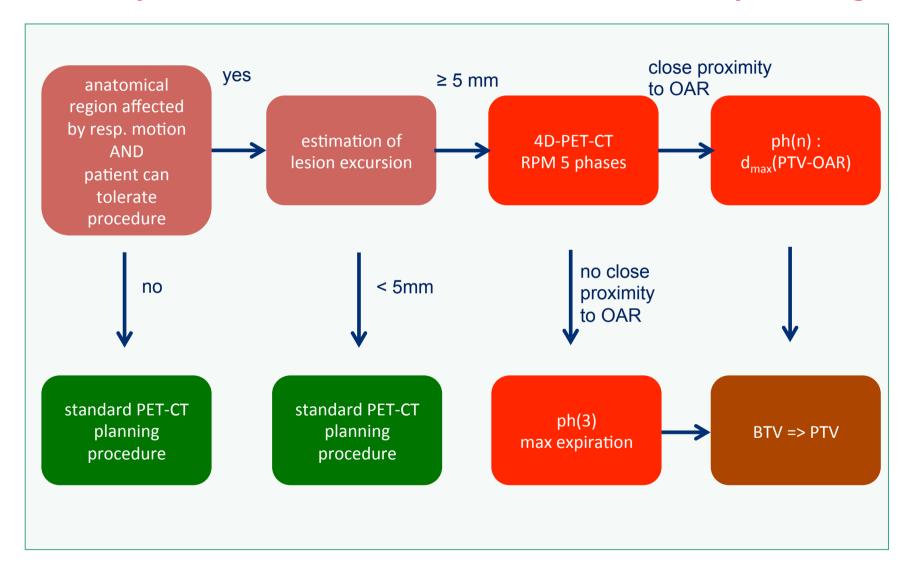


- available for 4D-CT
- inserts and accessories for **PET-CT** easily found (or custom-made)
- **3D motion** difficult to reproduce in full detail
- MR-compatible instruments not easily found

#### **EXPERIMENTAL VALIDATION – VERIFICATION**

- analisys and tests on **system logfiles**
- consistency checks (e.g. volume preservation of solid tumors in different respiratory phases)
- expert judgment definitely required

# **Example of decision-tree - 4D-PET-CT for RT planning**



#### TAKE HOME MESSAGES

- **1.tumor/organ motion** shall always be considered and accounted for, but an explicit management is not always necessary
- **2.explicit methods** of motion management might prolong treatment time and/or introduce significant uncertainties (e.g. of dose to OARs)
- **3.temporal coherence** is necessary between imaging used for planning and treatment administration technique
- **4.validation experimental verification** is necessary when implementing a motion-management program (including easily-performed consistency tests)
- **5.balance** between accuracy and **clinical applicability** must be considered