

STEREOTACTIC RADIOSURGERY

CONCEPTS AND IMPLEMENTATION

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OUTLINE

Stereotactic Radiosurgery Concepts – targets and dose distributions

Some History

Commissioning and Quality Control

Image Fusion and Target delineation

Dose delivery methods

SRS treatment process

Stereotactic Radiosurgery

"A single high dose of radiation, stereotactically directed to an intracranial region of interest. May be from X-ray, gamma ray, protons or heavy particles." (Lars Leksell, 1951)

Historical Development of Stereotactic Ablative Radiotherapy Timothy D. Solberg, Robert L. Siddon, and Brian Kavanagh

http://www.springer.com/cda/content/document/cda_downloaddocument/ 9783642256042-c2.pdf?SGWID=0-0-45-1346463-p174268967

Stereotactic Radiosurgery (SRS) – Stereotactic Radiotherapy (SRT)

SRS and SRT use a stereotactic system and high energy beams to irradiate a volume.

- (1) Requires an image based volume defined and indexed to a stereotactic coordinate system.
- (2) Planning and treatment delivery indexed to the same coordinate system.



SRS and SRT produce a sharp dose gradient outside the treatment volume.

Stereotactic Localization

A localizer head frame, rigidly attached to the cranium, defines a precise and rigid frame of reference.

All points within that space can be referenced to a unique coordinate system.

All structures and points can be identified in all the imaging studies that include the localization frame, which is uniquely and rigidly attached to the base frame.





Localization of points



The "z" coordinate



SRS treatment strategy

Position the point or volume to be treated at the point of convergence or intersection of all the beams

History



Clarke RH, Horsley VA, On a method of investigating the deep ganglia and tracts of the central nervous system (cerebellum). Br Med J 1799-1800, 1906.

Clinke's sterestactic appendua for directing an insulated nordle by gealuated movement in three planes (locar, Hersieg V, Clinke RE: Thestructure and functions of the controllars examined by a nets method. Brain 31:45–124, 1909).

Horsley VA, Clarke RH, The structure and functions of the cerebellum examined by a new method. Brain 31:45-124, 1908.

History

- Dr. Lars Leksell (1951) introduced the concept of Radiosurgery as the ablation of a lesion by radiation in a single procedure, similar to surgery
- Initially used a 200kV x-ray tube
- In 1968 developed the "Gamma knife"
 - 179 Co-60 sources
 - A spherical cavity covering 60° x 160°





Gamma Knife

201 Co-60 sources arranged hemispherically around a common 'focal' point

The isocenter precision <0.5mm

A system of collimators (4, 8, 14 and 18mm) (diameter of 50% isodose level on a 16cm phantom)

Used for spherical targets in one isocenter





Initial application for treatment of artero-venous malformations (AVM)





Radiographic localization requires a reference frame

Images are registered, not fused. There is no such thing as "frameless" 2D angio localization, and you cannot "fuse" 2D angios.







Incomplete information



Laser-Angiographic Target Localizer (LATL)

Used for Angiography to register the nidus to a CT data set





Gamma knife



5 Shots

Irregular target volumes
require multiple 'shots'

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X-Knife

- Collimator sizes: 5 to 45 mm in 2.5 mm steps
- Conformal SRT: with jaws/circles; mMLC; IMRT.
- Extra-cranial: head and neck; body localization, spine localization, other targets

Gamma Knife

- Collimator sizes: 4,8,14,18 mm
- Conformal is only attained through multiple isocenters
- No extra-cranial targets possible

Radiosurgery AVM

Pre-Radiosurgery

Post-Radiosurgery



History

Linac Radiosurgery - 1984



First linac- based SRS system. Betti et al., Buenos Aires, Argentina

Ref: Historical Development of Stereotactic Ablative Radiotherapy, by Timothy D. Solberg, Robert L. Siddon, and Brian Kavanagh. In S. S. Lo et al. (eds.), Stereotactic Body Radiation Therapy, Medical Radiology. Radiation Oncology,

DOI: 10.1007/174_2012_540, Springer-Verlag Berlin Heidelberg 2012

Radiation delivery techniques

Arcs with circular collimators

Conformal beams

Arcs with Conformal Dynamic beams

IMRT

Linac SRS with

cones

- One or more isocenters
- Multiple arcs per isocenter
 - Arcs of 100° to 160°
 - Fixed couch angle for each arc
 - Spherical dose distributions for each irradiación



LINEAR ACCELERATOR NONCOPLANA CONVERGING ARCS Arcs 260° Arc Arcs with circular cross sections are obtained by rotating the source (linac gantry) in various planes in the patient, corresponding to various couch angles.





Tertiary Collimation Cone



Collimation



Linac SRS on Linac + cones

- 5-40mm diameter cone set
- Circular beam projection
- Collimator mounted assembly







Verification of gantry isocenter with cones

Laser alignment







Stereotactic Set-up QA

Winston Lutz Quality Assurance

- Phantom Pointer verifies laser accuracy prior to SRS
- Embossed laser lines for easy alignment with wall lasers
- Integrated tungsten sphere for film verification
- Irradiation of film at different gantry angles
- Shadow in field center verifies accuracy





Precisión mecánica

Ball Centroid: Row = 62.22, Column = 59.38 Cone Centroid: Row = 60.87, Column = 60.66 Distance = 1.86 pixels, 0.35 mm



Delta Y = 1.25 pixels, -0.24 mm Delta Y = 1.35 pixels, 0.25 mm Ball Centroid: Row = 60.20, Column = 64.43 Cone Centroid: Row = 60.58, Column = 61.11 Distance = 3.34 pixels, 0.62 mm



Delta X = 3.32 pixels, 0.62 mm Delta Y = -0.38 pixels, -0.07 mm Ball Centroid: Row = 60.64, Column = 59.42 Cone Centroid: Row = 60.63, Column = 60.49 Distance = 1.07 pixels, 0.20 mm Ball Centroid: Row = 61.96, Column = 61.32 Cone Centroid: Row = 61.07, Column = 61.16 Distance = 0.90 pixels, 0.17 mm



5 10 15 20 Delta X = 0.16 pixels, 0.03 mm Delta Y = 0.88 pixels, 0.16 mm Ball Centroid: Row = 59.57, Column = 63.07 Cone Centroid: Row = 61.04, Column = 61.16 Distance = 2.42 pixels, 0.45 mm



Delta X = 1.91 pixels, 0.36 mm Delta Y = -1.48 pixels, -0.27 mm

Gantry	210°	270°	0°	90°	150°
∆GT (mm)	0.25	0.03	0.62	0.36	0.20
∆AB (mm)	0.24	0.15	0.07	0.27	0.0
Vector (mm)	0.35	0.15	0.62	0.45	0.20

AAPM TG42: Tolerance = 1mm
















Planning strategies for SRS with arcs

- Spherical targets:
 - Use up to 9 arcs with collimator diameter corresponding to the target diameter
- Elliptical targets:
 - If the major axis is in the coronal plane, eliminate perpendicular arcs, or use different cone sizes





Circular collimators







Considerations according to the type of target



< **3-4** cm

- Circular Cones + Arcs Best
- Sharp Penumbra avoids OAR
- Precise Geometry
- Low Integral Dose to Brain
- **3-6 cm**
 - (a) XJaws = Jaws and Cones and Arcs
 - Simple
 - Low Integral Dose to Brain
 - Optimal Conformal Index
 - (b) MMLC Okay
 - Exact Conformation not an issue.



Conformal Arc BEV



Standard Arc Conformal Arc



Considerations according to the type of target



< 3-4 cm

- Circular Cones + Arcs Best
- Sharp Penumbra avoids OAR
- Precise Geometry
- Low Integral Dose to Brain
- 3-6 cm
 - (a) XJaws = Jaws and Cones and Arcs
 - Simple
 - Low Integral Dose to Brain
 - Optimal Conformal Index
 - (b) MMLC Okay
 - Conformation not the issue.
- **> 6 cm**
 - Penumbra Increases, not very effective to use Cones and Arcs
 - Better N ≥ 6 Non-Coplanar Static Fields
 - Need XPlan, OAR, Beam Model
- MMLC necessary.
- 2 π Access Reduces IMRT Need.











Micro MLC (mMLC)

- Add-on system attached to the regular collimator
- MODULEAF, Siemens
 - 80 leaf
 - 40Kg (require special mount to move around)
 - Leaf width at isocenter 2.5 mm
 - Positioning precision 0.5 mm
 - Penumbra 2.5 3.5mm
 - Transmission < 2.5%</p>
 - Maximum field size 12 x 10 cm²



Isocenter precision Winston - Lutz test





Ball Centroid: Row = 54.88, Column = 51.06 Cone Centroid: Row = 51.62, Column = 51.73 Distance = 3.33 pixels, 0.66 mm

5 10 15 Delta X = -0.68 pixels, -0.13 mm Delta Y = 3.26 pixels, 0.64 mm Ball Centroid: Row = 52.32, Column = 53.69 Cone Centroid: Row = 51.76, Column = 51.63 Distance = 2.04 pixels, 0.40 mm



Delta X = 1.96 pixels, 0.39 mm Delta Y = 0.55 pixels, 0.11 mm Ball Centroid: Row = 53.13, Column = 51.08 Cone Centroid: Row = 51.25, Column = 51.52 Distance = 1.93 pixels, 0.38 mm



5 10 15 Delta X = -0.44 pixels, -0.09 mm Delta Y = 1.88 pixels, 0.37 mm Ball Centroid: Row = 53.74, Column = 50.48 Cone Centroid: Row = 51.78, Column = 51.31 Distance = 2.14 pixels. 0.42 mm



Delta X = -0.83 pixels, -0.17 mm Delta Y = 1.97 pixels, 0.39 mm















Procedure







Relocatable Head Frame (Gill-Thomas-Cosman) for fractionated SRT



SRS with GTC relocatable head frame



Daily reproducibility of the head frame position

<u>DEPTH CONFIRMATION HELMET</u>: Mounts on stereotactic base ring; allows for 25 'helmet to scalp' measurements which are repeated following frame attachment, removal, replacement, and for SRT prior to each treatment (accuracy +/-1.5 mm)





Patient Immobilization (SRT)

3 piece Mask System Extends treatment area to T1 Set-up errors from 1.7 to 0.9 mm Indexed bite plates Carbon fiber Tilt compensation for set-up Suitable for elderly patients & children













Patient positioning accuracy in a thermoplastic mask with upper jaw support. J. Ahlswede et al. AAPM Annual Meeting 2001 Poster Display

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Frameless Immobilization



MRI



Patient setup



CT angiography







CT angiography





Angiography Localizer frames for Stereotactic Imaging





Transfer of Coordinates TPS plan -> Treatment unit







Optical tracking of Stereotactic position space

The CT images of the spheres are used to transfer the coordinate space to the treatment room



Image fusion or Registration





CT – MR – SPECT - PET







Stereo Images



Image fusion

Volume definitions





Uncertainties achievable in SRS

CT slice Thickness	1 mm	3 mm
Stereotactic Frame	1 mm	1 mm
Isocenter Alignment	1 mm	1 mm
CT Image resolution	1.7 mm	3.2 mm
Tissue Motion	1.0 mm	1 mm
Angio (Point identification)	0.3 mm	0.3 mm
Std. Dev. of Pos. Uncertainty	2.4 mm	3.7 mm

AAPM Report No 54:Stereotatic Radiosurgery



PLANING WITH CONFORMAL ARCS





PLANING WITH CONFORMAL FIXED FIELDS







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PLANING with Intensity Modulated Radio Surgery (IMRS)













Single isocenter for irregular targets with better conformality and homogeneity than cones



Dynamic Conformal Arc

- Automatic leaf adaptation to tumor contour
- Straight-forward arc optimization with collision map
- MLC control must be synchronized with gantry rotation

Advantages

- Fast, semi-automatic single isocenter treatment planning
- Critical structures are easier to avoid for most beam angles
- Most conformal and homogeneous dose distribution with reduced irradiation of normal tissue



<DPF, NSUH-LIJ :
Comparison of plans

Conformal mMLC Plan 1 Isocenter -6 Static Fields

Dynamic Conformal Arc Plan 1 Isocenter - 3 Dynamic Arcs

Volume of irradiated Normal Tissue (cm³)







Courtesy of Universitätsklinkum Charité, Berlin

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Circular Arc,

8 Isocenters

Conformal Beam, **19 Beams (1 isocenter)**

4.0 Gv

Dynamic Conformal Arc, 5 Arcs (1 isocenter)

Improved normal tissue sparing **Tight margin around target**

Dynamic Arc Radiosurgery Field Shaping: A Comparison with Static Field Conformal and non-coplanar circular arcs. T. Solberg et al. Int. J. Radiation Oncology Biol Physics. Vol 49, No. 5, pp1481–1491, 2001

Comparison Acoustic Neuroma

Homogenous Dose Distribution Greater sparing of normal tissue and structures at risk



Dynamic Arc Radiosurgery Field Shaping: A Comparison with Static Field Conformal and non-coplanar circular arcs. T. Solberg *et al.* Int. J. Radiation Oncology Biol Physics. Vol 49, No. 5, pp1481–1491, 2001

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QA of Isocenter



Coordinate verification

- Templates and Laser -





Beam dosimetry of small fields and treatment planning commisioning

Beam parameters

- PDD
- Profiles
- Field size dependent output factors
- Transmission
- <u>Absolute dose</u>





Beam Dose Measurements

- Issues with small field dosimetry:
 - Detector size vs. Small field dimensions
 - Lack of lateral charged particle equilibrium
 - Large dose gradients in SRS penumbra
- Equipment:
 - Water tank, polystyrene slabs, ion chamber, diodes, TLD's and Film
 - Very small Detector diameter required to reproduce a penumbra of ~1mm



Beam Profiles

<u>Welhofer</u> Laser Film Digitizer (Lumisys) Film Digitizer

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Gamma Knife - Beam profiles



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Stereotatic Output Factor Curve $(S_t = S_c S_p)$

@ Isocenter, d_{max}

6 MV

Coll. Diam.:12.5mm to 20.0mm



Verification of dose calculations



Verification of dose calculations

- IMRS Patient specific dose measurements
 - Absolute total plan dose
 - Relative doses per field
 - Relative plan dose distribution

Verificación DOS IS IBIET PRIMUS Incisaus i PLABILIA 002 Pagina 144 2 Verificación DOS IS IBIET PRIMUS Incisaus i PLABILIA 002 Primus Incisaus i
Control de Calidad específico Paciente IMRT Paciente: D0 (KonRAD): Utilizza D0 (KonRAD):
Image: States
B Image: Name OA RIT 10 Image: Name Image: Name Image: Name Last Status Last Status Image: Name Image: Name Image: Name Last Status Last Status Image: Name Image: Nam Image: Nam Image: Name



Dose Evaluation Tools

•Volume Dose
•Surface Dose
•Dose Summary
•Slice Dose
•Dose Volume Histograms



Plan quality indices

Conformity (CI):	Ratio of the prescription isodose volume V(p)to the target Volume V(T)
Homogeneity (HI)	Ratio of maximum dose D(max) to Prescription Dose D(p)
Dose gradient :	Ratio of V(T) to Volume of the 50% isodose (V _{50%})

	Conformity	Homogeneity	Gradient
Reference value	1 – 2	<u>HI <</u> 2	<u>></u> 0.3
Minor deviation (acceptable)	0.9< CI < 1 o 2 < CI < 2.5	2 < HI <u>< </u> 2.5	
Major deviation (unacceptable)	CI < 0.9 0 CI <u>></u> 2.5	HI > 2.5	

Total system verification – external audit





Plan according to "RTOG Quality Assurance Guidelines"

Phantom

- Target F = 19mm
- Gafchromic film in two orthogonal planes
- 2 TLD-100at the target center
- http://rpc.mdanderson.org



Report



Preliminary studies suggest that the precision of the TLD is $\pm 3\%$, and the localization precision from the film is ± 1 mm.

Summary of results:

	Ratio	Criteria (a)
Dose to the center of the target (RPC/Institution)	0.98	0.95 - 1.05
Treated Volume (b): (Measured/Institution)	0.78	0.75 - 1.25 ^(c)
Ratio of Measured Treated Volume to Target Volume ^(d)	1.17	1.00 - 2.00
Minimum Dose to Target (Minimum Dose/Prescription Dose) ^(e)	0.91	> 0.90

(a) Criteria are adapted from the RTOG QA guidelines. Int. J. Onc. Biol. Phys. 27, 1231-39, 1993.

(b) The treated volume is assumed to be an ellipsoid with diameters taken from the "Film Results" table.

(c) Average discrepancy of approximately 2 mm on each diameter.

(d) The target is the 1.9 cm. sphere.

(e) Minimum dose is taken from the 3 dose profiles.

TLD and Film Analysis by: Paola Alvarez, MS

TLD Results:

Dose to TLD Capsules (Gy)		Average Dose (Gy)	Institution Dose	Ratio	
Upper	Lower	(Dose to Center)	(Gy)	Measured/Institution	
30.5	29.4	30.0	30.5	0.982	

Film Results:

	Fi	Offset (80% Line)		
Measured Along	Measured (cm)	Measured - Institution	(cm)	
Right/Left Profile (x)	2.1	2.2	-0.1	0.0
Anterior/Posterior Profile (y)	2.0	2.1	-0.2	0.0
Superior/Inferior Profile (z)	1.9	2.2	-0.3	-0.1

Treated Volume (cm³)** 4.19 5.40

* Offset is the distance between the center of the specified isodose line and the center of the physical target.

** Treated Volume= (π•x•y•z)/6





Superior Inferior Profile - Coronal Plane



Table 1. List of radiosurgery events reported to the NRC during the period 2005-2010

Event Description	Treatment Implication
Patient orientation entered incorrectly at MR Scanner	Wrong location treated
Fiducial box not seated properly during CT imaging	Wrong location treated
Malfunction of automatic positioning mechanism following re-initialization	Wrong location treated
Right trigeminal nerve targeted instead of left	Wrong location treated
Facial nerve targeted instead of trigeminal nerve	Wrong location treated
Mistake in setting isocenter coordinates	Wrong location treated
Head not secured to stereotactic device (2 events)	Wrong location treated
Selected collimators did not match planned	Wrong dose/distribution delivered
Physician mistakenly typed 28 Gy instead of 18 Gy into planning system	Wrong dose delivered
Physicist calculated prescription to 50% isodose instead of 40%	Wrong dose delivered
Microphone dislodged, causing stereotactic device to break	Treatment halted after 2 of 5 fractions
Couch moved during treatment	None; personnel interrupted treatment

from: Quality and safety in stereotactic radiosurgery and stereotactic body radiation therapy: can more be done? Timothy D. Solberg, and Paul M. Medin Jour. of Radiosurgery and SBRT, Vol. 1, pp. 13-19

LESSONS FROM RECENT ACCIDENTS IN RADIATION THERAPY IN FRANCE

S. Derreumaux*, C. Etard, C. Huet, F. Trompier, I. Clairand, J.-F. Bottollier-Depois, B. Aubert and P. Gourmelon Institut de Radioprotection et de Súreté Nucléaire, Direction de la Radioprotection de l'Homme, IRSN, BP 17, F-92262 Fontenav-aux-Roses Cedex, France Radiation Protection Dosimetry (2008), Vol. 131, No. 1, pp. 130–135



Figure 2. Stereotactic radiotherapy treatment delivery with successive beam entrance positions as a function of accelerator and table rotation angles (left). The plate used in the centre (Case 2) to hold the cylindrical additional collimator (right). Single fraction SRS for AVM, November, 2004

Prescription dose not reported; plan/treatment used multiple isocenters, with collimators from 10 -30 mm

Jaws set to 40 x 40 cm² instead of 40 x 40 mm². Physicist told therapist "40 x 40"

Some areas of normal brain received in more than dose to intended target

Severe complications: "fibrosis and oseotracheal fistula that required surgical operation." Patient died several days later as a result of a "brutal haemorrhage."

A written checklist system, and/or a proper R/V system can minimize events like this

AAPM Report 54 (1995) Task Group #42 - <u>Stereotactic Radiosurgery</u>

XI. APPENDIX I

PROBABLE RISK ANALYSIS FLOWCHART: EXAMPLE 1



RADIOSURGERY PROCEDURE CHECK LIST

Patient Name: Date:					
+					
ISOCENTER NAME :					
EXTERNAL TARGET	AP	LAT	VERT	SIGN	IATU E
Phantom Base Measurements			+ 2.4 =		
Plan-32 Calculation					
External test target acceptable:					
TRUE TARGET (ISO)	AP	LAT	VERT		
Eleor. Stand (target) coord.					
Floor Stand Redent Check					
Collimator size					
Collimator Inserted					
Jaw 5 x 5, Collimator: 270°					
Target Simulator	AP	LAT	VERT		
Coordinates			+15.4 =		
Target Simulator Film Acceptabble.	Exposure	Gantry	Couch		
	1	130°	180 °		
	2	65°	180°		
	3	295°	180 °		
	4	230°	180°		
	5	130°	270 °		
	6	67°	270 °		
	7	230°	90 °		
	8	297°	90 °		
Anti-collision switches in place					
Couch Disabled					

LONG ISLAND JEWISH MEDICAL CENTER DEPARTMENT OF RADIATION ONCOLOGY RADIOSURGERY PROCEDURE CHECK LIST

Patient Name:		ID: Date:					
ISOCENTER NA	ME:						
EXTERNAL TARGE	т	AP(Y)	LAT(X)		VERT(Z)	SIGNATURES	
Phantom Base Mean	urements				+2.4 =		
Radionics Calculation	1 (mm)						
Treatment Planning S	System(mm)						
External test targe	t acceptable:	Yes No		D			
TRUE TARGET (IS	0)	AP(Y)	LAT(X)		VERT (Z)		
Restiliniar Phantom	Pointer(RLPP)						
RLPP(target) Coord	instes (mm)						
RLPP read out check	: (mm)						
Collimator (cone)	size planed			m	m (diameter)		
Collimator Inserte	d	mm (diameter)					
Jaw 5 x 5,Collimat	or: 0°	Yes No					
Laser Target Localiz	Laser Target Localizer Frame (LTLF)		LAT(X) VERT(Z)				
LTLF Coordinates (mm)						
Target Simulator I	Film Acceptable	Exposure	Gantry	Couch			
		1	0.		90*		
Yes	No	2	270*		0.		
		3	90*		0.		
		4	0.		270*		
Couch Morion Disab	led	Yes No					
Dep th	Point	Helmet	Port	I	epth (mm)		
Confirmation	1						
Helmet Check	2						
	3						
	4						
	5						
	6						

